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Reduced voltage-activated Ca²⁺ release flux in muscle fibers from a rat model of Duchenne dystrophy

Running title: Impaired Ca²⁺ release in dystrophic muscle

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Summary

Defective Ca^{2+} signaling in muscle cells is thought to play a role in Duchenne muscular dystrophy. Schreiber et al report that voltage-activated SR Ca^{2+} release is moderately depressed in muscle fibers isolated from a rat model that well reproduces the human disease.

Abstract

The potential pathogenic role of disturbed Ca^{2+} homeostasis in Duchenne muscular dystrophy (DMD) remains a complex, unsettled issue. We used muscle fibers isolated from 3-month-old DMD^{mdx} rats to further investigate the case. Most DMD^{mdx} fibers exhibited no sign of trophic or morphology distinction as compared to WT fibers and mitochondria and t-tubule membrane networks also showed no stringent discrepancy. Under voltage-clamp, values for holding current were similar in the two groups whereas values for capacitance were larger in DMD^{mdx} fibers, suggestive of enhanced amount of t-tubule membrane. The Ca²⁺ current density across the channel carried by the EC coupling voltage sensor (Cav1.1) was unchanged. The maximum rate of voltage-activated sarcoplasmic reticulum (SR) Ca²⁺ release was reduced by 25 % in the DMD^{mdx} fibers, with no change in voltage-dependency. Imaging resting Ca²⁺ revealed rare spontaneous local SR Ca²⁺ release events with no sign of elevated activity in *DMD^{mdx}* fibers. Under current-clamp, *DMD^{mdx}* fibers generated similar trains of action potentials as WT fibers. Results suggest that reduced peak amplitude of SR Ca²⁺ release is an inherent feature of this DMD model, likely contributing to muscle weakness. This occurs despite a preserved amount of releasable Ca^{2+} and with no change in excitability. Cav1.1 channel activity and SR Ca²⁺ release at rest. Although we cannot exclude that fibers from the 3-month-old animals do not yet display a fully developed disease phenotype, results

provide limited support for pathomechanistic concepts frequently associated with DMD such as membrane fragility, excessive Ca^{2+} entry or enhanced SR Ca^{2+} leak.

Key words

skeletal muscle, excitation-contraction coupling, ryanodine receptor, sarcoplasmic reticulum Ca^{2+} release.

Introduction

A number of mechanisms involved in the control of Ca^{2+} homeostasis and excitationcontraction (EC) coupling have been reported altered in dystrophin-deficient muscle cells. This is now to the point that emphasizing abnormal or defective Ca²⁺ homeostasis in the associated DMD disease situation has become a common place, with cytosolic Ca^{2+} overload being one frequently assumed pathogenic driver of multiple detrimental effects. Specifically, altered Ca²⁺ fluxes at the plasma/t-tubule membrane level have been reported carried by membrane tearing (Mokri et al., 1975; Pestronk et al., 1982; Petrof et al., 1993; Pasternak et al., 1995), -TRPC or other types of sarcolemmal Ca^{2+} leak channels (Fong et al., 1990; Franco and Lansman, 1990; Mallouk and Allard, 2002; Vandebrouck et al., 2002; Ducret et al., 2006; Gervasio et al., 2008; Krüger et al., 2008; Teichmann et al., 2008; Millay et al., 2009; Matsumura et al., 2011; Lin et al., 2022), - the store-operated Ca²⁺ entry complex (Boittin et al., 2006; Edwards et al., 2010; Cully et al., 2012; Zhao et al., 2012; García-Castañeda et al., 2022), -connexin hemichannels (Cea et al., 2016; Nouet et al., 2020), -P2X purinoreceptors (Jiang et al., 2005; Yeung et al., 2006); in intracellular compartments by sarcoplasmic reticulum (SR) ryanodine receptors (Woods et al., 2004; Hollingworth et al., 2008; Bellinger et al., 2009; Cully and Launikonis, 2016; Cully and Rodney, 2020), inositol 1,4,5-trisphosphate receptors (Balghi et al., 2006a b; Mondin et al., 2009; Cárdenas et al., 2010) and the SERCA pump (Divet et al., 2002; Morine et al., 2010; Schneider et al., 2013; Kargacin and Kargacin, 2016); and there are also reported changes in the expression level of Ca²⁺-binding proteins (Niebroj-Dobosz et al., 1989a b; Doran et al., 2004; Lohan and Ohlendieck, 2004; Pertille et al., 2010). Still, in most cases there remains considerable uncertainty as to up to what extent these changes affect physiological Ca²⁺ cycling in intact muscle fibers, and whether or not they play a significant role in either muscle fiber weakness or muscle fiber necrosis. Detection of membrane current and cytosolic Ca^{2+} under voltage

control in intact isolated muscle fibers offers exclusive integrative insights into plasma membrane integrity, ion channel activity, and intracellular Ca^{2+} regulation with specific relevance to EC coupling function. We have used this approach, complemented by confocal imaging of associated relevant parameters, in muscle fibers isolated from DMD^{mdx} rats (Larcher et al., 2014). Rationale is that most previous studies relied on the C57BL/10ScSn mdx (from here on referred to as mdx) mouse model of DMD, which is commonly admitted to exhibit a mild, non-progressive disease phenotype (see for review Willmann et al., 2009; Greevy et al., 2015; Wilson et al., 2017). In comparison, the DMD^{mdx} rat exhibits a progressively aggravating status characterized, between 3 and 7 months of age, by a loss of body weight and of muscle mass, and myo-necrosis/-degeneration (Larcher et al., 2014). DMD^{mdx} rat muscles also present with fibrosis that expands with time, resulting in marked endomysial and perimysial infiltration of connective tissue in 7-month-old animals (Larcher et al., 2014). In contrast, fibrosis remains minimal in muscles other than the diaphragm in the *mdx* mouse (Tanabe et al., 1986; Stedman et al., 1991). *DMD^{mdx}* rats suffer from defects in cardiac structure and function in 3-month-old animals, which become more severe with time (Larcher et al., 2014) with the extent of cardiac fibrous area being doubled between 3 and 7 months of age. In *mdx* mice, although MRI is able to identify early cardiac abnormalities, cardiac defects are usually reported less pronounced and/or to develop over a more delayed time frame (Quinlan et al., 2004; Van Erp et al., 2010; Stuckey et al., 2012). At last, the *mdx* mouse exhibits a slightly reduced lifespan relative to WT mice (Pastoret and Sebille, 1995; Chamberlain et al., 2007), whereas median survival of the DMD^{mdx} rat is ~1 year (personal communication, Huchet C.). Of importance, the severity of the DMD disease in the rat has been confirmed in the other DMD rat models developed by Nakamura et al. (2014) and Taglietti et al. (2022) which also showed progressive and severe skeletal muscle loss associated with fibrotic deposition and fat infiltration leading to severe muscle, respiratory

and cardiac dysfunction, resulting in premature death (at ~1 year of age, Taglietti et al., 2022). Altogether, there are thus clear indications that the DMD^{mdx} rat reproduces classical features of Duchenne dystrophy patients better than the mdx mouse. We speculated that it could help enlighten the DMD Ca²⁺ issue.

Materials and methods

This work was achieved following the ethics principles of the French Department of Veterinary Services and the French Ministry for Higher Education, Research and Innovation, in accordance with the guidelines of the local committee in charge of animal well-being (SBEA) at University of Nantes, the French Ministry of Agriculture (decree 87/848), and the revised European Directive 2010/63/EU. Animals were housed at the accredited Therassay (University of Nantes) animal facility. Investigations were approved by the Ethics Committee on Animal Experimentation of the Pays de la Loire Region, in accordance with the guidelines from the French National Research Council for the Care and Use of Laboratory Animals (APAFIS#10792–2017061316021120).

Isolation and preparation of muscle fibers for electrophysiology

Experiments were performed on muscle fibers isolated from the *flexor digitorum brevis* (FDB) muscles of 3-month-old WT and *DMD^{mdx}* littermate male rats (Larcher et al., 2014). Rats were sacrificed by intravenous administration of sodium pentobarbital (300 mg, Dolethal, Vetoquinol UK Ltd, Buckingham, UK). All procedures for fiber isolation and preparation for silicone-clamp electrophysiology were identical to those described in our previous works (e.g. Sanchez et al., 2021; Jaque-Fernandez et al., 2023). In brief, FDB muscles were dissected and stored at 4°C in Tyrode solution during 6 hours, the time needed for dedicated express transport from Nantes to Lyon. Muscles were then incubated for 60 min at 37 °C in Tyrode solution containing 2 mg/ml collagenase (Sigma type 1). Single isolated fibers were obtained by gently mechanical trituration of the muscles within the experimental chamber (50-mm wide culture μ -dish, Ibidi). For this, the μ -dish had its floor covered with a thin layer of silicone grease and was then filled with culture medium containing 10% bovine fetal serum (MI199; Eurobio). Following mechanical trituration of an FDB muscle, single isolated fibers were partially covered with silicone so that an end-portion of fiber ~100-200 um long remained silicone-free, in contact with the extracellular medium. For voltage-clamp experiments, the culture medium was then replaced by our standard TEA-containing extracellular solution. The tip of a borosilicate glass micropipette filled with a solution mimicking the composition of the intracellular medium (intracellular-like solution, see Solutions) and also containing the Ca²⁺-sensitive dye rhod-2 and 15 mM EGTA, was inserted in the silicone-embedded portion of fiber. The chloride silver wire in the micropipette was connected to a RK400 amplifier (Bio-Logic, France). A 30-minute period of equilibration was allowed before delivering voltage-clamp pulses from a holding voltage of -80 mV. For actionpotentials measurements, the culture medium was replaced by Tyrode solution and the micropipette was filled with the intracellular-like solution. Following impalement of the silicone-embedded portion of fiber, the current-clamp mode of the amplifier was established and a 5 minutes period of equilibration was allowed before delivering short (typically 0.5 mslong) supra-threshold depolarizing current pulses to trigger action-potentials at frequencies ranging between 1 and 80 Hz, over a 3 s duration. The resting membrane potential was maintained at -80 mV by passing a constant hyperpolarizing current. All experiments were performed at room temperature (20–22°C).

Cav1.1 Ca²⁺ current

Voltage-clamped fibers were depolarized by 0.5 s long-depolarizing test pulses from -50 to +60 mV. The linear component of the current was removed by subtracting the appropriately scaled value of the steady current measured at the end of a 0.5 s-long -20 mV step applied before each test pulse. This did not entirely eliminate the outward current measured during pulses to values between -50 and -30 mV, below the activation threshold of the Ca²⁺ current. For this reason, the voltage-dependence of peak Ca²⁺ current (values normalized to the capacitance), was fitted with the following equation which included a linear slope component: $I(V) = G_{max}(V-V_{rev})/(1+[\exp(V_{0.5}-V)/k]) + slope(V+80),$

with I(V) the peak current density at the command voltage V, G_{max} the maximum conductance, V_{rev} the apparent reversal potential, $V_{0.5}$ the half-activation potential, k the steepness factor, and *slope* the conductance of the residual linear component.

Ca²⁺ imaging and Ca²⁺ release calculation

Procedures were similar to those described previously for mouse muscle fibers (e.g. Kutchukian et al., 2016; Jaque-Fernandez et al., 2020). A Zeiss LSM 800 microscope equipped with a 63× oil immersion objective (numerical aperture 1.4) was used. Measurements of voltage-clamp activated rhod-2 Ca²⁺ transients were achieved with the line-scan (*x*,*t*) mode of the microscope: a 50.7 µm-long line was scanned every 1.02 ms using excitation from the 561 nm diode laser. Rhod-2 fluorescence transients were expressed as F/F_0 , F_0 being the pre-pulse baseline fluorescence. Quantification of the Ca²⁺ release flux (dCa_{Tot}/dt) from the rhod-2 fluorescence transients was achieved according to previously described procedures (e.g. Kutchukian et al., 2016). In brief, the time derivative of the total released Ca²⁺ ([Ca_{Tot}]) was calculated from the occupancy of intracellular calcium binding sites and Ca²⁺ transported back across the SR membrane by the SERCA pump. For this,

changes in $[Ca^{2+}]$ were calculated from the rhod-2 transients using the pseudo-ratio equation described by Cheng et al. (1993), assuming a resting $[Ca^{2+}]$ level of 0.1 µM and an equilibrium dissociation constant of 1.2 µM. From this, the time course of Ca^{2+} bound to troponin C, to parvalbumin and of Ca^{2+} back-transported across the SR membrane by the SERCA pump were calculated using values described by Sanchez et al. (2021) for binding sites concentrations, equilibrium dissociation constants and *on* and *off* rate constants, and with the value for maximum pump rate assumed to be 5 µM.ms⁻¹. This value was adapted from the 3.14-4.49 µM.ms⁻¹ range estimated by Garcia and Schneider (1993) in rat fast-twitch fibers, taking into account the difference in temperature (16°C *vs* 20-22°C in our conditions). For Ca^{2+} binding to EGTA, the total concentration of effective binding sites was assumed to be 7.2 mM, and values for *on* and *off* rate constants and corresponding equilibrium dissociation constant were taken from the Ca^{2+} -removal analysis performed by Schuhmeier and Melzer (2004): 0.02 µM⁻¹.ms⁻¹, 0.00271 ms⁻¹ and 0.1355 µM, respectively. With the large concentration of EGTA used in our experiments, Ca-EGTA makes a predominant contribution to the calculated Ca^{2+} release flux.

The voltage-dependence of the peak Ca²⁺release flux from each muscle fiber was fitted with a Boltzmann function:

 $dCa_{Tot}/dt = Max \ dCa_{Tot}/dt / (1 + \exp[(V_{0.5} - V)/k]),$

with $Max \, dCa_{Tot}/dt$ the maximum Ca²⁺ release flux, $V_{0.5}$ the mid-activation voltage and k the steepness factor.

Imaging of t-tubule and mitochondria networks

This was achieved with the $63 \times$ oil immersion objective of the same above-mentioned Zeiss LSM 800 microscope. For t-tubule staining, single isolated FDB muscle fibers dispersed within an Ibidi μ -dish filled with Tyrode solution were incubated for 60 minutes in the

presence of 10 μ M of Di-8-anepps. For mitochondria staining, separate batches of fibers were incubated under the same conditions in the presence of 10 nM Tetramethyl Rhodamine Methyl Ester (TMRM) for 10 minutes. Di-8-anepps and TMRM fluorescence were imaged using excitation from the 488 nm and 561 diode lasers, respectively. Quantification was achieved with ImageJ (NIH, Bethesda, MD, USA) from frames of 512×512 pixels at 0.2 and 0.1 μ m per pixel for Di-8-anepps and TMRM and Di-8-anepps, respectively.

The t-tubule density was estimated following the approach described by Kutchukian et al. (2017). A largest possible region of interest excluding the plasma membrane was selected. Automatic Otsu's method thresholding was used to create a binary image of the surface area occupied by t-tubules. A t-tubule density index was calculated as the percentage of positive pixels within the region. Analysis was performed within two images taken at distinct locations of each fiber, and the two corresponding index values were averaged. The coefficient of variation for the t-tubule density index was 10.2 % and 7.9 % in the WT and *DMD^{mdx}* groups, respectively. Of note, different from the initial procedure described by Kutchukian et al. (2017), the 'skeletonize' function was not used to delineate the t-tubule network (as also done in Ghasemizadeh et al., 2021). For measurements of the distance between adjacent t-tubules, average fluorescence profiles were generated from a large region of interest (e.g. Kutchukian et al., 2017) in two images taken at distinct locations of each fiber. The average peak-to-peak distance was measured from each profile and the mean from the two images was calculated. Under the conditions used, lateral resolution is ~200 nm. The coefficient of variation for ttubule spacing was 2.9 % and 3.1 % in WT and *DMD^{mdx}* groups, respectively. From the TMRM images, ImageJ isodata method thresholding followed by particle analysis was used to compare the area of what is referred to as mitochondrial objects, between the two groups.

Imaging of spontaneous Ca²⁺ release events

Single isolated FDB muscle fibers dispersed within an Ibidi μ -dish filled with Tyrode solution were incubated for 30 minutes in the presence of 10 μ M Fluo-4 acetoxymethyl ester (AM). Recording and quantification of Ca²⁺ release events were achieved similarly to previously described procedures (see Jaque-Fernandez et al., 2021). In brief, two series of forty consecutive confocal frames of Fluo-4 fluorescence (512×512 pixels at 0.2 μ m per pixel, 636 ms per frame) were acquired in each fiber. Images in each stack were smoothed and the standard deviation (SD) of fluorescence intensity at each pixel position, along the stack, was calculated. The 20% largest values in the SD image were removed to calculate the mean standard deviation of silent areas. Active areas were then defined as pixel positions exhibiting at least 1.5 × larger values of standard deviation than the mean standard deviation value from silent areas.

Solutions

Tyrode solution contained (in mM): 140 NaCl, 5 KCl, 2.5 CaCl₂, 2 MgCl₂, 10 HEPES. The standard extracellular solution for voltage-clamp experiments contained (in mM) 140 TEAmethane-sulfonate, 2.5 CaCl₂, 2 MgCl₂, 1 4-aminopyridine, 10 HEPES and 0.002 tetrodotoxin. The standard intracellular-like solution contained (in mM) 120 K-glutamate, 5 Na₂-ATP, 5 Na₂-phosphocreatine, 5.5 MgCl₂, 5 glucose, 5 HEPES. For measurements of rhod-2 Ca²⁺ transients it also contained 15 EGTA, 6 CaCl₂ and 0.1 rhod-2. All solutions were adjusted to pH 7.20

Data and statistical analysis

Randomization was not used and experimenters were not blinded to the source of muscle fibers being studied. Individual data points and corresponding mean \pm SD values are presented for groups of fibers from a same animal. Statistical comparison was achieved using a hierarchical/nested analysis implemented in GraphPad Prism 10 software (Eisner, 2021) preventing pseudoreplication: measurements from fibers from a same animal were considered as technical replicates; clustering of replicates from the same animal was corrected for by the hierarchical approach (see Sikkel et al., 2017). Unless otherwise stated, this procedure was used for comparison of all parameters between the WT and *DMD^{mdx}* groups. For negative results (P>0.05), the 95% confidence interval (95% CI) for the difference between the mean value in the *DMD^{mdx}* group minus the mean value in the WT group is given. In all presented bar graphs, each individual bar represents one animal and each symbol represents a fiber from that animal.

Results

T-tubule and mitochondria networks in DMD^{mdx} muscle fibers

Enzymatic dissociation of the FDB muscles generated generous batches of healthy-looking muscle fibers, the WT and *DMD^{mdx}* groups being qualitatively indistinguishable, except from the routine presence of 10-15% branched *DMD^{mdx}* fibers. Those were not included in any of the present analysis. No difference in apparent fiber width could be detected between the WT and *DMD^{mdx}* groups (Fig. 1). Staining of the plasma membrane/t-tubules with Di-8-anepps revealed a globally unaltered network (Fig. 2A) in *DMD^{mdx}* fibers, with no sign of change in t-tubule density, nor in t-tubule transverse spacing (Fig. 2B). Dystrophin-deficient muscles were reported to suffer from a decline in mitochondria function and content (see Reid and Alexander, 2021) although not all studies concur on this issue, possibly because of the

heterogeneous nature of mitochondrial stress during progression of the disease (Bellissimo et al., 2022). We took advantage of our isolated fiber preparation to examine the mitochondrial network pattern using TMRM staining (Desai et al., 2023).

The red images in Fig. 3A correspond to the TMRM fluorescence from the above shown transmitted light images of a WT and a DMD^{mdx} muscle fiber. Overall, there was no striking difference that could be visually pinpointed between the two groups of images. The density of staining, normalized to fiber surface area, did not differ between the two groups (P=0.16, nested t-test, 95% CI for the difference between mean values: -2.8 - 13.9), with mean (± SD) values from the 4 WT animals being 20.2 ± 2.5 % (n=5 fibers), 20.7 ± 3.9 % (n=6 fibers), 27.1 ± 4.6 (n=5 fibers) and 20.3 ± 5.2 % (n=10 fibers), and mean values from the 4 DMD^{mdx} animals being 28.3 ± 4.5 % (n=5 fibers), 27.6 ± 8.1 % (n=6 fibers), 34.5 ± 9.3 % (n=5 fibers) and 20.7 ± 5.8 % (n=10 fibers).

Particle analysis showed that the large majority of spatially individualized objects occupied an area less than 5 μ m² in both groups (Fig. 3B), likely corresponding to single pairs of mitochondria on both sides of the Z line. Mean values for the area of this class of objects did not differ between WT and *DMD^{mdx}* fibers (Fig. 3C). When examining larger objects, the frequency was increased in *DMD^{mdx}* fibers with 117 objects larger than 20 μ m² detected in a total of 21 out of 28 fibers, as compared to 38 detected in a total of 15 out of 26 WT fibers (Fig. 3D-E). A nested t-test comparing the number of large events (>20 μ m², Fig. 3E) detected in each tested fiber from the different animals in the two groups, showed that the mean number was significantly elevated in the DMD group (P=0.043). It should be acknowledged that since TMRM accumulation is driven by mitochondrial membrane potential, we cannot exclude a difference in the density of undetected, depolarized mitochondria between WT and *DMD^{mdx}* fibers. Nevertheless, we can at least ascertain that the density of polarized mitochondria is similar in the two groups.

Passive electrical properties

Dystrophin, together with its associated protein complex, is believed to play an important role in securing plasma membrane stability, to the point of preventing membrane rupturing/tearing which are commonly admitted consequences of dystrophin deficiency. Measurements of ion current across the plasma membrane should help define whether leakiness is enhanced in the DMD muscle fibers. Using voltage-clamp, we compared the properties of the membrane current at rest and in response to small hyperpolarizing pulses between WT and DMD^{mdx} fibers. The capacitance of each voltage-clamped fiber portion was estimated from the running integral of the transient current change elicited by a -20 mV pulse from -80 mV. The inset in Fig. 4A shows the capacitive current surges at the onset and termination of the pulse, averaged from all tested WT (black) and *DMD^{mdx}* fibers (blue). The two bars-and-dots graphs in Fig. 4A show individual and mean values for capacitance in fibers from each animal, in the two groups. Unexpectedly, values were significantly larger in *DMD^{mdx}* than in WT fibers (Fig. 4A, P=0.006) with the overall mean value being 1.65 times that in WT fibers. Since fiber apparent width did not differ between the two groups (Fig. 1) and a similar length of fiber portion was always left outside the silicone (typically ~150-200 µm), this suggests an elevated density of plasma membrane in fibers from the DMD^{mdx} model. The bottom graph in Fig. 4A shows another representation of this dataset with capacitance values plotted versus the corresponding amount of surface membrane approximated from the length and apparent width (assumed to be representative of the diameter) of each fiber, assuming it is a cylinder. Fitting a linear relationship in each group gave values consistent with commonly admitted levels of ttubule/surface membrane ratio, but with a value 1.5 times larger in the DMD^{mdx} group. Figure 4B and Fig. 4D show the individual and mean absolute values for holding current (at -80 mV)

and for the steady change in current elicited by the -20 mV pulse, respectively, from the same fibers. Those did not differ between the two groups. However, when normalized to the corresponding capacitance, values for both holding current (Fig. 4C) and steady change upon 20 mV hyperpolarization (Fig. 4E), are significantly lower in DMD^{mdx} fibers as compared to WT fibers (P=0.005 and 0.02, respectively).

Voltage-activated Cav1.1 Ca²⁺ current

 $Ca_V 1.1$ is the most well accredited (Robin and Allard, 2015) and characterized Ca^{2+} entry pathway in differentiated muscle fibers. Considering the amount of literature pointing to exacerbated Ca^{2+} entry in dystrophin-deficient muscle cells, assessing $Ca_V 1.1$ channel function in *DMD^{mdx}* fibers was of prime interest. Our measurements of membrane current taken in response to 0.5 s-long depolarizing pulses of increasing amplitude showed that the current exhibited very similar properties in the two groups (Fig. 5A), and none of the parameters fitted from the voltage-dependency of the peak current differed between WT and *DMD^{mdx}* fibers (Fig. 5B-C).

Voltage-activated SR Ca²⁺ release

Figure 6 shows representative Ca^{2+} release datasets from a WT fiber (left) and from a *DMD*^{*mdx*} fiber (right). A line-scan F/F₀ image taken during application of a pulse to -10 mV is shown in Fig. 6A. Figure 6B shows the superimposed line-averaged F/F₀ traces from the two fibers in response to all tested pulses. The corresponding calculated traces for the rate of Ca²⁺ release (Fig. 6C) displayed the classical early peak, the amplitude of which increased with the pulse amplitude, that declined rapidly towards a very small level in both groups. For intermediate voltages, a hump-like component was routinely detected most likely reflecting the Ca²⁺ storage/release function of calsequestrin in the SR lumen (Royer et al., 2010). Overall, the

time-course of the fluorescence transients and of the corresponding release fluxes presented no specific feature in DMD^{mdx} fibers that would visually distinguish them from those in WT fibers. But, the maximum amplitude of the peak Ca²⁺ release was lower in the diseased condition. The running integral of each Ca^{2+} release trace during the voltage pulses is shown in Fig. 6D. Despite a maximum peak amplitude of Ca^{2+} release smaller by ~25% in the DMD^{mdx} fiber, the maximum amount of released Ca²⁺ (expressed with respect to myoplasmic volume) was similar in the two fibers. All values for peak Ca^{2+} release and total amount of released Ca^{2+} from the tested 29 WT fibers and 27 *DMD^{mdx}* fibers are presented, *versus* voltage, in Fig. 7A and Fig. 7B, respectively. The voltage dependency of peak Ca²⁺ release in each fiber was fitted with a Boltzmann function, the result of which is shown as a superimposed curve on each corresponding dataset in Fig. 7A. Individual values (circles) and corresponding mean (±SD) values (from groups of fibers from the same animal, bars) for maximum peak Ca²⁺ release, mid-activation voltage and slope factor are presented in Fig. 8A-C, respectively, whereas values for total amount of released Ca^{2+} for the largest pulse (to +60 mV) are in Fig. 8D. Statistical analysis showed that the maximum peak amplitude of Ca^{2+} release was significantly depressed in the DMD^{mdx} fibers, by 25%, as compared to WT fibers, whereas all other parameters did not differ. The preserved total amount of released Ca²⁺ in the DMD^{mdx} group indicates that the time-course of the release flux must differ from that in the WT group. To test for this, in each fiber, the decay of Ca^{2+} release triggered by the pulse to +60 mV was fitted with a 2-exponential plus constant function. Values for the parameters (amplitude and time constant for the fast and slow components, and final level/constant) were compared using the nested analysis. Respective values in WT (n=7) and DMD^{mdx} animals (n=7) for the amplitude (mean of $36.6 \pm 10.3 \text{ vs} 32.2 \pm 3.8 \mu \text{M.ms}^{-1}$) and time constant (mean of 4.3 ± 1.2 vs 6.0 ± 1.9 ms) of the fast component, and for the final level (mean of $0.34 \pm$ $0.18 vs 0.34 \pm 0.17 \mu M.ms^{-1}$) did not differ. In contrast, the slow exponential component in

the *DMD^{mdx}* group exhibited a reduced amplitude (mean of $26.7 \pm 6.7 vs 49.1 \pm 14.8 \mu M.ms^{-1}$, P=0.002) and a larger time constant (mean of $53.7 \pm 14.9 vs 30.2 \pm 9.6 ms$, P=0.007). Thus, the slower late decay of Ca²⁺ release in the *DMD^{mdx}* fibers may well explain for the lack of significant difference in total Ca²⁺ released between the two groups, despite the lower peak amplitude in the *DMD^{mdx}* group.

Spontaneous Ca²⁺ release at rest

Enhanced SR Ca²⁺ leak through RyR1 channels was proposed to contribute to dysfunction and damage of dystrophic muscle fibers (Bellinger et al., 2009). Because we have previously revealed RyR1 overactivity at rest, under the form of Ca²⁺ sparks, in intact muscle fibers from other models of muscle diseases (Kutchukian et al., 2017, 2019), we tested whether this would be also the case in the *DMD^{mdx}* condition. The bottom images in Fig. 9A correspond to the standard deviation of fluo-4 fluorescence intensity at each pixel position, along a sequence of 40 consecutive *x*, *y* confocal frames. Local spots of elevated SD correspond to locations of Ca²⁺ sparks occurrence. In these conditions, a few sparks were routinely detected, in both the WT and the *DMD^{mdx}* fibers. The relative fiber area showing sparks activity was quantified. Individual values from each fiber and corresponding mean values from fibers from a same animal are shown in Fig. 9B. Values were very low: less than 0.5 % of the fiber's area presented with Ca²⁺ release activity, consistent with the notorious very low incidence or absence, of Ca²⁺ sparks in healthy intact mammalian muscle fibers. There was no significant difference between the WT and the *DMD^{mdx}* groups.

Action-potentials

Lack of dystrophin in muscle cells is presumed to impair plasma membrane stability so that contraction would induce membrane rupture and/or impairment of excitability; this would be

involved in muscle strength loss (Petrof et al., 1993; Call et al., 2013; Roy et al., 2016). With the aim of identifying functional signs of such processes, we challenged WT and DMD^{mdx} muscle fibers with trains of action-potentials (APs), in the absence of intracellular Ca²⁺ buffering, thus allowing full contraction of the fiber portion under study. Representative examples of trains of APs are shown in Fig. 10, from a WT and a *DMD^{mdx}* muscle fiber at the different tested frequencies. Overall, we found no indication that electrical activity of the diseased fibers would be specifically sensitive to either repeated or tetanic contractions. Figure 11 presents values for the voltage level preceding each AP and for the peak amplitude of each AP, during the course of the trains, at the different frequencies, in each fiber tested. At 80 Hz, 2 out of 6 WT fibers and 4 out of 8 *DMD^{mdx}* fibers presented with a substantial drop in AP amplitude. Otherwise, in no case did we detect depolarization of the resting (pre-AP) levels that would witness substantial membrane damage and or loss of excitability. We also quantified the rate of voltage return to the resting level, at the end of the 20, 50 and 80 Hz trains, by fitting an exponential function to this time course (highlighted in red in Fig. 10): there was no significant difference between the groups of WT and DMD^{mdx} fibers. With respect to single AP properties, peak values did not differ between the two groups but the half-width was significantly enhanced (P=0.02) in the DMD^{mdx} condition with mean (±SD) values of 1.45 ± 0.27 (n=4 fibers), 1.46 ± 0.1 (n=3) and 1.24 ± 0.13 ms (n=3) in the fibers from 3 WT animals, and 1.61 ± 0.19 (n=4), 1.76 ± 0.34 (n=4) and 1.60 ± 0.09 ms (n=3), in fibers from 3 DMD^{mdx} animals.

Discussion

Multiple molecular and cellular consequences of dystrophin-deficiency have been documented (see for instance Allen et al., 2016), but the exact mechanisms that determine

muscle fibers weakness and muscle fibers necrosis in DMD remain controversial. Altered Ca^{2+} fluxes affecting intracellular Ca^{2+} handling has been proposed, for more than 40 years (e.g. Bodensteiner, and Engel, 1978), to underlie or at least contribute. However, despite recurrent authoritative statements in the literature regarding the critical role of Ca^{2+} entry across the plasma membrane, or of Ca²⁺ leak across the SR membrane, direct evidence of how exactly (and quantitatively to what extent and along which time frame) these mechanisms affect muscle fiber function and integrity remains nebulous. Further understanding of these issues requires detailed knowledge of the functional properties of the diseased muscle fibers, keeping in mind that conditions allowing either control or reading of the plasma membrane voltage are precious when it comes to investigate the properties of transmembrane Ca²⁺ fluxes and of SR Ca²⁺ release. We used here a combination of electrophysiology and imaging that has proved efficient in the past, to identify and quantify defects in Ca²⁺ signaling and EC coupling in other muscle diseases (e.g. Kutchukian et al., 2016, 2017, 2019; Huntoon et al., 2018; Pelletier et al., 2020; Silva-Rojas et al., 2022). We applied this combination to muscle fibers isolated from a rat model (DMD^{mdx}) that reproduces the DMD patient's condition better than the standard *mdx* mouse. One limitation of the preparation is that collagenase treatment was used for isolation, so that the extracellular matrix is largely removed. Intact isolated DMD^{mdx} muscle fibers looked fine, with no sign of widespread or local sarcomere shortening (Fig. 2B) that would be expected in the presence of membrane damage. Measurements of the apparent width of the FDB muscle fibers showed no difference between the WT and DMD^{mdx} groups, which contrasts with the smaller diameter values reported by Larcher et al. (2014) in DMD^{mdx} fibers, from analysis of frozen sections from the biceps femoris muscles. It cannot be excluded that the FDB muscles exhibit a milder phenotype than the *biceps femoris* muscles. However, diameter values determined from a muscle section cannot distinguish between nonbranched and branched fibers and it is very possible that this contributed to the difference

between the two studies as we did not consider branched fibers in our analysis. Membrane current measurements also provided no indication for an increase in resting membrane conductance, that would also be anticipated from a leaky or damaged plasma membrane. WT and *DMD^{mdx}* fibers contracting in response to trains of action potentials behaved very similarly, with no sign that the contractile activity would specifically affect plasma membrane polarization in the diseased fibers. Of course, one cannot exclude that more stringent conditions, for instance eccentric contractions (Call et al., 2013), are required to induce membrane damage and/or electrophysiological alterations in the diseased fibers. However, single muscle fiber measurements of either membrane current or membrane voltage are very sensitive to the integrity of the plasma membrane and, with respect to the widely acknowledged concepts of membrane frailty and rupturing, that are traditionally associated with dystrophin deficiency, we find it puzzling that this does not show in the electrical measurements.

In fully differentiated fibers, t-tubules and mitochondria form dense, well-organized networks. The t-tubule network integrity is mandatory for proper EC coupling function. Our di-8-anneps images did not show any obvious alteration in the DMD^{mdx} fibers, at least nothing that would come any close to the t-tubule loss observed, for instance, in muscle fibers from the mouse model of myotubular myopathy (Al Qusairi et al., 2009; Kutchukian et al., 2016) which make fibers suffer from EC coupling failure (Szentesi et al., 2023). On the contrary and quite intriguing, we found that DMD^{mdx} fibers presented with a larger capacitance than WT fibers. This may result from enhanced t-tubule tortuosity at a resolution level inaccessible to di-8-anneps imaging. Interesting in this respect are results from early electron microscopy studies of biopsies from DMD patients, which described alterations of the t-tubule system taking the form of abnormal course and tangle formation (Oguchi and Tsukagoshi, 1980; Oguchi et al.,

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1982). We are currently exploring the possibility that this is happening in the DMD^{mdx} muscle fibers.

With respect to mitochondria, there has been reports of changes in mitochondria morphology and of concurrent metabolic defects in dystrophic muscle, possibly related to altered mitochondrial Ca²⁺ content (Pant et al., 2015; Moore et al., 2020; see Mareedu et al., 2021) although absence of differences in aspects of mitochondrial content and dynamics has also been reported (Barker et al., 2018). Our TMRM measurements showed that the global mitochondrial network pattern is similar in WT and DMD^{mdx} fibers, with a majority of small single objects in the two populations. Interesting though was the propensity for more numerous large objects (area >20 μ m²) in *DMD^{mdx}* fibers that, we speculate, may be related to the previously acknowledged changes in mitochondria dynamics and mitophagy in dystrophin-deficient muscle cells (Pant et al., 2015; Reid and Alexander, 2021). Properties of the Ca_V1.1 Ca²⁺ current are unaffected in DMD^{mdx} fibers. Although this Ca²⁺ entry is not mandatory for muscle function (Dayal et al., 2017), our data at least prove that there is no enhanced Ca^{2+} entry through $Ca_V 1.1$ in the *DMD^{mdx}* fibers, which does not exclude that it may occur through alternate pathways. This result may also be viewed with reference to muscle disease conditions affecting EC coupling, with depressed SR Ca²⁺ release being paralleled by depressed Cav1.1 Ca²⁺ current (Al Qusairi et al., 2009; Kutchukian et al., 2017; Huntoon et al., 2018; Pelletier et al., 2020; Silva-Rojas et al., 2022). The situation is obviously different here, even though the maximum peak amplitude of Ca^{2+} release was depressed by a similar extent as, for instance, in the model of myopathy due to reduction in RyR1 content (Pelletier et al., 2020). This indicates that the reason for reduced Ca^{2+} release in DMD^{mdx} fibers is likely to be mechanistically distinct. In comparison, previous studies using the *mdx* mouse provided contrasting results, some groups reporting reduced SR Ca^{2+} release in the *mdx* fibers (Woods et al, 2004; Hollingworth et al., 2008) whereas other reported either

minor or no differences with the WT fibers (Head, 1993; Collet et al., 1999; Tutdibi et al., 1999). Here, the reduced peak SR Ca²⁺ release occurred with no significant change in the total amount of released Ca²⁺ at the end of the 0.5 s-long pulses. A lower SR content, which could occur as a consequence of an increased SR Ca²⁺ leak, was thus likely not involved. Also arguing against an enhanced SR Ca²⁺ leak in the *DMD^{mdx}* fibers was the absence of any difference in the spontaneous Ca²⁺ release activity at rest.

Altogether, the present characterization of intact DMD^{mdx} muscle fibers failed to identify functional signs of plasma membrane compromised integrity, fragility, unspecific leakiness or enhanced Ca²⁺ entry across Cav1.1 channels. It though revealed a significant reduction of peak SR Ca²⁺ release during EC coupling, the extent of which (25%) likely contributes to muscle weakness, without being expected to dramatically compromise muscle function (if remaining at that level). We found no indication that this decrease is related to an enhanced SR Ca²⁺ leakage. We cannot exclude that the previously proposed enhanced plasma and SR membrane leakiness to Ca²⁺ occur within a range and/or time scale that are not accessible to our measurements. We also cannot exclude that the pathophysiological impact of such alterations is of limited relevance with respect to the dramatic outcome of the disease in terms of muscle function and integrity.

In summary, muscle fibers from 3-month-old DMD^{mdx} rats present no obvious deleterious alteration of plasma/t-tubule membrane properties that would be consistent with fragility, compromised excitability or excess Ca²⁺ entry. Yet, these fibers exhibit a reduced maximum rate of voltage-activated SR Ca²⁺ release which likely contributes to depressed force production, without being expected to dramatically impair muscle function. Future investigations at later stages of the disease should help define whether these features remain stable or deteriorate as the disease progresses.

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Data availability

All generated datasets are presented in the article. Raw data will be made available upon request.

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Author contributions

JS and LR conducted single muscle fibers experiments, performed data analysis and contributed to preparation of figures. YT performed image analysis and was involved in data interpretation and discussion, and in preparation of the manuscript. BA and CB provided critical input throughout the project, contributed to study design and to data analysis, interpretation and discussion and to manuscript preparation. AL and CH provided the muscle samples and were involved in the design and planning of experiments and in data interpretation and discussion and manuscript preparation. VJ performed experiments on single muscle fibers, contributed to data analysis and preparation of figures and wrote the manuscript. VJ and CH designed, coordinated and supervised the study.

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Abbreviations

Cav1.1	α1 subunit of the dihydropyridine receptor
dCa _{Tot} /dt	Sarcoplasmic reticulum Ca ²⁺ release flux
F ₀	Baseline fluorescence
FDB	Flexor digitorum brevis
EC	Excitation-contraction
RyR1	Type 1 ryanodine receptor
SERCA	Sarco-endoplasmic reticulum Ca ²⁺ ATPase
SR	Sarcoplasmic reticulum
T-tubule	Transverse tubule

FIGURE LEGENDS

Figure 1. Apparent width of WT and *DMD^{mdx}* **muscle fibers.** Individual and corresponding mean (\pm SD) values for the apparent width of WT and *DMD^{mdx}* fibers (n=126 fibers from 7 animals in each group). Five measurements were taken from each fiber, using equally-spaced lines, transverse to the longitudinal axis. Each data point corresponds to the average from these 5 measurements. Each bar (and superimposed data points) shows data from a same animal. Main graphs show values from fibers used for di-8-anepps, TMRM and fluo-4 staining. WT and *DMD^{mdx}* values did not significantly differ (P=0.95, nested t test, 95% CI for the difference between mean values: -7.8 - 8.3). Insets shows values from the voltage-clamped fibers (n=29 fibers from 7 WT animals and 27 fibers from 7 *DMD^{mdx}* animals. P=0.17, nested t test, 95% CI for the difference between mean values: -2.4 - 12.0).

Figure 2. T-tubule network in WT and DMD^{mdx} muscle fibers. (A) Confocal images of di-8-anepps fluorescence in a WT and in a DMD^{mdx} fiber, at two magnifications. The white trace superimposed on each bottom image corresponds to the average fluorescence intensity profile along the region of interest enclosed within the yellow rectangle. Transmitted light images are shown on top. All scale bars correspond to 10 µm. (B) Top, individual and corresponding mean (± SD) values for the t-tubule density index in WT and DMD^{mdx} fibers (n=52 fibers from 5 animals in each group. P=0.94, nested t test, 95% CI for the difference between mean values: -3.2 - 3.0). Bottom, individual and corresponding mean (± SD) values for the average distance between adjacent t-tubules (spacing) in WT and DMD^{mdx} fibers (n=48 fibers from 5 WT animals and n=51 fibers from 5 DMD^{mdx} animals. P=0.61, nested t test, 95% CI for the difference between mean values: -0.023 - 0.015). Each bar and superimposed data points correspond to data from a same animal.

Figure 3. TMRM staining of mitochondria in WT and *DMD^{mdx}* muscle fibers. (A)

Confocal images of TMRM fluorescence in a WT and in a *DMD^{mdx}* fiber at two distinct magnifications. Corresponding transmitted light images are shown on top. Black and white frames at the bottom correspond to the binary images obtained after thresholding the above images. (B) Distribution of the values for the area of separate mitochondrial objects in the two groups, up to $20 \,\mu m^2$. Each symbol corresponds to the percentage of identified objects exhibiting à given surface, with an increment of 0.2 μ m², from all WT and *DMD^{mdx}* muscle fibers. (C) Individual and corresponding mean $(\pm SD)$ values for the area of mitochondrial objects smaller than 5 μ m² (data are from 26 fibers from 4 WT animals and 28 fibers from 5 DMD^{mdx} animals. P=0.38, nested t test, 95% CI for the difference between mean values: -0.29 - 0.13). Each bar and superimposed data points correspond to data from a same animal (arrows point to the series of large events detected in the same groups of fibers in E). (D) Distribution of the values for the area of mitochondrial objects larger than $20 \,\mu m^2$ in the two groups. Each symbol corresponds to the percentage of identified objects exhibiting à given surface, with an increment of 50 μ m², from all WT and *DMD^{mdx}* muscle fibers. (E) Individual values for the area of all mitochondrial objects larger than 20 μ m² in fibers from each animal (each column of data points corresponds to fibers from the same animal as in C; each symbol corresponds to an individual area in a given fiber). The red inset shows an example of binary image from a large object detected in a DMD^{mdx} fiber (190 μ m², corresponding datapoint also shown in red in the graph).

Figure 4. Membrane current in WT and DMD^{mdx} **muscle fibers.** (A) Individual and corresponding mean (± SD) values for the capacitance (Cm in nanofarad, nF) of WT and DMD^{mdx} fibers (n=29 fibers from 7 WT animals and n=27 fibers from 7 DMD^{mdx} animals.

P=0.006, nested t test). Each bar and superimposed data points correspond to data from a same animal. The inset shows the mean membrane current transients at the onset and termination of a -20 mV pulse from -80 mV, from all tested WT and in DMD^{mdx} muscle fibers. The bottom graph shows values for the capacitance as a function of the estimated surface membrane area of each corresponding fiber. Straight lines correspond to the result of a linear fit in each group. (**B**) Individual and mean (± SD) absolute values for holding current (I_H) in WT and DMD^{mdx} fibers (n=29 fibers from 7 WT animals and n=27 fibers from 7 DMD^{mdx} animals. P=0.42, nested t test, 95% CI for the difference between mean values: -1.35 - 3.00). Each bar and superimposed data points correspond to data from a same animal. (**C**) Corresponding individual and mean (± SD) values for the holding current normalized to the capacitance (P=0.005, nested t test). (**D**) Individual and corresponding mean (± SD) absolute values for the steady change in membrane current ($\Delta L/20mV$) measured at the end of the -20 mV pulse (P=0.85, nested t test, 95% CI for the difference between mean values: -0.73 - 0.61). (**E**) Corresponding individual and mean (± SD) values for the steady current, normalized to the capacitance (P=0.02, nested t test).

Figure 5. Voltage-activated Cav1.1 Ca²⁺ current in WT and *DMD^{mdx}* muscle fibers. (A) Representative examples of Ca²⁺ current traces in the two groups, in response to the indicated pulse protocol. (B) Values for the peak Ca²⁺ current *versus* voltage in WT and *DMD^{mdx}* fibers (data are from 29 fibers from 7 WT animals and 27 fibers from 7 *DMD^{mdx}* animals). For the sake of clarity, only mean (\pm SD) values from fibers from a same animal are shown. (C) Individual and corresponding mean (\pm SD) values for the parameters (G_{max} the maximum conductance, V_{0.5} the mid-voltage, V_{rev} the reversal potential and k the slope factor) fitted from the peak current *vs* voltage relationship in each fiber. Each bar and superimposed data points correspond to data from a same animal. For G_{max}, V_{0.5}, V_{rev} and k, P=0.85, 0.79, 0.79 and 0.29, respectively (nested t tests, corresponding 95% CIs for the difference between mean values: -0.035 - 0.029, -6.83 - 5.32, -9.58 - 7.46, -0.77 - 2.39, respectively).

Figure 6. Voltage-activated SR Ca²⁺ release in WT and *DMD^{mdx}* muscle fibers. (A)

Examples of confocal line-scan images of rhod-2 fluorescence collected from a WT and from a DMD^{mdx} muscle fiber, while applying a depolarizing pulse to -10 mV. (**B**) Line-averaged rhod-2 fluorescence changes elicited by the pulses shown on top, in the same WT and DMD^{mdx} fibers as in (A). (**C**) Rate of SR Ca²⁺ release calculated from the rhod-2 F/F₀ records shown in (B). (**D**) Running integral of the SR Ca²⁺ flux traces shown in (C) during the depolarizing pulses.

Figure 7. Voltage-dependence of SR Ca²⁺ release in WT and *DMD^{mdx}* muscle fibers. (A) Values for peak SR Ca²⁺ release flux *versus* voltage in all tested WT and *DMD^{mdx}* muscle fibers (data are from 29 fibers from 7 WT animals and 27 fibers from 7 *DMD^{mdx}* animals). An identical symbol is used for fibers from a same animal. Each dataset was fitted with a Boltzmann function (superimposed lines). The inset in each graph shows the mean (\pm SD) values calculated using the average from fibers from a same animal (n=7 in each group). (B) Corresponding values for the voltage-dependency of the total amount of released Ca²⁺ in the two groups of fibers.

Figure 8. SR Ca²⁺ release parameters in WT and *DMD^{mdx}* muscle fibers. (A-D) Individual and corresponding mean (\pm SD) values for maximum rate of SR Ca²⁺ release (Max), voltage of mid-activation (V_{0.5}), slope factor (k), and total amount of released Ca²⁺ ([Ca_{Tot}]), respectively, in WT and *DMD^{mdx}* fibers (data are from 29 fibers from 7 WT animals and 27 fibers from 7 *DMD^{mdx}* animals). Each bar and superimposed data points correspond to data from a same animal. Values in (A-C) were obtained from fitting a Boltzmann function to the peak SR Ca²⁺ release *versus* voltage relationships. For Max, V_{0.5}, k and [Ca_{Tot}], P=0.011, 0.21, 0.42 and 0.49, respectively (nested t test). For V_{0.5}, k and [Ca_{Tot}], the 95% CIs for the difference between mean values are: -11.07 - 2.69, -2.29 - 1.03 and -910.6 - 461.5, respectively.

Figure 9. SR Ca²⁺ release events at rest in WT and *DMD^{mdx}* **muscle fibers. (A)** Green images show the spatial distribution of the standard deviation of fluo-4 fluorescence intensity throughout a sequence of 40 *x*, *y* consecutive confocal frames, in a WT and in a *DMD^{mdx}* muscle fiber. Transmitted light images of the two fibers are shown on top. (B) Individual and corresponding mean (\pm SD) values for the relative fiber area exhibiting spontaneous Ca²⁺ release in the two groups (data are from 50 fibers from 5 animals in each group. P=0.42, nested t test, 95% CI for the difference between mean values: -0.065 - 0.14). Each bar and superimposed data points correspond to data from a same animal.

Figure 10. Trains of action-potentials in WT and *DMD^{mdx}* **muscle fibers.** Representative records of the changes in membrane voltage elicited by short supra-threshold depolarizing current pulses delivered during 3 s at the indicated frequency, in a WT and in a *DMD^{mdx}* muscle fiber. Superimposed red lines at the end of the 20, 50 and 80 Hz records correspond to the result of a single exponential fit (see text for details).

Figure 11. Evolution of the membrane voltage during the course of 3 s-long trains of action potentials. Graphs show voltage values measured just before each action-potential and at the peak value in all tested WT and DMD^{mdx} muscle fibers. (data are from 10 fibers from 3

WT animals and 11 fibers from 3 DMD^{mdx} animals). An identical symbol is used for fibers from a same animal.