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Main Manuscript for

Silicon chambers for enhanced incubation and imaging of microfluidic droplets

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Author Contributions:

N.L.D. designed the chambers, fabricated them and tested them. R.D built and tested the thermal control platform. N.L.D. & RD performed experiments, and analyzed the data. G.G performed the digital assay and analyzed the data. A.B provided support on the biochemical reactions and advice on initial chamber designs. B.N.H. and S.O tested the chamber and gave feedback to improve it. G.M. worked on the chamber sealing to reach high temperatures. S.Q. and D.B. scaled and characterized the process to 6 inch wafers. M.D. assisted with the design of the thermal control platform. L.J, S.H.K, H.F, Y.R. and H.T provided advice for the design and fabrication. T.F and A.J.G supervised the research.

Abstract

Droplet microfluidics has become a powerful tool in life sciences, underlying digital assays, single-cell sequencing or directed evolution, and it is making foray in physical sciences as well. Imaging and incubation of droplets are crucial, yet they are encumbered by the poor optical, thermal and mechanical properties of PDMS, a material commonly used in microfluidics labs. Here we show that Si is an ideal material for droplet chambers. Si chambers pack droplets in a crystalline and immobile monolayer, are immune to evaporation or sagging, boost the number of collected photons, and tightly control the temperature field sensed by droplets. We use the mechanical and optical benefits of Si chambers to image ≈ 1 million of droplets from a multiplexed digital assay - with an acquisition rate similar to the best in-line methods. Lastly, we demonstrate their applicability with a demanding assay that maps the thermal dependence of Michaelis-Menten constants with an array of $\approx 150,000$ droplets. The design of the Si chambers is streamlined to avoid complicated fabrication and improve reproducibility, which makes Si a complementary material to PDMS in the toolbox of droplet microfluidics.

Introduction

In the past decade, emulsions of droplets have enabled groundbreaking advances in life sciences. Their massive generation rate ($\approx 100\text{Hz}-10\text{MHz}^{1,2}$), their monodispersity (a few %) and their minute volume ($\approx 1-1000$ pL) make droplets ideal reactors for applications that need high-throughput, low consumption of reagents and quantitiveness. Droplet microfluidics has become routine in single-cell analysis³⁻⁶, digital Polymerase Chain Reaction (PCR)⁷⁻⁹ or directed evolutions¹⁰⁻¹⁴, where it is used to digitally encapsulate oligonucleotides, plasmids or cells. Droplets are also finding applications in other fields, ranging from chemical synthesis^{2,15,16} and nonlinear chemistry¹⁷⁻²⁰, enzymology¹⁴, drug screening²¹ and toxicology²², to microbiology²³, cell biology, and tissue engineering²⁴. In recent years, the use of droplets has even extended to study the physics of crystallization, phase separation, gelation and colloidal aggregation²⁵⁻²⁷.

In typical end-point assays (e.g. digital assays), droplets are first generated in a Polydimethylsiloxane (PDMS), chip, incubated in a controlled temperature profile off-chip (e.g. in thermocycler), and then interrogated with a dedicated device. In other applications, timing is important and droplets must be continuously imaged while incubated (time lapse imaging) - for instance to monitor cellular growth or gene expression²⁸. Lastly, some advanced applications call for both temporal *and* thermal resolution - for instance in enzymology, directed evolution, phase separation, or colloidal self-assembly - where kinetics and temperature are tightly linked.

However, it remains challenging to continuously image a large population of droplets, even more so when their temperature must be controlled. In-line methods (e.g. droplets cytometry^{29,7,30,31}) circulate droplets inside a channel and read their fluorescence with detectors located at fixed positions in the channel. In-line methods offer a high throughput but with few time points and over a short duration³². They are limited by the residency time of droplets in the channel. They also lack morphological information about the content of the droplets, are difficult to set up and multiplex in several fluorescent channels, and are hardly compatible with temperature-resolved measurements where each droplet experiences a different temperature. On the other hand, large field of view imaging works the opposite way: droplets are immobilized in a chamber and scanned by a moving microscope stage. Large field of view imaging brings significant advantages. First, it is

easy to set up and automatize: commercial fluorescence microscopes can automatically scan a droplet array in several channels with limited hands-on time. Secondly, it is thermally, spatially, and temporally resolved: each droplet can be kept at a constant and distinct temperature (when placed in a temperature gradient), and repeatedly imaged with a spatial resolution of $\approx 1\text{-}10\ \mu\text{m}$ and a time resolution ranging from ms to min or h. Lastly, large field of view imaging also offers a high-throughput thanks to the large surface of Complementary Metal–Oxide–Semiconductor (CMOS) cameras, which capture tens of thousands of droplets in a single field of view. Indeed, manufacturers of microscope have been pushing toward larger and larger field of view, spurred by the demands from biologists who need to image large organisms or complex systems. But the benefit of microscopes with large field of view imaging cannot be realized without cameras with large sensors to avoid any resolution loss.

The microfluidics community has designed a variety of droplet chambers to maximize the benefit of large field of view imaging. While some chambers have been realized in materials like glass^{18,33} or Poly(methyl methacrylate) (PMMA)³⁴, most have been made from PDMS, the standard material for prototyping in academic microfluidics. Starting with the DropSpot array in 2009, droplet chambers made of PDMS have been reported for application in digital PCR, live-cell imaging, screening of biomolecules, molecular diagnostics or microbiology^{28,35–42,24,43–46}.

While these PDMS chambers enabled groundbreaking studies, they kept running into the same limitations of PDMS. First, PDMS is not mechanically rigid, which makes it difficult to fabricate large freestanding chambers because they collapse under their own weight. This was addressed by adding supporting structures like pillars^{36,47}, but at the cost of reducing the filling factor, which often falls short of the maximal packing density of droplets ($\approx 90\%$ in 2D). Secondly, the poor thermal conduction of PDMS makes it delicate to control the temperature field sensed by the droplets. Thirdly, PDMS expands upon heating and is not airtight, which causes evaporation and displacements of droplets during incubation. Lastly, the autofluorescence of PDMS degrades the optical signal, especially when the droplets must be imaged through the PDMS slab.

The ideal droplet chamber should meet stringent mechanical, thermal, optical and storage criteria. The chamber should maximize the packing density of droplets. It should be mechanically robust and airtight to prevent the compression, stacking, displacement or evaporation of droplets, and should not thermally expand when heated. The chamber should be wide enough to store millions of droplets across its surface, but be sufficiently thin and flat to hold only a single droplet across its depth - which imposes an extreme form factor and requires mechanical rigidity. The ideal chamber should be highly thermally conductive to keep the temperature locally uniform and quickly transmit temperature jumps to the droplets (like in PCR cycling). Lastly the chamber should not autofluoresce.

We reasoned that Si - a crystalline material - would make better droplet chambers than PDMS - an elastomer - because it is more mechanically rigid, more thermally conductive, more reflective and less permeable to water vapor (Table S1). The surface of Si is flat, and easy to micro pattern and modify, for instance to tune wettability^{48,49}. Those benefits have led Si to be used as substrate for industrial DNA synthesis⁵⁰. Digital PCR in arrays of Si microchambers (where the PCR reaction is directly done in a micrometric Si chamber

rather than in droplets) has been demonstrated – highlighting the good thermal performance of Si^{51,52}.

Yet PDMS has largely been preferred to Si for microfluidic devices due to the (perceived) complexity of Si processing. Firstly, Si chips must be processed in a cleanroom and cannot be replicated from a master mold like PDMS chips. Secondly, bonding Si chips to glass (e.g. anodic bonding) and connecting them to the outside world, by drilling or back-etching access ports, is undeniably more complex and expensive than for PDMS chips, which just needs punching and tubing. While those points apply to classical microfluidic Si devices (e.g. for generating droplets), we reasoned that they would not necessarily apply to Si devices for storing droplets. If the design of Si chambers could be streamlined to remove complicated processes (bonding, drilling and back etching), then Si could become a competitive alternative to PDMS. Here we report Si droplet chambers for the imaging and incubation of droplets. The Si chambers enjoy superb mechanical, optical and thermal properties - making them ideal for imaging digital assays and time-resolved thermal studies of biosystems.

Results

Fabrication and filling

The design of the chamber is shown in Fig. 1. A chamber is made of a square or rectangular recess in a Si wafer, surrounded by short inlet and outlet channels for filling, and covered by a coverslip. The depth of the chamber matches the diameter of the droplets - forcing them to spread into a monolayer. This monolayer corresponds to a compact arrangement of droplets in a single plane. The Si block is noticeably thinner (≈ 0.5 -1mm) than a PDMS slab (≈ 1 -5 cm), while being more thermally conductive and mechanically rigid.

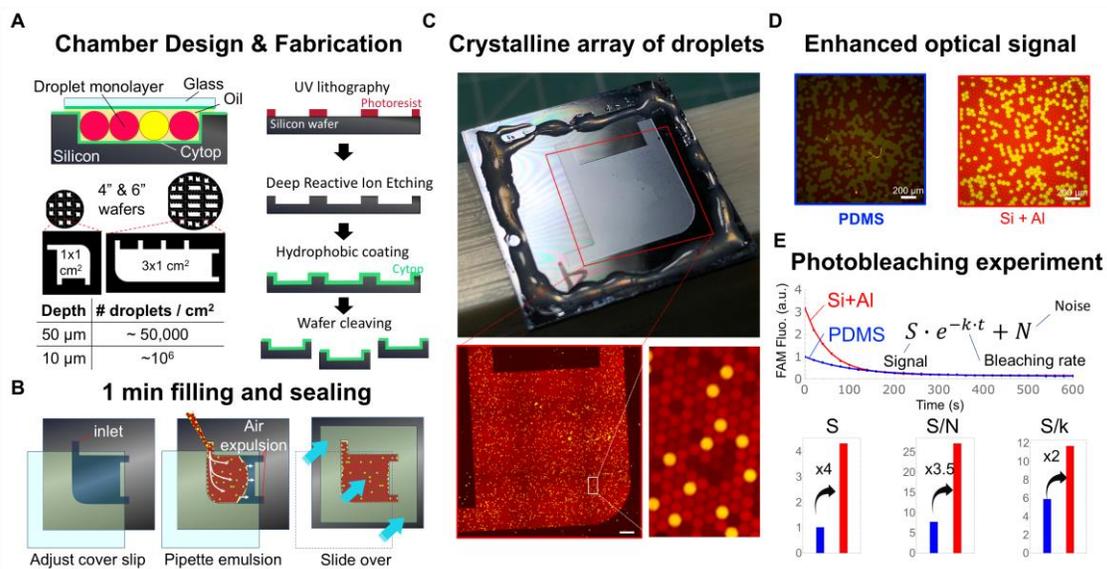


Figure 1: Fabrication, filling and optical observation of Si droplets chambers. **A**, Fabrication. The chambers are fabricated by standard processing in the clean room. The depth of the chamber is tightly controlled by the etching time. After fabrication, the chambers are cut out by breaking the wafer along its crystal planes, or by slicing the wafer. **B**, Filling (Extended Video 1). The chamber is covered with a coverslip, and filled from one of the inlets, forcing air out of the chamber. After filling the chamber is closed either by capillary forces, or with epoxy glue **C**, Chamber after filling and sealing with glue (Extended Image 1). The chamber contains $\approx 50,000$ droplets that are organized in macroscopic crystalline domains. **D**, Optical enhancement. An emulsion of droplets containing Rhodamine, alexa 647 and FITC dextrans was imaged under identical conditions in a Si/Al chamber and a PDMS chamber for reference. **E**, Prolonged illumination bleaches FITC, yielding the optical background (N), the bleaching rate (k), and the optical signal (S). From this, we extract the signal-to-noise ratio (S/N), as well as the total number of photons collected (S/k, expressed in arbitrary units).

The Si chambers were fabricated with a streamlined process: spin-coating of the resist, UV exposure, resist development, deep reactive ion etching, and wafer slicing. Note that those steps can be automated in a modern cleanroom. Since the chamber does not contain micrometric features in the xy plane, a chrome mask was unnecessary and we used an inexpensive plastic film as a mask for prototyping. Complex processing, like mask alignment, anodic bonding, back-etching or drilling, was not needed either. Overall, we fit ≈ 30 chambers of 1 cm^2 on a 6" inch wafer, which brings the fabrication cost of a single chamber to $\approx 5\text{-}10\text{€}$ in an academic cleanroom (including wafer cost and processing time).

The depth of the chamber - controlled by the etching time - is highly uniform despite the extreme form factor of the chamber ($\approx 200\text{-}1000$). We profiled the depth of a dozen of chambers distributed along the diameter of a 6-inch wafer (Table S2). For a nominal depth of $50 \text{ }\mu\text{m}$, the measured depth at the center of each chamber is close to the nominal depth, and varies little between chambers: $(49.6 \pm 2.1) \text{ }\mu\text{m}$. Inside a chamber, the depth displays a slightly concave profile with a trenching on the edges. The depth deviates by $\approx 3 \text{ }\mu\text{m}$ on average between the center and the edge of the chamber, which represents $\approx 6\%$ of the nominal depth ($50 \text{ }\mu\text{m}$) and 0.03% of the length of the chamber (1 cm). (Results are similar for the $10 \text{ }\mu\text{m}$ chambers, Table S2).

The uniformity of depth and the mechanical rigidity of Si ensures that droplets do not form a bilayer during filling, and that they do not get compressed or dislodged during incubation. It would be almost impossible to get the same uniformity and mechanical rigidity from a free-standing PDMS chamber. PDMS is an elastomer that notoriously sags under its own weight, which makes the fabrication of PDMS structures with a large aspect ratio difficult⁵³. Even with supporting structures like pillars to prevent the deformation or collapse of the chamber, the depth profile of a PDMS chamber is still determined by the thickness profile of the SU8 master, which is hard to uniformize because it is governed by spin-coating, and problems like edge beads, striations, dusts, and air bubbles are common occurrence in spin-coating that impact the uniformity of thickness.

Filling and sealing

Filling and sealing the chamber are fast and reliable. Filling does not need specialized equipment (such as a pressure pump), but rather relies on physical forces that pack the emulsion into a crystalline monolayer of droplets. It is very similar to glass-hemocytometers often used for imaging. First, a coverslip is laid on top of the chamber

(both coated with a hydrophobic polymer), leaving the inlet and outlets open. The water-in-oil droplet emulsion is then pipetted in the chamber through the inlet. The emulsion fills the chamber by capillarity, expelling air through the outlets. The corner opposite the inlet and outlets is rounded to prevent air bubbles from stagnating. After filling, the coverslip is gently slid over the Si block to cover and close the inlet and outlets. This sliding is facilitated by the oil lubrication layer and the flatness of the top Si surface that is in contact with the coverslip. This surface is not etched and corresponds to the original Si wafer surface which is extremely flat. The chamber is then sealed, either by capillarity (by leaving a film of oil around the chamber), or by gluing the edges of the coverslips to the Si block. Capillary closing is sufficient for incubating the array at moderate temperatures ($<60^{\circ}\text{C}$), and allows for retrieval of the droplet arrays. Glue improves the air tightness and mechanical stability when chambers are heated at high temperatures ($\approx 60\text{-}80^{\circ}\text{C}$, vide supra), but makes retrieval more involved. The filling and sealing procedure takes 1 min and is presented in detail in the Extended Video 1. Additional time is required if glue is used, mostly to let the glue dry.

Although filling is simple, it is remarkably efficient. The droplets self-organize into a crystalline monolayer whose large domains can be directly seen with the naked eye (Fig. 1C). Under the microscope, the droplets are packed into a honeycomb lattice, an arrangement which maximizes storage density. There are few visible air bubbles (a common issue in droplets microfluidics), and the droplet arrays remain hydrated at room temperature for days or weeks, without signs of coalescence. The simplicity of filling and sealing contrasts with the usual practice for connecting Si chips to the real world, which is to etch or drill the back of the wafer to open access ports for filling, and to seal the device with anodic bonding⁵⁴. Back etching is more time-consuming than front etching because the whole wafer must be etched through ($\approx 0.5\text{-}1\text{ mm}$ vs $50\text{ }\mu\text{m}$). In addition, anodic bonding requires clean and flat surfaces, high temperatures and large voltages, which complicates fabrication and increases the likelihood of failed devices. Tubing is not necessary either, which further simplifies operation.

Optical enhancement

While Si chambers block transmitted light, their superb optical properties make them ideal for epifluorescence imaging - the readout modality for the vast majority of droplet assays. Note that if brightfield imaging is needed, it would need to be conducted in reflected mode rather than transmission mode.

First, Si chambers are mechanically rigid and can be sealed with a thin coverslip of standard thickness ($\approx 170\text{ }\mu\text{m}$) - making the chambers compatible with the vast majority of objectives (Figure S1). By contrast, PDMS devices are not rigid and are usually sealed with a thick ($\approx 1\text{ mm}$) glass slide for bonding and handling. But this millimetric thickness causes optical aberrations (most objectives correct aberrations for a thickness $\approx 170\text{ }\mu\text{m}$) and imposes a long working distance - excluding lenses with a high numerical aperture and reducing resolution and brightness (Figure S1). However, a good numerical aperture is necessary to resolve the content of droplets, for instance to monitor inhomogeneous processes, like polymerization, jellification or phase separation. These kinds of measurements need to spatially resolve the content of the droplet on the microscale, which mandates a short working distance and high numerical aperture.

In addition, we hypothesized that the flat and reflective surface of the Si chamber enhances the optical signal by acting as a mirror⁵⁵. The reflectivity of Si is $\approx 40\%$ (in the 400-600 nm wavelength range), and increases to almost 100% with the coating of aluminum. Aluminum coating is a simple clean room process that can be performed on several wafers at once. Assuming a perfect reflection from the surface, the flux of excitation photons coming from the objective and exciting the droplets is doubled, and the flux of photons emitted by the droplets and collected by the objective is also doubled, resulting in 4-fold enhancement of brightness (Figure S2). Noting that in epifluorescence microscopy the brightness of the sample scales typically like the 4th power of the numerical aperture⁵⁶, this 4-fold enhancement is equivalent to increasing the numerical aperture of the objective by 40%. (e.g. collecting the light of a hypothetical 40X NA=0.55 objective while benefitting from the field of view of a 20X NA=0.4 objective).

We tested these assumptions by comparing the optical properties of a PDMS chamber and an Al-coated Si chamber. To focus on comparing their constitutive materials we used PDMS chambers with the same geometry as the Al-coated Si chamber. We prepared an emulsion of identical droplets containing Dextran molecules conjugated to FITC fluorophores (a dye with fast photobleaching). After spreading the droplets in their respective chambers, we illuminated and imaged each chamber under identical conditions (Fig. 1D). As expected, the Al/Si chamber quadruples the photon flux S (as measured by the initial average fluorescence), and doubles the bleaching rate k , which overall doubles the number of photons S/k collected from the dyes over their lifetime. We were concerned that the fluorescence background could have been large because the excitation light is reflected back to the objective by the Si surface. While this light is filtered out by the dichroic mirror and the emission filter, even a small leak could result in an overwhelming background. However, this turns out not to be a cause for concern, and the background N of the Si/Al chamber is only slightly worse ($\approx 20\%$) than in PDMS chambers. Overall, the Si/Al chamber has an optical signal-to-noise ratio ≈ 3 fold larger than for PDMS chambers. This optical enhancement shortens the acquisition time and reduces illumination power, allowing to scan more droplets in a given time and to reduce phototoxicity. It also boosts the apparent numerical aperture of the objective, which improves resolution⁵⁵. This could improve the imaging of fine structures inside droplets, for instance to distinguish the morphology of cells or colloidal aggregates²⁷.

Imaging of a digital assay

We then exploited the mechanical rigidity and optical enhancement of the Si chamber to quickly image a large array of droplets from a digital assay, one of the major applications of droplet microfluidics^{8,9,36,57}. The turnaround time, limit of detection and dynamic range of a digital assay are directly related to the size and number of droplets imaged. Small droplets ($\approx 10 \mu\text{m}$) yield quicker reactions (by raising the effective concentration of a single molecule) and digitalization through Poisson encapsulation, while large populations of droplets ($\approx 10^4$ - 10^5) give a wider dynamic range and a lower limit of detection.

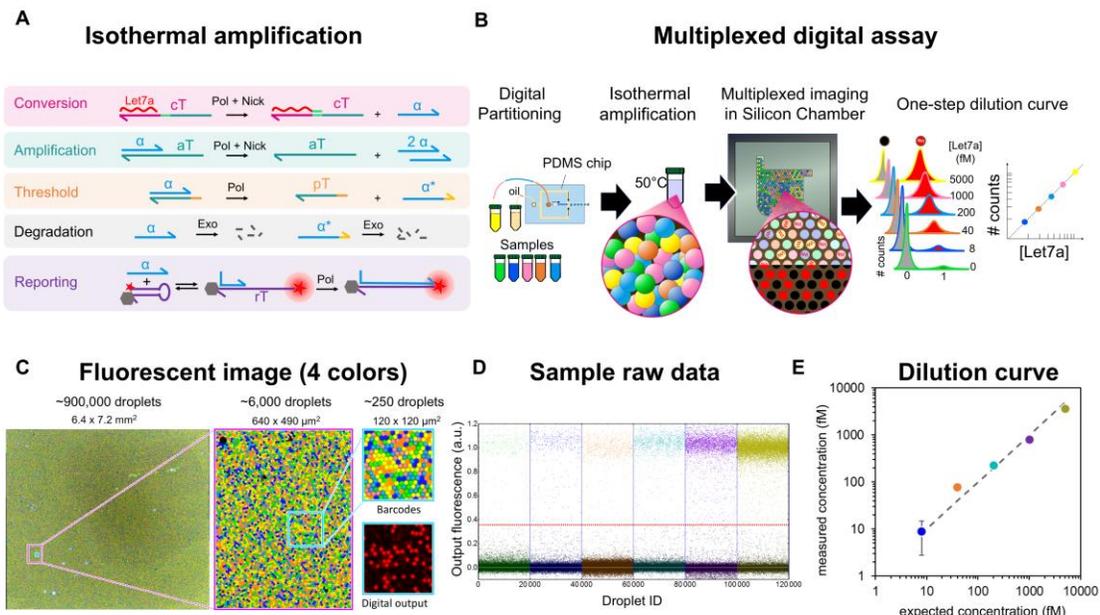


Figure 2: Imaging of a multiplexed digital assay with the Si chambers. **A**, Schematic of the isothermal assay. It comprises five molecular modules that exponentially amplify a target (*Let7a* miRNA) and report a molecular signal. **B**, Workflow. The isothermal assay is first digitally partitioned into droplets (*i.e* droplets contain either 0 or 1 strand of *Let7a*). We use a sample-changer to multiplex the assay and generate populations of droplets with varying dilution rates. After amplification, the droplets are arrayed in a Si chamber and imaged with multicolor fluorescence microscopy, which after processing yields the dilution curve of the digital assay. **C**, Raw image of the ≈ 1 million droplets array (Extended Image 2). Three colors encode the dilution rate of the droplet, and one colour reports the presence or absence of a *Let7* strand. **D**, For each dilution rate, we plotted the output fluorescence of $\approx 20,000$ randomly chosen droplets. **E**, Dilution curve plotting the measured concentration of *Let7* against its expected concentration, for $\approx 500,000$ droplets that passed quality filters. The error bars (only visible for the most diluted sample) show the standard deviation on the concentration measurement.

We used a Si chamber to image a multiplexed population of droplets (≈ 1 million of $10 \mu\text{m}$ droplets), and capture in a single run the dilution curve of an isothermal digital assay for microRNA quantification⁵⁷. The whole chamber with $\approx 900,000$ droplets was imaged in 4 fluorescent channels in about ≈ 25 minutes - an average acquisition time of $\approx 420 \mu\text{s}/\text{droplet}/\text{fluorescent channel}$. Although acquisition was not optimized (most of the acquisition time was spent by the software on focusing), this throughput compares favorably with some of the fastest reported throughput in droplet cytometry ($\approx 500 \mu\text{s}/\text{droplet}/\text{fluorescent channel}$)^{29,31}. The hands-on time (filling of the chamber and setting up of acquisition) was ≈ 10 minutes, which again compares favorably with droplet cytometry (which can take much longer to set up and run). However, we noted that filling the Si chamber with $10 \mu\text{m}$ droplets was slightly more difficult than with $50 \mu\text{m}$ droplets, which is likely due to the increased resistance in very thin layers of fluid.

Thermal enhancement

We exploited the thermal properties of the Si chambers for high-throughput enzymology. In molecular diagnosis and enzymology, a deviation of a few degrees from the designed temperature can change the enzymatic activity and alter the validity of the results⁵⁸. Yet droplets are often incubated in materials that are poor thermal conductors: mostly PMMA or Polypropylene (PP) when droplets are incubated off-chip in PCR tubes, or PDMS and glass when they are incubated on-chip.

Si chambers enjoy excellent thermal properties by virtue of their high thermal diffusivity ($D \approx 90 \text{ mm}^2/\text{s}$), which is on par with copper ($\approx 111 \text{ mm}^2/\text{s}$), ≈ 300 fold larger than glass ($\approx 0.34 \text{ mm}^2/\text{s}$), and ≈ 1000 larger than PDMS, PP or PMMA ($\approx 0.10 \text{ mm}^2/\text{s}$). In addition to being an excellent thermal conductor, Si has other advantages over PDMS for prolonged heating: it expands minimally when heated and has a low gas permeability (a common cause of evaporation in PDMS chambers).

A chamber with high thermal diffusivity improves the incubation of droplets. Thermal diffusivity of a material has unit of m^2/s , and thus it gives an intuitive measure of how the length scale and time scale of thermal diffusion are linked. First, thermal diffusivity reduces the bias between the temperature set by the heater and the actual temperature felt by the droplets, which can reach $\Delta T = 0.75^\circ\text{C}$ for a glass slide (Supplementary Information). Secondly, it shortens the time for thermal equilibration. The timescale τ to equilibrate temperature over a thickness of L is $\tau \approx L^2/D$. For $L = 1 \text{ mm}$, $\tau \approx 10 \text{ ms}$ for Si, but on the order of $\tau \approx 10 \text{ s}$ for material like PDMS or polypropylene. This timescale is matched by measurements of equilibration time in PCR tubes⁵⁹. Lastly, a good thermal conductor maintains a uniform temperature over the droplet array by smoothing out local sources or sinks of temperature (air pockets between the heater and the chamber, air convection in the room, air bubbles in the array, dust, local heating by the objective light and else). According to the steady-state heat equation, the contribution of a heat source to the temperature field T is attenuated in the Fourier space by a factor of Dk^2 (where k is the spatial frequency). So, Si attenuates spatial inhomogeneities on a length scale ≈ 30 times larger than PDMS.

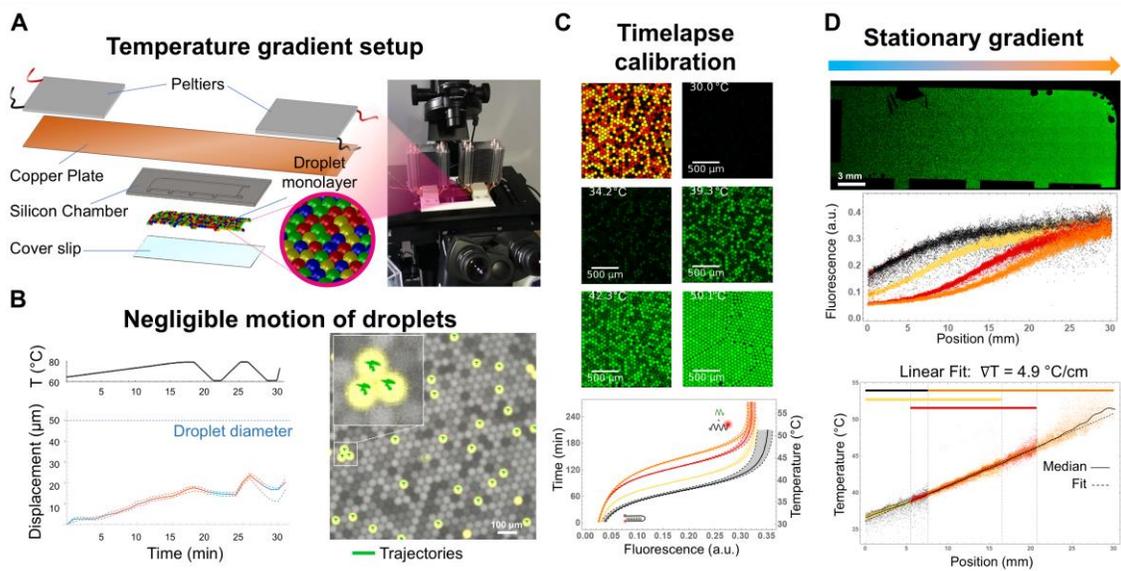


Figure 3. Thermal setup. **A**, Exploded view of the thermal setup. To gain control over the temperature field, we placed the Si chamber against a copper plate which is heated by two independent Peltier elements. The setup is encased in a 3D printed frame, and set inside the stage of the microscope. **B**, We measured the stability of the droplets array upon repeated temperature cycling between 60°C and 80°C (top plot). The yellow droplets are fiduciary droplets (see Extended video 2), and the green curves show their individual trajectories during heating and cooling (summarized in the bottom plot). **C**, Calibration of temperature measurements. We measured the temperature of droplets *in situ* with DNA thermometers, which are DNA nanostructures whose fluorescence responds nonlinearly to temperature. Each DNA thermometer maps temperature in a distinct range. We slowly heated an array of droplets with 4 distinct DNA thermometers and recorded the resulting fluorescence. **D**, *In situ* mapping of the temperature gradient. We placed an array of droplets with DNA thermometers in a stationary temperature gradient at 5°C/cm. Mapping fluorescence back to temperature reveals the temperature field in the droplets.

In order to fully exploit the thermal benefit of Si, we set up a thermal platform⁶⁰ (Fig.3A) - which we operated in two temperature regimes (uniform or gradient). In the first regime, the temperature is uniform in space (the same temperature is imposed to both Peltier elements), and either kept constant in time (for incubation) or varied in time between room temperature and ≈ 80 °C (*e.g.* to establish the melting curves of DNA strands). In the second regime, we established a stationary spatial gradient of temperature (by setting one Peltier element slightly above the room temperature and the other between 60 and 65 °C). In both cases, the temperature measured by the Pt100 sensors fluctuated by less than ≈ 0.015 °C over the course of ≈ 10 minutes (Figure S3). We also mapped the spatial profile of temperature actually sensed by the droplets with *in situ* DNA thermometers^{51,59}. We measure a linear temperature gradient of 4.9 °C/cm, close to the nominal gradient imposed by the Peltier elements (5 °C/cm). This confirms that thermal losses are negligible as Si faithfully transmits the temperature field from the copper plate to the droplet array.

We tested the stability of an array of droplets to repeated temperature cycling. Given the large size of the droplets (~ 50 μm), Brownian motion exists, but it is not likely to play a major role. Convective flows are the main culprits, and they are caused by undesirable

events such as evaporation or thermal expansion. It is usually challenging to maintain the spatial integrity of a droplets array in PDMS upon heating because it is often accompanied by dislocation, merging or local evaporation of the droplets. This is due to the unfavorable properties of PDMS (thermal expansion and porosity) that cause movement and evaporation of the array. We observed that large movements of droplets nucleates coalescence and forces merging of droplets through Ostwald ripening⁶¹. The merging of few droplets give birth to a large droplet, which coalesces with smaller droplets nearby (because it lowers the overall surface), eventually leading to the merging of a large part of the droplet array. Since Si prevents evaporation and severe movement of droplets, we find in practice that it also leads to much less coalescence of droplets. Evaporation in PDMS devices is usually addressed with fixes such as a vapor barrier (i.e., a glass slide embedded in the PDMS slab) or water tanks (hydrated channels running around the water chamber²⁸), but those fixes complicate the fabrication and operation of the chamber.

In our heating experiment, we repeatedly cycled the Si chamber between 60°C and 80°C, and tracked the fiduciary droplets that register the local displacement of the droplet arrays (yellow in Fig. 3B). Satisfyingly, the vast majority of the droplets remain neatly packed and immobile during temperature cycling - in spite of the growth of a gas bubble near one of the outlets (see Extended video 2). The average displacement of fiduciary droplets is well below one droplet diameter (Fig. 3B), which we attribute to the mechanical rigidity of Si as it is ≈ 1000 times less susceptible to thermal expansion than PDMS (Table S1). Si is also less permeable than PDMS to gas, and thus less susceptible to evaporation. The temperature stability of the chamber could be further improved by degassing the oil solution and emulsion before incubation.

Enzymology

Lastly, we combine these properties (high-throughput and controlled temperature field) to measure *en masse* the temperature dependence of an enzymatic process - a fine-grained enzymology study which would have been difficult by other means. As a proof-of-principle, we measured the Michaelis-Menten curves for the enzymatic conversion step in our digital assay (Fig. 2A). In this step, a substrate (the input DNA strand) binds to a DNA template, which triggers its extension by a polymerase, and then nicking by nickase, releasing an output DNA strand. Although conversion is a two-step enzymatic process, it can be approximated as an apparent one-step process with the Michaelis-Menten equation. To map this dependence, we prepared with microfluidic scanning droplets with varying concentrations of the input DNA, keeping other reagents at a fixed concentration across the droplets^{17,18}. We arrayed the droplets in a long Si chamber (3 cm x 1 cm, amounting to $\approx 150,000$ droplets), placed them in a thermal gradient and imaged in time-lapse mode (Extended Video 3). After imaging, we binned the droplets by temperature, and for each bin we constructed the Michaelis-Menten curve relating the speed of the conversion reaction to the concentration of substrate. These curves yield for each temperature the apparent V_{\max} (maximum production speed at full saturation of substrate) and K_M (concentration of input to reach $V_{\max}/2$). The velocity V_{\max} is not monotonic with temperature and peaks around ≈ 47 °C. The K_M constant is well fitted by a Boltzmann law (Figure S4), suggesting that it is determined by a thermodynamically reversible process: the binding of the input DNA to the template. Those observation results would have been difficult with a low throughput process (such as bulk measurement in thermocycler), where only a few temperatures and only a few concentrations per temperature are tested.

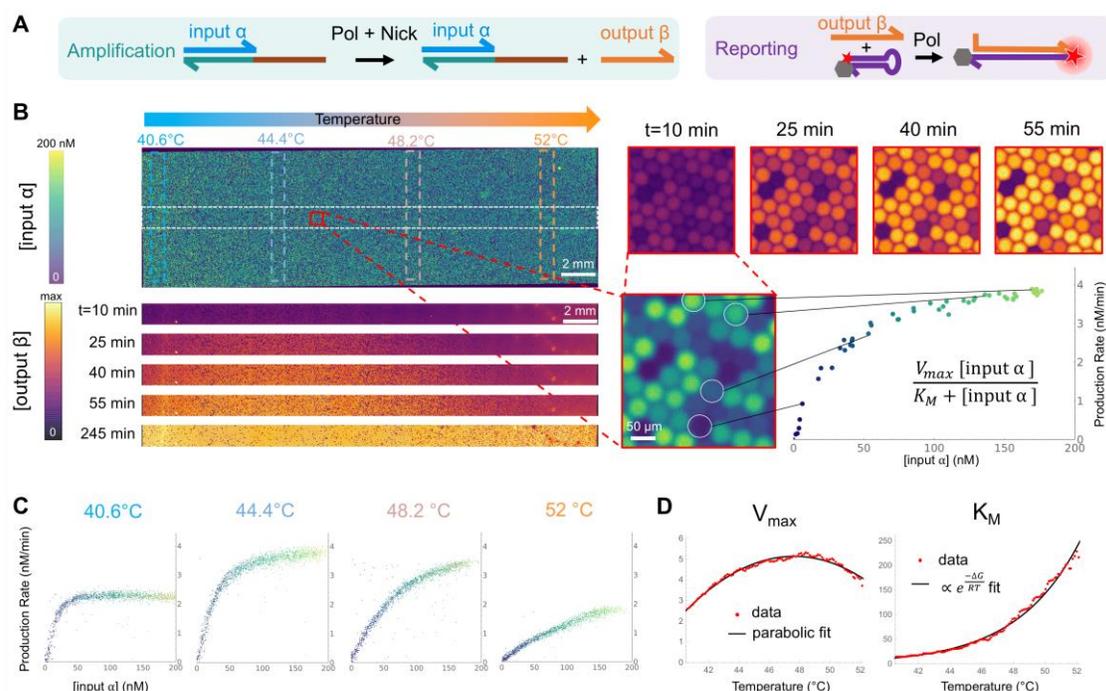


Figure 4. *En masse* thermal mapping of Michaelis-Menten constants. **A**, Enzymatic process studied. An input strand α (the substrate) binds to a DNA template, is elongated by a polymerase and nicked by nickase, releasing a strand (the product). The process is monitored by a separate reporter. **B**, Droplets with varying concentrations of α were prepared and arrayed in a Si chamber. The top image shows the array of droplets in the barcode channel (which is proportional to the concentrations of α). The bottom strips show the time evolution of the reporter's fluorescence (Extended Video 3). The right side shows how a Michaelis-Menten curve is constructed. Each point corresponds to the derivative of the β fluorescence in a single droplet. **C**, Michaelis-Menten plots for various temperatures. The plot shows the production rate of β against the concentration of α . **D** Plots of Michaelis-Menten constant V_{max} and K_M for varying temperatures, extracted from the Michaelis-Menten plots (each data point in red corresponding to ≈ 1000 droplets).

Discussion

We have shown that Si is an ideal microfluidic material for imaging and incubating droplets. The standardized fabrication process enhances reproducibility, as each chamber is made with precise and reproducible specifications. The chambers are simple to operate and do not require specialized equipment. Their filling shares a lot of similarities with commonly used glass-hemocytometers but the sealing of Si chambers avoids evaporation, even when incubated in the 50-80 °C temperature range which makes them superior for time-lapse imaging. Lastly, they boast better optical, mechanical, thermal and storage performance than PDMS or glass chambers. This makes Si chambers ideal for experiments that mandate continuous imaging of many immobile droplets in a graded temperature field, for instance for high-throughput enzymology⁶².

We foresee various applications for the Si chambers in the life sciences: for real-time digital assays, directed evolution of enzymes, or live-cell imaging (thanks to their reduced phototoxicity, although long term incubation would be difficult due to the limited porosity to gases). The chambers could also benefit the physical sciences to map the phase diagram (temperature, concentration) of the many processes that can be followed with optical microscopy such as colloidal self-assembly, phase separation, gelation, coacervate, solubility studies, crystallization. The chambers could also find application beyond droplet microfluidic, for instance in super-resolution microscopy where it could boost the number of photons collected and improve resolution for a modest cost and complexity.

Materials and Methods

Si chamber microfabrication:

For the in-house process, 4 inch Si wafers (525 μm thick) were first cleaned with acetone, ethanol and water, dried and spin-coated with S1818 positive photoresist at 500 rpm for 30s followed by spinning at 3000 rpm for 30s and then baked at 110°C on a heat plate for 2 min. Photolithography was performed by directly adjusting a printed plastic (PET) film on top of the wafer to ensure that the chambers were aligned with the wafer orientation and exposing it to UV radiation (Union Optical, PEM-800 mask aligner) for 30s and developed for 1 min using a developer solution containing tetramethylammonium hydroxide (NMD-3, TMAH: 2.38 wt %). This rather long exposure and development help correct the imperfections from the PET mask. The wafer was then etched using Deep Reactive Ion Etching (DRIE) (SPT, Predeus Si deep reactive ion etching system). Chambers were etched to 110% of the desired droplet diameter to allow for a better flow of the droplets in the chamber while avoiding double layer. For the 50 μm chambers etching was performed by steps of 10 μm with 2 min break in between to prevent the wafer from overheating. Indeed, such overheating damages the photoresist resulting in particle deposition which after etching form pillars in the chamber. The Si wafer was finally cleaned with acetone, ethanol and water and spin-coated with a hydrophobic fluoropolymer (CYTOP) at 500 rpm for 30s and 1000 rpm for 30s and baked at 180°C for 1h. Finally single chambers were obtained by cleaving the wafer.

To increase the fabrication throughput, we developed a process on 6 inch wafers (675 μm thick) performed in a national academic cleanroom (FEMTO-ST, Besancon, France). The (100) face is the main plane for the fabrication process. The etching mask is S1813 photoresist 1.3 μm thick deposited on a SussMicrotech ACS200. The dry etch is performed on an SPTS Rapier C2L etcher. We used different etching times depending on the desired etching depth. After etching, the photoresist was stripped with acetone and O₂ plasma. The etching depths and homogeneities were characterized with a Dektak stylus profilometer. All the etching features with same dimensions are measured from bottom to top. Finally, all the structures are diced on a high precision dicing saw disco DAD3350.

Samples preparation

Nucleic acid strands were purchased from Integrated DNA technology (IDT) or from Biomers and purified by high-performance liquid chromatography. All sequences are presented in Table S3-S6. Fluorescent Dextrans with a molecular weight of 10,000 Da were purchased from Thermo Fischer. Nb.BsmI, Vent (exo-), Bsm1, NBI enzymes as well as BSA were purchased from New England Biolabs (NEB). ttRecJ, a thermophilic exonuclease, was purified in the laboratory following a previously published protocol⁶³.

The working solution at 1.53 μM was obtained using Diluent A (NEB) and 1% Triton X-100, and stored at $-20\text{ }^{\circ}\text{C}$. For each experiment, all common reagents were mixed into a mastermix to assure constant concentrations. We first added the DNA, RNA strands to the buffer and the Dextrans, BSA then vortexed for 10s. For experiments using enzymes (Figure 2 & Figure 4), these were added last followed by a gentle vortexing and everything was assembled on ice to prevent an early start of the reaction. Once completed the mastermix was split into several tubes and we added the varying reagents as well as their respective fluorescent barcode. Bulk fluorescence (Figure 3C) was acquired using a CFX96 thermocycler (Biorad). The complete composition of each solution is described in Table S7-S11

Microfluidic droplet encapsulation

We used an in-house microfluidic platform to generate water in oil droplets by hydrodynamic flow focusing using a pressure pump controller (MFCS-EZ, Fluigent, France) and PDMS microfluidic devices following previously published protocols: droplets of 50 μm diameter with discretely (Figure 1 & Figure 3) or continuously (Figure 4) varying content used a simple 3 channels PDMS device^{17,18} and 6 populations of droplets in the 10 μm range using a PDMS device with 2 different channel heights⁵⁷ and a 3D printed sample changer⁶⁴. Briefly, the PDMS devices were replicated using a Si patterned with SU8 mold, and plasma bonded to a $\approx 1\text{mm}$ thick glass slide. They were then heated to 200°C for 5h to recover PDMS native hydrophobic state⁶⁵. We used a fluorinated oil (HFE 7500, Novec) to which we added a surfactant (FluoSurf, Emulseo) at 3% w/v. The device is then placed onto a fluorescent microscope and each aqueous solution is plugged into a different inlet, all merging into one single channel that intersects with the oil channel. This produces monodisperse droplets whose size and composition can be finely tuned by changing the pressure ratio of water and oil. To create 50 μm droplets the pressure water:oil is 1:2. We scripted the pressure profiles to control the contribution of each aqueous channel, thus continuously varying the concentration inside droplets (Figure 4B). The droplets were collected in a pipette tip at the outlet before being transferred to the Si chamber for imaging. This allows us to easily measure the volume of emulsion, collect separately different droplet populations or face any trouble without having to change device or to restart the whole experiment.

Si chamber filling procedure

The collected emulsion is inserted in the Si chamber (Figure 1B). A tutorial for the filling of the chamber is presented in Extended Video 1.

Incubation and imaging

The Si chamber was set under a copper plate (16 cm x 4 cm x 0.5cm) whose temperature is monitored using a Peltier controller (TEC-1122, Meerstetter) coupled to Pt100 sensors (RS-Pro, 10 mm x 2mm probe, 4-wire, Class A) and two Peltier elements (Adaptative, 40 x 40 mm ET-161-12-08-E) surmounted by a CPU cooler (Enermax, AM4 ETS-N31-02) as shown on Figure 3A. The chamber was imaged using a motorized Nikon Ti2-E epifluorescence microscope connected to an LED light source (pE-4000, CoolLED) and a sCMOS camera (Prime 95B 25 mm, Photometrics). We used 4x, 10x and 20x objectives (CFI Plan Apo Lambda NA: 0.2, 0.45, 0.75, Nikon) and filters corresponding to the desired wavelength (purchased from Semrock and Chroma). Large images were obtained by unshading with the BasiC plugin⁶⁶ and stitching⁶⁷ in ImageJ.

Data analysis

Analysis from fluorescence images was performed using Mathematica as described in previous protocols^{17,57}. Briefly, droplets were detected and tracked using the channel corresponding to a Dextran of constant concentration. Droplets composition were obtained by transforming barcodes fluorescence into concentration levels. Temperature was obtained using the position of each droplet and the value of the temperature gradient.

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