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### ► To cite this version:

Chen Zhang, Caroline Lafond, Anaïs Barateau, Julie Leseur, Bastien Rigaud, et al.. Automatic segmentation for plan-of-the-day selection in CBCT-guided adaptive radiation therapy of cervical cancer. *Physics in Medicine and Biology*, 2022, 67 (24), pp.245020. 10.1088/1361-6560/aca5e5 . hal-03882318

**HAL Id: hal-03882318**

**<https://hal.science/hal-03882318>**

Submitted on 2 Dec 2022

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# Automatic segmentation for plan-of-the-day selection in CBCT-guided adaptive radiation therapy of cervical cancer

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*Objective:* Plan-of-the-day (PoD) adaptive radiation therapy (ART) is based on a library of treatment plans, among which, at each treatment fraction, the PoD is selected using daily images. However, this strategy is limited by PoD selection uncertainties. This work aimed to propose and evaluate a workflow to automatically and quantitatively identify the PoD for cervix cancer ART based on daily CBCT images.

*Approach:* The quantification was based on the segmentation of the main structures of interest in the CBCT images (clinical target volume [CTV], rectum, bladder, and bowel bag) using a deep learning model. Then, the PoD was selected from the treatment plan library according to the geometrical coverage of the CTV. For the evaluation, the resulting PoD was compared to the one obtained considering reference CBCT delineations.

*Main results:* In experiments on a database of 23 patients with 272 CBCT images, the proposed method obtained an agreement between the reference PoD and the automatically identified PoD for 91.5% of treatment fractions (99.6% when considering a 5% margin on CTV coverage).

*Significance:* The proposed automatic workflow automatically selected PoD for ART using deep-learning methods. The results showed the ability of the proposed process to identify the optimal PoD in a treatment plan library.

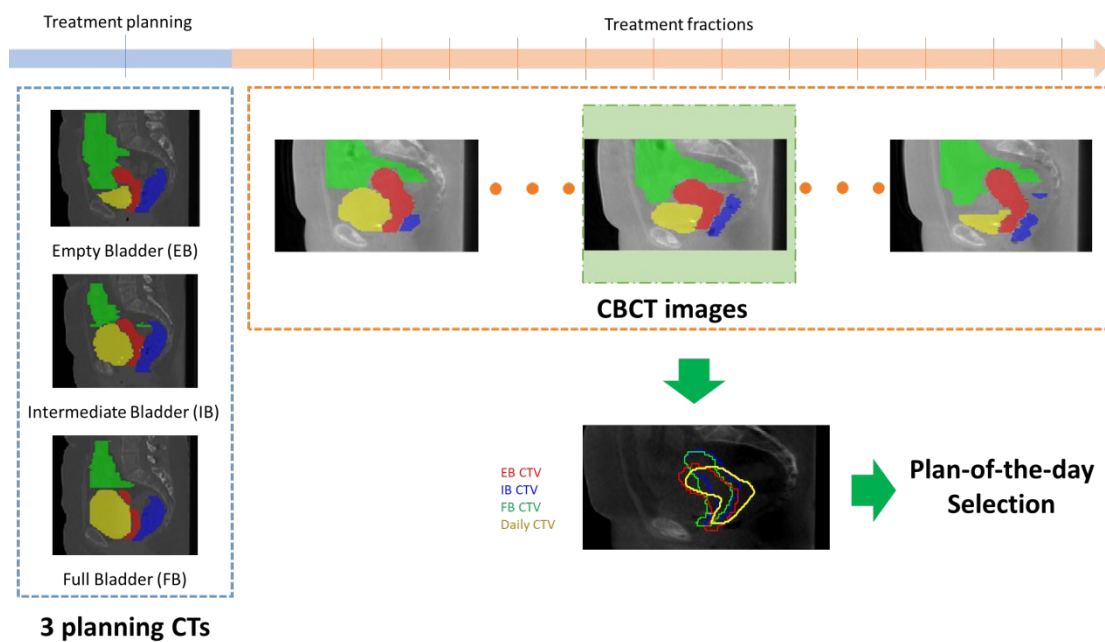
## 1. Introduction

The standard treatment for locally advanced cervical cancer (LACC) is external beam radiotherapy (EBRT) with chemotherapy, followed by brachytherapy. Although Intensity-Modulated Radiation Therapy (IMRT) is used to reduce normal tissue toxicity (Naik *et al* 2016, Gandhi *et al* 2013), it is limited by large and complex intrapelvic anatomical variations occurring between the treatment fractions (Buchali *et al* 1999, Han *et al* 2006). The position and shape of the clinical target volume (CTV, including the cervix, uterus, upper-vagina, and parametrium) are highly dependent on bladder and rectum filling, and on tumor regression during treatment (Jadon *et al* 2014, Chan *et al* 2008, Beadle *et al* 2009). In the context of adaptive radiation therapy (ART), plan-of-the-day (PoD) strategies have been proposed based on the generation of a treatment plan library, including several treatment plans optimized according to multiple planning CTs (pCT) acquired with various bladder fillings (Bondar *et al* 2012, Heijkoop *et al* 2014, van de Schoot *et al* 2017). At each treatment fraction, the treatment plan is then selected among those of the library (“plan-of-the-day”) based on an in-room image (e.g., CBCT image, see Figure 1). Although this strategy appears to be adequate to compensate for uterine motions (Heijkoop *et al* 2014, van de Schoot *et al* 2017, Gobeli *et al* 2015), it remains complex in a clinical workflow.

Different factors limit the rapid advancement of PoD ART. The PoD selection is actually a difficult process, mainly due to the poor contrast of CBCT images and large anatomical deformations. Thus, the expert needs to visualize the full 3D volume to assess the coverage of the whole target by the available treatment plans. The PoD selection is therefore a time-consuming process which is submitted to interobserver variability, as demonstrated in (Gobeli *et al* 2018) where 26 operators manually selected PoD on 24 CBCT images. This study showed a high inter-observer variability since the optimal PoD was chosen on average by 60% of users.

In order to automatize PoD selection, the automatic segmentation of CBCT images has been proposed to measure, at each treatment fraction, the ability of the treatment plans to treat the target (Bondar *et al* 2013). Langerak *et al.* (Langerak *et al* 2014) proposed to use a multi-atlas-based segmentation method. On a total of 224 CBCT, the CBCT images corresponding to low confidence levels were firstly removed, resulting to 187 images on which the Dice values were 0.85, 0.81, and 0.80 for the uterus, bladder, and rectum, respectively. However, the CBCT image quality is limited by noise, artifacts, and low soft-tissue contrast, making automatic segmentation very challenging. Recently, with the widespread use of deep learning (DL) in medical imaging, Beekman *et al.* (Beekman *et al* 2022) compared different DL models, performing either direct segmentation or a segmentation prior deformation by diffeomorphic image registration. The deformation-based model performed the best on the CBCT test set, with a median Dice score of 0.80.

In the context of PoD-based ART for LACC, this work aimed to propose a strategy to automatically select the optimal treatment plan. It relies on a deep learning-based segmentation of the CBCT images, enabling the selection of the optimal treatment plan regarding the CTV coverage based on a geometrical criterion. This strategy was simulated and compared to a reference obtained from expert manual delineations.

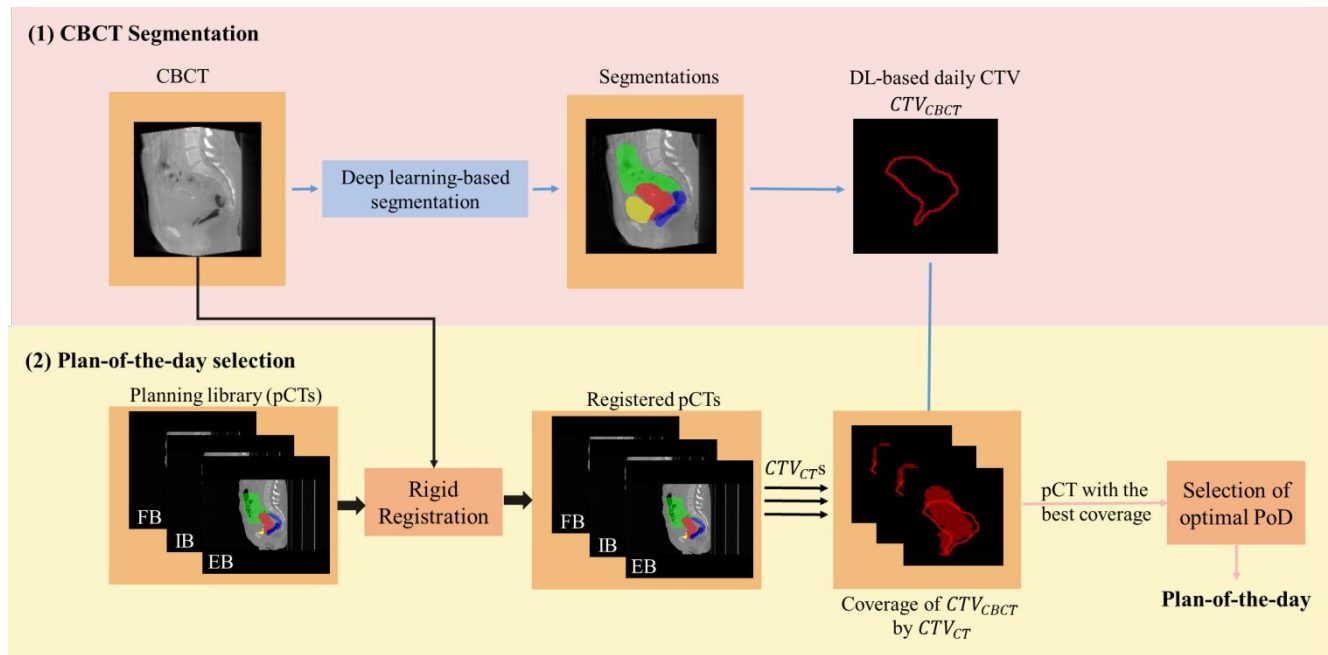


**Figure 1. Flowchart of plan-of-the-day ART for cervical cancer.** The process includes three steps (1) Planning: acquisition of multiple planning CT scans with variable bladder volumes. (2) Acquisition of the CBCT image of the day. (3) Selection of the most appropriate treatment plan to maximize the target coverage.

The CTV, bowel bag, bladder, and rectum are represented as red, green, yellow, and blue-filled contours. For plan-of-the-day selection, empty bladder (EB), intermediate bladder (IB), full bladder (FB), and daily CTV are represented on the daily CBCT as red, blue, green, and yellow contours, respectively.

## 2. Materials and methods

Figure 2 describes the flowchart of the study. Based on three planning CT scans, corresponding to empty bladder, intermediate bladder and full bladder, and on daily CBCT scans, it contains two parts applied to each daily CBCT image: (1) segmentation of the CBCT image using a deep learning network; (2) selection of the most appropriate PoD among the available planning CTs (pCTs). For this second step, the three pCTs in the planning library were registered to the daily CBCT image to simulate patient repositioning. Then, the coverage of the segmented daily CTV by the CTVs of pCTs was computed. Finally, the best treatment plan was selected as the one corresponding to the highest daily CTV coverage.



**Figure 2. Flowchart of the study.** The steps are: (1) CBCT segmentation using deep learning and (2) plan-of-the-day (PoD) selection using clinical target volume (CTV) contours. The PoD selection relies on: (a) Bone-based rigid registration of the planning CTs (pCTs) with the daily CBCT to simulate patient repositioning; (b) computation of the coverage between the daily CTV ( $CTV_{CBCT}$ ) and CTV of the pCTs ( $CTV_{EB}$ ,  $CTV_{IB}$ ,  $CTV_{FB}$ ); (c) selection of the best treatment plan based on target coverage: the pCT corresponding to the highest coverage was selected. (EB: empty bladder; IB: intermediate bladder; FB: Full bladder; cov: coverage value).

### 2.1 Data acquisition and experimental settings

In this study, we collected 272 CBCT scans and 63 CT scans from 23 patients. All patients were treated with a combination of external beam radiation therapy (EBRT) and pulse-dose-rate brachytherapy (PDR-BT). EBRT delivered a total dose of 45 Gy to the pelvis (supine position), at 1.8 Gy per fraction, using IMRT along with concomitant weekly cisplatin (40 mg/m<sup>2</sup>). PDR-BT was delivered following the GEC-ESTRO recommendations. All patients provided signed informed consent.

Each patient underwent two or three planning CTs with different bladder volumes: empty bladder (EB), intermediate bladder (IB), and full bladder (FB). One hour before the first IB CT, the patient had to drink 250 mL of water. Then another 500 mL of water should be consumed to obtain FB CT after 20 minutes. For EB CT, the patient emptied her bladder. All CTs were scanned (Big Bore, Philips) with voxel spacing ranging from 0.87×0.87×3.00 mm<sup>3</sup> to 1.21×1.21×3.00 mm<sup>3</sup>. The dimensions range of CT volumes was from 75×512×512 to 168×512×512.

During the radiation therapy treatment, 5 to 16 CBCT images were acquired (XVI mounted on a Synergy linac, Elekta) for each patient with voxel spacing of 1.00×1.00×2.00 mm<sup>3</sup> and dimensions of 132×410×410.

All images (i.e., planning CTs and CBCTs) were manually contoured slice-by-slice by one radiation oncologist. These contours were the primary CTV, including the cervix, uterus, and upper-vagina, and the rectum, bladder, and bowel bag (including the sigmoid). These delineations were considered as the reference in this study.

## 2.2 CBCT segmentation using deep-learning

The segmentation model was trained using the deep learning-based method nnU-Net, which has been demonstrated to be efficient in multiple medical image segmentation tasks (Isensee *et al* 2021). nnU-Net's automatic configuration runs without human intervention when it is applied to a new dataset. The nnU-Net focuses on pre-processing, training, inference strategies, and post-processing. The 3D full resolution U-Net was used since it has been shown to be one of the best performing models in many medical image segmentation tasks (Malimban *et al* 2022, Isensee *et al* 2021).

All images were cropped to the region of nonzero values with a cropping size of  $84 \times 410 \times 410$  voxels. The resampling voxel size was the median voxel spacing of the dataset, i.e.,  $1.00 \times 1.00 \times 2.00$  mm<sup>3</sup>. A z-score normalization was applied to each image. In the post-processing procedure, a connected component analysis was performed to eliminate the detection of spurious false positives. The model was trained using Pytorch and stochastic gradient descent (SGD) optimizer. The initial learning rate was set to 0.01 and decreased according to the ‘‘Poly’’ scheme (Chen *et al* 2017). The loss function was the sum of Dice similarity coefficient and cross-entropy with the same weight.

We randomly split all 23 patients into four folds using a cross-validation scheme. Table 1 presents the partition of the dataset. Multiple images (i.e., planning and daily images) from individual patients were not distributed among datasets. The test data was only used to evaluate the performance of the model in this fold and was not involved in training. nnU-Net further divided the training data into training and validation sets and performed a five-fold cross-validation to automatically select the best network configuration. In the end, the model (or ensemble) which got the best performance was chosen to perform the inference on the test sets of this fold. The number of epochs during training was 1000 for every fold. The evaluation of the segmented volumes is described in part 2.4.1. Table 2 reports the network configurations generated by nnU-Net for the considered dataset.

## 2.3 Plan-of-the-day selection

After obtaining the segmentation results for each CBCT image, the following three steps were performed: (1) Bone-based rigid registration between each pCT with different bladder fillings (FB, IB, EB) and the daily CBCT to simulate patient repositioning; (2) computation of the coverage between the CTV of CBCT ( $CTV_{CBCT}$ ) and CTV of the CTs ( $CTV_{EB}$ ,  $CTV_{IB}$ ,  $CTV_{FB}$ ); (3) selection of the pCT corresponding to the best coverage.

Model	#Patient		#CBCT volume	
	Train	Test	Train	Test
1	18	5	216	56
2	17	6	197	75
3	17	6	206	66
4	17	6	199	73

**Table 1. Partition of the dataset for the deep learning network training and testing.** The population was randomly separated into four folds using a cross-validation scheme to evaluate the model performance. Multiple images (i.e., planning and daily images) from individual patients were not distributed among datasets.

Parameters	3D full resolution U-Net
Normalization	Z normalization
Patch size	$56 \times 192 \times 160$
Batch size	2
Downsampling strides	[[1, 2, 2], [2, 2, 2], [2, 2, 2], [2, 2, 2], [1, 2, 2]]
Convolution kernel sizes	[[1, 3, 3], [3, 3, 3], [3, 3, 3], [3, 3, 3], [3, 3, 3], [3, 3, 3]]

**Table 2. Network configurations generated by nnU-Net.**

### 2.3.1 Rigid registration

For each patient, a bone-based rigid registration was performed between each CBCT and each pCT, using the ROI of the CBCT which was limited to the treated region. The goal of rigid registration was, in this study, to simulate patient repositioning. In the clinical setup, the rigid transform would result from the applied couch shift/rotation. The library Elastix was used (Klein et al 2009) to estimate the rigid transform (translation and rotation) with normalized correlation as the metric, applied to thresholded images. The resulting rigid transform was visually validated by checking bone alignment and was applied to the pCT's corresponding delineations.

### 2.3.2 Selection of the PoD

To evaluate the ability of each treatment plan to treat the CTV in its daily position, a coverage index was computed between the  $CTV_{CBCT}$  segmented by the deep learning model and the different CTV of the patients's library ( $CTV_{CT} \in \{CTV_{EB}, CTV_{IB}, CTV_{FB}\}$ ):

$$cov = \frac{|CTV_{CBCT} \cap CTV_{CT}|}{|CTV_{CT}|} \quad (1)$$

where  $|\cdot|$  is the cardinality of the set. In this way, each CBCT had a coverage value associated with each of the three pCTs (IB, EB, FB) of the patient.

All the three pCTs of the considered patient were ranked according to the corresponding coverage. The pCT corresponding to the highest coverage value was selected as the PoD of the considered treatment fraction.

## 2.4 Evaluation

The data of the 23 patients were used to evaluate the proposed PoD selection process.

### 2.4.1 Segmentation evaluation

The segmentation of CBCT images was evaluated using four-fold cross-validation, considering the manual expert delineations as the reference. The following geometric metrics were computed for CTV, bowel bag, rectum, and bladder.

#### i) Volume-based metric

The Dice similarity coefficient (DSC) allows for comparing the automatic segmentation results ( $S_p$ ) with the reference delineation ( $S_r$ ) where a perfect overlap returns 1, and no overlap returns 0:

$$DSC = 2 \frac{|S_r \cap S_p|}{|S_r| + |S_p|} \quad (2)$$

## ii) Distance-based metrics

Distance-based metrics allow for evaluating the segmentation in terms of the location and shape accuracies of the segmented region boundaries. They use two point sets, A and B, from  $S_p$  and  $S_r$ . N is the number of points in A.

Mean absolute distance (MAD) measures the average distance of one boundary pixel to the closest boundary pixels in the other segmentation:

$$MAD = \frac{1}{N} \sum_{a \in A} \min_{b \in B} \|a - b\| \quad (3)$$

Hausdorff distance (HD) measures the similarity between two boundaries and can be expressed as:

$$HD = \max(h(A,B), h(B,A)) \quad (4)$$

where  $h(A,B) = \max_{a \in A} \min_{b \in B} \|a - b\|$ . We reported HD95, i.e., the 95<sup>th</sup> percentile of HD, to limit the influence of small outliers.

### 2.4.2 PoD selection evaluation

For each treatment fraction, the PoD resulting from the proposed automatic process was compared to the one obtained using the reference delineation of the CTV in the CBCT image. Thus, this reference PoD corresponded to the best coverage between the manual delineation of the  $CTV_{CBCT}$  and  $CTV_{CT} \in \{CTV_{EB}, CTV_{IB}, CTV_{FB}\}$ .

To consider that multiple treatment plans may provide a satisfying coverage of the target, a 5% tolerance was applied to the maximum coverage, and the corresponding treatment plan(s) were also selected.

The accuracy of the PoD selection was determined by calculating the number of automatically selected PoD that were identical to the reference PoD or included in the selected treatment plans.

## 3. Results

### 3.1 Performance of segmentation

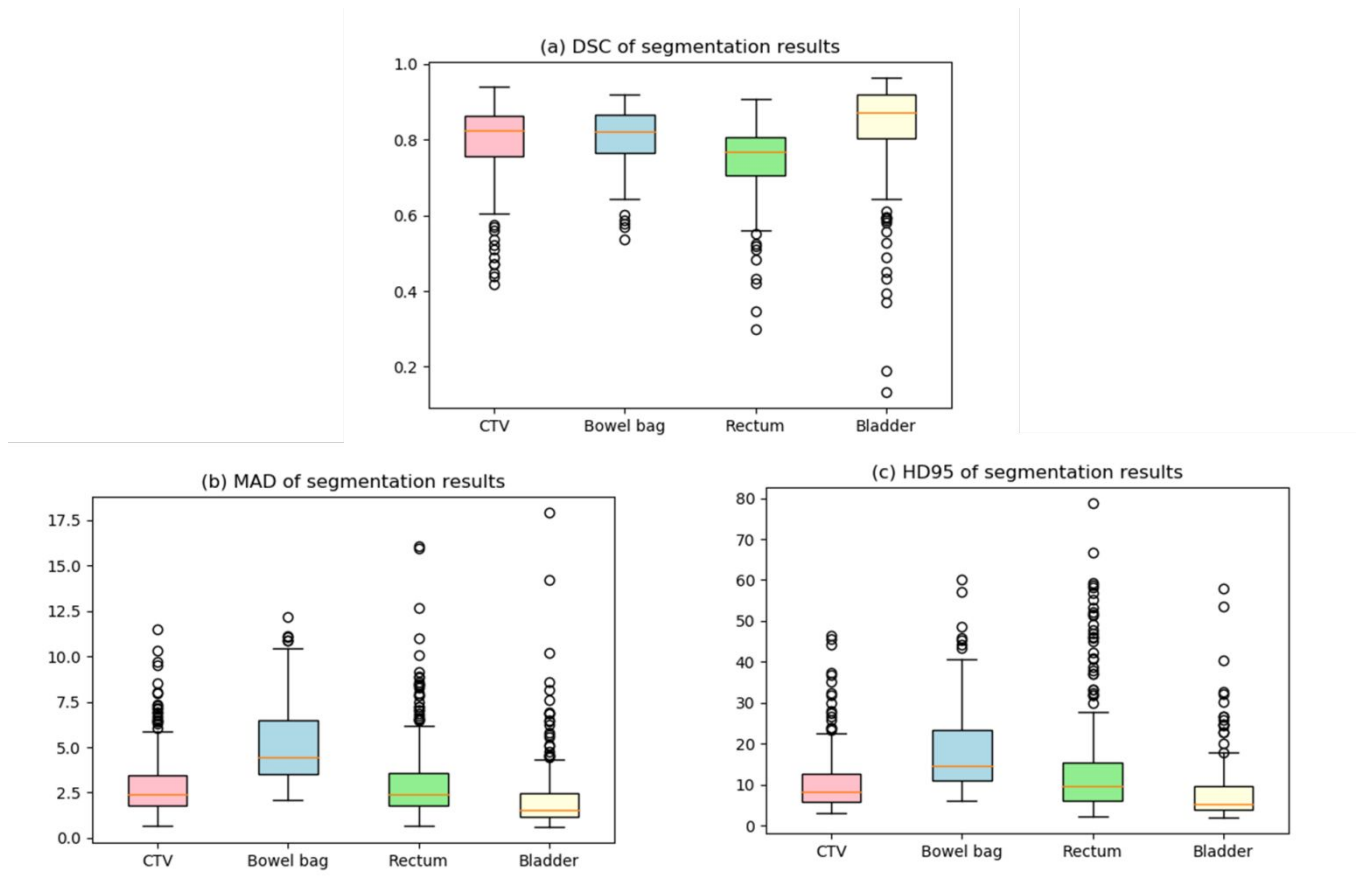
Table 3 reports the mean (range) values of the geometric metrics for the automatic segmentation. Figure 3 summarizes the quantitative results in boxplots. The median DSC of primary CTV, bowel bag, rectum, and bladder were 0.79, 0.81, 0.75, and 0.84, respectively. Figure 4 shows the results of automatic contouring for four patients in axial and sagittal views.

Organ	DSC	MAD (mm)	HD95 (mm)
CTV	0.79 (0.42 - 0.94)	2.90 (0.65 - 11.48)	10.49 (3.02 - 46.43)
Bowel bag	0.81 (0.53 - 0.92)	5.22 (2.12 - 12.15)	18.40 (6.12 - 60.43)
Rectum	0.75 (0.30 - 0.91)	3.14 (0.65 - 16.04)	14.19 (2.24 - 78.79)
Bladder	0.84 (0.13 - 0.96)	2.91 (0.61 - 17.9)	9.45 (2.03 - 58.22)

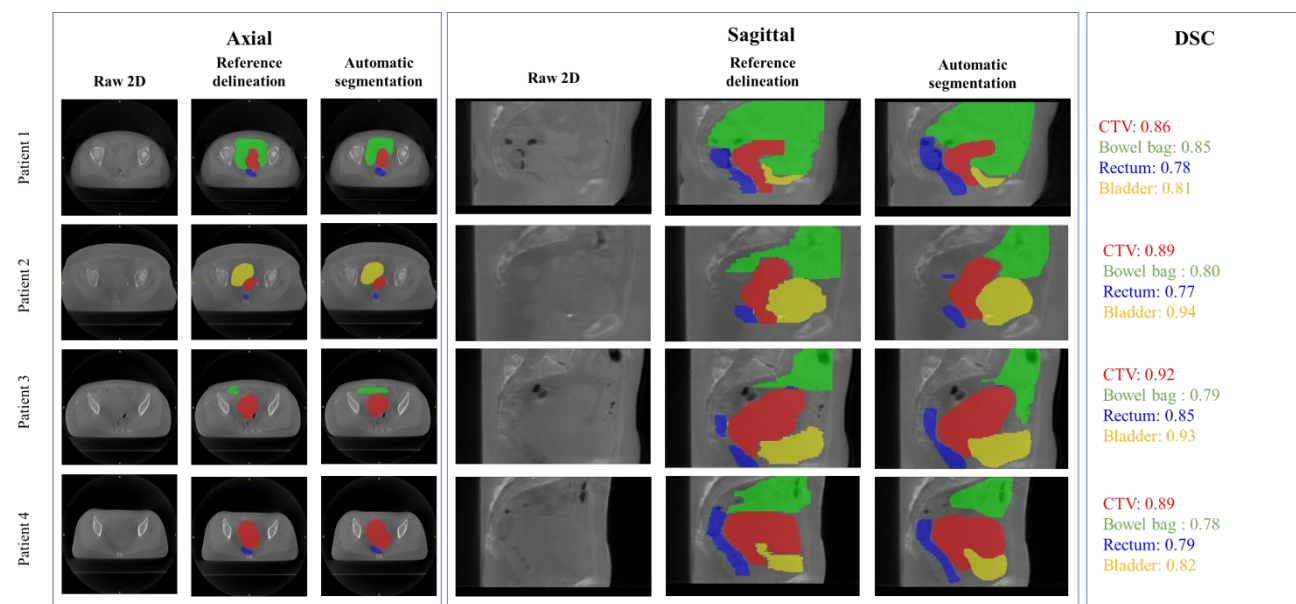
Table 3. Quantitative evaluation results of CBCT segmentation.



DSC = Dice similarity coefficient ; MAD = Mean absolute distance ; HD95 = 95 th percentile Hausdorff Distance



**Figure 3. Quantative segmentation results of CTV (uterus), bowel bag, rectum and bladder presented as boxplots. (a) DSC = Dice similarity coefficient ; (b) MAD = Mean absolute distance ; (c) HD95 = 95<sup>th</sup> percentile Hausdorff Distance**

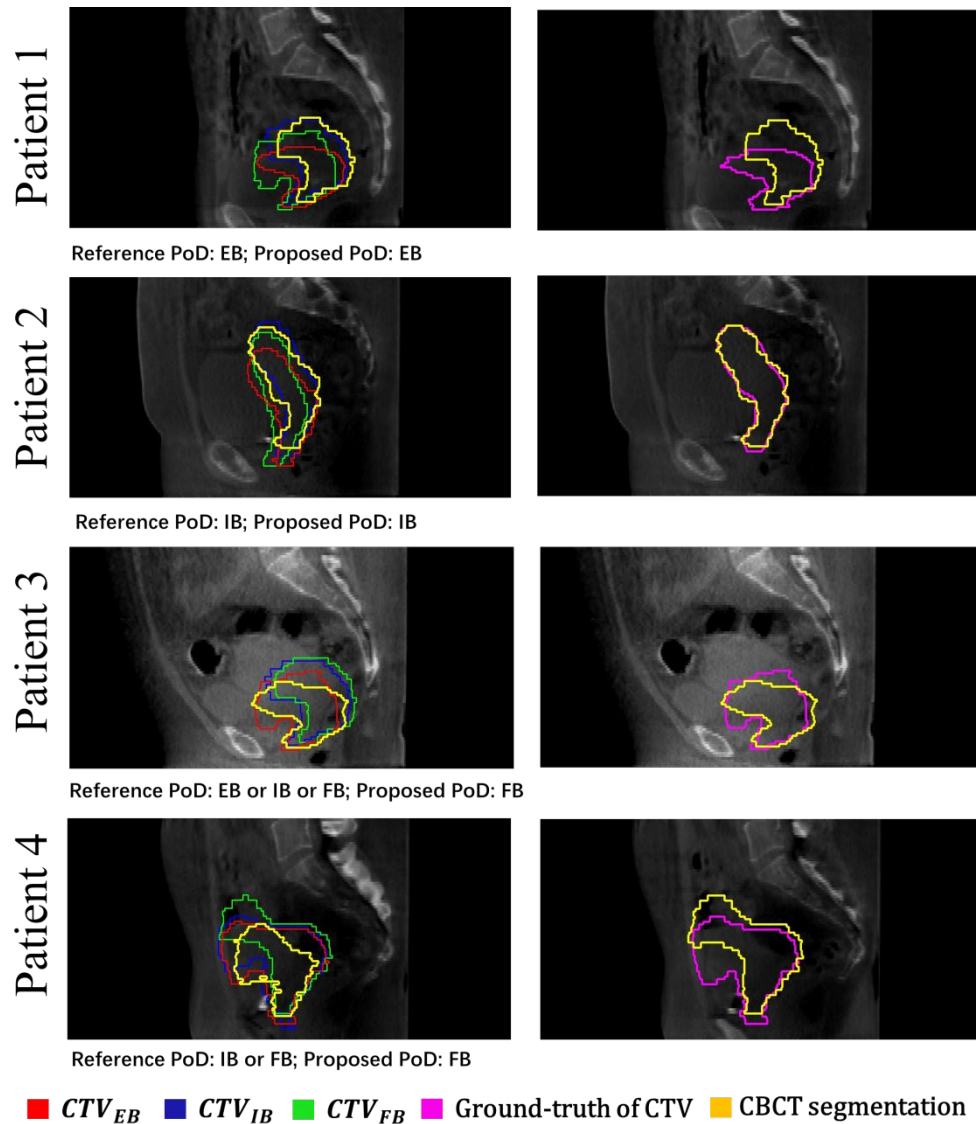


**Figure 4. Examples of segmentation on CBCT.** The contours are represented on the axial and sagittal views in red, green, yellow and blue for the primary CTV, bowel bag, bladder and rectum, respectively. DSC: Dice similarity coefficient.

### *3.1 Performance of treatment plan selections*

Considering the accuracy of automatic PoD selection without the 5% tolerance, an agreement between the reference PoD and the automatically identified PoD was observed for 91.5% of CBCTs. This resulted in 23 out of 272 tested CBCTs having a suboptimal selected PoD, compared to the reference.

Using the 5% tolerance value for PoD selection, multiple (up to three) pCTs could be selected as optimal PoD. This resulted in



**Figure 5. Examples of automatic PoD selection for four patients.** (Left) Result of segmentation and clinical target volumes (CTVs) corresponding to the planning library for PoD selection; (Right) Automatic and reference CTV segmentations. Illustrated patients were selected based on the following criteria: single selected PoD (Patients 1 and 2); multiple PoD selections due to the tolerance value of 5% (Patient 3 and 4).



Reference PoD: IB or FB; Proposed PoD: EB; Dice: 0.52

■  $CTV_{EB}$  ■  $CTV_{IB}$  ■  $CTV_{FB}$  ■ Ground-truth of CTV ■ CBCT segmentation

**Figure 6. One case with suboptimal PoD selection.** (Left) Result of segmentation and clinical target volumes (CTVs) corresponding to the planning library for PoD selection; (Right) Automatic and reference CTV segmentations. The poor segmentation of CTV results in the suboptimal PoD selection.

an increased PoD selection agreement to 99.6%, with one CBCT having suboptimal PoD selection. Figure 5 shows the PoD selection on four different patients corresponding to an agreement between the proposed and selected PoDs. Figure 6 illustrates the only case with suboptimal PoD selection. For this case, the automatic segmentation results were poor (Dice of CTV segmentation was 0.52), which resulted in the wrong proposed PoD.

#### 4. Discussion

This study aimed at improving the PoD selection for LACC ART on CBCT images. Simulating the proposed process on 272 treatment fractions, it resulted in an agreement between the reference PoD and the automatically identified PoD for all fractions except one.

The first step of the process was based on the automatic segmentation of the daily images using a deep learning network. The resulting average DSC on the 272 CBCT images were higher than 0.75 for the primary CTV and the three main OARs (bowel bag, rectum, and bladder).

Only two works in the literature, to the best of our knowledge, have proposed cervix CBCT automatic segmentation (Langerak *et al* 2014, Beekman *et al* 2022). Langerak *et al.* (Langerak *et al* 2014) used a multi-atlas-based segmentation method. On a total of 224 CBCT, the images corresponding to low confidence levels were firstly removed, resulting to 187 images on which the Dice values were 0.85, 0.81, and 0.80 for the uterus, bladder, and rectum, respectively. Without discarding any CBCT image, the DSC values obtained in our study were close to these ones, with lower values for CTV and rectum, and higher values for bladder. More recently, Beekman *et al.* (Beekman *et al* 2022) compared different deep learning approaches and showed that the best performances were obtained by a deformation-based registration network with a mean DSC of 0.80 on the uterus, computed on a test set of 20 CBCT images. In our study, we obtained similar DSC on 272 CBCT images. This study and (Beekman *et al* 2022) are the only ones using deep learning for cervix CBCT segmentation. Although 2D and 3D U-Net (or V-Net) networks have been used on planning CT images (Liu *et al* 2020, Rhee *et al* 2020, Rigaud *et al* 2021) resulting to larger DSC for CTV ( $0.86 \pm 0.08$ ), lower contrast, higher noise, but also limited availability of reference segmentation, challenge the exploitation of these methods on CBCT. To our knowledge, this is the first study exploiting nnU-Net on CBCT images and on the uterine region. It confirms its good performances which have been shown on other imaging modalities (Isensee *et al* 2021).

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3 In this study, the deep learning model was trained to segment not only the CTV (which is important for PoD selection), but  
4 also the main OARs. Intuitively, a binary segmentation task (segmenting only CTVs) could be easier than a multi-class  
5 segmentation task (segmenting OARs and CTVs) and thus could achieve better segmentation results. However, in terms of  
6 geometric considerations, multi-class segmentation provides a positional prior (e.g. the uterus should be between the bladder  
7 and rectum). Such a positional prior helps the convolutional neural network to constrain the position of the uterus during  
8 segmentation. Preliminary experiments have validated this assumption, with better results when including OARs in the  
9 segmentation task.  
10  
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12

13 The evaluation of the proposed process, not only in terms of segmentation accuracy (e.g., with Dice score) but in terms of  
14 PoD selection, is of clinical interest since this PoD selection is, in this adaptive strategy, the most important and difficult step.  
15

16 In the current clinical practice, the treatment plan is selected visually, resulting in potentially high inter-observer variations  
17 (Gobeli *et al* 2018). The identification of the optimal treatment plan appears particularly difficult in the context of complex  
18 deformations and limited image quality. Langerak *et al.* (Langerak *et al* 2014) proposed a PoD selection, after CBCT  
19 segmentation, by comparing the segmented bladder volume to the preoperative planning library (empty and full bladder).  
20 However, the CTV shape may be influenced by other factors than bladder filling, including rectum filling, tumor shrinkage, or  
21 non-moving cervix. The PoD selection should thus ideally be primarily based on the shape of the target.  
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23  
24

25 In this paper, the criteria used to select the PoD was the coverage of the daily CTV by the CTVs corresponding to the  
26 different planning CTs. It enabled to consider directly the treatment of the target instead of a surrogate of the target position.  
27 Moreover, selecting the best plan as the one providing the best CTV coverage is the approach considered in the literature  
28 (Gobeli *et al* 2018, Heijkoop *et al* 2014). On the other hand, since the OARs were also segmented in the proposed process,  
29 considering the OARs in the PoD selection is technically possible. However, it would require the definition of a decision  
30 process, or a metric, considering and weighting the different criteria (CTV and OARs coverage).  
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34 In our study, only 1 case (out of 272) resulted in wrong PoD selection (Figure 6). This case with a relatively small uterus,  
35 was caused by poor segmentation result. In a clinical context, this kind of result would be easily visually detected. Then, the  
36 treatment plan could be manually selected in the library or a backup plan could be used as proposed in (Heijkoop *et al* 2014).  
37

38 Online adaptive radiotherapy has recently seen important improvements, especially with the development of MRI-linac and  
39 CBCT-based online optimization. For both of them, some challenges remain and hamper their clinical deployment to treat  
40 cervical cancer, including the limited quality of CBCT images and long treatment times of MRI-Linac. Very few studies have  
41 thus considered these kinds of systems to treat cervical cancer patients (Shelley *et al* 2021, Yock *et al* 2021). Moreover, the  
42 combination of online adaptation with PoD strategies may be of interest to optimize the clinical workflow and limit treatment  
43 times.  
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46 There are some limitations to our study. The PoD selection criterion was only based on geometrical coverage. It may be of  
47 interest to consider dosimetric criteria, which is challenging since it would require computing the dose distribution on the CBCT  
48 images. Another limitation is related to the limited number of patients in this study. The proposed workflow will have to be  
49 evaluated on a larger cohort. Especially, the evaluation of the segmentation network will have to be deepened, potentially  
50 resulting in the need to improve the robustness of the model by training it with new data. Finally, the PoD ART strategy based  
51 on multiple planning CTs has shown some limitations, and some more complex strategies have been proposed to improve the  
52 libraries. For example, an “evolutive library” strategy has been proposed, enriching the library by including some CBCT  
53 anatomies into the library when the daily clinical target volume (CTV) shape differed from the ones in the library (Rigaud *et al*  
54 2018). Including modeled anatomies resulting from a population analysis has also been proposed (Rigaud *et al* 2019). All  
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these strategies are based on daily PoD selection, and thus combining the proposed PoD selection method with them should be investigated.

## 5. Conclusion

This work proposed and evaluated an automatic workflow to select PoD for LACC ART. Based on CBCT image segmentation using a deep-learning method, it selects the optimal treatment plan based on daily CTV geometrical coverage. The evaluation of 272 treatment fractions showed a high agreement with the reference resulting from expert delineation. The proposed workflow should be further evaluated in a clinical workflow and on a larger number of patients.

## Acknowledgments

This work was partly funded by the French National Research Association (ANR) as part of the Investissement d'Avenir programme (Labex CAMI) under reference ANR- 11-LABX-0004, by the DELPEL project with financial support from ITMO Cancer AVIESAN (National Alliance for Life Sciences & Health) within the framework of the Cancer Plan, by the French organizations "Ligue contre le Cancer" and "La Vannetaise", and by the Embassy of France in China.

## Ethical Statement

This research was conducted in accordance with the principles embodied in the Declaration of Helsinki and in accordance with local statutory requirements. It has been approved by the regional research ethics committee (Comité de Protection des Personnes, Ouest V, Rennes, AR-COL 2015-02-45-01). All participants gave written informed consent to participate in the study.

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