

Optical nanotweezers for single cell deformability measurements

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Mechanical phenotype for diagnostic applications

Asthma



Wadsworth et al. Asthma and Glycosylation in Airway Epithelial Repair, (2012)

Cancer



www.proteinatlas.org

Sickle Cell Disease





www.clinicaladvisor.com

Hereditary Spherocytosis



www.askhematologist.com

Mechanical signature of cells appears to be a relevant physical biomarker

www.lifl.fr



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www.blog.rottenecards.com





For example: detection of malaria



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Current detection methods:



Not suitable for on field analysis



World Health

Organization

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"247 million cases of malaria in 2021, and the estimated number of malaria deaths stood at 619 000. The WHO African Region carries a disproportionately high share of the global malaria burden."

www.who.int/



False-positive leading to unnecessary drug use which contributes to the emergence of treatment-resistant strains

Direct detection of the presence of parasites within the host cell \rightarrow mechanical phenotyping



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http://inl.cnrs.fr

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Mechanical phenotyping techniques



Mechanical phenotyping using optical tweezers

Manipulation of microspheres diametrically attached to the RBCs membrane



Significant increase of malaria infected RBCs with parasite growth at different maturation stages

- Single cell scale measurement
- Low throughput analysis (~ 100 cells/hour)



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Optical tweezers coupled with microfluidics





Single cell scale measurement

Medium throughput analysis (~ 1 cell/min)

In order to improve further the throughput performances it would require avoiding image analysis step



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Our approach : Optical Nanotweezers based on Photonic Crystal



Measurement of a reference on an empty cavity,



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The experimental setup

□ The 5 µm wide Photonic Cristal (PhC) cavity

Double periode





The setup





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The samples

rRBC	hRBC no treatment	
Chemical treatment ~ 12 % glutaraldehyde for 1H00		
Young's modulus : $E_{rRBC} = 1,5 * 10^4 \text{ Pa}$	Young's modulus : $E_{hRBC} = 0.5 * 10^2 \text{ Pa}$	



The buffer

20 µm

Due to electrostatic interactions, non specific adhesion of RBCs on SOI substrates is observed despite passivation treatment (Bovin Serum Albumin or silane)

Solution	Morphologie de RBCs	Non-adhésion sur la surface
sucrose (285 mM)	:	98 % de RBCs libres
sucrose + PBS	:	56 % de RBCs
$\frac{V_{sucrose\ 285\ mM}}{V_{PBS}} = 3.3$		libres
sucrose + PBS $\frac{V_{sucrose \ 285 \ mM}}{V_{PBS}} = 0.4$:	16 % de RBCs libres
PBS 1X	:	0% _ 0.5 % de RBCs libres



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Reflectivity spectrum



 $\lambda_{resonnance}$ varies with :

- optical indice at the PhC surface vincinity, $\succ \Delta \lambda_{1_{hRBC}} = \Delta \lambda_{1_{rRBC}} \rightarrow$ no difference in optical indice
- distance between object and PhC surface,
- object surface area interacting with Ph mode.

Discrimination possible between hRBCs and rRBCs without imaging

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Effect of trapping laser power



- > In the deformation regime: Combinaison of displacement + deformation
- > In the displacement regime: Pure displacement



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Approach of the rRBCs of roughly 60 nm



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Conclusions:

- We developped a biosensor device able to probe withough imaging the deformability of RBCs
- ✓ We demonstrated that $\lambda_{resonance}$ can be used to detect cell deformation → It's a premiere !!
- ✓ We were able to discriminate hRBCs from rRBCs



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