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## ▶ To cite this version:

Kannara Mom, Max Langer, Bruno Sixou. Deep Gauss–Newton for phase retrieval. Optics Letters, 2023, 48 (5), pp.1136. 10.1364/OL.484862 . hal-04177989

# HAL Id: hal-04177989 https://hal.science/hal-04177989

Submitted on 7 Aug 2023

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## Deep Gauss-Newton for phase retrieval

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Compiled January 24, 2023

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We propose the Deep Gauss-Newton (DGN) algorithm. The DGN allows to take into account the knowledge of the forward model in a deep neural network by unrolling a Gauss-Newton optimization method. No regularization or step size need to be chosen, they are learned through convolutional neural networks. The proposed algorithm does not require an initial reconstruction and is able to retrieve simultaneously the phase and absorption from a single-distance diffraction pattern. The DGN method was applied to both simulated and experimental data and permitted large improvements of the reconstruction error and of the resolution compared to a state of the art iterative method and another neural network based reconstruction algorithm. © 2023 Optica Publishing Group

### 2 http://dx.doi.org/10.1364/ao.XX.XXXXXX

Phase contrast imaging has higher sensitivity compared to attenuation-based techniques, and permits tomography at the 5 microscopic and nanoscopic scales [1]. It has found many ap-6 plications such as in materials science and biomedical imaging [2]. Due to the high coherence and brilliance of synchrotron 8 sources, resolutions down to tens of nanometers can be routinely achieved [3]. Several phase-sensitive imaging techniques 10 have been developed [4], among them, propagation-based imag-11 ing [5] requires no equipment other than the source, object and 12 detector. The absorption and phase shift induced by a sample 13 can be retrieved from one or several such images, which is a 14 nonlinear and ill-posed inverse problem. 15

Direct inversion formulas can be obtained by linearization 16 of the problem [6–8]. Such analytical methods can work well 17 under certain imaging conditions, but impose restrictions on 18 the imaging setup [6] or the object [7, 8]. To overcome these 19 limitations, for example in high resolution imaging [9], iterative 20 algorithms that do not rely on linearization of the problem can 21 be used. Among them are the methods of alternating projections 22 on constraints in the object and the Fourier domain, e.g. the 23 Hybrid Input-Output (HIO) algorithm [10]. Another class of 24 algorithm is the so-called variational approaches that consist in 25 minimizing a criterion defined by a data fidelity term and regu-26 larization terms. These algorithms permit a flexible inclusion of 27 28 prior information, such as sparsity or Tikhonov regularization [11]. More recently, an iteratively regularised Gauss-Newton 29 30 (IRGN) method was proposed, exploiting the regularity of the



**Fig. 1.** Architecture of the network  $\Gamma_{\theta}$ , representing one iteration of the Deep Gauss-Newton method.

solution to obtain better robustness to high-frequency errors by regularizing with Sobolev norms [12]. Such approaches take into account the non-linearity of the problem, and yield better reconstructions with less artifacts than linearized methods. Unfortunately, the computation time is high and the choice of appropriate regularization remains a difficult problem.

The development of deep learning methods in recent years has led to many advances in image and signal processing [13]. Specifically, deep neural networks (DNNs) have been used to solve a wide variety of inverse problems [14]. Despite this progress, the black-box nature of DNNs, i.e., their lack of interpretability, is one of the primary obstacles for their use. Several approaches to exploiting DNNs for the solution of inverse problems have been proposed. DNNs can be used to reconstruct the unknown image directly from an available measurement, or some parts of an algorithm can be replaced by DNNs. Algorithm unrolling is an emerging technique based on the incorporation of convolutional neural networks (CNNs) into an iterative optimization scheme in order to give the DNN a specific role in the reconstruction [15]. Such approaches have found many applications [16] and unrolling has been applied to several optimization approaches: gradient descent algorithms [17], primal-dual schemes [18], and Alternating Direction Method of Multipliers [19]. For phase retrieval, several architectures have been proposed, including MS-D Net [20] and PhaseGAN [21]. This kind of network is trained to approximate the inverse operator and often require large training sets as well as long training time. Other methods have incorporated neural networks into iterative schemes, but they are either computationally demanding [22, 23] or rely on a linearization of the forward model [24].

Table 1. Parameters for the Neural Networks

	MS-D Net	DGN	
Loss function	MSE	MSE	
Training epochs	100	100	
Learning rate	$10^{-3}$	$5 \times 10^{-4}$	
Batch size	10	10	
Activation function	ReLU	LReLU	
Training time	35h	21h	
Number of parameters	$46  imes 10^3$	$31  imes 10^3$	

Here, we present a new learned iterative scheme, the Deep 61 Gauss-Newton (DGN) algorithm, which is obtained by unrolling 62 a Gauss-Newton iteration. The proposed method combines 63 CNNs and knowledge of the imaging physics given by the for-64 ward operator and its Fréchet derivative. The rationale behind 65 this choice is to take a well-known algorithm that is known 66 to converge quickly and enhance it with machine learning by 67 unrolling. We expect this scheme to inherit or improve the con-68 vergence properties of the Gauss-Newton method. Another 69 advantage of this approach is that no regularization has to be 70 chosen, instead it is adaptively learned from the data during 71 training. We demonstrate the capability of the method to re-72 trieve phase and attenuation from a single phase contrast image 73 74 on simulated data as well as experimental data.

Under the projection approximation, the interaction of a co-75 103 herent and parallel X-ray beam with matter can be described 76 104 by a transmittance function [6]. In the experimental conditions 77 105 considered here, the intensity at a distance *D* from the sample 78 106 is well described by the Fresnel formalism, and is given by the 79 107 convolution of the transmittance and the Fresnel propagator  $P_D$ : 80 108

$$\mathbf{F}_{D}(B,\varphi) = |\mathbf{e}^{-B+i\varphi} * P_{D}|^{2} \text{ with } P_{D}(\cdot) = \frac{1}{i\lambda D} \exp^{i\frac{\pi}{\lambda D}|\cdot|^{2}}. \text{ (1)} \prod_{111}^{109}$$

The operator  $\mathbf{F}_D$  describes the nonlinear relationship between 112 81 the absorption *B* and phase shift  $\varphi$  induced by the object and 82 113 the intensity of the diffraction pattern. In the following, we will 114 83 note  $f = (B, \varphi)$  the couple we aim to retrieve. 84

The inverse of  $\mathbf{F}_D$  can be approximated using variational 116 85 methods such as IRGN, corresponding to Tikhonov regulariza- 117 86 tion of the Newton steps: 87

$$f_{k+1} = \underset{f}{\operatorname{argmin}} \left\{ \left| \left| \mathbf{F}_{D}(f_{k}) + \mathbf{F}_{D}'(f_{k}) \left(f - f_{k}\right) - \mathbf{I}_{D}^{\operatorname{obs}} \right| \right|_{2}^{2} + \alpha_{k} \left| |f| \right|_{2}^{2} \right\} \quad \textbf{(2)} \quad \underset{121}{\overset{119}{120}}$$

where  $\mathbf{F}'_D(f_k)$  is the Fréchet dérivative [25] of  $\mathbf{F}_D$  at the point  $f_k$ , 122  $\alpha_k > 0$  is a regularization parameter at iteration k, and  $\mathbf{I}_D^{\text{obs}}$  is a 123 noisy measured intensity. Eq. (2) has a unique solution

$$f_{k+1} = f_k + \begin{bmatrix} \mathbf{F}'_D(f_k)^* \mathbf{F}'_D(f_k) + \alpha_k \mathrm{Id} \end{bmatrix}^{-1} \begin{bmatrix} 126 \\ 127 \\ \left\{ \mathbf{F}'_D(f_k)^* \begin{bmatrix} \mathbf{I}_D^{\mathrm{obs}} - \mathbf{F}_D(f_k) \end{bmatrix} - \alpha_k f_k \end{bmatrix}$$
(3) 128 129

where  $\mathbf{F}'_D(f_k)^*$  is the adjoint of the linear map  $\mathbf{F}'_D(f_k)$  and Id is the identity. Usually, a step size for the update of  $f_k$  is introduced as regularization. Here, we propose instead to learn a regularization by replacing the Tikhonov term  $\alpha_k f_k$  with a CNN  $\mathbf{G}_{\theta_{k}^{g}}$  with parameters  $\theta_{k}^{g}$ , and to approximate the inverse of the operator  $[\mathbf{F}'_D(f_k)^*\mathbf{F}'_D(f_k) + \alpha_k \mathrm{Id}]$  with another CNN  $\mathbf{H}_{\theta^h}$  with parameters  $\theta_k^h$ , based on the current iterate  $f_k$  and on the approximate Hessian  $\mathbf{F}'_D(f_k)^* \mathbf{F}'_D(f_k)$ . The network *H* then replaces the classical approximation of the inverse of the Hessian used in the traditional Gauss-Newton scheme by a potentially better and

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faster learned approximation. If the algorithm is stopped after *N* iterations, we get  $f_N = (\Gamma_{\theta_N} \circ \cdots \circ \Gamma_{\theta_1})(f_0)$ , where  $f_0$  is the initial guess,  $\theta_k = (\theta_k^g, \theta_k^h)$  and

$$\Gamma_{\theta_{k}}(f_{k}) = f_{k} + \mathbf{H}_{\theta_{k}^{h}}\left[f_{k}, \mathbf{F}_{D}'(f_{k})^{*}\mathbf{F}_{D}'(f_{k})\left\{\mathbf{F}_{D}'(f_{k})^{*}\left[\mathbf{I}_{D}^{\mathrm{obs}} - \mathbf{F}_{D}(f_{k})\right] + \mathbf{G}_{\theta_{k}^{g}}\left(f_{k}\right)\right\}\right]$$
(4)

Unrolling this scheme, we can consider  $\Lambda_{\Theta} = \Gamma_{\theta_N} \circ \cdots \circ \Gamma_{\theta_1}$ as a deep neural network representing N iterations with  $\Theta =$  $(\theta_1, \ldots, \theta_N)$  its parameters. Recent work on unrolling schemes has shown that using the same transformation at each iteration so that  $\theta_k = \theta$  for  $k \in \{1, ..., N\}$ , yields good results [26].  $\Lambda_{\Theta}$ can then be seen as a recurrent neural network. The architecture of the network  $\Gamma_{\theta}$  used for each iteration is shown in Fig. 1.

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The network  $\mathbf{G}_{\theta s}$  takes the current iterate  $f_k$  as input, spreads it to 16 and then 32 channels by a convolutional layer with kernel size  $5 \times 5$  using a leaky rectified linear unit (LReLU) as non-linearity, defined as  $LReLU_{\alpha}(x) = max(x, \alpha x), \alpha > 0$ . The output of the network  $\mathbf{G}_{\theta^{g}}$  is added to  $\mathbf{F}'_{D}(f_{k})^{*} \left[ \mathbf{I}_{D}^{\text{obs}} - \mathbf{F}_{D}(f_{k}) \right]$ , stacked with the current iterate and then fed to the network  $\mathbf{H}_{\theta^h}$ which consists of the same set of operations as  $G_{\theta 8}$  (except it has four input channels instead of two). Finally, the output is added to the current iterate and projected onto positive numbers by a LReLU. The architectures of the networks are kept simple for several reasons. A shallow network added to the iterative update saves computational time and the memory required, while giving good reconstruction results.

To evaluate the algorithms, we created a database of 3D objects consisting of random combinations of one to ten ellipsoid and paraboloid shapes of three different materials (gold, palladium and zinc). We then computed 2D tomographic projections of the real and imaginary parts of the refractive index, corresponding to the phase shift and absorption. The X-ray energy was set to 13 keV for a wavelength of  $\lambda = 0.095$  nm, and the propagation distance was set to D = 20 mm to yield a pixel size of 12 nm corresponding to the experimental conditions below. The phase contrast images were generated from the projection images according to the forward model Eq. (1). The propagation was calculated using 4 times oversampling with an image size of  $2048 \times 2048$ , yielding a final image size of  $512 \times 512$  (Fig. 2). Gaussian noise with different amplitudes was added to the images to yield a peak to peak signal to noise ratio (PPSNR) between 10 and 100 dB. 12 000 pairs of one input image (simulated intensity) and two output images (absorption and phase) were generated. From this dataset, 10000 pairs were used for training, 1000 for validation during the training, and 1000 for evaluation. We compare the unrolling framework to the standard IRGN method [12] as well as to the Mixed-Scale Dense Network (MS-D Net), a direct reconstruction method that does not include prior knowledge on the imaging physics [20].



Fig. 2. (a) Simulated and (b) experimental intensity.

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Method	<b>NMSE (%)</b>		FRCM (%)		Resolution (nm)		Time (s)
	Absorption	Phase	Absorption	Phase	Absorption	Phase	
IRGN	85.5 (40.7)	39.3 (15.0)	71.2 (9.95)	68.1 (5.45)	238 (136)	154 (43)	116
MS-D Net DGN	13.6 (12.8) <b>12.1 (13.5)</b>	10.6 (10.8) <b>4.61 (6.20)</b>	48.8 (13.8) <b>35.7 (15.7)</b>	47.8 (13.3) <b>23.0 (16.6)</b>	102 (77.4) 72.2 (55.2)	98.5 (135) 62.3 (37.0)	<b>2.60</b> 5.88

Table 2. Results (mean and standard deviation) on 1000 simulated images.

In the IRGN, the positive-definite linear operator in Eq. (3) 185 131 can be inverted efficiently by a conjugate gradient (CG) method 186 132 [12]. We used 100 Newton steps and 10 iterations for the CG. 187 133 For the DGN method, we used N = 10 iterations, which means 188 134 that the derivative  $\mathbf{F}'_{D}(f_{k})$  and its adjoint  $\mathbf{F}'_{D}(f_{k})^{*}$  are evaluated <sup>189</sup> 135 10 times. The number of iterations was chosen empirically so 190 136 that the NMSE stagnates. As opposed to [17], where several 13 networks are trained sequentially, i.e. iteration by iteration, here, 192 138 given a training set  $\{y^i, f^i\}$  where  $y_i$  denotes the intensity  $\mathbf{F}_D(f^i)$ 139 193 corrupted by noise, we use one network  $\Gamma_{\theta}$  applied *N* times in 194 140 a recurrent fashion to obtain the DNN  $\Lambda_{\theta}$ , which is trained to 141 195 perform end-to-end reconstruction. The DGN was trained using 142 196 100 epochs with a batch size of 10, the ADAM optimizer, an 143 197 initial learning rate of  $5 \times 10^{-4}$  and a cosine annealing learning 144 198 rate schedule [27]. The LReLU activation function parameter 145 199 was set to the default  $\alpha = 0.3$ . Warm-up initialization decreased 146 200 training time but did not yield better final results. Therefore, for 147 201 simplicity, zero initialization,  $f_0 = (0, 0)$ , was used throughout. 148 202 For the MS-D Net, we used the same settings as in [20]. Using 149 203 LReLU in the MS-D Net did not improve the reconstructions. 150 The hyperparameters for the networks are summarized in Tab. 15 152 1 and were optimized using grid search. Both DGN and MS-D Net were trained on the same training set. 153

To quantify reconstruction quality on simulated data, we 154 used the normalized mean square error (NMSE). The frequency 155 domain correlation between ground truth and recovered image 156 was evaluated using the Fourier Ring Correlation (FRC). From 157 this the Fourier Ring Correlation Metric (FRCM) [21] and the 158 resolution were calculated. FRCM is the mean square difference 159 between the FRC and unity over all spatial frequencies. A small 160 FRCM implies a higher similarity in the Fourier domain. To 161 assess the capability to retrieve high frequencies and reconstruct 162 163 thin details, a metric to estimate the resolution was computed by the  $2\sigma$  criterion [28]. The mean and standard deviation of the 164 metrics were calculated on the test dataset. The average com-165 putation time for one reconstruction was measured to compare 166 the execution time. The results are summarized in Tab. 2. Phase 167 and absorption reconstructions from one simulated image pair 168 are shown in Fig. 3. Both deep learning methods performed 169 better than the IRGN method, which tended to leave artifacts 170 in the absorption and yield a blurred phase. On average, the 171 deep learning approaches performed better than the IRGN, both 172 in terms of reconstructed values and resolution. In terms of 173 NMSE, the deep learning approaches gave similar results for the 174 absorption, but the DGN performed better than the MS-D Net 175 for phase recovery. Moreover, the DGN yielded better resolu-176 tion as well as better correlation in the frequency domain. As 177 expected, the MS-D Net was fastest, since it only requires one 178 application of a neural network. The DGN is efficient despite the 179 need to compute the derivative of the foward operator as well as 180 its adjoint several times and is 20 times faster than its standard 181 iterative counterpart. For comparison, an unrolled simple gradi-182 ent descent scheme [17] vielded less convincing results despite 183 using more parameters  $(41 \times 10^3)$ : for the absorption 13.2 (17.3) 184

% NMSE, 37.6 (15.2) % FRCM 82.2 (116) nm resolution and for the phase 4.74 (6.99) % NMSE, 23.9 (16.7) % FRCM, 69.3 (62.6) nm resolution, confirming our choice of network structure.

The proposed approach was applied on data acquired at beamline NanoMAX at the MAX IV synchrotron (Lund, Sweden) [29]. The diffraction pattern in Fig. 2 was obtained using the same image conditions as above. The sample consists of a stack of palladium, zinc, palladium, gold layers with thicknesses of 21, 10, 11, 163 nm, respectively, deposited on a 1 mm-thick silicon nitride substrate, resulting in expected values for absorption and phase of 0.0483 and 0.217 respectively. To evaluate the reconstructions quantitatively, we used the normalized error (NE) and relative standard deviation (RSD), calculated as NE =  $\frac{l_t - l_m}{L}$ and RSD =  $\frac{s_m}{l_m}$ , where  $l_t$  is the expected value,  $l_m$  the measured mean value and  $s_m$  the standard deviation in the corresponding material. The shape of the object was estimated from a phase reconstruction using an iterative method, and chosen so that the calculation of  $l_m$  and  $s_m$  was done in homogeneous parts to avoid the influence of blur at the edges. The resolution was mea-



**Fig. 3.** Reconstructions from simulated data. Reconstruction quality is given as (NMSE (%), FRCM (%), resolution (nm)).



**Fig. 4.** Reconstructions for experimental data. The profiles along the red line were measured to estimate the resolution. Values correspond to (NE (%) (RSD (%)), resolution (nm)).

sured by fitting an error function to a line profile across an object
 edge and calculating the corresponding Gaussian full width at
 half maximum based on the error function fitting parameters.

270 The reconstructions obtained in Fig. 4 show that the DGN 207 271 yields very high quality reconstructions of the object with almost 208 272 no remaining visible artifacts. Although the MS-D Net performs 209 well on simulations, it seems to not generalize as well as the 210 274 DGN to the experimental data given the chosen training strat-211 275 egy. This could be due to the DGN explicitly taking into account 276 212 the physics model, learning the noise statistics from the data 213 yielding an adapted regularization, while leveraging the conver- 278 214 gence properties of the optimization method [16]. On the other 279 215 hand, the MS-D Net was trained to reconstruct directly from the 280 216 281 measurements, without knowledge of the physics model. 217

282 A limitation of the proposed algorithm is that the forward 218 283 model has to be fully known, e.g. the propagation distance has to 219 284 be precisely measured. In future work we will study possibilites 220 285 to correct errors in the forward model. We will also investigate 221 286 out-of-distribution generalization error, e.g. with respect to dif-222 287 ferent noise properties. The developed DGN algorithm allows 288 223 to efficiently retrieve both the phase and absorption from a sin- 289 224 gle phase contrast image. By exploiting recent developments in 290 225 deep learning and integrating CNNs into a regularized Gauss- 291 226 Newton scheme, with the DGN we overcome the limitations of 292 227 classical iterative approaches while leveraging the power of neu-<sup>293</sup> 228 294 ral networks. Since no regularization term needs to be chosen, 229 the DGN network is trained to learn an optimal one for the ab-230 sorption and the phase respectively, which improves the quality 231 297 of the reconstructions. Taking into account the knowledge of the 232 298 forward model in a simple network enhances the reconstructions 233 299 and allows a better generalization on real data. Compared to the 300 234 standard IRGN, the DGN method both substantially improved 301 235

- Optics Letters 4
- <sup>236</sup> the reconstruction and reduced the calculation time.
- 237 Acknowledgments. Pablo Villanueva-Perez (Lund University, Lund,
- 238 Sweden) and Sebastian Kalbfleich (MAX IV Laboratory, Lund, Sweden)
- 239 for the experimental data, and Jesper Wallentin and Lert Chayanun
- 240 (NanoLund and Lund University, Lund, Sweden) for the sample.
- 241 **Disclosures.** The authors declare no conflicts of interest.
- 242 Data Availability Statement. Data underlying the simulated results
- <sup>243</sup> presented in this paper can be generated using *TomoPhantom* software
- [30]. The data underlying the experimental results presented are avail-
- <sup>245</sup> able through the *PyPhase* package [31].

### 246 **REFERENCES**

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- 247 1. M. Langer and F. Peyrin, Osteoporos. Int. 27, 441 (2016).
- M. Langer, In-Line X-Ray Phase Tomography of Bone and Biomaterials for Regenerative Medicine (Springer, Cham, 2018).
  - J.-P. Suuronen, B. Hesse, M. Langer, M. Bohner, and J. Villanova, J. Synchrotron Radiat. 29, 843 (2022).
  - 4. S. Tao, C. He, C. Kuang, and X. Liu, Appl. Sci. 11, 2971 (2021).
  - A. Snigirev, I. Snigireva, V. Kohn, S. Kuznetsov, and I. Schelokov, Rev. Sci. Instruments 66, 5486 (1995).
  - 6. D. M. Paganin, Coherent X-ray optics (Oxford University Press, 2006).
  - P. Cloetens, W. Ludwig, J. Baruchel, D. Van Dyck, J. Van Landuyt, J. P. Guigay, and M. Schlenker, Appl. Phys. Lett. 75, 2912 (1999).
  - J. P. Guigay, M. Langer, R. Boistel, and P. Cloetens, Opt. Lett. 32, 1617 (2007).
  - R. Mokso, P. Cloetens, E. Maire, J.-Y. Buffiere, and W. Ludwig, Applied Physics Letters p. 1 (2007).
  - 10. J. R. Fienup, Appl. Opt. 21 (15), 2758 (1982).
  - 11. V. Davidoiu, B. Sixou, M. Langer, and F. Peyrin, Appl. Opt. **52**, 3977 (2013).
  - S. Maretzke, M. Bartels, M. Krenkel, T. Salditt, and T. Hohage, Opt. Express 24, 6490 (2016).
  - 13. Y. LeCun, Y. Bengio, and G. Hinton, Nature 521, 436 (2015).
  - G. Ongie, A. Jalal, C. A. Metzler, R. G. Baraniuk, A. G. Dimakis, and R. Willett, IEEE J. on Sel. Areas Inf. Theory 1, 39 (2020).
  - S. Arridge, P. Maass, O. Öktem, and C.-B. Schönlieb, Acta Numer. 28, 1–174 (2019).
  - 16. V. Monga, Y. Li, and Y. C. Eldar, IEEE Signal Proc. Mag. 38, 18 (2021).
  - A. Hauptmann, F. Lucka, M. Betcke, N. Huynh, J. Adler, B. Cox, P. Beard, S. Ourselin, and S. Arridge, IEEE Trans. on Med. Imaging **37**, 1382 (2018).
  - 18. J. Adler and O. Öktem, IEEE Trans. on Med. Imaging 37, 1322 (2018).
  - Y. Yang, J. Sun, H. Li, and Z. Xu, IEEE Transactions on Pattern Analysis Mach. Intell. 42, 521 (2020).
  - 20. K. Mom, B. Sixou, and M. Langer, Appl. Opt. 61, 2497 (2022).
  - Y. Zhang, M. A. Noack, P. Vagovic, K. Fezzaa, F. Garcia-Moreno, T. Ritschel, and P. Villanueva-Perez, Opt. Express 29, 19593 (2021).
  - C. A. Metzler, P. Schniter, A. Veeraraghavan, and R. G. Baraniuk, CoRR abs/1803.00212 (2018).
  - 23. C. Işil, F. S. Oktem, and A. Koç, Appl. Opt. 58, 5422 (2019).
  - C. Bai, M. Zhou, J. Min, S. Dand, X. Yu, P. Zhang, T. Peng, and B. Yao, Opt. Lett. 44 (21), 5141 (2019).
  - 25. V. Davidoiu, B. Sixou, M. Langer, and F. Peyrin, Opt. Express **19**, 22809 (2011).
  - 26. R. Dabre and A. Fujita, AAAI Conf. on Artif. Intell. 33, 6292 (2019).
  - 27. I. Loshchilov and F. Hutter, "Sgdr: Stochastic gradient descent with warm restarts," in *ICLR 2017*, (2016).
  - N. Banterle, K. H. Bui, E. A. Lemke, and M. Beck, J. Struct. Biol. 183, 363 (2013).
  - S. Kalbfleisch, M. Kahnt, K. Buakor, M. Langer, T. Dreier, H. Dierks, P. Stjärneblad, E. Larsson, K. Gordeyeva, L. Chayanun, D. Söderberg, J. Wallentin, M. Bech, and P. Villanueva-Perez, J. Synch. Radiat. 29 (2022).
  - D. Kazantsev, V. Pickalov, S. Nagella, P. Edoardo, and P. J. Withers, SoftwareX 7, 150 (2018).
  - M. Langer, Y. Zhang, D. Figueirinhas, J.-B. Forien, K. Mom, C. Mouton, R. Mokso, and P. Villanueva-Perez, J. Synch. Radiat. 28, 1261 (2021).

#### Optics Letters

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#### **FULL REFERENCES**

- M. Langer and F. Peyrin, "3D X-ray ultra-microscopy of bone tissue," 372
   Osteoporos. Int. 27, 441–455 (2016).
- M. Langer, In-Line X-Ray Phase Tomography of Bone and Biomaterials for Regenerative Medicine (Springer, Cham, 2018).
- J.-P. Suuronen, B. Hesse, M. Langer, M. Bohner, and J. Villanova, 376
   "Evaluation of imaging setups for quantitative phase contrast nanoCT of 377
   mineralized biomaterials," J. Synchrotron Radiat. 29, 843–852 (2022). 378
- 4. S. Tao, C. He, C. Kuang, and X. Liu, "Principles of different x-ray phase-contrast imaging: A review," Appl. Sci. **11**, 2971 (2021). 380
- A. Snigirev, I. Snigireva, V. Kohn, S. Kuznetsov, and I. Schelokov, "On 381
   the possibilities of x-ray phase contrast microimaging by coherent highenergy synchrotron radiation," Rev. Sci. Instruments 66, 5486–5492
   (1995).
- 316 6. D. M. Paganin, Coherent X-ray optics (Oxford University Press, 2006). 385
- P. Cloetens, W. Ludwig, J. Baruchel, D. Van Dyck, J. Van Landuyt, J. P. 386
   Guigay, and M. Schlenker, "Holotomography: Quantitative phase tomography with micrometer resolution using hard synchrotron radiation x rays," Appl. Phys. Lett. **75**, 2912–2914 (1999).
- J. P. Guigay, M. Langer, R. Boistel, and P. Cloetens, "Mixed transfer generation of intensity approach for phase retrieval in the generation of transport of intensity approach for phase retrieval in the generation of the second second
- R. Mokso, P. Cloetens, E. Maire, J.-Y. Buffiere, and W. Ludwig,
   "Nanoscale zoom tomography with hard x-rays using kirkpatrick-baez
   optics," Applied Physics Letters p. 1 (2007).
- J. R. Fienup, "Phase retrieval algorithms: a comparison," Appl. Opt. 21 (15), 2758–2769 (1982).
- V. Davidoiu, B. Sixou, M. Langer, and F. Peyrin, "Nonlinear approaches for the single-distance phase retrieval problem involving regularizations with sparsity constraints," Appl. Opt. **52**, 3977–3986 (2013).
- S. Maretzke, M. Bartels, M. Krenkel, T. Salditt, and T. Hohage, "Regularized newton methods for x-ray phase contrast and general imaging problems," Opt. Express 24, 6490–6506 (2016).
- 13. Y. LeCun, Y. Bengio, and G. Hinton, "Deep learning," Nature 521, 436–44 (2015).
- G. Ongie, A. Jalal, C. A. Metzler, R. G. Baraniuk, A. G. Dimakis, and
   R. Willett, "Deep learning techniques for inverse problems in imaging,"
   IEEE J. on Sel. Areas Inf. Theory 1, 39–56 (2020).
- S. Arridge, P. Maass, O. Öktem, and C.-B. Schönlieb, "Solving inverse problems using data-driven models," Acta Numer. 28, 1–174 (2019).
- V. Monga, Y. Li, and Y. C. Eldar, "Algorithm unrolling: Interpretable, efficient deep learning for signal and image processing," IEEE Signal Proc. Mag. 38, 18–44 (2021).
- A. Hauptmann, F. Lucka, M. Betcke, N. Huynh, J. Adler, B. Cox,
   P. Beard, S. Ourselin, and S. Arridge, "Model-based learning for accelerated, limited-view 3-d photoacoustic tomography," IEEE Trans. on
   Med. Imaging **37**, 1382–1393 (2018).
- I8. J. Adler and O. Öktem, "Learned primal-dual reconstruction," IEEE
   Trans. on Med. Imaging **37**, 1322–1332 (2018).
- Y. Yang, J. Sun, H. Li, and Z. Xu, "Admm-csnet: A deep learning approach for image compressive sensing," IEEE Transactions on Pattern Analysis Mach. Intell. 42, 521–538 (2020).
- K. Mom, B. Sixou, and M. Langer, "Mixed scale dense convolutional networks for x-ray phase contrast imaging," Appl. Opt. 61, 2497–2505 (2022).
- Y. Zhang, M. A. Noack, P. Vagovic, K. Fezzaa, F. Garcia-Moreno,
   T. Ritschel, and P. Villanueva-Perez, "PhaseGAN: a deep-learning
   phase-retrieval approach for unpaired datasets," Opt. Express 29,
   19593–19604 (2021).
- C. A. Metzler, P. Schniter, A. Veeraraghavan, and R. G. Baraniuk,
   "prdeep: Robust phase retrieval with flexible deep neural networks,"
   CoRR abs/1803.00212 (2018).
- C. Işil, F. S. Oktem, and A. Koç, "Deep iterative reconstruction for phase retrieval," Appl. Opt. 58, 5422–5431 (2019).
- C. Bai, M. Zhou, J. Min, S. Dand, X. Yu, P. Zhang, T. Peng, and
   B. Yao, "Robust contrast-transfer-function phase retrieval via flexible
   deep learning networks," Opt. Lett. 44 (21), 5141–5144 (2019).
- 25. V. Davidoiu, B. Sixou, M. Langer, and F. Peyrin, "Non-linear iterative

phase retrieval based on frechet derivative," Opt. Express **19**, 22809– 22819 (2011).

370

371

- R. Dabre and A. Fujita, "Recurrent stacking of layers for compact neural machine translation models," AAAI Conf. on Artif. Intell. 33, 6292–6299 (2019).
- I. Loshchilov and F. Hutter, "Sgdr: Stochastic gradient descent with warm restarts," in *ICLR 2017*, (2016).
- N. Banterle, K. H. Bui, E. A. Lemke, and M. Beck, "Fourier ring correlation as a resolution criterion for super-resolution microscopy," J. Struct. Biol. 183, 363–367 (2013).
- S. Kalbfleisch, M. Kahnt, K. Buakor, M. Langer, T. Dreier, H. Dierks, P. Stjärneblad, E. Larsson, K. Gordeyeva, L. Chayanun, D. Söderberg, J. Wallentin, M. Bech, and P. Villanueva-Perez, "X-ray in-line holography and holotomography at the nanomax beamline," J. Synch. Radiat. 29 (2022).
- D. Kazantsev, V. Pickalov, S. Nagella, P. Edoardo, and P. J. Withers, "TomoPhantom, a software package to generate 2D–4D analytical phantoms for CT image reconstruction algorithm benchmarks," SoftwareX 7, 150–155 (2018).
- M. Langer, Y. Zhang, D. Figueirinhas, J.-B. Forien, K. Mom, C. Mouton, R. Mokso, and P. Villanueva-Perez, "*PyPhase* – a Python package for X-ray phase imaging," J. Synch. Radiat. 28, 1261–1266 (2021).