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# scientific reports



## **OPEN** New atrio-ventricular indices derived from conventional cine MRI correlate with functional capacity in patients with asymptomatic primary mitral regurgitation

Perrine Marsac<sup>1</sup>, Thomas Wallet<sup>2</sup>, Alban Redheuil<sup>3</sup>, Moussa Gueda Moussa<sup>1</sup>, Jérôme Lamy<sup>4</sup>, Vincent Nguyen<sup>1</sup>, Etienne Charpentier<sup>3</sup>, Nadjib Hammoudi<sup>2</sup>, Emilie Bollache<sup>1</sup> & Nadjia Kachenoura<sup>1</sup>

Mitral regurgitation (MR) is associated with morphological and functional alterations of left atrium (LA) and ventricle (LV), possibly inducing LA-LV misalignment. We aimed to: (1) characterize angulation between LA and mitral annulus from conventional cine MRI data and feature-tracking (FT) contours, (2) assess their associations with functional capacity in MR patients, as assessed by oxygen consumption (peak-VO<sub>2</sub>) and minute ventilation to carbon dioxide production (VE/VCO<sub>2</sub>) slope, in comparison with MRI LA/LV strain indices. Thirty-two asymptomatic primary MR patients (56 [40; 66] years, 12 women) underwent cardiac MRI resulting in LA/LV conventional FT-derived strain indices. Then, end-diastolic angles were derived from FT LA contours: (1) α, centered on the LA centre of mass and defined by mitral valve extremities, (2) y, centered on the mitral ring anterior/lateral side, and defined by LA centre and the other extremity of the mitral ring. Cardiopulmonary exercise testing with simultaneous echocardiography were also performed; peak-VO<sub>2</sub> and VE/VCO<sub>2</sub> slope were measured. While peak-VO<sub>2</sub> and VE/VCO<sub>2</sub> slope were not correlated to LA/LV strains, they were significantly associated with angles ( $\alpha$ : r = 0.50, p = 0.003 and r = -0.52, p = 0.003; y: r = -0.53, p = 0.002 and r = 0.52, p = 0.003; respectively), independently of age and gender ( $R^2 \ge 0.29$ ,  $p \le 0.03$ ). In primary MR, the new LA/mitral annulus angles, computed directly from standard-of-care MRI, are better correlated to exercise tolerance than conventional LA/LV strain.

Primary mitral valve regurgitation (MR) is the second most frequent valvular heart disease in Europe<sup>1</sup>. Due to volume overload, MR induces morphological and functional changes in both left ventricle (LV) and left atrium (LA), and the enlargement of left heart chambers in chronic primary MR occurs progressively even before symptoms appearance<sup>2</sup>. Therefore, MR precise characterization and severity assessment along with evaluation of LV and LA involvement are essential to help patient management and therapeutic or surgical decision-making<sup>3</sup>.

Imaging modalities play a major role in the exploration of patients with MR. Indeed, echocardiography is the first intent and an effective method for MR quantification. Furthermore, recent cardiac MRI studies highlighted that MRI phase-contrast and volumetric measures could provide additional information and may achieve higher performances in MR severity assessment and outcome prediction<sup>4,5</sup>.

Beyond the ability of MRI to accurately assess heart chamber volumes and myocardial fibrosis, the use of feature tracking (FT) on conventional cine images, without any extra acquisition, is evolving for the exploration of both LV<sup>6,7</sup> and LA<sup>8-11</sup> function in various disease conditions including MR<sup>12,13</sup>. Such simultaneous LA and LV exploration on cine long axis MRI images can provide further investigations into LA and LV misalignment and mitral annulus inclination, without extra complex analysis since FT time-resolved contours are readily available.

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As such, horizontal inclination of the mitral annular plane has been recently shown in patients with MR and atrial dilatation, and such horizontal tilt decreased with surgical plication while LA size was lower<sup>14</sup>. Another study<sup>15</sup> proposed an LA-LV angulation index, which was described as a measure of LA and LV remodelling and predicted by LV and LA size and mitral regurgitation.

Accordingly, in the present study, we took advantage of LV and LA FT time-resolved contours derived from MRI long axis images: (1) to define new LA/LV angles based on mitral inclination and LA/LV remodelling; (2) to compare associations of such angle indices and conventional FT-derived LV and LA strain indices with MRI-independent indicators of exercise tolerance, including peak VO<sub>2</sub> oxygen consumption and minute ventilation to carbon dioxide production slope as a reflect of ventilatory efficiency, in patients with asymptomatic chronic primary MR and preserved ejection fraction.

### Materials and methods

#### Study population and data acquisition

This retrospective study included 32 patients (median age: 56 [40; 66] years; n = 12, 38% women) with asymptomatic primary MR and preserved LV ejection fraction (LVEF), who underwent exercise transthoracic echocardiography (TTE) combined with gas exchange measurements and cardiac MRI. Based on the European Society of Cardiology guidelines<sup>3</sup>, asymptomatic was defined as a patient who has not reported exercise intolerance as assessed using New York Heart Association (NYHA) classification. Hence, we only included Class I NYHA patients. While TTE and MRI were performed within a median delay of 22 [5; 62] days, more than half of patients underwent these explorations within the same month (n = 18, 56%). Exclusion criteria were: Class I recommendation of mitral surgery (symptoms, TTE LVEF ≤ 60% or LV systolic diameter ≥ 40 mm), aortic regurgitation, prior surgical interventions, known coronary artery disease, congenital cardiomyopathy or inability to perform exercise. This clinical study was carried out according to the principles outlined in the Declaration of Helsinki. Exercise TTE combined with gas exchange measurements and MRI are performed in routine practice in asymptomatic MR patients, a written informed consent for such investigations was signed by all participants. The retrospective use of these data was allowed by the Research Ethics Committee of Sorbonne Université under the reference CER-2021-095. This study complies with the reference methodology (MR004) of the French National Commission for Informatics and Liberties. According to the French national legislation, the use of retrospective data is rendered legal through such MR004, which provides the ethics approval. MRI data of additional 17 healthy volunteers with similar age and gender balance to the MR patients were also selected from control groups of previous local databases (Clinical Trials #NCT02517944, NCT02059538).

TTE proximal isovelocity surface area (PISA) method was used to measure effective regurgitant orifice area (EROA) as well as regurgitant volume. Conventional LV forward stroke volume and the ratio of mitral inflow to aortic outflow velocity–time integrals (VTI) were also assessed by pulsed wave Doppler<sup>16</sup>. After baseline evaluation, a maximal symptom-limited cardiopulmonary exercise testing with simultaneous echocardiography (Vivid E9, General Electric, Horten, Norway) was performed on semi-supine cycle ergometer (Ultra Koch, Le Haillan, France) using a standardized incremental ramp protocol (start with 10 W, followed by increments of 10–20 W per min depending on patient predicted maximal exercise capacity)<sup>17,18</sup>; maximal workload as well as maximal and % predicted maximal heart rate were reported. Oxygen consumption (VO<sub>2</sub>), minute ventilation (VE), and carbon dioxide production (VCO<sub>2</sub>) were assessed throughout the examination (CARDIOVIT CS-200, Schiller, Baar, Switzerland). Peak VO<sub>2</sub> was expressed as the highest VO<sub>2</sub> measurement obtained during exercise and was indexed to body weight. VE/VCO<sub>2</sub> slope was calculated via least squares linear regression at peak. Peak respiratory exchange ratio (RER), as an indicator of maximal exercise effort, was defined as the highest VCO<sub>2</sub>/VO<sub>2</sub> ratio obtained during exercise. Exercise capacity was also expressed as percentage of predicted peak VO<sub>2</sub> according to age and sex. Finally, peak tricuspid regurgitation velocity (TRV) was recorded as an index of systolic pulmonary artery pressure (SPAP) at rest as well as at low exercise (30 W) and peak exercise levels.

MRI was performed on a 1.5 T scanner (Aera, Siemens, Erlangen, Germany). Standard cine images were obtained using a balanced steady-state free precession (SSFP) sequence with multiple breath-holds and ECG gating. Short- and long-axis (2- and 4-chamber views) SSFP imaging was performed with the following acquisition parameters, reported as median value (minimal-maximal values): echo time (TE): 1.2 (0.9–1.4) ms; repetition time (TR): 2.8 (2.1–3.1) ms; temporal resolution: 38 (23–54) ms; 25 reconstructed images per cardiac cycle; flip angle: 53 (50–62)°; acquisition matrix:  $(128–256) \times (66–256)$ ; pixel size: 1.5 (1.2–3.2) mm; slice thickness: 6 (4–8) mm. Furthermore, a 2D phase-contrast (PC) sequence was acquired in a cross-sectional slice perpendicular to the ascending aorta at the level of the pulmonary trunk bifurcation, under breath-hold using ECG gating and the following acquisition parameters: TE: 3.3 (2.5–4.3) ms; TR: 5.5 (4.6–6.5) ms; temporal resolution: 16 (10–21) ms; 60 reconstructed images per cardiac cycle; flip angle: 20°; acquisition matrix: 192 × (97–119); pixel size: 2.1 (1.8–2.6) mm; slice thickness: 6 mm; encoding velocity: 150 cm/s.

#### **MRI** image analysis

LA and LV volumes were conventionally measured using QMass software (Medis Medical Imaging, Leiden, The Netherlands). LV end-diastolic and end-systolic volumes and mass were estimated from short-axis cine images through tracing of endocardial and epicardial contours from base to apex at end-diastole and end-systole. Maximal and minimal LA volumes were estimated from 2- and 4-chamber views while using the area-length method. LV stroke volume as well as LV and LA ejection fractions were further calculated. Cardiac volumes and mass were indexed to body surface area. Aortic ejection volume was measured using PC images and a previously described and validated semi-automated delineation of ascending aortic wall borders throughout the cardiac cycle<sup>19</sup>; finally, common MRI-derived mitral regurgitation volume was computed as LV stroke volume—PC images-derived aortic ejection volume<sup>20</sup>. Cine images were further analysed using an in-house FT software (CardioTrack, LIB, Sorbonne Université) widely validated for myocardial strain estimation on both human<sup>6,8,11,21,22</sup> and animal<sup>23,24</sup> MRI data. Briefly, after endocardial (LA, LV) and epicardial (LV) contours initialization on a single temporal phase, tracking was performed on the adjacent time-phases successively toward the beginning and the end of the cardiac cycle. For such tracking, a region of interest is defined around each point of the initial contour. Then a map with the cross-correlation values between this region and its spatial neighbourhood on the next time phase is calculated. This cross-correlation map is weighted with additional maps derived from image properties and constraints related to physiological knowledge regarding contractile function, as described in Ref.<sup>6</sup>. FT contours were used to estimate time-resolved strain curves for both the LV, as an average of epicardial and endocardial strain, and the LA. Then LV peak systolic circumferential and longitudinal strains, as well as reservoir, conduit and booster LA longitudinal strains, which were averaged from 2- and 4-chamber view measures, were derived.

Finally, FT long-axis contours derived from both 2- and 4-chamber views were further used to estimate LA to mitral annulus angulation (Fig. 1) through the two following angles:  $\alpha$  was the angle centered on the LA centre of mass and defined by mitral valve extremities;  $\gamma$  was the angle centered on the anterior/lateral side of the mitral annulus and defined by the LA centre of mass and the mitral annulus plane. End-diastolic angles were finally extracted from time-resolved curves and maximal value between 2- and 4-chamber views was collected.

Reproducibility of end-diastolic  $\alpha$  and  $\gamma$  was assessed in the 17 healthy individuals after analysis of MRI data by 2 independent users (PM and MGM).

#### **Statistical analyses**

We determined sample size with a power calculation; indeed, in order to detect a correlation above 0.50 (Pearson's coefficient) between the primary end-point MRI angle indices and indicators of exercise capacity with 80% power and 5% alpha level, a sample of 24 patients is required. Continuous variables were expressed as median and interquartile range. Patients were divided into subgroups according to exercise capacity, as defined by peak VO<sub>2</sub> tertiles. Comparisons across peak VO<sub>2</sub> and control groups were performed using a Kruskal–Wallis test for continuous variables and Fisher's exact test for discrete variables. Associations of the proposed angles and conventional echocardiographic TRV as well as MRI LV and LA volume and strain indices with peak VO<sub>2</sub>, % age-predicted peak VO<sub>2</sub> and VE/VCO<sub>2</sub> slope as prognostic and MRI-independent parameters of functional capacity in MR patients<sup>25</sup>, were studied using linear regressions. Pearson's correlation coefficients were reported. For significant relationships, further adjustment for age and sex was performed using multivariate models. Finally, inter-operator reproducibility was assessed through intraclass correlation coefficient. Tests were two-tailed and statistical significance was set to a p value < 0.05. Statistical analyses were carried out using JMP software (Cary, NC, USA).



**Fig. 1.** LA-mitral annulus angles extracted from FT-derived contours on cine SSFP long-axis images. 2- (left) and 4- (right) chamber view cine SSFP image at diastolic phase for a patient with high exercise capacity (**a**) and low exercise capacity (**b**). (**c**) Angle curves with end-diastolic values (black filled stars) of patient with high (solid line) and low (dashed line) exercise capacity.

#### Results

Table 1 summarises patient and control characteristics along with patient TTE parameters, exercise testing measures as well as MRI regurgitant volume, LV and LA volumes, strain and angle indices according to VO<sub>2</sub> tertiles. As per study design, healthy volunteers and patients had similar age (p=0.19) and proportion of men (p=0.71). All included patients performed maximal exercise effort as reflected by RER values. Five patients (16%) had atrial fibrillation (AF), among which 4 had paroxysmal AF and were investigated in sinus rhythm, while the last patient had permanent AF but had a heart rate of 68 bpm at rest so imaging quality was not altered by tachycardia. All patients had a heart rate below 87 bpm during MRI. There were no significant differences across groups in age, BMI and gender. Although regurgitant volume whether assessed using echocardiography or MRI, as well as TTE EROA, LV forward stroke volume and mitral to aortic VTI ratio were similar across the 3 VO<sub>2</sub> tertile groups, EROA, forward stroke volume and mitral/aortic VTI ratio were higher in the second group. TRV

	1st VO <sub>2</sub> tertile	2nd VO <sub>2</sub> tertile	3rd VO <sub>2</sub> tertile	Controls	p-value
Peak VO <sub>2</sub> (mL/kg/min)	Peak VO <sub>2</sub> < 25	25≤Peak VO <sub>2</sub> <29	Peak $VO_2 \ge 29$	-	
n	11	10	11	17	
Basic characteristics					
Age (years)	63 [48; 71]	62 [39; 67]	50 [37; 60]	50 [36; 57]	0.18
BMI (kg/m <sup>2</sup> )	25.9 [23.8; 30.6]	23.6 [21.1; 25.2]	22.4 [19.2; 26]	24.7 [22.7; 27.5]	0.11
Males (N)	6	6	8	10	0.84
Heart rate during MRI (bpm)	61 [55; 69]	68 [57.8; 72.3]	57 [50; 65]	63 [57.5; 68]	0.29
TTE parameters and exercise testing characteristics					
Effective regurgitant orifice area (cm <sup>2</sup> )	0.32 [0.22; 0.41]	0.43 [0.36; 0.72]	0.30 [0.22; 0.59]	-	0.13
Forward stroke volume (mL)	73.7 [69.1; 86.5]	78.5 [71.8; 101]	72.3 [60.8; 108]	-	0.71
Regurgitant volume (mL)	60.2 [29.9; 70.0]	59.6 [43.5; 124.1]	39.9 [31.2; 80.3]	-	0.33
Mitral/aortic VTI ratio	1.16 [0.96; 1.37]	1.41 [1.25; 1.51]	1.32 [1.10; 1.79]	-	0.27
Rest TRV (m/s)	2.8 [2.4; 3.1]	2.5 [2.4; 2.8]	2.3 [2.0; 2.3]	-	0.007
Low exercise level TRV (m/s)	3.1 [3.0; 3.3]	3.0 [2.7; 3.4]	2.7 [2.6; 2.9]	-	0.05
Peak exercise TRV (m/s)	3.4 [2.9; 3.6]	3.6 [3.3; 3.6]	3.4 [2.9; 3.6]	-	0.58
Maximal workload (W)	129 [90; 181]	145 [116; 204]	186 [162; 229]	-	0.08
Maximal heart rate (bpm)	150 [143; 161]	152 [138; 164]	160 [156; 172]	-	0.21
% predicted maximal heart rate (%)	92 [88; 95]	92 [87; 96]	94 [90; 98]	-	0.53
RER at peak exercise	1.32 [1.22; 1.38]	1.29 [1.22; 1.45]	1.25 [1.07; 1.38]	-	0.39
Peak VO <sub>2</sub> (mL/kg/min)	21.3 [16.4; 24.0]	27 [26.1; 27.6]	30.4 [30; 34.5]	-	< 0.0001
% age-predicted peak VO <sub>2</sub> (%)	79 [70; 93]	100 [76; 115]	102 [94; 105]	-	0.008
VE/VCO <sub>2</sub> slope	25.0 [24.8; 28.4]	23.4 [21.2; 26.4]	22.7 [20.0; 22.7]	-	0.002
MRI parameters					
Regurgitant volume (mL)	62.9 [40.8; 75.8]	43.0 [34.8; 59.9]	47.9 [36.4; 64.2]	-	0.56
Indexed LV mass (g/m <sup>2</sup> )	47.4 [43.1; 54.7]	50.6 [48.4; 55.6]	48.4 [44.5; 59.5]	49.0 [45.5; 54.9]	0.57
Indexed LVEDV (mL/m <sup>2</sup> )	101 [89; 114]	113 [99; 127]	122 [95; 144]	84 [75; 92]	< 0.0001
Indexed LVESV (mL/m <sup>2</sup> )	35 [30; 41]	41 [33; 49]	43 [35; 54]	34 [28; 38]	0.02
Indexed LV stroke volume (mL/m <sup>2</sup> )	67 [59; 70]	71 [65; 86]	69 [63; 88]	48 [42; 57]	< 0.0001
LVEF (%)	64 [60; 70]	64 [61; 68]	63 [57; 66]	60 [55; 67]	0.21
Indexed LA max volume (mL/m <sup>2</sup> )	59 [52; 71]	82 [62; 105]	70 [52; 81]	39 [34; 45]	< 0.0001
Indexed LA min volume (mL/m <sup>2</sup> )	31 [21; 39]	43 [30; 73]	35 [23; 40]	15 [14; 17]	< 0.0001
LAEF (%)	49 [47; 53]	48 [44; 60]	50 [47; 55]	60 [57; 63]	0.0001
LV circumferential strain (%)	-18.7 [-21.2; -18.2]	-19.5 [-23.1; -18.4]	- 18.5 [- 20.0; - 15.8]	-20.5 [-21.4; -18.3]	0.22
LV longitudinal strain (%)	-20.7 [-21.8; -19.0]	-21.0 [-23.1; -18.0]	- 18.9 [- 19.8; - 18.2]	-20.6 [-21.4; -18.5]	0.43
LA reservoir longitudinal strain (%)	25.7 [23.5; 31.0]	24.5 [15.2; 29.3]	24.1 [19.0; 27.1]	42.3 [36.5; 45.7]	< 0.0001
LA conduit longitudinal strain (%)	15.7 [11.4; 20.1]	15.3 [12.7; 18.5]	15.8 [11.1; 16.8]	21.6 [16.8; 24.4]	0.01
LA booster longitudinal strain (%)	12.1 [8.5; 13.5]	7.6 [3.8; 12.0]	8.9 [7.7; 10.8]	21.3 [18.0; 24.6]	< 0.0001
End-diastolic a angle (°)	84.5 [76.4; 92.5]	86.8 [83.2; 99.6]	99.0 [92.6; 108.5]	95.8 [92.8; 100.2]	0.004
End-diastolic γ angle (°)	45.5 [41.1; 51.9]	42.9 [37.2; 48.7]	37.7 [34.4; 40.5]	41.7 [40.3; 45.0]	0.01

**Table 1.** Patient and control characteristics, TTE, functional capacity parameters and MRI indices according to VO<sub>2</sub> tertiles. Values are shown as median [interquartile range]. Significant values are in bold. *BMI* body mass index, *LA* left atrium, *LV* left ventricle, *LVEDV* LV end-diastolic volume, *LVESV* LV end-systolic volume, *LVEF* LV ejection fraction, *LAEF* LA ejection fraction, *RER* respiratory exchange ratio, *TTE* transthoracic echocardiography, *TRV* tricuspid regurgitation velocity, *VE* minute ventilation, *VCO*<sub>2</sub> carbon dioxide production, *VTI* velocity–time integral, *VO*<sub>2</sub> oxygen consumption rate, *bpm* beats per minute.

Scientific Reports | (2024) 14:21429 |

at rest was gradually and significantly higher in patients with lower peak VO<sub>2</sub>, and increased during exercise at low and then peak levels in all 3 groups. Finally, as expected, % age- and sex-predicted peak VO<sub>2</sub> was significantly lower and VE/VCO<sub>2</sub> slope was significantly higher across groups as peak VO<sub>2</sub> decreased.

Indexed LV mass and LA volumes were higher in the second  $\dot{VO}_2$  group, but only indexed LA maximal volume reached significant difference across the 3 patient groups (p = 0.02). Indexed LV volumes increased gradually across VO<sub>2</sub> patient groups but such difference did not reach statistical significance (p  $\ge$  0.05). As per inclusion criteria, LV ejection fraction (LVEF) and LA ejection fraction (LAEF) lied within normal ranges in all groups, and LV and LA strains were equally distributed across VO<sub>2</sub> groups, except for a light drop in LA booster strain in the second group, which however did not reach statistical significance (p = 0.14). As expected, healthy volunteers had significantly lower LV and LA volumes, as well as higher LA ejection fraction and strains. Finally, regarding LA angle indices, a gradual increase in  $\alpha$  angle and decrease in  $\gamma$  angle were observed across groups, reaching statistical significance for all indices (p  $\le$  0.01). Of note, measurement of end-diastolic angle indices was reproducible, as reflected by high intraclass correlation coefficients = 0.81 for  $\alpha$  and = 0.78 for  $\gamma$ .

In univariate analyses, peak VO<sub>2</sub> and VE/VCO<sub>2</sub> slope were significantly correlated to TRV measured using TTE at rest (r = -0.41, p = 0.03 and r = 0.55, p = 0.004, respectively) and low exercise level (r = -0.44, p = 0.02 and r = 0.51, p = 0.009, respectively), but not at peak exercise level (p = 0.89 and p = 0.39, respectively). Importantly, while peak VO<sub>2</sub> and VE/VCO<sub>2</sub> slope were not significantly correlated to any of the MRI-derived LV and LA strain indices, they were significantly associated with angle indices (Fig. 2), resulting in overall stronger and higher associations with  $\alpha$  (r = 0.50, p = 0.003 and r = -0.52, p = 0.003, respectively) and with  $\gamma$  (r = -0.53, p = 0.002 and r = 0.52, p = 0.003, respectively). The following relationships obtained with TRV and angle indices were independent of age and sex: rest TRV (peak VO<sub>2</sub>:  $R^2 = 0.39$ , p = 0.007 and VE/VCO<sub>2</sub> slope:  $R^2 = 0.37$ , p = 0.02), low exercise TRV (peak VO<sub>2</sub>:  $R^2 = 0.31$ , p = 0.03), end-diastolic  $\alpha$  (peak VO<sub>2</sub>:  $R^2 = 0.45$ , p = 0.0008 and VE/VCO<sub>2</sub> slope:  $R^2 = 0.29$ , p = 0.03). Of note, among volume indices, the only significant correlates of peak VO<sub>2</sub> and VE/VCO<sub>2</sub> slope were LV volumes (indexed LV end-diastolic volume (LVEDV): r = 0.45, p = 0.009 and r = -0.49, p = 0.007, respectively;



**Fig. 2.** Linear regressions of peak VO<sub>2</sub> and VE/VCO<sub>2</sub> slope with end-diastolic angle indices. (a) End-diastolic LA  $\alpha$  angle. (b) End-diastolic LA  $\gamma$  angle.

indexed LV end-systolic volume (LVESV): r = 0.45, p = 0.01 and r = -0.51, p = 0.004, respectively; indexed LV stroke volume: r = 0.37, p = 0.04 and r = -0.37, p = 0.04, respectively). However, these associations were no longer significant after adjustment for sex and age. Finally, no significant relationship was obtained against % age- and sex-predicted peak VO<sub>2</sub>.

#### Discussion

In the present study, we proposed indices related to LA-mitral annulus angulation, which can be directly quantified from standard-of-care MRI cine images combined with feature-tracking which is commonly used to derive myocardial strain. We demonstrated in patients with asymptomatic primary MR and preserved LVEF, that peak  $VO_2$  and  $VE/VCO_2$  slope, which are standard measures of exercise capacity and ventilatory efficiency linked to prognosis<sup>25-28</sup>, were associated with angle indices, independently of age and gender. In contrast, peak  $VO_2$  and  $VE/VCO_2$  slope were not significantly correlated to any of the conventional LV and LA strain indices. An advantage of such mitral annulus angulation indices is that they do not require additional MRI scan or analysis time.

MRI strains in our study were in agreement with previous speckle tracking echocardiographic studies. Indeed, Mentias et al. and Alashi et al. reported LV longitudinal strain mean values of  $-21.5\pm2.0$  and  $-20.6\pm2\%$ , respectively, in patients with primary MR and preserved LVEF before surgery<sup>29,30</sup>. Yang et al. further studied 136 patients with severe primary MR and preserved LVEF, and found that LA peak reservoir strain was  $25.86\pm9.89\%^{31}$ , which is in line with our findings. Ahmed et al. measured LV strain rates of patients with severe MR using tagged MRI<sup>32</sup> but to the best of our knowledge, no studies previously investigated strain measurement using cine SSFP images in patients with primary MR. Indeed FT has been used in recent MRI studies rather to perform slice tracking and enhance mitral flow measurements in MR patients than to specifically evaluate strain<sup>33</sup>.

While there was a drop in LA strains in MR patients as compared to controls, LV strain values were in a normal range despite LV dilatation in our MR patients. Indeed, loading conditions which are affected by the large regurgitant volume in MR patients are associated with LV and LA enlargement. Such dilatation is compensated by mechanical adaptation of left heart chambers, according to Frank-Starling law<sup>34</sup>, maintaining a certain level of myocardial strains. This probably partially explains why strain was not a significant correlate of peak VO<sub>2</sub> and VE/VCO<sub>2</sub> slope in this study.

LV shape has been widely associated to exercise capacity<sup>35</sup>, beyond LV function<sup>36</sup>. This is in line with our findings, where LV volume was significantly associated to peak VO<sub>2</sub> and VE/VCO<sub>2</sub> slope. Such LV remodelling in asymptomatic MR patients was required to maintain sufficient stroke volume and reasonable exercise capacity. The newly proposed angle indices, which are driven by both LA geometry and mitral annulus shape and angulation, were found to be strongly and independently associated with exercise capacity-related peak VO<sub>2</sub>. Interestingly, LA to mitral annulus angles were further found to be significantly and independently correlated with VE/VCO<sub>2</sub> slope, which reflects ventilatory efficiency. Indeed, elevated VE/VCO<sub>2</sub> slope indicates abnormal ventilatory response to exercise, that could be explained by elevation of filling or pulmonary pressures, increase in dead space, and reduction of pulmonary flow. This parameter was previously found to be associated with clinical outcomes and prognosis in heart failure, hypertrophic cardiomyopathy<sup>37</sup>, and in valvular heart disease<sup>28,38</sup>. Such VE/VCO<sub>2</sub> slope-related findings are consistent with the revealed significant correlations with peak VO<sub>2</sub>.

Chronic severe MR induces volume overload that progressively leads to compensatory mechanisms from LA and LV, with a chronic remodelling process and enlargement of left cardiac chambers. Eventually, compensatory adaptation fails, leading to deleterious LA and LV dilatation and LV dysfunction. However, transition from a compensated remodelling to decompensated stage of MR remains unclear. LA and LV remodelling includes dilatation but also further changes in heart shape and geometry as well as myocardial and annulus stiffness, which may induce annular tilt in the course of cardiac cycle. LA to LV angulation indices, as assessed from Computed Tomographic Angiography, have been previously described as new markers of cardiac remodelling, and were found to be correlated with MR severity, suggesting that they could be a complementary parameter of cardiac remodelling in chronic MR<sup>15</sup>. In the current study, we proposed new LA to mitral annulus angulation from standardized MRI left heart views and automated myocardial tracking, which integrates both LA and LV dilatation and reshape, as well as changes in mitral annulus dimensions and angulation, which are important components in primary MR. Such remodelling-related angle indices might complement flow and volume indices for MR severity grading, and ultimately help distinguish compensated remodelling from decompensated stage and thus improve prognosis evaluation in chronic primary MR.

Systolic pulmonary artery pressure (SPAP) is an important parameter in chronic MR. Indeed, it has been found to be associated with prognosis, especially mortality after mitral surgery<sup>39</sup>. Exercise-induced pulmonary hypertension (ExPHT), which was notably demonstrated to predict cardiovascular outcome in chronic MR, is also a valuable parameter<sup>40</sup>. Since echocardiographic SPAP assessment during exercise can be challenging due to a loss in Doppler signal, peak TRV was recorded during our TTE protocols as an index of SPAP. We found that it was significantly and independently correlated to peak VO<sub>2</sub> both at rest and during low exercise, albeit to a lesser degree than our MRI angle indices.

Our study has some limitations. First, our population was small. However, it is well phenotyped, and our primary objective was to perform a head-to-head comparison between the newly proposed angle indices and conventional volumetric and strain parameters, in regard to patients exercise capacity. Also, this was a cross-sectional study thus we did not have any follow-up data to assess the prognostic value of our new angle indices, as well as their additive performance to SPAP or ExPHT evaluations. In addition, the fact that our LA-mitral annulus angles are measured from 2-dimensional images, which are further centred on the left ventricle, could be viewed as a limitation. However, in a generalizability purpose, our goal was to propose indices readily available from conventional and highly standardized cine images that are acquired during any cardiac MRI protocol. Associations of angle indices with VO<sub>2</sub> and VE/VCO<sub>2</sub> slope attest on the consistency of our measures. To date,

there is no 3D + t cine MRI sequence easily usable in clinical routine to afford 3D angles estimation, hence we designed our study rational based on existing standardized sequences. The emergence of such sequences in the near future will strengthen true angle estimates. Exercise TTE and MRI assessments were not performed on the same day. Indeed, our data were collected within a real-life setting in the course of clinical routine protocols, where TTE was performed first and MRI was achieved while considering pragmatic constraints, allowing a maximal interval of around 6 months. We did our best all along inclusions to ensure that both examinations were carried out within the shortest interval, and more than half of patients underwent these explorations within the same month. Slow progression of symptoms and LV remodelling in asymptomatic chronic primary MR was previously reported<sup>41</sup>. Finally, we chose not to exclude patients with AF since such condition is frequently encountered in primary MR. Although cine MRI and echocardiography can be more challenging in case of AF, such explorations remain fully interpretable and validated for MR evaluation. Indeed, most echocardiographic standardized methods to assess MR severity including EROA, which is considered as the most robust quantitative method, are not influenced by the presence of AF<sup>42</sup>. Beta blockers can alternately be used before the MRI exam in case of patients with rapid ventricular rate to optimize image quality.

#### Conclusion

This study shows that new LA to mitral annulus angulation parameters, which were computed directly from available feature tracking-derived contours on standard-of-care MRI cine images, showed stronger, significant and independent associations with exercise capacity in patients with asymptomatic primary MR and preserved LVEF than commonly used parameters of cardiac function. Therefore, these parameters, which are driven by both annulus size and orientation as well as LA geometry, might complement existing flow and geometry parameters in MR severity grading.

#### Data availability

The datasets used and/or analysed during the current study are available from the corresponding author on reasonable request.

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#### Author contributions

All authors contributed significantly to this manuscript. All authors: manuscript drafting or manuscript revision for important intellectual content. All authors: approval of final version of submitted manuscript. All authors: literature research. PM, TW, MG, EB, EC, AR, NH, NK: study concepts/study design or data acquisition or data and statistical analysis or findings interpretation. PM, MG, JL, VN, NK: software design for quantification and analysis.

#### **Competing interests**

The authors declare no competing interests.

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