

Induction of a strong and long-lasting neutralizing immune response by dPreS1-TLR2 agonist nanovaccine against hepatitis B virus

Myriam Lamrayah, Fanny Charriaud, Manon Desmares, Céline Coiffier, Simon Megy, Evelyne Colomb, Raphaël Terreux, Julie Lucifora, David Durantel, Bernard Verrier

▶ To cite this version:

Myriam Lamrayah, Fanny Charriaud, Manon Desmares, Céline Coiffier, Simon Megy, et al.. Induction of a strong and long-lasting neutralizing immune response by dPreS1-TLR2 agonist nanovaccine against hepatitis B virus. Antiviral Research, 2023, 209, pp.105483. 10.1016/j.antiviral.2022.105483 . hal-03923266

HAL Id: hal-03923266 https://hal.science/hal-03923266v1

Submitted on 4 Jan 2023

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers. L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

Induction of a strong and long-lasting neutralizing immune response by dPreS1-TLR2 agonist nanovaccine against Hepatitis B Virus

4

6

9

5 Authors

Myriam Lamrayah^a, Fanny Charriaud^a, Manon Desmares^b, Céline Coiffier^a, Simon Megy^c, Evelyne
 Colomb^a, Raphaël Terreux^c, Julie Lucifora^b, David Durantel^b, Bernard Verrier^a

^a Colloidal vectors and therapeutic targeted engineering, UMR5305, LBTI, Institut de Biologie et
 Chimie des Protéines, Université Lyon 1, 7 Passage du Vercors, 69367 Lyon Cedex 07, France.

^b HepVir team, Centre International de Recherche en Infectiologie (CIRI), INSERM U1111, CNRS
 UMR_5308, University of Lyon (UCBL1), Lyon, France

- ¹⁵ ^c ECMO team, UMR5305, LBTI, Institut de Biologie et Chimie des Protéines, Université Lyon 1, 7
- 16 Passage du Vercors, 69367 Lyon Cedex 07, France.
- 17

* Corresponding author : School of Life Sciences, Ecole Polytechnique Fédérale de Lausanne, SV
 Station 19, 1015 Lausanne, Switzerland. E-mail address : myriam.lamrayah@epfl.ch.

20

21 Abstract

22

23 Hepatitis B virus remains a major medical burden with more than 250 million chronically infected 24 patients worldwide and 900,000 deaths each year, due to the disease progression towards severe 25 complications (cirrhosis, hepatocellular carcinoma). Despite the availability of a prophylactic 26 vaccine, this infection is still pandemic in Western Pacific and African regions, where around 6% of 27 the adult population is infected. Among novel anti-HBV strategies, innovative drug delivery 28 systems, such as nanoparticle platforms to deliver vaccine antigens or therapeutic molecules have 29 been investigated. Here, we developed polylactic acid-based biodegradable nanoparticles as an 30 innovative and efficient vaccine. They are twice functionalized by (i) the entrapment of Pam₃CSK₄, 31 an immunomodulator and ligand to Toll-Like-Receptor 1/2, and by (ii) the adsorption/coating of 32 myristoylated (2-48) derived PreS1 from the HBV surface antigen, identified as the major viral 33 attachment site on hepatocytes. We demonstrate that such formulations mimic HBV virion with an 34 efficient peptide recognition by the immune system, and elicit potent and durable antibody 35 responses in naive mice during at least one year. We also show that the most efficient in vitro viral 36 neutralization was observed with NP-Pam₃CSK₄-dPreS1 sera. The immunogenicity of the derived 37 HBV antigen is modulated by the likely synergistic action of both the dPreS1 coated nanovector 38 and the adjuvant molety. This formulation represents a promising vaccine alternative to fight HBV 39 infection.

41 Keywords

42

Hepatitis B virus, neutralizing antibodies, PreS1 peptide, TLR agonist, nanoparticle, poly(lacticacid)

45

46 Highlights

- 47 48
- PreS1 peptide derived from HBV surface protein was successfully adsorbed on PLA NP
- Vectorized Pam₃CSK₄ does not influence the colloidal characteristics of NP-dPres1
- NP-dPreS1 activates murine lymph nodes after subcutaneous administration
- Pam₃CSK₄ adjuvant positively modulates the quality of immune response triggered by NP
- NP-Pam₃CSK₄-dPreS1 induces the most efficient murine IgG for *in vitro* neutralization

53 1. Introduction

54

55 Nearly 3.5% of the world population suffer from chronic hepatitis B virus (HBV) (Polaris Observatory 56 Collaborators, 2018) and predictions for the future are not optimistic, as the mortality rate is increasing and outweighing those of tuberculosis, malaria, and HIV (Bray et al., 2018; Graber-57 58 Stiehl, 2018). Even though existing prophylactic vaccines widely protect the rich countries 59 benefiting from it, they present some drawbacks that make it difficult to implement in developing 60 countries: cold storage, a strict three-shot immunization schedule, the failing to induce an effective 61 antibody (Ab) response in 5-10% of healthy "non responders" (Saco et al., 2018) and the 62 emergence of vaccine escape strains (Qin and Liao, 2018). New potent vaccines have to be 63 considered via (i) the use of drug delivery systems to optimize the administration (Zhu et al., 2019), 64 (ii) the modification of the antigen (Ag) sequence for a more immunogenic portion, (iii) the adjuvantation to enhance the immune response (Fanning et al., 2019; Lang et al., 2019; Meng et 65 66 al., 2019). This has been confirmed recently in the course of SARS-CoV-2 countermeasures, when 67 the numerous failed clinical trials have highlighted the importance to generate innovative and 68 highly-immunogenic formulations through efficient systems (Monrad et al., 2021; Peplow, 2021).

69

70 Multiple drug delivery systems (*i.e.* virus-like particles, nanoparticles) and innovative gene-based 71 formulations (DNA/RNA vaccines) have been largely exploited in vaccinology for their added value 72 compared to a conventional soluble Ag (Fries et al., 2020) and thus, for their ability to face a global 73 health emergency, such as the ongoing SARS-CoV-2 pandemic (Brisse et al., 2020). Nanoparticle 74 (NP) systems aim at overcoming the limitations of conventional delivery by : improving the stability 75 and solubility of molecules, facilitating the transport across membranes to modulate the traffic and 76 the delivery of vaccine components throughout the lymphatic tissue (Mitchell et al., 2020; Schudel 77 et al., 2019), thus improving the Ag presentation and overall the prophylactic activity (Fries et al., 78 2020). By efficiently targeting the lymph nodes (LN), nanovaccines induce a more persistent B cell 79 immune response compared to conventional forms (Singh, 2021). Biodegradable polymeric NP are 80 one of the most extensively studied in the field for their low immunogenicity and biocompatibility 81 and our previous results showed the polylactic acid (PLA) as a great polymer candidate for such 82 scaffolds (Coolen et al., 2019; Pavot et al., 2016; Rességuier et al., 2017). They offer a versatile 83 platform for vectorization (Pavot et al., 2013) and/or adsorption (Dalzon et al., 2016) of various 84 molecules (Ag, immunomodulators) and are promising candidates for vaccine development 85 (Gutjahr et al., 2016; Peres et al., 2017).

86

87 Yan et al elegantly identified the myristoylated oligopeptide (amino acids sequence 2-48) named 88 PreS1 from the large surface protein, as the molecule enabling HBV to enter into the hepatocyte 89 (Yan et al., 2012) through a high-affinity binding with the sodium taurocholate cotransporting polypeptide (NTCP) receptor (Meier et al., 2013). The inhibition of this PreS1-NTCP interaction 90 91 effectively blocks HBV and hepatitis D virus (HDV) infections (Ni et al., 2014; Ye et al., 2016). 92 Bulevirtide (also known as myrcludex B), the GMP-version of the myristoylated (2-48) PreS1, was 93 recently approved in Europe for HDV treatment (Cheng et al., 2021). Yato et al suggested the 94 potential ability of a vaccine Ag containing the preS1 region to overcome the weakness of current hepatitis B vaccines (Yato et al., 2020). Indeed, monoclonal Abs against the conventional HBsAg 95 96 protein cannot neutralize HBV in case of vaccine escape mutations such as the G145R mutation 97 which causes a conformational change in the HBsAg antigenic loop. This lack of neutralization is 98 not observed with Abs against PreS1/2-48. Two other studies recently highlighted also the added 99 value of using this PreS1 domain by bypassing the host immune tolerance observed with HBsAg 100 vaccines (Bian et al., 2017; Dembek et al., 2018). Inducing specific anti-PreS1 Abs may therefore 101 be optimal when the conventional HBV vaccine targeting the main antigenic region (AR). Here, a 102 derived PreS1 (dPreS1) sequence of the virus was successfully nanovectorized in PLA NP and 103 investigated.

104 As an adjuvant, the Toll-Like-Receptor (TLR) 1/2 agonist Pam₃CSK₄ was included in the 105 nanosystem for an enhanced magnitude and durability of the immune response (Pulendran et al., 106 2021). The literature demonstrates the efficacy of synthetic TLR ligands on rodents and non-human 107 primates by promoting a more durable and stronger Ab response to vaccination with live or heat-108 killed viruses (Hennessy et al., 2010; Kasturi et al., 2011). More specifically for HBV, Heplisav-B is 109 an FDA-approved vaccine composed of HBsAg mixed with a synthetic oligonucleotide cytosine 110 phosphor-guanine (CpG) that stimulate innate immunity through TLR9 (Lee and Lim, 2021). In case 111 of TLR2, multiple experimental evidences show the promising adjuvanticity of Pam₃-related ligands 112 as strong inducers of virus-specific T and B cells in mice (Dou et al., 2020; Lee and Park, 2018; 113 Rammensee et al., 2019). Desmares et al (Desmares et al., 2022) illustrate recently the direct 114 inhibitory anti-HBV phenotypes induced by this TLR2 ligand itself supporting our assumption of an 115 added value in using Pam₃CSK₄. Despite the numerous preclinical and clinical studies applied to 116 TLR ligands, their mechanisms of action suggest failures related to toxicity issues limiting a human 117 use (Anwar et al., 2019).

118

119 For all these reasons, we propose a highly immunogenic doubly-functionalized NP vaccine against 120 HBV, incorporating both the unique dPreS1 domain and a TLR1/2 ligand for adjuvanticity. We have 121 previously discussed the successful chemical entrapment of Pam₃CSK₄ in PLA NP (Lamrayah et 122 al., 2019). Here, in order to validate the immunological relevance and the effective design of our 123 NP-dPreS1vaccine, we first performed in silico structural and physicochemical modulations. Then, 124 the immune responses elicited by a prime-boost administration were evaluated in comparison with 125 different formulations. The NP-Pam₃CSK₄-dPreS1 (hereafter designated NP-P-dPreS1) system 126 aims at stimulating the production of neutralizing Abs directed specifically against the dPreS1 127 epitope all the while favorably modulating the immune response for an optimal immune protection. 128 Finally, the in vitro neutralization capacity of the generated antibodies was tested to evaluate their 129 antiviral efficacy. Overall, this work offers a promising platform for a novel anti-HBV vaccine and 130 maybe a potential strategy to achieve a functional cure in a therapeutic context, as it induces a high 131 level and persistent anti-PreS1 response that could help in clearing circulating HBV virions as well 132 as infected hepatocytes in vivo by various mechanisms (e.g., neutralization, ADCC, etc..).

133

134 2. Materials and methods

135 **2.1. Preparation and characterization of formulations**

PLA NP were prepared by nanoprecipitation technique as previously described (Lamalle-Bernard et al., 2006). Briefly, the polymer was dissolved in acetone and this solution was added dropwise to an aqueous solution under 250 rpm stirring. Organic solvents were then removed under reduced pressure at 30°C with a Rotavapor R-300 (Buchi, France).

Pam₃CSK₄ (purchased from InvivoGen, San Diego, CA, USA) was incorporated during the NP
synthesis, following the procedure already described (Lamrayah et al., 2019). The final
concentration of Pam₃CSK₄ was 2.5 µg/injection.

143 The near infrared DiR XenoLight Fluorescent Dye (DiIC18(7), 1,1'-dioctadecyltetramethyl 144 indotricarbocyanine lodide), purchased from Perkin Elmer (Waltham, MA, USA), was incorporated 145 during the NP synthesis step at a fluorophore:PLA ratio of 0.02% and was manufactured by 146 Adjuvatis (Lyon, France).

147The 2-48 AA sequence of the HBV PreS1 peptide with a myristoylation in N-terminal148(GTNLSVPNPLGFFPDHQLDPAFRANSNNPDWDFNPNKDHWPEANKVG) was produced by149GenScript Biotech (Piscataway, NJ, USA). The purity was higher than 98% and the observed

150 molecular weight was 5499.5 g/mol. For the preparation of dPreS1 PLA NP, the lyophilized dPreS1 151 was rehydrated in PBS 1X (Thermo Fisher Scientific, Waltham, MA, USA) at the desired 152 concentration and added volume to volume in NP, NP(DiR) or NP-Pam₃CSK₄ suspensions, previously diluted at 20 mg/mL of polymer in DPBS 1X. The passive adsorption reaction occurred 153 within 2 h at room temperature with moderate overhead stirring. The coating efficiency was 154 assessed by measuring the unbound peptide. A certain volume of dPreS1 PLA NP was centrifuged 155 156 15 min at 15,000 xg and the absorbance of the supernatant was measured at 280 nm using a 157 Tecan i-control Infinite M1000 (Tecan, Männedorf, Switzerland). The results were compared to a calibration curve previously established (correlation coefficient of R²=0.998). The encapsulation 158 efficiency was calculated as the following formula: EE (%) = (1 - amount of dPreS1 in supernatant 159 160 / Total amount of dPreS1) x 100. The final concentration of dPreS1 was 20 µg/injection.

The average hydrodynamic diameter and the size distribution (mentioned as polydispersity index or PDI) of formulations were determined by dynamic light scattering at 25°C and a scattering angle of 173° using a Zetasizer Nano ZS (Malvern, UK). The colloidal suspensions were a hundred time diluted in filtrated 1 mM NaCl solution and each value was the mean of four independent measurements. The electrophoretic mobilities (mentioned as zeta potential) were measured by laser Doppler velocimetry using the same equipment, at a scattering angle of 12.5°.

For KLH-dPreS1 formulation, 200 µg of dPreS1 was conjugated with 200 µg of mariculture Key
Limpet Hemocyanin (mcKLH) in EDC conjugation buffer, following the manufacturer's instructions
(Imject[™] EDC mcKLH Spin Kit, Thermo Fisher Scientific, USA). The mix was incubated for 2 h
statically at room temperature. The conjugate was purified by successive desalting steps to remove
the non-reacted crosslinker.

172 **2.2. Molecular Modeling**

173 MD simulations were performed using the Amber 14 force field implemented in the Molecular 174 Operating Environment (MOE) software (ChemComp). This type of atomistic simulation allows for 175 the modeling of various system sizes but is less efficient with larger systems, especially when the total number of atoms reaches millions, which is the amount typically found in a 150 nm diameter 176 177 NP. Thus, in order to mimic the behavior of a PLA NP while keeping the total number of atoms in 178 the simulation under a reasonable limit, we chose to use instead a smooth flat layer of PLA with a 179 35 Å thickness, located in a replicative cell measuring 60x60x120 Å. To simulate the NP PLA 180 surface, we used PLA molecules constructed as linear repetitions of 50 units of Lactic Acid 181 monomers (LA). Those molecules were generated using the "Build" module of the Material Studio 182 software (Biovia). Water molecules were added for the solvation of the replicative cell. The 183 simulation box was then thoroughly minimized using the Forcite module of Material Studio. The 184 PLA molecules and the replicative cell were then exported in .pdb format and imported into the 185 MOE software. Then, a molecular model of the dPreS1 peptide was constructed. As no single 186 relevant template could be found in the PDB database, we used the online software I-TASSER 187 (Iterative Threading ASSEmbly Refinement) from the Zhang Lab ("I-TASSER server for protein 188 structure and function prediction," n.d.). Five models were computed using the software default options, and the best one was further imported into MOE. The lipidic myristoyl anchor of dPreS1 189 190 was constructed using the MOE Build module and the molecule was briefly minimized using the 191 Amber 14 EHT force field. The final model was added to the PLA periodic cell and located close to 192 the PLA surface. The geometry of all the molecules, bonds and charges were checked using the Structure Preparation tool in MOE, to start molecular simulations. Water molecules, Na⁺ and Cl⁻ 193 194 ions were added to simulate a 0.1 M ionic force, and pH was set at 7.4. The total number of atoms 195 in the simulation cell was 38,403. Standard Amber 14 EHT parameters were used for the molecular 196 dynamics. A quick minimization was performed prior to the start of the MD simulations. After a

preliminary equilibration phase, a 200 ns molecular simulation was performed. A frame was savedevery 20 ps, leading to a total number of 10,000 frames.

199

200 201

2.3. Docking

202 The docking experiments were performed between the CSKKKK peptidic part of the Pam₃CSK₄ 203 lipopeptide and the 47 AA sequence of PreS1. The protocol involved a first global approach step 204 of peptide/protein docking using the Haddock (High Ambiguity Driven protein-protein DOCKing) 205 web server (van Zundert et al., 2016) and the Cluspro 2.0 web server ("ClusPro 2.0: protein-protein 206 docking," n.d.). No constraints about the binding area were specified and all the residues of the 207 CSKKKK peptide were treated as flexible. The two servers produced 42 poses, which were 208 selected and sent for further docking refinement to the Rosetta docking software, version 3.12 209 (Chaudhury and Gray, 2008). All initial Haddock and Cluspro pose were refined 100 times with 210 Rosetta, leading to 4200 refined poses. The top ten results were evaluated with the Rosetta 2015 211 scoring function (Park et al., 2016) and exhibited a mean average reweighted score of 60.1 Rosetta 212 Energy Units.

213

214 215

2.4. Electron microscopy observations

Morphology of formulations was visualized through a transmission electron microscope (JEM-2100F, JEOL, Japan). For sample preparation, NP solutions were diluted ten times in water and deposited on a grid. The excess liquids were absorbed using filter paper and the grids were negatively stained by sodium silicotungstate for contrast. Images were recorded at a magnification between x10K and x20K.

221

222 **2.5.** *In vivo* imaging of fluorescent NP biodistribution

223 Ten-week-old SKH1 female mice (n=4 per group) were bred at Charles River Laboratories 224 (L'Arbresle, France) and housed at the AniCan animal facility of the CRCL (Cancer Research 225 Center of Lyon, France). The experiments were approved by the relevant local ethics committee 226 (CECCAPP CLB 2017 006) and were conducted according to the rules for the care and use of 227 laboratory animals. The mice received a single subcutaneous injection in the neck of 0.96 µM 228 DiR/mouse loaded in NP or in dPreS1-NP, corresponding to 20 µg of dPreS1/mouse (injection 229 volume: 100 µl). Whole body fluorescence was recorded at determined time points (2, 24 h and 7 230 days after injection) using the FMT4000 fluorescence tomography imaging system (Perkin Elmer, 231 USA). On the day of imaging, mice were anesthetized under 4% isoflurane and positioned in the 232 FMT system imaging chamber. Filter set was chosen depending on the fluorophore parameters, 233 with an excitation at 750 nm and a collection at 782 nm. The collected fluorescence data were 234 reconstructed by TrueQuant software for the quantification of three-dimensional fluorescence 235 signals. Acquired images were analyzed by drawing regions of interest (ROI). The total amount of 236 fluorescence (in pmoles) per ROI was generated for all studies, and then percentage of residual 237 fluorescence was calculated as: residual fluorescence (%) = [amount of fluorescence at tx / amount 238 of fluorescence at t0] x 100.

239 **2.6. Lymph nodes immunofluorescence staining**

Seven-to-eight-week-old mice were divided into five groups of nine animals and received a single
immunization of the different formulations in a 100 µl final volume of PBS 1X, subcutaneously above
the left inguinal LN. Mice were retro-orbitally bled before immunization and 7-, 14-, 21- and 28-days
post-immunization. Three mice of each group were euthanized at 7-, 14-, 21- and 28-days postimmunization to harvest the draining inguinal LNs. They were snap frozen in cryomolds full of

245 Optimal Cutting Temperature compound (Tissue-Tek O.C.T, Sakura Finetek, USA) placed on dry 246 ice and stored at -80°C until cryosection. Serial sections, 8 µm thick, were collected through each 247 LN using a cryostat microtome (cryostat CM3050, Leica Biosystems, Germany). The central section 248 and the two sections spaced 250 µm apart were fixed on glass slides with acetone. They were first 249 incubated with a rat anti-mouse IgD primary Ab (Biolegend, San Diego, CA, USA) to detect B cells 250 follicles and with biotinylated PNA (Vectors Laboratories, Burlingame, CA, USA) to detect GC. They 251 were then incubated with goat anti-rat IgG secondary Ab conjugated with Alexa Fluor 488 (Thermo 252 Scientific, Rockford, IL, USA) to reveal anti-IgD (green), and with Streptavidin conjugated with 253 DyLight 550 (Thermo Scientific, Rockford, IL, USA) to reveal biotinylated PNA (red). Images of LN 254 sections were captured using an inverted microscope (Nikon Ti-E microscope, Nikon Instruments 255 Inc., Melville, NY, USA) equipped with a 4x objective. Measurements of B cells and GCs areas 256 were carried out using Image J software (U. S. National Institutes of Health, Bethesda, MD, USA). 257 GCs were manually counted.

258 2.7. CXCL13 ELISA

259 The mouse CXCL13/BLC/BCA-1 DuoSet (R&D Systems, USA) was used for quantification of 260 CXCL13 in sera samples, according to the manufacturer's recommendations. Briefly, ninety-six-261 well Nunc maxisorp plates were coated with 100 µL of Capture Ab at 1 µg/mL, overnight at room 262 temperature. Capture Ab excess was eliminated and plates were washed 3 times with PBS/0.05% 263 Tween-20 (PBS-T20) using a Thermo Scientific autoplate washer. Plates were blocked with 300 264 µL of Block buffer (R&D Systems, USA) for 1 h at room temperature, to prevent non-specific binding 265 of the CXCL13 protein. Fresh serum samples from immunized mice were diluted five times in 266 Reagent Diluent (RD) (R&D Systems, USA). A seven-point standard range using two-fold serial 267 dilutions in RD of the recombinant mouse BLC/BCA-1 Standard was realized. Then, 100 µL of each 268 sample and standard in duplicate were incubated on washed plates for 2 h at room temperature. 269 Wells were washed and incubated 2 h at room temperature with Detection Ab diluted at 25 ng/mL 270 in RD. Plates were washed again and incubated with 100 µL per well of diluted Streptavidin-HRP 271 in RD (1:200) for 20 min at room temperature, in the dark. Plates were washed again, revealed 272 using 100 µL per well of tetramethylbenzidine (TMB) substrate (BD BioSciences, USA) and stopped 273 using 2N H₂SO₄ (Merck, USA). The optical density (OD) at 450 nm (OD₄₅₀) with a correction at 620 274 nm was measured using a Thermo Scientific plate reader spectrophotometer.

275 **2.8. Immune evaluation of formulations in naive mice**

CB6F1 female mice were bred at Charles River Laboratories (L'Arbresle, France) and housed at the Plateau de Biologie Expérimentale de la Souris (PBES, Lyon, France). The experiments were approved by the relevant local ethics committee (CECCAPP_ENS_2017_017) and were conducted according to the rules for the care and use of laboratory animals.

280 Seven-to-eight-week-old mice were equally distributed into six groups in the indicated experimental 281 groups. They were subcutaneously immunized (above the left inguinal LN) with NP-dPreS1, NP-282 Pam₃CSK₄-dPreS1, soluble dPreS1, NP as negative control and KLH-dPreS1 as positive control. 283 The injection scheme followed a prime boost injection strategy, based on Aditec consortium 284 protocol for harmonization with three immunizations each three weeks. A sixth group received a 285 retro-orbitally intravenous injection of NP-Pam₃CSK₄-dPreS1, following the same scheme of 286 immunization. Components were administered equally for each group, namely 2.5 µg of dPreS1, 287 20 µg of Pam₃CSK₄, 10 mg/mL of PLA and all formulations were diluted in PBS 1X for a 100 µl final 288 volume of injection.

Then, a heterologous boost was performed at W27, with a unique formulation subcutaneously injected for all groups, meaning dPreS1 NP. Control groups received a homologous injection, 291 meaning NP and KLH-dPreS1 respectively as negative and positive controls, to maintain the 292 reference consistent.

Mice were retro-orbitally bled before immunization and at determined times (W2, 4, 6, 8, 11, 13, 17, 22, 27, 32, 44 and 47 weeks post-immunization). The blood samples were heated 30 min at 37°C for coagulation, then centrifuged twice 10 min at 16,000 ×g and sera were stored at -20°C for further analyses. Mice were weighted regularly to verify the potential general toxicity of immune stimulation in naive organisms and the evolution rate for each group was measured as: ((W47 weight - W7 weight)/ W7 weight) x 100 = evolution rate (%). Mice were sacrificed at W47 by cervical dislocation.

300 2.9. dPreS1 specific IgG ELISA

301 Collected sera were tested for the quantification of dPreS1 specific IgG, IgG1 and IgG2a by 302 enzyme-linked immunosorbent assay (ELISA). Ninety-six-well Nunc maxisorp plates 303 (ThermoFisher Scientific, USA) were coated with 100 µL of dPreS1 at 1 µg/mL, overnight at room 304 temperature. The dPreS1 excess was eliminated and plates were blocked with 200 µL of 10% non-305 fat dry milk in PBS for 1 h at 37°C to prevent non-specific binding of the Abs. Plates were washed 306 3 times with PBS/0.05% Tween-20 (PBS-T20) using a Thermo Scientific autoplate washer. Serum 307 samples from immunized mice were serially diluted in Dulbecco's PBS (DPBS) containing 1% (w/w) 308 of Bovine Serum Albumin (Euromedex, Souffelweyersheim, France). Then, 100 µL of each sample 309 in duplicate were incubated on blocked plates for 1 h at 37°C. Wells were washed three times and 310 incubated 1 h at 37°C with anti-mouse IgG-HRP (horseradish peroxidase) conjugate (1:10,000) 311 from Southern Biotech, Birmingham, AL, USA (ref 1030-05). Plates were washed again, revealed 312 using 100 µL per well of tetramethylbenzidine (TMB) substrate (BD Biosciences, USA) and stopped 313 using 1N sulfuric acid. The optical density (OD) at 450 nm with a correction at 620 nm was 314 measured using a microplate reader spectrophotometer (Multiskan FC, Thermo Fisher, USA). The 315 limit of detection was evaluated using an unconjugated mouse monoclonal anti-Hep B PreS1 (ref 316 SC-57761) from Santa Cruz Biotechnology, Inc. (Dallas, TX, USA).

Sera from W0, 11, 22, 32 and 47 were also evaluated for the presence of dPreS1 specific IgG1
and IgG2a, using the same protocol than for total IgG, except the last incubation with IgG1-HRP
(ref 1070-05) or IgG2a-HRP (ref 1080-05) conjugate, both from Southern Biotech.

320 The avidity indices of IgG at W6, 11, 22, 32 and 47 were determined by the Ab-Ag binding 321 resistance to 8M of urea. Samples were prediluted to give an OD₄₅₀ readout of between 1.0 and 322 1.5, with a correction at 620 nm, and were added to dPreS1 coated plates. Then, they were washed 323 three times with either PBS-T20 or 8 M urea in PBS-T20, before incubating with anti-mouse IgG-324 HRP. Samples were developed with TMB as described above. The avidity index (in percent) was 325 calculated as the ratio of absorbance of bound Ag in the plate with and without urea as denaturing 326 reagent = (OD urea/OD PBS-T20) x 100. Index values exceeding 50% were ascribed a high avidity, 327 those between 30 and 50% were ascribed intermediate avidity, and those below to 30% were 328 ascribed a low avidity.

329 **2.10. Cell culture**

330 *In vitro* experiments were performed with a HepaRG cell line (Gripon et al., 2002). Cells were 331 maintained in William's E medium (Life technologies, USA) supplemented with 10% fetal calf serum 332 (FCS) (Eurobio, Hyclone), 100 U/mL of penicillin and 100 μ g/mL streptomycin (Gibco, Life 333 technologies, USA), 2 mM GlutaMAX (Gibco, Life technologies, USA), 5 μ g/mL of human insulin 334 solution (Sigma-Aldrich, USA) and 5.10⁻⁵ M hydrocortisone hemisuccinate (Serb, France) at 37°C in humidified incubator and 5% CO₂ for two weeks. Two additional weeks are needed for differentiation in standard medium supplemented with 1.8% DMSO (Sigma-Aldrich, MO, USA).

337 **2.11. Neutralization of HBV by mice antisera**

338 Sera from W11, 27 and 47 were diluted into infectious mediums. This last medium was prepared 339 using a differentiation medium containing 4% PEG 8000 (Sigma-Aldrich, MO, USA) and infected 340 with HBV genotype D inoculum prepared from HepAD38 (Lucifora et al., 2018). The infectious 341 medium containing immunized mice sera were maintained during 16 h on HepaRG cells at 37°C 342 and 5% CO₂. Cells were then washed with PBS and the medium of differentiation was added. All 343 in vitro experiments were stopped one week after infection and treatment with immunized mice 344 sera. Myrcludex was used as positive control (0.5 ng/mL and 5 ng/mL) after determination of IC50 345 and IC90 on studied cell lines.

346 2.12. HBe antigen ELISA

From cell culture supernatants, secreted HBeAg and the amount produced were analyzed by ELISA, using a chemiluminescence immunoassay kit (Autobio, China) according to the manufacturer's instructions.

350 2.13. Statistical analyses

Statistical analyses were performed using GraphPad Prism Version 9.0 software. For each dataset,
 normality or lognormality was assessed via d'Agostino & Pearson test or Shapiro-Wilk when n was
 too small and further analyzed accordingly. P<0.05 was considered significant. Differences
 between groups were analyzed as described in figure legends.

355

356 **3. Results**

357 358

359

3.1. Design and molecular dynamics studies of HBV-specific NP formulations

360 PLA NP were prepared according to an adjuvant-free nanoprecipitation method (Lamalle-Bernard 361 et al., 2006) and Pam₃CSK₄ was simultaneously entrapped in PLA NP as previously described (Lamrayah et al., 2019). Secondly, dPreS1 peptide (2-48 AA construct from a consensus sequence 362 363 with a N-terminal myristoylation) was added at the surface of the NP by passive adsorption (Dalzon 364 et al., 2016; Pavot et al., 2016). The functionalization of PLA NP by Pam₃CSK₄ and dPreS1 did not 365 significantly change the colloidal size (150 nm), the surface charge (-65 mV) and the dispersity 366 (0.1) (Fig. 1B). Additionally, the NP morphology observed by transmission electron microscopy was 367 also unchanged (Fig. S1). For the drug loading, the encapsulation efficiency of Pam₃CSK₄ was 100%, as previously described by the authors (Lamrayah et al., 2019), for a 90% adsorption 368 369 efficiency of dPreS1 (passively measured by the absorbance of the unbound peptide, unshown 370 data). The weights ratio of Pam₃CSK₄, dPreS1 and PLA in the final formulation was fixed at 371 0.12:1:30.

- 372
- 373



Fig. 1. NP formulations synthesis was validated and molecular dynamics confirmed the 375 376 absence of interaction between vectorized dPreS1 and TLR2 agonist. (A) dPreS1 construct (2-48 AA with N-ter myristoylation) is derived from the HBsAg-L surface protein. (B) Standard 377 378 colloidal properties of formulations (size, PDI and surface charge) were verified in order to control 379 the homogeneity and stability. (C) Picture extracted from video S1 at the end of the dPreS1-PLA 380 surface interaction simulation showing that the biologically relevant epitope of dPreS1 (9-15 AA 381 sequence, showed in cyan) has a stable conformation and is totally accessible for intermolecular 382 interactions after the adsorption. The lipidic anchor is in yellow, the rest of the peptide in dark blue, 383 PLA chains in dark grey, red and light grey for carbon, oxygen, and hydrogen atoms respectively. 384 The boundaries of the periodic cell are highlighted in dark green. PDI = polydispersity index. 385

386 The PreS1 domain of HBsAg (Fig. 1A) is known to specifically bind to the NTCP receptor located 387 at the basolateral side of hepatocytes, allowing the viral entry to the cell. More precisely, both the myristoylated tail (on glycine residue at position 2) and the highly conserved motif 9-NPLGFFP-15 388 389 are crucial for receptor binding and infectivity (Glebe et al., 2005). The behavior of the dPreS1 390 peptide onto the surface of the PLA NP was thus investigated by performing Molecular Dynamics 391 (MD) simulations. Previously published molecular modeling studies evidenced the major role of 392 fatty acid chains for the interaction of biological molecules with PLA NP (Lamrayah et al., 2019; 393 Megy et al., 2020). Consequently, the MD was initiated with the lipidic anchor of dPreS1 (myristic 394 acid) directly facing the PLA surface. After a preliminary equilibration phase, a 200 ns molecular 395 simulation was performed. As illustrated in the video (Video S1), the biologically relevant epitope 396 (9-15 NPLGFFP, in cyan) was not entirely accessible for intermolecular interactions at first, and 397 progressively undergone several adjustments in its conformation, leading to an improved 398 accessibility of the relevant epitope after 100 ns of simulation time. The simulation showed the 399 binding process is possible, and the interaction between dPreS1 and PLA NP evidenced the 400 stabilization of the epitope in an accessible and opened conformation (Fig. 1C). Noteworthy, the lipidic anchor stayed in close contact with the PLA chains during the complete simulation without 401 penetrating the layer, and both their respective conformations were slightly modified, suggesting 402 403 hydrophobic interactions. Previous findings demonstrated that the three palmitic chains of 404 Pam₃CSK₄ are buried into PLA surface, limiting hindrance of both lipidic parts in the final formulation 405 (Lamrayah et al., 2019). Concerning both peptidic parts, the absence of interactions which could 406 lead to unexpected results in terms of epitope stability or accessibility had to be verified. In this 407 regard, docking experiments were performed between the CSKKKK peptidic part of Pam₃CSK₄ and 408 the 47 AA sequence of dPres1. All the results exhibited high positive scores, with a top ten average 409 reweighted score of 60.1 Rosetta Energy Units, demonstrating that there is absolutely no possible

interaction between the peptides of the respective molecules (data not shown). As a result, dPreS1
and Pam₃CSK₄ did not interact in our system and thus, neither the structure nor the stability of the
dPreS1 epitope could be affected by the presence of Pam₃CSK₄. Thus, the chemical stability of the
NP-P-dPreS1 formulation was validated and results confirm that the relevant epitope (9-15
NPLGFFP) is unchanged and available for recognition by the lymphatic system.

- 415
- 416 417

3.2. PLA NP efficiently accumulates in the draining lymph nodes and the TLR adjuvant influences the kinetics of germinal center formation

418

419 The importance of germinal center (GC) formation for generating a high-quality and robust Ab 420 response is largely highlighted in the literature (Arulraj et al., 2019; Victora and Nussenzweig, 421 2012). Here, since the antiviral strategy is based on the induction of a strong neutralizing Ab 422 response, it appears essential to explore the early uptake of the formulations following 423 subcutaneous (s.c) administration as well as the subsequent effects in the secondary lymphoid 424 organs (i.e. LN). Recent studies have demonstrated the ability of nanovectors to reach the LN after 425 s.c injections (Havenar-Daughton et al., 2019; Singh, 2021). Precisely, NP with a diameter of 100 426 nm and more are entrapped at the injection site by peripheral DCs available in the local interstitial 427 matrix and carried to LN for B cell presentation (Schudel et al., 2019). Thus, the lymphatic 428 biodistribution after s.c administration of the PLA nanovaccines was monitored, and the GC 429 formation, underlying the immune activation within the draining LNs (dLN), was assessed.

430

431 For this, the biodistribution profile of fluorescent PLA NP vectorizing the near infrared DiR probe 432 was investigated using a whole-body 3D fluorescence tomography. These fluorescent NP(DiR) are 433 similar to the active nanovaccine candidates NP(DiR)-dPreS1 in terms of physicochemical 434 characteristics (Fig. S2A) and in the elimination kinetic profile (Fig. S2B and S2C). SKH1 mice were 435 monitored for seven days after a unique s.c injection in the neck region and the detected 436 fluorescence was quantified at 2, 24 hours and 7 days post injection. Noteworthy, the choice of 437 both a hairless strain and a near infrared probe prevented the bias of autofluorescence. A whole-438 body observation following two axes (dorsal and sagittal) revealed an efficient diffusion and 439 accumulation of the NP to the dLN (Fig. 2). More specifically, these data showed the PLA 440 nanoplatform yields a prolonged and diffused uptake through the lymphatic system, reaching the 441 dLN from 2 hours onwards. The analysis 7 days post immunization also highlighted the persisting 442 biokinetic profile of the NP at the injection site as well as the greater diffusion to non-dLN. 443



444

Fig. 2. Biodistribution profile of the fluorescent NP-dPreS1 following subcutaneous
administration shows prolonged retention time and diffusion. A single s.c injection (neck
region, the injection site is shown by the asterisk) was performed on SKH1 female mice with
fluorescent NP(DiR)-dPreS1. The fluorescence intensity (750/780 nm) was monitored for 7 days

using FMT imaging (Fluorescence Molecular Tomography, FMT4000, Perkin Elmer). Two
observation axes were imaged to prove the high penetration score of the fluorescent PLA NP after
s.c administration: through the lymphatic system, PLA NP can reach the proximal (white arrows)
and distal (yellow arrow) LN.

453

The first immunization in a protein prime-boost regimen is critical for the subsequent unfolding of 454 455 the immune response. To confirm the nanovaccine draining uptake and validate the immune 456 activation in LN, CB6F1 mice were immunized once subcutaneously with NP-dPreS1 or NP-P-457 dPres1 formulations and LN were harvested at predetermined time points for histological analyses 458 (Fig. 3A). NP and soluble dPreS1 injections were both used in control groups. Classically, the GC 459 formation kinetic is described as fully established 7 days after immunization by a soluble Ag (De 460 Silva and Klein, 2015), but considering the prolonged retention effect of nanoparticulate 461 formulations, three mice per group were euthanized at days 14, 21 and 28 post-immunization for a 462 more precise understanding of the biokinetics. The draining inguinal LNs were stained to identify 463 the follicular B cells (using IgD Ab) and the mature GCs (using peanut agglutinin (PNA)). NPdPreS1 showed a GC response at day 21 post-immunization (Fig. 3B) which decreased at day 28 464 465 when in parallel it appeared for NP-P-dPreS1 (Fig. 3C).

466

To understand this delay, the B-cell-recruiting factor CXC chemokine ligand 13 (CXCL13)
expression was monitored in mice serum. This chemokine plays an important role in B cell follicle
migration (Havenar-Daughton et al., 2016). Serum levels of CXCL13 increased at day 14 only for
NP-P-dPreS1 (Fig. 3D).

471 472





Fig. 3. Draining lymph node responses after a unique s.c administration reveals distinct GC
kinetics and numbers. (A) Microscopic observation of GC formation over time. LN were harvested
and some cryosections were stained with anti-IgD for follicular B cells (*green*) and PNA for GCs
(*red*). Scale bar = 500 µm. (B) Analyses and number of GC area 21 days after immunization. (C)
Analyses and number of GC area 28 days after immunization, only for nanovaccines (NP-dPreS1
and NP-P-dPreS1). (D) Blood levels of CXCL13 monitored during 28 days.

482 483

484

3.3. Nanovaccines provides a long-lasting and strong humoral response in naïve mice

485 Next, to assess the ability of the nanovaccines to induce a specific anti-dPreS1 response, an 486 immunization assay with naïve mice following a prime boost regimen was performed and the serum 487 IgG titers were longitudinally investigated over one year. CB6F1 female mice were randomly 488 distributed (n=6 per group) and were subcutaneously immunized three times each three weeks as 489 described in Methods and in Fig. 4A. NP-dPreS1 and NP-P-dPreS1 nanovaccine candidates were 490 compared with soluble dPreS1, KLH-dPreS1 (as positive immunogenic control) and NP (as vector 491 control) (Fig. 4B).



Fig. 4. Detailed study design. (A) Five experimental treatments were formulated and 494 immunologically evaluated on naive CB6F1 mice. At times of injection, all formulations had 495 equivalent quantities of NP (20.10¹²/mouse), Pam₃CSK₄ (2.5 µg/mouse) and dPreS1 (20 496 497 µq/mouse). NP and KLH-dPreS1 conditions respectively represent negative and positive controls. 498 (B) Mice were kept in experiment during 47 weeks with regular blood analyses to investigate the 499 immune responses after NP-based formulation injections. The following immune parameters were 500 monitored: total anti-dPreS1 IgG, IgG1 and IgG2a titers, Ab avidity, in vitro HBV neutralization 501 efficacy of the antisera. At W27, a final heterologous s.c boost was performed: all mice received 502 the NP-dPreS1 formulation (yellow boost) except for the control groups (KLH-dPreS1 and NP) 503 which received their own formulations. Mice were euthanized at W47 using cervical dislocation. 504

505 The NP-dPreS1 formulation rapidly elicited elevated titers of anti-dPreS1 IgG reaching about 10⁷ 506 during the plateau phase and remaining still high (10⁶) after six months with insignificant difference 507 compared to the positive immunogenic control KLH-dPreS1 (Fig. 5). Soluble dPreS1 was 508 immunologically recognized, which is in accordance with the literature (Bian et al., 2017), but still 509 elicited significantly lower quantities of anti-dPreS1 IgG titers reaching 10⁵ during the plateau phase 510 to decrease by one log six months later. Noteworthy, only 50% of the subjects (3/6) responded to 511 immunization in this group (Fig. S5). The addition of Pam₃CSK₄ as an adjuvant in NP forms decreased by two log the induced specific IgG quantities, overlapping the IgG profile of the dPreS1 512 513 group.

- 514
- 515



Weeks post immunization

Fig. 5. For each group, anti-dPreS1 lgG titer was analyzed on mice sera from W1 post immunization onwards. A dPreS1 specific in-house ELISA (limit of detection = $0.01 \mu g/mL$, see Fig. S3) was developed. Each symbol represents an individual animal and full bars indicate the mean of the group for each timepoint. Statistical analysis was performed by ANOVA test with multiple comparisons and Dunnett's correction using positive control KLH-dPreS1 condition as reference. *alpha=0.05, *p<0.05, ***p<0.001, ns = not significant.*

523

524 To qualitatively describe the immune responses, the avidity and isotype of induced IgGs were 525 evaluated. The avidity index represents the total binding strength of the Ag-Ab interaction and can 526 vary during the immune response depending on the affinity maturation and clonal selection 527 processes. Indexes were measured by the ability of the mice antisera to remain in binding with 528 dPreS1 in the presence of 8M urea as detergent (Badamchi-Zadeh et al., 2016). All formulations 529 had low mean avidity indexes after the first immunization, except for KLH-dPreS1 group which 530 showed an intermediate mean index, unchanged until W22. Since KLH is described as strongly 531 immunogenic due to its high molecular mass, the constant intermediate avidity level is not 532 surprising (Harris and Markl, 1999; Swaminathan et al., 2014). In contrast, the Ab avidity increased 533 progressively with time and reached an intermediate mean index for both NP-dPreS1 (31%) and 534 NP-P-dPreS1 (42%) at W22. Interestingly, when considering results individually, NP-dPreS1 formulation induced the most homogenous response at W22 (5/6 mice over 30%) compared to NP-535 536 P-dPreS1 which offered the highest response (3/6 mice over 50%). Soluble dPreS1 induced Ab 537 with low or none average avidity (Fig. 6A). Further characterization indicates the Th1/Th2 skewing 538 of the immune response via IgG1/IgG2a titer quantification. IgG1 isotype was predominant for all groups, suggesting a major Th2 cell polarization for all vaccine regimens (Bretscher, 2019) (Fig. 539 540 6B).



Fig. 6. Antibody response characterization. (A) Avidity indexes of anti-dPreS1 IgG were measured in mice sera at W6, W11, and W22. Antisera with index values exceeding 50% were attributed a high avidity, those with index values of 30% to 50% were attributed intermediate avidity, and those below to 30% were attributed a low avidity. Each symbol represents an individual animal and full bars indicate the mean of the group for each timepoint. (B) IgG1 and IgG2a subtype titers were monitored in mice W13 and W22 sera. Data are expressed in individual points with bars representing mean.

550 551

552

3.4. TLR2 agonist in the nanosystem generates strong neutralizing Ab

553 The in vitro neutralizing efficiency of the anti-dPreS1 Ab was investigated using infected 554 differentiated HepaRG (dHepaRG) (Marion et al., 2010) and HBeAg was quantified as a parameter 555 of viral infection establishment. While W11 sera from soluble dPreS1 immunization showed a weak neutralization effect (75% of HBeAg at 1/100 dilution), other groups induced strong neutralizing Ab 556 557 against HBV, in a concentration-dependent manner (25%, 24% and 3% of HBeAg for respectively 558 NP-P-dPreS1, NP-dPreS1 and KLH-dPreS1 at 1/100 dilution) (Fig. 7). W27 antisera was 559 investigated similarly and HBV neutralization effect globally decreased (47%, 51% and 7% 560 respectively for NP-P-dPreS1, NP-dPreS1 and KLH-dPreS1 groups). Immunization by soluble 561 dPreS1 did not show any neutralization at W27, echoing the results from W11 (Fig. S5). 562





washed the day after and then HBeAg concentrations were measured by ELISA after 7 days. Myrcludex, a polypeptide with HBV entry inhibitory properties, was use as positive control. Data is expressed as the percentage of HBeAg compared to non-treated (mean (SEM)). Two-way ANOVA was used for group comparisons (at 1/100 condition), with Dunnett's multiple comparison *post hoc* test for analysis of specific differences using either KLH-dPreS1 (black bars) or NP-dPreS1 (blue bar) as reference condition. *alpha=0.05*.

572

573 Surprisingly, the correlation of neutralizing data to the corresponding IgG titers suggests that 574 Pam₃CSK₄ provides a distinct adjuvant-like effect to the immune response. At both W11 and 27, 575 IgG from adjuvanted group showed a comparable neutralization profile as NP-dPreS1 IgG with 576 100-fold lower Ab level (4/6 mice in the red squared area) (Fig. 8).

577



578

Fig. 8. Pam₃CSK₄ modulates the interactions between NP-dPreS1 and the immune system leading to IgG with the strongest neutralizing activity. For each murine serum at W11 and 27, HBV neutralization activity (y axis) is represented according to the corresponding anti-dPreS1 IgG titer (x axis). Red squared areas highlight conditions with high neutralization power and low IgG titer, the most efficient combination. In contrast, gray squared areas highlight conditions with low neutralization power and high IgG titer. Data was gathered separately for easier visualization and each point represents one subject.

586 587

588

589

3.5. Late heterologous boost confirms the essential role of nanovectorization for immune benefit

590 The effect of a heterologous boost at W27 using the NP-dPreS1 candidate was investigated on 591 NP-dPreS1 and NP-P-dPreS1 groups. Both received a s.c injection of NP-dPreS1 while control 592 groups (KLH-dPreS1 and NP) received their respective formulations. The rational was based on 593 the literature suggesting that heterologous prime-boost can be more immunogenic than simple 594 homologous strategy (Kardani et al., 2016; Lu, 2009). Concerning the soluble dPreS1 prime/NP-595 dPreS1 boost group (purple data), IgG titer and avidity index strongly increased without any effect 596 in neutralization activity, confirming the crucial role of the prime immunization (Fig. 9A) (Havenar-597 Daughton et al., 2019). For the NP-P-dPreS1 prime/NP-dPreS1 boost group (blue data), we 598 observed a similar increase of IgG titer and avidity index (Fig. 9B) with, more interestingly, a Th1 599 cell polarization is induced with the emergence of IgG2a at W32 (Fig. 9D). The neutralization 600 activity of these Ab is also greatly impacted with two-fold lower of HBeAg % level (from 46.5% at W27 to 23.5% at W47). Regarding NP-dPreS1 (green data) and KLH-dPreS1 (black data), they 601 602 received their own homologous boost (to maintain the thoroughness of the controls), consolidating 603 the strong existing immune response with highest avidity indexes changing from both medium to 604 high levels. The neutralization level is higher for NP-dPreS1 (from 51.2% to 33.0%), while it is

605 unchanged for KLH-PreS1. Similar to the conventional prime-boost-boost regimen, NP-P-dPreS1

606 group showed high neutralization efficiency while IgG titer is the lowest (blue dots), with 5/6 mice

607 in the most efficient area (Fig. 9C).

608



609

610 Fig. 9. NP-dPreS1 s.c boost immunization on W27 improves the IgG titer and the 611 neutralization effect (A) Anti-dPreS1 IgG profiles from W22 to 47 with increase of titers for dPreS1 612 and NP-P-dPreS1 formulations following final heterologous boost (yellow arrow). Data is expressed 613 as mean (SD) and statistical analysis was performed by ANOVA test with multiple comparisons 614 and Dunnett's correction using positive control KLH-dPreS1 condition as reference. alpha=0.05, 615 *p<0.05, **p<0.005, ***p<0.001. (B) Avidity Index (%) after the final W27 boost also increases for 616 all conditions. Full bars represent the mean for each condition. (C) Interestingly, IgG2a titers 617 increase for nanoparticulate formulations (blue and green) but not for soluble dPreS1 (purple), 618 following the final heterologous boost. (D) Neutralization effect compared to specific IgG titer at 619 W47 hints at the added value of using a TLR adjuvant in therapy. 620

621 Concerning the toxicity profile of nanoformulations, the body weight of the mice was regularly 622 monitored as well as the liver and spleen weights at the endpoint. Any general toxicity regarding 623 these weights couldn't be detectable (Fig. S6). Further studies are intended to precisely describe 624 the toxicological aspect, precisely the immunological consequence of a such treatment.

625

627

626 4. Discussion

In 2016, the World Health Organization stated the HBV elimination for 2030 as a global public health aim, by notably increasing the vaccine coverage from 82% to 90%. The development of novel vaccine technologies is thus crucial to reach it seeing as the current vaccine is sub-optimal (Block et al., 2021; Dolgin, 2022). Here, we have investigated the combination of a multivalent nanoplatform for an optimized Ag presentation with a TLR ligand entrapped in the delivery system to strengthen the neutralizing immune response. First, the nanosystem platform (PLA NP) is 634 synthesized by nanoprecipitation, an easy-to-use and industrially transposable process which 635 enables the production of reproducible and stable formulations. Second, an optimized antigenic 636 peptide, already used in clinical settings and derived from HBsAg, was adsorbed at the surface of 637 the NP. Lastly, since the induction of a strong and durable Ab response to vaccination is highly 638 dependent on the use of effective adjuvants that stimulates the innate immune system (Pulendran 639 and Ahmed, 2011), we chose to vectorize a TLR 1/2 agonist, Pam₃CSK₄ entrapped in the PLA NP 640 core to potentiate the immunization process.

641

642 In the first part of this study, straightforward molecular modeling results show that the choice of 643 Pam₃CSK₄ as the adjuvant and dPreS1 as the protein Ag is highly relevant in terms of chemical 644 mechanics. Indeed, both molecules do not interact with each other when formulated within the NP. 645 More precisely, vectorizing the antigen should be able to expose the dPreS1 epitopes, in presence 646 or not of Pam₃CSK₄, with no structural modification, and subsequently trigger identical 647 conformational Ab responses. This delivery system elegantly increases the immunogenicity and 648 stability of the Ag, by gathering it in nano-scale clusters and decreasing its risks of degradation. 649 Next, via crossed bioimaging and histological evaluations, we documented that an efficient entry of 650 vaccine into the lymphatic vessels can lead to an immune response by favoring the right timing and 651 right location in dLN. The biodistribution profile of fluorescent PLA nanosystems in mice show a 652 long-term stay in the secondary lymphoid organs, which is in favor of a slow and localized delivery 653 of the Ag. Interestingly, the adsorption of dPreS1 on the NP generates higher accumulation of the 654 vaccine in the draining areas but also facilitates the transport across tissues, leading to a greater 655 spatial diffusion over time. These data demonstrate that NP formulations have appropriate colloidal 656 and surface properties required for the dynamic process of immunization (Kelly et al., 2019). 657

658 Next, and despite initial delays in B cell activation and GC formation compared to controls, we 659 showed that the anti-PreS1 IgG titers and avidity indexes reached higher levels for the dually 660 functionalized formulation (NP-P-dPreS1). It is worth noting that both these read outs emphasize 661 the advantage of the nanovectorization on the bioavailability of the antigen and/or TLR1/2 adjuvant, 662 based on the intragroup response heterogeneity for the soluble dPreS1 compared to the NP groups 663 (Fig. S4). The increase in titers and avidity is in accordance with the general (Pedersen et al., 2020) 664 and the TLR-specific (DeFranco et al., 2012) literature, explaining the simultaneous but delayed 665 stimulation of both BCR and TLR signaling pathways. These findings also corroborates with past 666 papers indicating that activation of the TLR2-mediated NF-κB pathway in GC B cells controls GC 667 maintenance and differentiation (Heise et al., 2014). Desmares et al recently confirmed Pam₃CSK₄ 668 specifically induced the activation of this canonical NF-kB pathway (Desmares et al., 2022). 669 Noteworthy, control groups (soluble Ag and NP) activated B cells after being taken in charge by 670 Ag-presenting cells but induced less GC formation and less or no IgG production. In parallel, we 671 report an elevation of serum CXCL13 levels during early immunization in presence of Pam₃CSK₄, 672 explained by the fact that CXCL13 expression occurred as a consequence of NF-kB activation 673 (Kazanietz et al., 2019). Altogether, these data are in favor of an enhanced spatiotemporal access 674 of the antigen and the adjuvant via their vectorization by the PLA NP.

675

676 Subsequently, we confirmed the higher neutralizing capacity of vaccine-specific IgG when the Ag 677 is loaded onto NP versus the soluble form. Here again, in absence of a delivery system, the soluble 678 dPreS1 protein is rapidly exposed to proteolytic enzymes after subcutaneous administration which 679 impeded its presentation to the immune system (Varkhede et al., 2020). This observation validates 680 the previously established belief that drug drivers (Collins et al., 2017), such as NP (Kelly et al., 681 2019), act as an efficient carrier for Ag transit, protection from the environment and presentation to 682 the lymphatic system. Likewise, vectorized dPreS1 is delivered to the LN for recognition and 683 internalization in higher-concentrated clusters, enhancing its immunogenicity (Kasturi et al., 2011).

Although there is no direct experimental explanation for this phenomenon yet, together with the MD
 data these findings prompted us to hypothesize that the doubly-functionalized NP has a synergistic
 effect between the adjuvant and the Ag and that the quality of the Ab prevails over their quantity.
 Future experiments are ongoing to verify this assumption.

688

The neutralization data also show evidence of direct HBV entry inhibition in dHepaRG cells, 689 690 indicating the Ab are effective at recognizing the 9-15 AA sequence of the viral surface protein and 691 obstructing the PreS1/NTCP interaction (Urban et al., 2014). This observation reveals the diversity 692 of B cell Ab-response to dPreS1 Ag in terms of immunoglobulin repertoire and neutralizing activity 693 depending on the vaccine candidate. Next, we prove the added value of Pam₃CSK₄ adjuvant 694 properties since mice immunized with NP entrapping this molecule led to greater humoral immune responses with higher virus-neutralizing Abs compared to NP formulated with dPreS1 only. The 695 696 TLR1/2 ligand reinforces the quality of the immune response via the upregulation of 697 proinflammatory genes subsequently leading to cytokine production and early B cell maturation 698 improvement. Overall, NP-P-dPreS1 vaccine illustrates relevant preventive immunization properties. Again, after the heterologous boost, the presence of the adjuvant elicited the most 699 700 interesting neutralizing activity of induced Ab with the highest neutralization efficiency adjusted to 701 the IgG titers, and sustainable all over the year.

702

703 We have summarized in Fig. 10 the current hypothesis regarding the immune key components 704 responsible for triggering such optimal immune response when combining an adjuvant and a 705 vaccine antigen onto the same polymeric particle. As one of the major challenges in vaccinology 706 these days is to pin point which critical parameters of the innate immunity participates in the 707 programming of the adaptive response, additional analyses of immune responses should be further 708 characterized for full appreciation of the mechanism involved when using such nanoformulations. 709 Typically, the enhanced quality of Ag produced could be studied by cloning and sequencing of B 710 cell to identify Ab sequence with improved neutralizing properties. 711





Fig. 10. Nanoadvantages and suggested immune mechanism triggered by soluble dPreS1
 versus adjuvanted or not NP-dPreS1 formulations. (a) Poor bioavailability of free-form soluble
 dPreS1 translates into suboptimal Ab production with late activation in dLNs of the immune cells.

(b) LN trafficking and Ag immunogenicity: Nanovectorization gives rise to high-concentrated
clusters of dPreS1 Ag able to traffic longer in the lymphatics, two parameters that may explain an
enhanced immunogenicity of the Ag. (c) Innate immunity boost: TLR2 stimulus by Pam₃CSK₄ may
synergize with dPreS1 response and improve the GC pathway of memory B cell formation via three
different signals namely the enhancement of (i) the Ag presentation by DC, (ii) the innate immune
pro-inflammatory cytokines, and (iii) the subsequent T cell priming of HBV-specific CD4+ and
CD8+. In fact, the affinity selection of GC B cells is dependent on T cells (Pulendran, 2009).

724

725 Altogether, these results give high hopes for developing a successful therapeutic solution against 726 chronic HBV infections. Abundant efforts have been made to develop therapeutic vaccines but 727 most candidates have missed their primary endpoints, which may be attributed to the fact that they 728 have been composed of free Ag or micro-delivery systems, contributing to low uptake in the 729 lymphatics and failure to induce optimal protection (Kosinska et al., 2017; Li et al., 2017). With the 730 recent exception of two elegant studies, nearly no nanosystem solution has been explored (Qiao 731 et al., 2021; Wang et al., 2020). Qiao and colleagues propose a nanosystem based on chitosan 732 and heparin while Wang and colleagues developed a system based on ferritin NP. In terms of 733 biomaterials, chitosan is known to be very expensive and hard to produce in a reproducible manner, 734 while ferritin is a metallic-based system, which is less biocompatible and biodegradable than PLA 735 (Bellich et al., 2016). Nonetheless, mirroring our results, both these nanosystems display excellent 736 lymph node targeting following subcutaneous injections, as well as high IgG titers ($10^7 \log_{10} at$ week 737 7). Our novel subcutaneous delivery system could be part of the next generation antiviral 738 treatments for hepatitis patients, considering the long-lasting and highly specific immune protection 739 it triggers against PreS1 epitope. Strong tolerance to HBsAg have been shown to limit the 740 therapeutic effect of conventional vaccinations in both preclinical models and patients with chronic 741 hepatitis B infections. In the latter, immune tolerance to PreS1, if any, appears to be much lower 742 than that to HBsAg, as it is only secreted in trace amounts compared to HBsAg that is present in a 743 10²-fold to 10⁵-fold excess over virions (Durantel and Zoulim, 2016). Now, the formulation needs 744 to be challenged in vivo against HBV. This working hypothesis in AAV-HBV transduced mice is 745 currently undergoing. Such platforms are easily tunable and could quickly be adapted to any viral 746 genotype if the corresponding antigen is carefully selected. We could also imagine delivering both 747 the adjuvant and the Ag in separate PLA NP, offering flexibility in coupling a generic adjuvant-748 containing NP with a novel antigen-containing NP (Boyoglu-Barnum et al., 2021; Singh et al., 2007). 749 Other nanoplatforms can also be envisaged such as polymeric micelles already proved as efficient 750 adjuvants for vaccine delivery (Lamrayah et al., 2022).

751

Taking an even bigger step back, the precise characterization of this nanosystem participates in
broadening the R&D opportunities for hard-to-get microbes, such as HIV, *Plasmodium falciparum*,
or *Mycobacterium tuberculosis*. Incorporating such PLA NP in delivery systems like microneedle
platforms or hydrogels for high-mucus penetration would enable a better protection, with a mucosalspecific immune activation at the localized site of entry of these pathogen (Du et al., 2022; Lavelle
and Ward, 2022).

- 758 759
- 760

761 Conflict of interest

All authors declare no conflict in interest except B.V. who holds some shares in Adjuvatis. The company had no role in the design of the study; in the collection, analyses, or interpretation of data; in the writing of the manuscript or in the decision to publish the results. The other authors declare no conflict of interest.

766

767 Authors contributions

B.V., J.L. and D.D. conceived the idea, designed and supervised the work. M.L. and F.C. wrote the
original manuscript. S.M. and R.T. performed all in silico experiments. C.C., M.D. and D.D.
performed all in vitro experiments. E.C. performed all ex vivo experiments. M.L. and F.C. performed
all in vivo experiments. All authors have read, revised and agreed to the published version of the
manuscript.

773

774 Acknowledgements

The authors would like to thank the staff of AniCan platform (CRCL, Lyon) and Thomas Barré for
his assistance in FMT4000 equipment, PHENOCAN for imaging devices [grant number ANR-11EQPX-0035 PHENOCAN], all the staff of Plateau de Biologie Expérimentale de la Souris (ENS,
Lyon) for the generous advice with animal care, CTµ platform (Université Lyon 1) and Altan Yavuz
for electron microscopy assistance.

780

781 Financial support

This work was supported by "La Ligue contre le Cancer" to BV and DD and a PhD scholarship to ML. This work was also supported by ANRS-MIE (French research agency on infectious and emerging diseases) to BV and DD (ECTZ 62760 and ECTZ 160315) and through PhD scholarships to FC (ECTZ158412) and MD (ECTZ137751). Global financial supports were also obtained from CNRS and INSERM.

787 Supplementary Data

788

790

789 Video attached to the manuscript

Video S1. This video highlights the last 20 ns of the 200 ns simulation experiment. The last 1000 frames out of the 10,000 total frames of the dynamic were used. The simulation has reached a stable state as no large molecular motion is observed. The biologically relevant epitope remains accessible for intermolecular interactions throughout the complete capture. The epitope is displayed in cyan, the lipidic anchor in yellow, and the rest of the PreS1 peptide in dark blue. PLA chains are displayed in dark grey, red and light grey for their carbon, oxygen, and hydrogen atoms respectively. The boundaries of the periodic cell are highlighted in dark green.

798

799



800 801

802 803

Fig. S1. Transmission electron microscopy images of blank NP (left), NP-dPreS1 (center) and NP-Pam₃CSK₄-dPreS1 (right). The three types of nanoformulations are morphologically similar (scale bar in each image).

804 805

805

807

Α

В

	Size (nm)	PDI	Zeta potential (mV)
NP(DiR)	160	0.078	-61
NP(DiR)-dPreS1	162	0.090	-64







813

814 Fig. S2. Comparative study of the biokinetics of the NP formulations functionalized or not with dPreS1. (A) Standard colloidal properties of fluorescent formulations (size, PDI and surface 815 816 charge) containing or not the modified dPreS1 peptide. (B) A single s.c injection (neck region, the 817 injection site is shown by the asterisk) was performed on SKH1 female mice with fluorescent 818 NP(DiR). The fluorescence intensity (750/780 nm) was monitored for 7 days using FMT imaging (Fluorescence Molecular Tomography, FMT4000, Perkin Elmer). (C) Fluorescence signal 819 820 quantification measured by FMT in NP(DiR) or NP(DiR)-PreS1 injected mice, at different time 821 points. Each point represents an individual animal and results are expressed as median (95% CI). 822 Statistical differences between the two groups at each time were evaluated using the non-823 parametric Wilcoxon test. There is no statistical difference between the two fluorescence signals at 824 each time.



825

Fig. S3. In-house sandwich ELISA for quantitative detection of specific dPreS1 Ab. We have serially diluted a solution of anti-PreS1 Ab in dPreS1-coated plates. The limit of detection (LOD) is defined as LOD = μ blank + 3 σ , and is represented by the dotted line.

- 829
- 830



832
833 Fig. S4 lgG anti-dPreS1 titers, schematically represented in individual values. See legend of
834 Figure 5

831



836

Fig. S5. Comparative data of the neutralization activity of mice antisera at W11, W27 and W47 in bar charts, at serum dilutions 1:100. Intragroup statistical analysis was performed by ANOVA test with multiple comparisons and Tukey's correction. For all groups, there was no intragroup difference ($\alpha = 0.05$) between the different time points.



844 Fig. S6. General safety evaluation based on weights is in favor of a safe-by-design 845 nanoplatform. For toxicity surveillance, mice body weights were monitored at W7 and W47 with 846 indicated each evolution rate (A). At endpoint, their liver (B) and spleen (C) were also weighed after 847 cervical dislocation and dissection. Upon evaluation, no statistical difference was observed 848 between groups (ANOVA test for A, Kruskal-Wallis test for B and C). Mice were physiologically 849 heavier at one year old with an increasing weight between + 23.6% and + 32.8% compared to W7 850 weight. This information is important because toxicity can easily become a serious obstacle in the 851 potential safety of a vaccine, especially when complemented by adjuvants. *ns* = *non significant*. 852

853 **REFERENCES**

- 854
- Anwar, M.A., Shah, M., Kim, J., Choi, S., 2019. Recent clinical trends in Toll-like receptor
 targeting therapeutics. Med. Res. Rev. 39, 1053–1090.
 https://doi.org/10.1002/med.21553
- Arulraj, T., Binder, S.C., Robert, P.A., Meyer-Hermann, M., 2019. Synchronous Germinal Center
 Onset Impacts the Efficiency of Antibody Responses. Front. Immunol. 10.
 https://doi.org/10.3389/fimmu.2019.02116
- Badamchi-Zadeh, A., McKay, P.F., Korber, B.T., Barinaga, G., Walters, A.A., Nunes, A., Gomes,
 J.P., Follmann, F., Tregoning, J.S., Shattock, R.J., 2016. A Multi-Component Prime-Boost
 Vaccination Regimen with a Consensus MOMP Antigen Enhances Chlamydia
 trachomatis Clearance. Front. Immunol. 7, 162. https://doi.org/10.3389/fimmu.2016.00162
- 865 Bellich, B., D'Agostino, I., Semeraro, S., Gamini, A., Cesàro, A., 2016. "The Good, the Bad and 866 the Ugly" of Chitosans. Mar. Drugs 14, 99. https://doi.org/10.3390/md14050099
- Bian, Y., Zhang, Z., Sun, Z., Zhao, J., Zhu, D., Wang, Y., Fu, S., Guo, J., Liu, L., Su, L., Wang, F.S., Fu, Y.-X., Peng, H., 2017. Vaccines targeting preS1 domain overcome immune
 tolerance in hepatitis B virus carrier mice. Hepatology 66, 1067–1082.
 https://doi.org/10.1002/hep.29239
- Block, T.M., Chang, K.-M., Guo, J.-T., 2021. Prospects for the Global Elimination of Hepatitis B.
 Annu. Rev. Virol. 8, 437–458. https://doi.org/10.1146/annurev-virology-091919-062728
- Boyoglu-Barnum, S., Ellis, D., Gillespie, R.A., Hutchinson, G.B., Park, Y.-J., Moin, S.M., Acton,
 O.J., Ravichandran, R., Murphy, M., Pettie, D., Matheson, N., Carter, L., Creanga, A.,
 Watson, M.J., Kephart, S., Ataca, S., Vaile, J.R., Ueda, G., Crank, M.C., Stewart, L., Lee,
 K.K., Guttman, M., Baker, D., Mascola, J.R., Veesler, D., Graham, B.S., King, N.P.,
 Kanekiyo, M., 2021. Quadrivalent influenza nanoparticle vaccines induce broad
 protection. Nature 1–6. https://doi.org/10.1038/s41586-021-03365-x
- Bray, F., Ferlay, J., Soerjomataram, I., Siegel, R.L., Torre, L.A., Jemal, A., 2018. Global cancer
 statistics 2018: GLOBOCAN estimates of incidence and mortality worldwide for 36
 cancers in 185 countries. CA. Cancer J. Clin. 68, 394–424.
 https://doi.org/10.3322/caac.21492
- Bretscher, P., 2019. On Analyzing How the Th1/Th2 Phenotype of an Immune Response Is
 Determined: Classical Observations Must Not Be Ignored. Front. Immunol. 10.
 https://doi.org/10.3389/fimmu.2019.01234
- Brisse, M., Vrba, S.M., Kirk, N., Liang, Y., Ly, H., 2020. Emerging Concepts and Technologies in
 Vaccine Development. Front. Immunol. 11, 583077.
 https://doi.org/10.3389/fimmu.2020.583077
- Chaudhury, S., Gray, J.J., 2008. Conformer Selection and Induced Fit in Flexible Backbone
 Protein–Protein Docking Using Computational and NMR Ensembles. J. Mol. Biol. 381,
 1068–1087. https://doi.org/10.1016/j.jmb.2008.05.042
- Cheng, D., Han, B., Zhang, W., Wu, W., 2021. Clinical effects of NTCP-inhibitor myrcludex B. J.
 Viral Hepat. 28, 852–858. https://doi.org/10.1111/jvh.13490
- 894ClusPro 2.0: protein-protein docking [WWW Document], n.d. URL https://cluspro.org/login.php895(accessed 7.19.21).
- Collins, D.S., Kourtis, L.C., Thyagarajapuram, N.R., Sirkar, R., Kapur, S., Harrison, M.W., Bryan,
 D.J., Jones, G.B., Wright, J.M., 2017. Optimizing the Bioavailability of Subcutaneously
 Administered Biotherapeutics Through Mechanochemical Drivers. Pharm. Res. 34, 2000–
 2011. https://doi.org/10.1007/s11095-017-2229-9
- Coolen, A.-L., Lacroix, C., Mercier-Gouy, P., Delaune, E., Monge, C., Exposito, J.-Y., Verrier, B.,
 2019. Poly(lactic acid) nanoparticles and cell-penetrating peptide potentiate mRNA-based
 vaccine expression in dendritic cells triggering their activation. Biomaterials 195, 23–37.
 https://doi.org/10.1016/j.biomaterials.2018.12.019
- Dalzon, B., Lebas, C., Jimenez, G., Gutjahr, A., Terrat, C., Exposito, J.-Y., Verrier, B., Lethias, C.,
 2016. Poly(Lactic Acid) Nanoparticles Targeting α5β1 Integrin as Vaccine Delivery
 Vehicle, a Prospective Study. PloS One 11, e0167663.
 https://doi.org/10.1371/journal.pone.0167663
- 908De Silva, N.S., Klein, U., 2015. Dynamics of B cells in germinal centres. Nat. Rev. Immunol. 15,909137–148. https://doi.org/10.1038/nri3804

- 910 DeFranco, A.L., Rookhuizen, D.C., Hou, B., 2012. Contribution of TLR signaling to germinal
 911 center antibody responses. Immunol. Rev. 247, 64–72. https://doi.org/10.1111/j.1600 912 065X.2012.01115.x
- 913 Dembek, C., Protzer, U., Roggendorf, M., 2018. Overcoming immune tolerance in chronic
 914 hepatitis B by therapeutic vaccination. Curr. Opin. Virol. 30, 58–67.
 915 https://doi.org/10.1016/j.coviro.2018.04.003
- 916 Desmares, M., Delphin, M., Chardès, B., Pons, C., Riedinger, J., Michelet, M., Rivoire, M.,
 917 Verrier, B., Salvetti, A., Lucifora, J., Durantel, D., 2022. Insights on the antiviral
 918 mechanisms of action of the TLR1/2 agonist Pam3CSK4 in hepatitis B virus (HBV)919 infected hepatocytes. Antiviral Res. 206, 105386.
 920 https://doi.org/10.1016/j.antiviral.2022.105386
- Dolgin, E., 2022. Closing in on a cure for hepatitis B. Nature 603, S46–S48.
 https://doi.org/10.1038/d41586-022-00812-1
- Dou, Y., Jansen, D.T.S.L., van den Bosch, A., de Man, R.A., van Montfoort, N., Araman, C., van Kasteren, S.I., Zom, G.G., Krebber, W.-J., Melief, C.J.M., Woltman, A.M., Buschow, S.I., 2020. Design of TLR2-ligand-synthetic long peptide conjugates for therapeutic vaccination of chronic HBV patients. Antiviral Res. 178, 104746.
 https://doi.org/10.1016/j.antiviral.2020.104746
- Du, G., Qin, M., Sun, X., 2022. Recent progress in application of nanovaccines for enhancing
 mucosal immune responses. Acta Pharm. Sin. B.
 https://doi.org/10.1016/j.apsb.2022.08.010
- Durantel, D., Zoulim, F., 2016. New antiviral targets for innovative treatment concepts for hepatitis
 B virus and hepatitis delta virus. J. Hepatol., Molecular Biology of Hepatitis B Virus 64,
 S117–S131. https://doi.org/10.1016/j.jhep.2016.02.016
- Fanning, G.C., Zoulim, F., Hou, J., Bertoletti, A., 2019. Therapeutic strategies for hepatitis B virus
 infection: towards a cure. Nat. Rev. Drug Discov. 18, 827–844.
 https://doi.org/10.1038/s41573-019-0037-0
- 937 Fries, C.N., Curvino, E.J., Chen, J.-L., Permar, S.R., Fouda, G.G., Collier, J.H., 2020. Advances
 938 in nanomaterial vaccine strategies to address infectious diseases impacting global health.
 939 Nat. Nanotechnol. https://doi.org/10.1038/s41565-020-0739-9
- Glebe, D., Urban, S., Knoop, E.V., Cag, N., Krass, P., Grün, S., Bulavaite, A., Sasnauskas, K.,
 Gerlich, W.H., 2005. Mapping of the hepatitis B virus attachment site by use of infectioninhibiting preS1 lipopeptides and tupaia hepatocytes. Gastroenterology 129, 234–245.
 https://doi.org/10.1053/j.gastro.2005.03.090
- Graber-Stiehl, I., 2018. The silent epidemic killing more people than HIV, malaria or TB. Nature
 564, 24–26. https://doi.org/10.1038/d41586-018-07592-7
- Gripon, P., Rumin, S., Urban, S., Le Seyec, J., Glaise, D., Cannie, I., Guyomard, C., Lucas, J.,
 Trepo, C., Guguen-Guillouzo, C., 2002. Infection of a human hepatoma cell line by
 hepatitis B virus. Proc. Natl. Acad. Sci. U. S. A. 99, 15655–15660.
 https://doi.org/10.1073/pnas.232137699
- Gutjahr, A., Phelip, C., Coolen, A.-L., Monge, C., Boisgard, A.-S., Paul, S., Verrier, B., 2016.
 Biodegradable Polymeric Nanoparticles-Based Vaccine Adjuvants for Lymph Nodes
 Targeting. Vaccines 4. https://doi.org/10.3390/vaccines4040034
- Harris, J.R., Markl, J., 1999. Keyhole limpet hemocyanin (KLH): a biomedical review. Micron 30, 597–623. https://doi.org/10.1016/S0968-4328(99)00036-0
- Havenar-Daughton, C., Carnathan, D.G., Boopathy, A.V., Upadhyay, A.A., Murrell, B., Reiss,
 S.M., Enemuo, C.A., Gebru, E.H., Choe, Y., Dhadvai, P., Viviano, F., Kaushik, K.,
 Bhiman, J.N., Briney, B., Burton, D.R., Bosinger, S.E., Schief, W.R., Irvine, D.J., Silvestri,
 G., Crotty, S., 2019. Rapid Germinal Center and Antibody Responses in Non-human
 Primates after a Single Nanoparticle Vaccine Immunization 35.
- Havenar-Daughton, C., Lindqvist, M., Heit, A., Wu, J.E., Reiss, S.M., Kendric, K., Bélanger, S.,
 Kasturi, S.P., Landais, E., Akondy, R.S., McGuire, H.M., Bothwell, M., Vagefi, P.A.,
 Scully, E., Tomaras, G.D., Davis, M.M., Poignard, P., Ahmed, R., Walker, B.D.,
 Pulendran, B., McElrath, M.J., Kaufmann, D.E., Crotty, S., 2016. CXCL13 is a plasma
 biomarker of germinal center activity. Proc. Natl. Acad. Sci. U. S. A. 113, 2702–2707.
 https://doi.org/10.1073/pnas.1520112113
- Heise, N., De Silva, N.S., Silva, K., Carette, A., Simonetti, G., Pasparakis, M., Klein, U., 2014.
 Germinal center B cell maintenance and differentiation are controlled by distinct NF-κB

- 968 transcription factor subunits. J. Exp. Med. 211, 2103–2118.
 969 https://doi.org/10.1084/jem.20132613
- Hennessy, E.J., Parker, A.E., O'Neill, L.A.J., 2010. Targeting Toll-like receptors: emerging
 therapeutics? Nat. Rev. Drug Discov. 9, 293–307. https://doi.org/10.1038/nrd3203
- 972 I-TASSER server for protein structure and function prediction [WWW Document], n.d. URL
 973 https://zhanglab.ccmb.med.umich.edu/I-TASSER/ (accessed 12.6.19).
- 874 Kardani, K., Bolhassani, A., Shahbazi, S., 2016. Prime-boost vaccine strategy against viral 975 infections: Mechanisms and benefits. Vaccine 34, 413–423.
 976 https://doi.org/10.1016/j.vaccine.2015.11.062
- Kasturi, S.P., Skountzou, I., Albrecht, R.A., Koutsonanos, D., Hua, T., Nakaya, H.I., Ravindran,
 R., Stewart, S., Alam, M., Kwissa, M., Villinger, F., Murthy, N., Steel, J., Jacob, J., Hogan,
 R.J., García-Sastre, A., Compans, R., Pulendran, B., 2011. Programming the magnitude
 and persistence of antibody responses with innate immunity. Nature 470, 543–547.
 https://doi.org/10.1038/nature09737
- Kazanietz, M.G., Durando, M., Cooke, M., 2019. CXCL13 and Its Receptor CXCR5 in Cancer:
 Inflammation, Immune Response, and Beyond. Front. Endocrinol. 10.
 https://doi.org/10.3389/fendo.2019.00471
- Kelly, H.G., Kent, S.J., Wheatley, A.K., 2019. Immunological basis for enhanced immunity of
 nanoparticle vaccines. Expert Rev. Vaccines 18, 269–280.
 https://doi.org/10.1080/14760584.2019.1578216
- Kosinska, A.D., Bauer, T., Protzer, U., 2017. Therapeutic vaccination for chronic hepatitis B. Curr.
 Opin. Virol., Viral pathogenesis Preventive and therapeutic vaccines 23, 75–81.
 https://doi.org/10.1016/j.coviro.2017.03.011
- Lamalle-Bernard, D., Munier, S., Compagnon, C., Charles, M.-H., Kalyanaraman, V.S., Delair, T.,
 Verrier, B., Ataman-Onal, Y., 2006. Coadsorption of HIV-1 p24 and gp120 proteins to
 surfactant-free anionic PLA nanoparticles preserves antigenicity and immunogenicity. J.
 Control. Release Off. J. Control. Release Soc. 115, 57–67.
 https://doi.org/10.1016/j.jconrel.2006.07.006
- Lamrayah, M., Charriaud, F., Hu, S., Megy, S., Terreux, R., Verrier, B., 2019. Molecular modelling
 of TLR agonist Pam3CSK4 entrapment in PLA nanoparticles as a tool to explain loading
 efficiency and functionality. Int. J. Pharm. 568, 118569.
 https://doi.org/10.1016/j.ijpharm.2019.118569
- Lamrayah, M., Phelip, C., Coiffier, C., Lacroix, C., Willemin, T., Trimaille, T., Verrier, B., 2022. A
 Polylactide-Based Micellar Adjuvant Improves the Intensity and Quality of Immune
 Response. Pharmaceutics 14, 107. https://doi.org/10.3390/pharmaceutics14010107
- Lang, J., Neumann-Haefelin, C., Thimme, R., 2019. Immunological cure of HBV infection. Hepatol. Int. 13, 113–124. https://doi.org/10.1007/s12072-018-9912-8
- 1005Lavelle, E.C., Ward, R.W., 2022. Mucosal vaccines fortifying the frontiers. Nat. Rev. Immunol.100622, 236–250. https://doi.org/10.1038/s41577-021-00583-2
- 1007Lee, G.-H., Lim, S.-G., 2021. CpG-Adjuvanted Hepatitis B Vaccine (HEPLISAV-B®) Update.1008Expert Rev. Vaccines 20, 487–495. https://doi.org/10.1080/14760584.2021.1908133
- Lee, S.-H., Park, S.-R., 2018. Toll-like Receptor 1/2 Agonist Pam3CSK4 Suppresses
 Lipopolysaccharide-driven IgG1 Production while Enhancing IgG2a Production by B
 Cells. Immune Netw. 18. https://doi.org/10.4110/in.2018.18.e10
- Li, J., Bao, M., Ge, J., Ren, S., Zhou, T., Qi, F., Pu, X., Dou, J., 2017. Research progress of therapeutic vaccines for treating chronic hepatitis B. Hum. Vaccines Immunother. 13, 986–997. https://doi.org/10.1080/21645515.2016.1276125
- Lu, S., 2009. Heterologous prime-boost vaccination. Curr. Opin. Immunol. 21, 346–351.
 https://doi.org/10.1016/j.coi.2009.05.016
- Lucifora, J., Bonnin, M., Aillot, L., Fusil, F., Maadadi, S., Dimier, L., Michelet, M., Floriot, O.,
 Ollivier, A., Rivoire, M., Ait-Goughoulte, M., Daffis, S., Fletcher, S.P., Salvetti, A., Cosset,
 F.-L., Zoulim, F., Durantel, D., 2018. Direct antiviral properties of TLR ligands against
 HBV replication in immune-competent hepatocytes. Sci. Rep. 8, 5390.
 https://doi.org/10.1038/s41598-018-23525-w
- 1022Marion, M.-J., Hantz, O., Durantel, D., 2010. The HepaRG Cell Line: Biological Properties and1023Relevance as a Tool for Cell Biology, Drug Metabolism, and Virology Studies, in: Maurel,1024P. (Ed.), Hepatocytes: Methods and Protocols, Methods in Molecular Biology. Humana1025Press, Totowa, NJ, pp. 261–272. https://doi.org/10.1007/978-1-60761-688-7_13

1026 Megy, S., Aguero, S., Da Costa, D., Lamrayah, M., Berthet, M., Primard, C., Verrier, B., Terreux, 1027 R., 2020. Molecular Dynamics Studies of Poly(Lactic Acid) Nanoparticles and Their 1028 Interactions with Vitamin E and TLR Agonists Pam1CSK4 and Pam3CSK4. 1029 Nanomaterials 10, 2209. https://doi.org/10.3390/nano10112209 Meier, A., Mehrle, S., Weiss, T.S., Mier, W., Urban, S., 2013. Myristoylated PreS1-domain of the 1030 1031 hepatitis B virus L-protein mediates specific binding to differentiated hepatocytes. 1032 Hepatol. Baltim. Md 58, 31-42. https://doi.org/10.1002/hep.26181 1033 Meng, Z., Chen, Y., Lu, M., 2019. Advances in Targeting the Innate and Adaptive Immune 1034 Systems to Cure Chronic Hepatitis B Virus Infection, Front, Immunol, 10, 3127. 1035 https://doi.org/10.3389/fimmu.2019.03127 1036 Mitchell, M.J., Billingsley, M.M., Haley, R.M., Wechsler, M.E., Peppas, N.A., Langer, R., 2020. 1037 Engineering precision nanoparticles for drug delivery. Nat. Rev. Drug Discov. 1–24. 1038 https://doi.org/10.1038/s41573-020-0090-8 Monrad, J.T., Sandbrink, J.B., Cherian, N.G., 2021. Promoting versatile vaccine development for 1039 1040 emerging pandemics. Npj Vaccines 6, 1-7. https://doi.org/10.1038/s41541-021-00290-y 1041 Ni, Y., Lempp, F.A., Mehrle, S., Nkongolo, S., Kaufman, C., Fälth, M., Stindt, J., Königer, C., 1042 Nassal, M., Kubitz, R., Sültmann, H., Urban, S., 2014. Hepatitis B and D viruses exploit 1043 sodium taurocholate co-transporting polypeptide for species-specific entry into 1044 hepatocytes. Gastroenterology 146, 1070-1083. 1045 https://doi.org/10.1053/j.gastro.2013.12.024 1046 Park, H., Bradley, P., Greisen, P., Liu, Y., Mulligan, V.K., Kim, D.E., Baker, D., DiMaio, F., 2016. 1047 Simultaneous Optimization of Biomolecular Energy Functions on Features from Small 1048 Molecules and Macromolecules. J. Chem. Theory Comput. 12, 6201–6212. 1049 https://doi.org/10.1021/acs.jctc.6b00819 1050 Pavot, V., Climent, N., Rochereau, N., Garcia, F., Genin, C., Tiraby, G., Vernejoul, F., Perouzel, E., Lioux, T., Verrier, B., Paul, S., 2016. Directing vaccine immune responses to mucosa 1051 1052 by nanosized particulate carriers encapsulating NOD ligands. Biomaterials 75, 327–339. 1053 https://doi.org/10.1016/j.biomaterials.2015.10.034 1054 Pavot, V., Rochereau, N., Primard, C., Genin, C., Perouzel, E., Lioux, T., Paul, S., Verrier, B., 1055 2013. Encapsulation of Nod1 and Nod2 receptor ligands into poly(lactic acid) 1056 nanoparticles potentiates their immune properties. J. Control. Release Off. J. Control. 1057 Release Soc. 167, 60-67. https://doi.org/10.1016/j.jconrel.2013.01.015 Pedersen, G.K., Wørzner, K., Andersen, P., Christensen, D., 2020. Vaccine Adjuvants 1058 1059 Differentially Affect Kinetics of Antibody and Germinal Center Responses. Front. 1060 Immunol. 11. https://doi.org/10.3389/fimmu.2020.579761 Peplow, M., 2021. Nanotechnology offers alternative ways to fight COVID-19 pandemic with 1061 1062 antivirals. Nat. Biotechnol. 39, 1172-1174. https://doi.org/10.1038/s41587-021-01085-1 Peres, C., Matos, A.I., Conniot, J., Sainz, V., Zupančič, E., Silva, J.M., Graça, L., Sá Gaspar, R., 1063 1064 Préat, V., Florindo, H.F., 2017. Poly(lactic acid)-based particulate systems are promising 1065 tools for immune modulation. Acta Biomater. 48, 41–57. https://doi.org/10.1016/j.actbio.2016.11.012 1066 1067 Polaris Observatory Collaborators, 2018. Global prevalence, treatment, and prevention of 1068 hepatitis B virus infection in 2016: a modelling study. Lancet Gastroenterol. Hepatol. 3, 1069 383-403. https://doi.org/10.1016/S2468-1253(18)30056-6 1070 Pulendran, B., 2009. Learning immunology from the yellow fever vaccine: innate immunity to 1071 systems vaccinology. Nat. Rev. Immunol. 9, 741-747. https://doi.org/10.1038/nri2629 1072 Pulendran, B., Ahmed, R., 2011. Immunological mechanisms of vaccination. Nat. Immunol. 12, 1073 509-517. https://doi.org/10.1038/ni.2039 Pulendran, B., S. Arunachalam, P., O'Hagan, D.T., 2021. Emerging concepts in the science of 1074 1075 vaccine adjuvants. Nat. Rev. Drug Discov. 1-22. https://doi.org/10.1038/s41573-021-1076 00163-v 1077 Qiao, D., Chen, Y., Liu, L., 2021. Engineered therapeutic nanovaccine against chronic hepatitis B virus infection. Biomaterials 269, 120674. 1078 1079 https://doi.org/10.1016/j.biomaterials.2021.120674 1080 Qin, Y., Liao, P., 2018. Hepatitis B virus vaccine breakthrough infection: surveillance of S gene 1081 mutants of HBV. Acta Virol. 62, 115-121. https://doi.org/10.4149/av_2018_210 1082 Rammensee, H.-G., Wiesmüller, K.-H., Chandran, P.A., Zelba, H., Rusch, E., Gouttefangeas, C., Kowalewski, D.J., Di Marco, M., Haen, S.P., Walz, J.S., Gloria, Y.C., Bödder, J., Schertel, 1083 J.-M., Tunger, A., Müller, L., Kießler, M., Wehner, R., Schmitz, M., Jakobi, M., 1084

1085 Schneiderhan-Marra, N., Klein, R., Laske, K., Artzner, K., Backert, L., Schuster, H., 1086 Schwenck, J., Weber, A.N.R., Pichler, B.J., Kneilling, M., la Fougère, C., Forchhammer, 1087 S., Metzler, G., Bauer, J., Weide, B., Schippert, W., Stevanović, S., Löffler, M.W., 2019. A 1088 new synthetic toll-like receptor 1/2 ligand is an efficient adjuvant for peptide vaccination in a human volunteer. J. Immunother. Cancer 7, 307. https://doi.org/10.1186/s40425-019-1089 1090 0796-5 1091 Rességuier, J., Delaune, E., Coolen, A.-L., Levraud, J.-P., Boudinot, P., Le Guellec, D., Verrier, 1092 B., 2017. Specific and Efficient Uptake of Surfactant-Free Poly(Lactic Acid) Nanovaccine 1093 Vehicles by Mucosal Dendritic Cells in Adult Zebrafish after Bath Immersion, Front. 1094 Immunol. 8, 190. https://doi.org/10.3389/fimmu.2017.00190 1095 Saco, T.V., Strauss, A.T., Ledford, D.K., 2018. Hepatitis B vaccine nonresponders: Possible mechanisms and solutions. Ann. Allergy Asthma Immunol. Off. Publ. Am. Coll. Allergy 1096 1097 Asthma Immunol. 121, 320–327. https://doi.org/10.1016/j.anai.2018.03.017 1098 Schudel, A., Francis, D.M., Thomas, S.N., 2019. Material design for lymph node drug delivery. 1099 Nat. Rev. Mater. 4, 415-428. https://doi.org/10.1038/s41578-019-0110-7 1100 Singh, A., 2021. Eliciting B cell immunity against infectious diseases using nanovaccines. Nat. 1101 Nanotechnol. 16, 9. 1102 Singh, M., Chakrapani, A., O'Hagan, D., 2007. Nanoparticles and microparticles as vaccine-1103 delivery systems, Expert Rev. Vaccines 6, 797-808. 1104 https://doi.org/10.1586/14760584.6.5.797 1105 Swaminathan, A., Lucas, R.M., Dear, K., McMichael, A.J., 2014. Keyhole limpet haemocyanin - a model antigen for human immunotoxicological studies. Br. J. Clin. Pharmacol. 78, 1135-1106 1107 1142. https://doi.org/10.1111/bcp.12422 Urban, S., Bartenschlager, R., Kubitz, R., Zoulim, F., 2014. Strategies to inhibit entry of HBV and 1108 1109 HDV into hepatocytes. Gastroenterology 147, 48-64. 1110 https://doi.org/10.1053/j.gastro.2014.04.030 van Zundert, G.C.P., Rodrigues, J.P.G.L.M., Trellet, M., Schmitz, C., Kastritis, P.L., Karaca, E., 1111 1112 Melguiond, A.S.J., van Dijk, M., de Vries, S.J., Bonvin, A.M.J.J., 2016. The HADDOCK2.2 1113 Web Server: User-Friendly Integrative Modeling of Biomolecular Complexes, J. Mol. Biol. 1114 428, 720-725. https://doi.org/10.1016/j.jmb.2015.09.014 1115 Varkhede, N., Bommana, R., Schöneich, C., Forrest, M.L., 2020. Proteolysis and Oxidation of 1116 Therapeutic Proteins After Intradermal or Subcutaneous Administration. J. Pharm. Sci. 1117 109, 191–205. https://doi.org/10.1016/j.xphs.2019.08.005 1118 Victora, G.D., Nussenzweig, M.C., 2012. Germinal Centers. Annu. Rev. Immunol. 30, 429–457. 1119 https://doi.org/10.1146/annurev-immunol-020711-075032 1120 Wang, W., Zhou, X., Bian, Y., Wang, S., Chai, Q., Guo, Z., Wang, Z., Zhu, P., Peng, H., Yan, X., 1121 Li, W., Fu, Y.-X., Zhu, M., 2020. Dual-targeting nanoparticle vaccine elicits a therapeutic antibody response against chronic hepatitis B. Nat. Nanotechnol. 15, 406-416. 1122 1123 https://doi.org/10.1038/s41565-020-0648-y Yan, H., Zhong, G., Xu, G., He, W., Jing, Z., Gao, Z., Huang, Y., Qi, Y., Peng, B., Wang, H., Fu, 1124 1125 L., Song, M., Chen, P., Gao, W., Ren, B., Sun, Y., Cai, T., Feng, X., Sui, J., Li, W., 2012. 1126 Sodium taurocholate cotransporting polypeptide is a functional receptor for human 1127 hepatitis B and D virus. eLife 1, e00049. https://doi.org/10.7554/eLife.00049 1128 Yato, K., Onodera, T., Matsuda, M., Moriyama, S., Fujimoto, A., Watashi, K., Aizaki, H., Tanaka, T., Moriishi, K., Nishitsuji, H., Shimotohno, K., Tamura, K., Takahashi, Y., Wakita, T., 1129 1130 Muramatsu, M., Kato, T., Suzuki, R., 2020. Identification of Two Critical Neutralizing 1131 Epitopes in the Receptor Binding Domain of Hepatitis B Virus preS1. J. Virol. 1132 https://doi.org/10.1128/JVI.01680-20 1133 Ye, X., Zhou, M., He, Y., Wan, Y., Bai, W., Tao, S., Ren, Y., Zhang, X., Xu, J., Liu, J., Zhang, J., 1134 Hu, K., Xie, Y., 2016. Efficient Inhibition of Hepatitis B Virus Infection by a preS1-binding 1135 Peptide. Sci. Rep. 6, 29391. https://doi.org/10.1038/srep29391 1136 Zhu, D.D., Zhang, X.P., Yu, H.L., Liu, R.X., Shen, C.B., Zhang, W.F., Cui, Y., Guo, X.D., 2019. 1137 Kinetic stability studies of HBV vaccine in a microneedle patch. Int. J. Pharm. 567, 1138 118489. https://doi.org/10.1016/j.ijpharm.2019.118489 1139