

# Iterative phase retrieval algorithm for medical applications

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# Bringing iterative phase retrieval methods to propagation-based phase contrast medical

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**Context** In X-ray medical imaging, phase sensitive techniques are known to provide useful information compared to classical absorption imaging, especially when tissues exhibit weak absorption contrast [1]. A new generation of table-top high-brightness X-ray sources and recent advances in detectors technology makes phase-contrast (PC) imaging using laboratory-scale setups possible, thus paving the way for widespread clinical use.

Goal In this work we are focused on 3D imaging using a propagation based, phase contrast tomography setup. Our goal is to optimize contrast and resolution in the reconstructed volume with a relatively short propagation distance, which keeps the setup compact but is not optimal for phase contrast formation. Direct phase retrieval (PR), such as the Paganin formula (PAG) [1], has proven helpful in medical imaging [2], but requires a priori knowledge of the material. We explore methods based on iterative phase retrieval (IPR) that don't require such a knowledge. In our conditions, IPR alone is not able to recover low frequencies, but allows to obtain a phase-shift only on string edges. We show that using IPR together with iterative volume reconstruction or using improved constraints Flowchart of the three iterative phase-retrieval algorithms implemented. Final result



The phase-contrast imaging setup We use the free-space propagation in order to achieve phase-contrast, for dose-efficiency and simplicity. The main drawback is optimal propagation distance. Here the sample-to-detector distance is 1.6m and image magnification is 8,9. The source used for the tests is an Excillum MetalJet microfocus with a Ga alloy anode (~50% of spectrum power around 9,25keV). The X-Ray camera is an Advacam WidePix CdTe photon-counting detector with a pixel size of 55 micrometers.

PAG phase retrieval approach can be applied

certain assumptions: the imaged sample

omogeneous and the  $\delta/\beta$  ratio must be known. By applying the PAG filter, high frequencies are lost and image

The Fresnel propagator (FP) of Ref. [3,4] has been implemented in the IPR method. Unfortunately, <sup>†</sup> low intensity of PC signal collected with our laboratory set-up still prevent to recover the frequencies. Additional constraints could b applied to improve the convergence of the algorithm as proposed in Ref. [5,6].





constraint among projections. Compared to

2D IPR, artefacts are less visible, and dynamics **Conclusion** IPR algorith **ased rig beo**mising for medical PC imaging but improvements are needed to make it more robust than PAG approach. Two additional constraints could be added to ensure the convergence of the algorithms: the 3D consistency, that has been proven fundamental in the case of IPR, and the PAG constraint for fast convergence without a priori information. Further developments will probably take into account the nonmonochromaticity of the incoming radiation preferring a multi-energy phase retrieval approach.



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