



HAL
open science

Energy dependent z-scores improve parallel imaging motion correction using trimmed autocalibrating k-space estimation (TAKE)

Jeremy Beaumont, Thomas Troalen, Swetali Nimje, Ludovic de Rochefort,
Stanislas Rapacchi

► To cite this version:

Jeremy Beaumont, Thomas Troalen, Swetali Nimje, Ludovic de Rochefort, Stanislas Rapacchi. Energy dependent z-scores improve parallel imaging motion correction using trimmed autocalibrating k-space estimation (TAKE). Proc. Intl. Soc. Mag. Reson. Med., May 2022, London, United Kingdom. pp.0352. hal-03859860

HAL Id: hal-03859860

<https://hal.science/hal-03859860v1>

Submitted on 18 Nov 2022

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

Energy dependent z-scores improve parallel imaging motion correction using trimmed autocalibrating k-space estimation (TAKE)

Jeremy Beaumont¹, Thomas Troalen², Swetali Nimje^{1,3}, Stanislas Rapacchi¹, and Ludovic de Rochefort¹
¹Aix Marseille Univ, CNRS, CRMBM, Marseille, France, ²Siemens Healthcare SAS, Saint-Denis, France, ³Aix Marseille Univ, CNRS, LIS, Marseille, France

Synopsis

MRI motion corruption prevents clinical interpretation and image analysis for research purposes. The trimmed autocalibrating k-space estimation based on parallel imaging and structured matrix completion (TAKE) algorithm was previously proposed to retrospectively correct motion corrupted raw k-space data. This study proposes specific modifications of the TAKE algorithm to decrease its computation time and improve the detection of motion-corrupted k-space data. The proposed changes significantly improve the TAKE motion detection sensitivity and specificity along with its motion correction performance, while sufficiently decreasing its computation time to allow for its use in a standard clinical routine workflow.

Introduction

Many motion correction algorithms have been proposed to allow for the clinical interpretation and quantitative analysis of motion-corrupted magnetic resonance images (MRI)¹. Among these algorithms, the trimmed autocalibrating k-space estimation based on structured matrix completion (TAKE) algorithm² was proposed to retrospectively correct raw k-space data collected with 2D MR sequences without requiring an additional navigator in the pulse sequence. Two major limitations prevent the use of TAKE in clinical practice: 1) the detection of motion-corrupted k-space lines depends on the local k-space energy, thus leading to both the non-detection of low energy motion-corrupted lines and false detection of non-corrupted lines characterized by a high energy; and 2) the computation time is prohibitive to allow for the algorithm to be used in a standard clinical workflow. In this context, the current study aims at providing a robust version of TAKE (Robust TAKE) characterized by both a lower dependency to the local k-space energy and a shorter computation time.

Methods

TAKE consists in detecting motion-corrupted k-space lines from residuals computed between the raw k-space data and its structured low rank matrix approximation². In TAKE, the motion detection was reduced to a 1D problem by summing the residuals in the frequency encoding (FE) and coil dimensions. Raw k-space phase encoding (PE) lines with the maximum residual value were iteratively detected as motion-corrupted and replaced by their approximation until all 1D residual robust z-scores were lower than a given threshold.

The improvements proposed in Robust TAKE compared to TAKE are the following: the raw k-space was subject to coil compression to decrease the computation time; the 2D kernel used for structured low rank matrix approximations was replaced by a 1D kernel in the PE dimension; the residuals were computed with the Berhu norm³ instead of the L1 norm; robust z-scores (denoted as energy dependent z-scores) were computed on the residuals as a function of the k-space center distance in order to reduce the local k-space energy dependency; the k-space was linearly subsampled in the FE dimension by a factor equals to twofold the PE subsampling rate in order to both reduce the local energy dependency and computation time; the 1D residuals were obtained by summing the energy dependent z-scores in the coil dimension and then computing their median in the FE dimension; and the motion corrupted k-space lines were replaced by their SPIRIT approximation⁴ instead of their structured low rank matrix approximation.

In-vivo MR experiments were conducted under written informed consent on a 3T system (MAGNETOM Vida, Siemens Healthcare, Erlangen, Germany) using a 20-channel head and neck coil. Raw k-space data was collected on two healthy volunteers that underwent T2-weighted turbo spin echo imaging (40 slices; resolution: 0.5 x 0.5 x 3 mm³; GRAPPA 2; TA: 2:52 mins) in two different head positions. Motion-corrupted Monte-Carlo experiments were generated by randomly replacing 5% of PE lines from one T2-weighted k-space data by their counterparts in the second T2-weighted k-space data (10 experiments per slice). Experiments from three randomly selected slices of the same subject were used as a training database to optimize kernel sizes and 1D residual z-score thresholds. The remaining experiments were used as a validation database on which the motion detection sensitivity and specificity were computed. The gradient entropy, a metric that was strongly related to observer ratings of MRI motion corruption in a previous study⁵, was computed on the TAKE and Robust TAKE reconstructed MR images and compared with the ground truth to assess the algorithms motion correction performances.

Results

The energy dependent z-scores used by Robust TAKE for motion detection showed a lower dependence to the local k-space energy than the residuals used by TAKE (Figure 1). The local k-space energy dependency remained lower in Robust TAKE when the motion detection was reduced to a 1D problem (Figure 2). The Robust TAKE lower k-space energy dependency allowed to significantly improve its motion detection sensitivity (76.7% vs 72.3%, $p < 0.0001$) and specificity (96.3% vs 95.1%, $p < 0.0001$) compared to TAKE (Table 1, Figure 3). Similarly, the motion correction performances provided by Robust TAKE were significantly better ($p < 0.0001$) than the ones provided by TAKE (Table 1, Figure 3).

In most cases, TAKE and Robust TAKE greatly reduced the presence of motion artefacts in reconstructed images (Figure 4, top rows). However, the TAKE reconstruction sometimes failed due to the false rejection of too many lines characterized by a high energy (Figure 4, bottom row). The TAKE and Robust TAKE performances can also greatly decrease for cases where the motion detection threshold is incoherent with the data, which either leads to a very low sensitivity or lowers the specificity.

The average Robust TAKE computation time (21 secs) was 97% lower than the average TAKE computation time (673 secs).

Discussion

Robust TAKE allowed to significantly improve both motion detection and correction performances compared to TAKE, while greatly reducing the algorithm computation time to reach performances more suitable for a clinical routine use. However, the Robust TAKE performances greatly decrease when the motion detection threshold is incoherent with the data. Future studies will aim at further improving the Robust TAKE

performances by using adaptive motion detection methods with data-driven threshold definitions.

Acknowledgements

This project is supported by Siemens Healthcare SAS, France and Aix-Marseille University around the industrial Chaire 7TEAMS

References

1. Zaitsev M, Maclaren J, Herbst M. Motion artifacts in MRI: A complex problem with many partial solutions. *J Magn Reson Imaging*. 2015;42(4):887-901. doi:10.1002/JMRI.248502.
2. Bydder M, Rapacchi S, Girard O, Guye M, Ranjeva JP. Trimmed autocalibrating k-space estimation based on structured matrix completion. *Magn Reson Imaging*. 2017;43:88-94. doi:10.1016/J.MRI.2017.07.0153.
3. Zwald L, Lambert-Lacroix S. The BerHu penalty and the grouped effect. Published online July 30, 2012. Accessed November 9, 2021. <https://arxiv.org/abs/1207.6868v14>.
4. Lustig M, Pauly JM. SPIRiT: Iterative self-consistent parallel imaging reconstruction from arbitrary k-space. *Magn Reson Med*. 2010;64(2):457-471. doi:10.1002/MRM.224285.
5. Mcgee KP, Manduca A, Felmlee JP, Riederer SJ, Ehman RL. Image Metric-Based Correction (Autocorrection) of Motion Effects: Analysis of Image Metrics. *J Magn Reson Imaging*. 2000;11:174-181. doi:10.1002/(SICI)1522-2586(200002)11:2

Figures

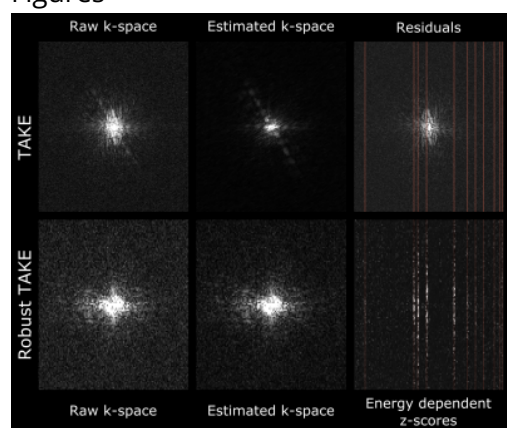


Figure 1. Raw (left) and estimated (center) k-space data from a given coil and motion corruption obtained during TAKE (top) and Robust TAKE (bottom) motion corrections (same window/level for all k-space images). The residuals used by TAKE (top right) for motion detection mainly depend on the local k-space energy. The energy dependent z-scores used by Robust TAKE (bottom right) for motion detection mainly depend on the motion corruption information. Red lines: ground truth motion corruption.

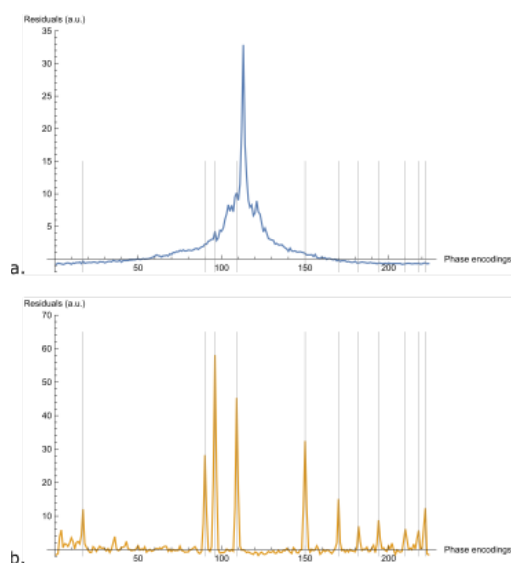


Figure 2. 1D residuals obtained during the TAKE (a) and Robust TAKE (b) motion correction of the data presented in Figure 1. Vertical gray lines design the motion corrupted lines. The 1D residuals obtained with TAKE depend both on the local k-space energy and the presence of motion

corruption (a), while the 1D residuals obtained with Robust TAKE depend only on the presence of motion corruption (b).

	Motion detection sensitivity (%)	Motion detection specificity (%)	Relative gradient entropy difference (%)
TAKE	72.3 (0 - 100)	95.1 (83.1 - 100)	-7.4 (-46.6 - +4.8)
Robust TAKE	76.7 (0 - 100)	96.3 (76.1 - 100)	+0.3 (-8.9 - +7.3)
p-value*	$p < 0.0001$	$p < 0.0001$	$p < 0.0001$

Sensitivity, specificity and relative gradient entropy ranges are shown in parentheses

*Bonferroni-corrected Wilcoxon signed-rank test

Table 1. Motion detection sensitivity and specificity obtained from TAKE and Robust TAKE on the validation database. Both sensitivity and specificity significantly increased in Robust TAKE compared to TAKE. The gradient entropy computed on Robust TAKE reconstructed images differed significantly less from the ground truth than the one obtained from the TAKE reconstructed images, suggesting that Robust TAKE provides a better correction of motion-corrupted k-space data in the validation database.

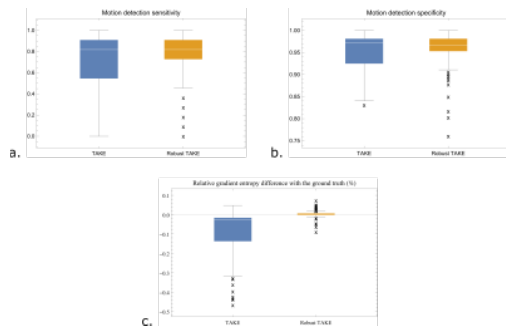


Figure 3. TAKE and Robust TAKE motion detection sensitivity (a), specificity (b) and image reconstruction relative gradient entropy differences with the ground truth (c) computed on the validation database. In line with the results presented in Table 1, Robust TAKE improves the motion detection sensitivity and specificity compared to TAKE. It also provides a motion corrected image that is closer to the ground truth (relative gradient entropy difference metric) in the validation database.

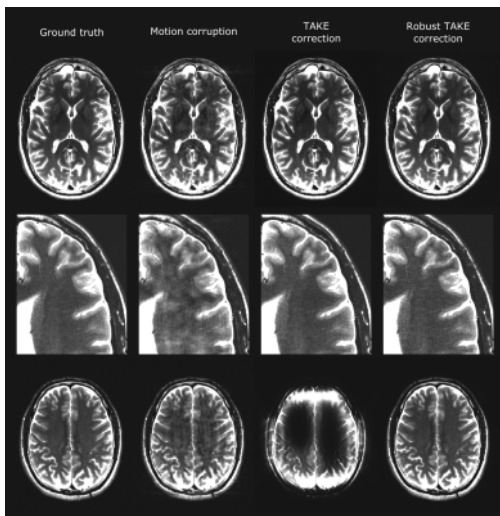


Figure 4. T2-w images obtained from GRAPPA reconstructions performed on the ground truth (left), motion-corrupted (center-left), TAKE-corrected (center-right) and Robust TAKE-corrected (right) k-space data for two different subjects, slices and motion corruptions. TAKE and Robust TAKE allowed to greatly reduce the presence of motion artefacts in most experiments (top rows). In some cases, TAKE rejects too many high k-space-energy lines, which prevents correct image reconstruction (bottom row).