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1 Atomic force microscopy characterization of polyethylene

2 terephthalate grafting with poly(styrene sulfonate)

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21 Abstract

Polyethylene terephthalate (PET) is widely used to elaborate biomaterials and medical devices in particular for long-term implant applications but tuning their surface properties remains challenging. We investigate surface functionalization by grafting poly(sodium 4styrene sulfonate, PNaSS) with the aim of enhancing protein adhesion and cellular activity.

Elucidating the topography and molecular level organization of the modified surfaces is 26 important for understanding and predicting biological activity. In this work, we explore 27 28 several grafting methods including thermal grafting, thermal grafting in the presence of 29 Mohr's salt, and UV activation. We characterize the different surfaces obtained using atomic force microscopy (AFM), contact angle (CA), and X-ray photoelectron spectroscopy (XPS). 30 We observe an increase in the percentage of sulfur atoms (XPS) that correlates with changes 31 32 in (CA), and we identify by AFM characteristic features, which we interpret as patches of polymers on the PET surfaces. This work demonstrates tuning of biomaterials surface by 33 34 functionalization and illustrates the capability of atomic force microscopy to provide insights 35 into the spatial organization of the grafted polymer.

Keywords: Peakforce Quantitative Nano-mechanical Properties (PF-QNM); Polyelectrolyte
 brushes; Polyethylene Terephthalate (PET), Poly(sodium 4-styrene sulfonate (PNaSS)

38

39 1. Introduction

Polyesters, in particular polyethylene terephthalate (PET), are used extensively in medical 40 41 devices. Surface functionalization is often required to improve biological properties. Poly (sodium 4-styrene sulfonate) (PNaSS) is a strong polyelectrolyte, which has been proposed 42 43 for the control of biological and biophysical properties including enhancing cell adhesion, 44 spreading, and proliferation, thus improving bone tissue response[1,2], fibroblast behavior for reconstructing injured ligament and wound healing[2–5], antibacterial infection[6] and 45 biocompatible surface[5,7]. PNaSS enhances the biological properties of PNaSS-grafted 46 surfaces: the mechanism at the origin of this activity involves specific interactions between 47 adsorbed binding proteins (fibronectin, FN) on functionalized surfaces and integrin at the 48 49 cell membrane^[1,2]. Briefly, the presence of sulfonate groups allows improving cell adhesion, proliferation, differentiation and/or biointegration in surrounding tissues when 50 51 implanted in vivo[1]. This has been shown in vitro with different types of cells (fibroblast, endothelial cell, and osteoblast) and in vivo in the case of PNaSS-grafted titanium, PET and 52 PCL implants. PNaSS immobilized on different materials such as titanium[1,8], polyethylene 53 54 terephthalate (PET)[2,3], nanoparticle[5,9,10] or polycaprolactone (PCL) has been reported.

Several surface functionalization methods with poly(styrene sulfonate) have been proposed, e.g. sulfonation polystyrene brush [10,11] and grafting methods[12–14]. Among those, "grafting-from" has the advantage of being a scalable approach to the modification of interfacial properties through immobilizing the functional groups on the substrate by covalent bonding. The "grafting from" method starts with activation of the surface via plasma[15], UV irradiation[7,16], heating[14,18], in the presence of CuBr₂[18–20], or Mohr's salt[13,14].

In this work, we activate PET surfaces by ozonation, a method convenient for materials with complex geometries such as implants[21]. Ozonation generates peroxide groups which decompose upon heating and UV irradiation[14,22,27] to generate radicals on PET; NaSS polymerizes from these active sites. The mechanism can be described as: the peroxides after decomposition form two types of free radicals, [•]OH and O•, and then C[•] (carbonyl) radicals[21] on the polymer chains. Free radicals [•]OH can be consumed by Fe²⁺ in Mohr's salt, thus reducing homopolymerization and promoting grafting[14,23,24].

Previous studies examined the effect of the graft PNaSS on the interaction of the modified surfaces with biological molecules yet the characterization of the grafted layer is often limited. Here, we investigate the topography of grafted polymers by atomic force microscopy (AFM) complemented by XPS and contact angle measurements.

73

74 2. Materials and Methods

75 **2.1. Materials**

Sodium 4- styrene sulfonate (NaSS), phosphate buffer saline (PBS), and Mohr's salt were
purchased from Sigma Aldrich. Polyethylene terephthalate (PET) (0.25 mm, biaxially
oriented plate) was purchased from Goodfellow (Paris, France). Ethanol absolute was from
Fisher.

80 **2.1.1. PET preparation:**

PET plate was cut into small squared pieces (1 cm \times 1 cm). The surface was cleaned in an ultrasonic bath with ultrapure water, acetone, and ethanol for 10 min respectively. The samples were dried under vacuum for 2 h and stored at 4°C until use.

84 **2.1.2.** Monomer purification:

The purification of NaSS was described [14,17,25] 90 g of NaSS was dissolved in 1.6 L of ethanol: distilled water (9:1, v/v) by stirring 12 h at 70°C. Thereafter, the solution was filtered by vacuum filtration. The filtered solution was kept at 4°C during 24 h for recrystallization. Recrystallized monomer was collected by vacuum filtration and was dried in vacuum at 30°C for 6 h. Finally, the product was kept at 4°C, away from the light.

90

91 2.2. Functionalization of polyester surfaces by PNaSS ("grafting from")

92 **2.2.1.** Activating the surfaces by ozonation

The functionalization of polyesters by PNaSS includes two main steps: ozonation and grafting (Scheme 1). In the first step, the polymer surfaces were activated by ozonation using ozone generator BMT 802N. 6 PET plates were ozonized into 100 mL distilled water by introducing ozone flow (0.6 bars, 100 mL/min) for 20 min for PET at 30° C.[14] Ozonized samples were quickly transferred from the ozonation reactor to the degassed NaSS solution (0.7 mol/L) for grafting.

99 **2.2.2. Grafting PNaSS from PET substrate**

After activation by ozonation, PNaSS was polymerized from the activated sites (Scheme 1). For determining the influence of ozonation on the surface, non-grafted-ozonized polymer or ozonized PET without grafting was used as a reference. Non-grafted-ozonized PET was prepared by ozonation of a PET plate for 20 min at 30°C.

104 Thermal radical polymerization (method 1 and 2):

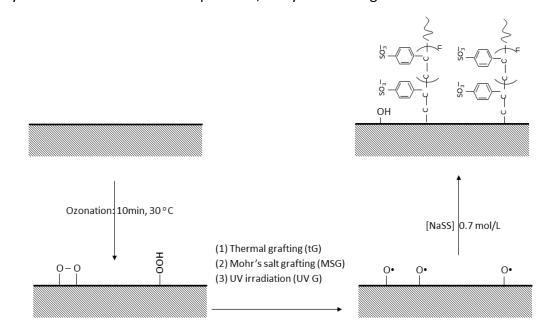
Method 1 - Thermal grafting (TG)[13,14]. 6 ozonized PET plates were transferred into 60 mL
 of degassed NaSS (0.7 mol/L) solution and heated for 1 h at 75°C. Peroxide decomposition
 generates the radicals on the surface for initiating PNaSS polymerization.

108 **Method 2-Thermal grafting in the presence of Mohr's salt (MSG).** 6 ozonized PET plates 109 were transferred into 60 mL degassed mixture solution of NaSS (9 g, 0.7 mol/L) and Mohr's 110 salt (60 mg, 0.1 %, w/v) and heated to 75° C for 1 h. Mohr's salt provides Fe(II) ions that 111 increases significantly the grafting efficiency[14].

112 Photoinitiated free radical polymerization (method 3):

113 **Method 3-UV irradiation (UVG)**[22]. Peroxides were decomposed by UV irradiation. 6 PET 114 plates were transferred into 60 mL of degassed NaSS solution (9 g, 0.7 mol/L). The solution 115 was irradiated by UV light for 30 min (lamp UV-Omnicure, 254 nm, 10 W/cm²) at 25°C under 116 stirring.

After polymerization via either of the three methods above, free homopolymer, oligomer, and monomer were removed from the grafted samples under stirring in double distilled water for at least 48 h. The washing solution was tested by UV-vis at 360 nm to check for the presence of any residue of free PNaSS (homopolymer and oligomer). Samples were finally dried under vacuum and kept at 4°C, away from the light before use.



123 Scheme 1. Grafting PNaSS from polyester surfaces by ozonation and radical polymerization

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125 2.3. Surface characterization

126 **X-ray photoelectron spectroscopy analysis (XPS).** X-ray photoelectron spectroscopy analysis 127 (XPS) (from Omicron Argus spectrometer, Germany) was performed using a 128 monochromated AlKα radiation source (hv = 1486.6 eV) working at an electron beam power 129 of 300 W with 90° of takeoff angle of photoelectrons emission, under ultra-high vacuum 130 ($\leq 10^{-10}$ Torr). Spectra were recorded at pass energy of 100 eV for the survey spectrum and 131 pass energy of 20 eV for the high-resolution regions. Binding energies were calibrated against the C1s binding energy of aliphatic carbon atoms at 284.8 eV. Spectral
deconvolution was carried out using Casa XPS v.2.3.15 software (Casa Software Ldt, UK). All
samples were dry films.

The equivalent thickness probed by XPS is estimated to be close to $3\lambda = 10$ nm representing 95% of the signal, λ being the inelastic mean free path of electrons from the PET substrate in the organic PNaSS film; for electrons having a kinetic energy around 1200 eV (from the C1s atomic level), λ is estimated to be equal to 3.23 nm.¹

139 The estimated thickness (*d*) of PNaSS on top of PET can then be calculated using the 140 following formula:

$$\frac{I_{S2p}}{I_{C1s\ 284\ eV}} = \frac{\rho_{PNaSS} M_{ET} \sigma_{S2p} T_{S2p} \lambda_{S2p}^{PNaSS} (1 - \exp\left(\frac{-d}{\lambda_{S2p}^{PNaSS} \sin(\theta)}\right))}{\rho_{PET} M_{NaSS} \sigma_{C1s} T_{C1s} \lambda_{C1S}^{PET} (\frac{-d}{\lambda_{C1s}^{PNaSS} \sin(\theta)})}$$

141

Wherein: θ is the photoelectron collection angle. TC1s and TS2p are the relative sensitivity factors of C and S, respectively, provided by the spectrometer manufacturer. The Scofield photoionization cross-sections σ are equal to 1 for C 1s and 1.44 for S2p.² λx y is the inelastic mean free paths of electrons x in the matrix y. They were calculated using the Quases program (QUASES-IMFP-TPP2M Ver.3.0) based on the TPP2M formula. pPNaSS and pPET are the density of PNaSS and PET, respectively.M_{NaSS} and M_{ET} are the molecular weight of NaSS (sodium styrene sulfonate) and ET (ethylene terephthalate), respectively.

149

Contact angle. DSA10 contact angle system from KRUSS GmbH was used to measure the surface tension by the sessile drop technique. Two solvents: water (polar), and diiodomethane (unpolar) (2 μ L, 25°C, 8s) were used. The surface tension of polymer (γ_s) was calculated by Young-Dupre and Fowker's equation[26].

154 **Atomic Force Microscopy.** Atomic force microscope (AFM) multimode-8 from Bruker was 155 used. AFM scans were carried out in air using Scanasyst probe (ScanAsyst cantilever (Silicon

¹ Tanuma, S.; Powell, C. J.; Penn, D. R. Calculation of electron inelastic mean free paths (IMFPs) VII. Reliability of the TPP-2M IMFP predictive equation. Surf. Interface Anal. 2003, 35, 268–275.

² Scofield J (1976) Hartree–Slater subshell photoionization cross-sections at 1254 and 1487 eV. J Electron Spectrosc Relat Phenom 8(2):129–37

Nitride), triangular, reflective aluminium, symmetric tip with radius \leq 10 nm, f₀: 70 KHz, 156 spring constant: ~ 0.4 N/m), scan rate 1 Hz, at different scan sizes: 500 nm × 500 nm, 2 μm × 157 2 μm (3 samples). The absolute calibration was performed for each cantilever: Deflection 158 159 Sensitive, Spring Constant (~ 0.4 N/m) using Thermal Tuning and Lorentzian fitting (air), and 160 Tip Radius by Tip Qualification on Titanium roughness sample for PeakForce QNM (from BRUKER). Samples were dried in vacuum chamber in 4 h before scanning. Scanning was 161 performed in the room conditions. 3 independent surfaces in the same grafting conditions 162 were analyzed. The roughness (Ra) was measured on 3 points/surface. 163

Nano-Scope Analysis v.1.5, Image-J and AtomicJ software[27] were used for image analysis.
Surface mechanical properties was measured by Peakforce Quantitative Nano-mechanical
Properties (PF-QNM) program[28]. When numbers of samples are indicated, they refer to
independent experiments (from sample preparation).

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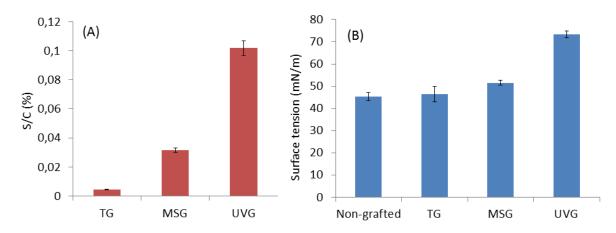
169 **3. Results**

170 **3.1.** Surface characterization

As a NaSS unit contains one atom of sulfur, the surface density of grafted PNaSS can be estimated based on the percentage of sulfur atoms in the elementary composition using XPS. Sulfur was not detected on the non-grafted-ozonized PET surfaces, but the S2p peak was visible (165 – 170 eV)[29] on the 4 grafted surfaces (see high resolution spectra in Figure S1). The quantification of those contributions indicated that the monomer surface density was much lower in the case of the thermal grafting than for the UV and Mohr's salt catalyzed grafting (Figure 1A).

Specifically, the S/C ratio for the UV and Mohr's salt samples was more than ten times 178 higher than for thermal grafting (Figure 1A). The PNaSS surface density (SD) by UV 179 irradiation was higher than when using Mohr's salt. The ranking was SD_{UVG-PET} > SD_{MSG-PET} > 180 SD_{TG-PET}. Whilst the XPS confirms the presence of PNaSS, the % S/C values themselves are 181 small indicating that the layers are thin and most probably patchy. Indeed, a rough estimate 182 value for the UVG PNaSS average layer thickness of 0.05 nm can be deduced from a simple 183 184 homogeneous model based on the depth probed by XPS being equal to 10 nm (Figure S2) and calculations thereafter. 185

Nevertheless, the surfaces were more hydrophilic after functionalization (Figure S3) and the 186 surface energy showed some correlation with the XPS results. The surface tension (γ_s) of 187 188 functionalized surfaces was measured by the contact angle method (Figure 1B). Non-grafted 189 and TG-PETs were similar: ~ 45-48 mN/m. However, surface tension increased significantly on UV grafting samples. Particularly, γ_s of UVG-PET increased by 54 % (73 mN/m) and 8 % 190 for MSG-PET (~ 52 mN/m). These variations correlate with the amount of SO_3^- groups (% 191 Sulfur by XPS) on the surface leading to the increase of surface tension (represented by the 192 S/C ratio in Figure 1A). 193



195 Figure 1. Surface characterization of non-grafted-ozonized and grafted PET: (a) S/C ratio196 from XPS and (b) surface tension by contact angle

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198 **3.2.** Investigating structure of PNaSS-grafted PET surface by AFM

The surface SEM images showed no obvious changes (Figure S4). Therefore, in this work, we 199 200 investigated the grafted surface using atomic force microscope (AFM). AFM can be used as a non-destructive method to analyze polymer surfaces[28,30–33]. Numerous parameters can 201 202 be investigated, e.g. the macromolecule structure^[18], thickness^[34–39], and adhesion. PNaSS-grafted PET surfaces were investigated by AFM peak force Quantitative Nano-203 mechanical properties (PF-QNM) in air at room temperature and compared to non-grafted-204 ozonized surface. Adhesion maps measure the interaction between the AFM tip and the 205 material : they can therefore provide clues as to the local chemical nature of the 206 207 surface^[40].

The surface topography and adhesion images of non-grafted-ozonized PET were used as a reference. The AFM images of the PET surfaces obtained after PNaSS grafting by the thermal grafting and Mohr's salt grafting methods are shown in Figure 2 and briefly described below.

211 Thermal radical polymerization:

Thermal grafting. TG-PET surface topography and adhesion were similar to the non-graftedozonized surface (Figure 2A-B). This was in agreement with the XPS and contact angle results which suggested a low degree of grafting. The surface roughness of TG-PET (Ra = 0.76 nm)-was similar with that of non-grafted PET (Ra = 0.96 nm), see in Figure 2E.

Thermal grafting in the presence of Mohr's salt. The topography of MSG-PET appeared similar but the surface roughness (Ra = 3.55 nm, see in Figure 2C) increased by a factor 3 (Figure 2E).

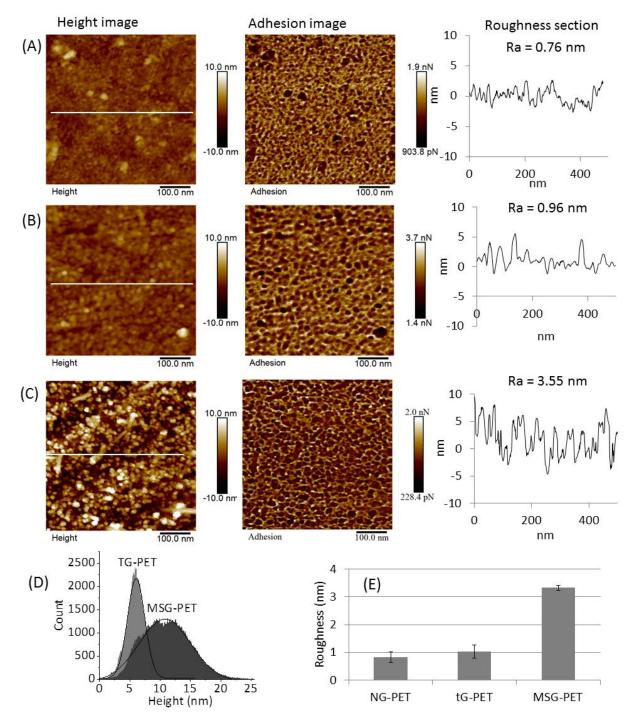
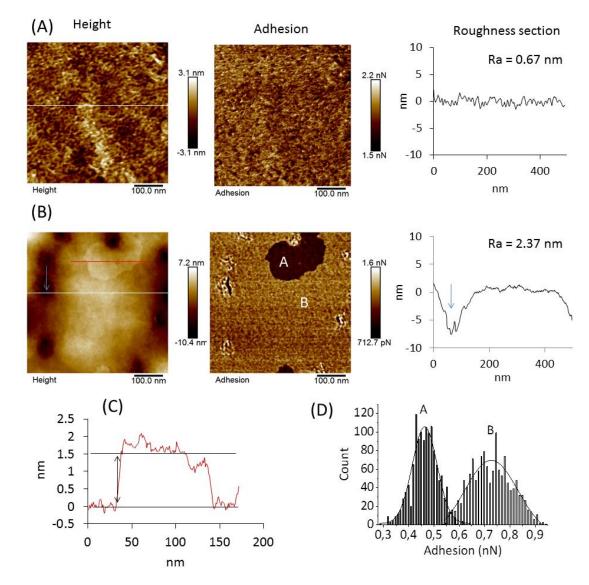


Figure 2. AFM images of non-grafted and thermal grafted PET: (A) non-grafted-ozonized PET
without grafting, (B) thermal grafting (TG-PET), (C) thermal grafting in the presence of
Mohr's salt (MSG-PET), (D) Height distribution of TG-PET and MSG-PET, (E) Roughness
values for each method; Scan in air, scan size 500 nm x 500 nm, 256 points/line, scan rate 1
Hz, PF-QNM

226 **Photoinitiated radical polymerization:**

227 UV grafting (UVG). Remarkably, in the case of UV grafting, both topography and adhesion 228 images (Figure 3) were drastically different from what had been observed in the other cases. 229 To evaluate whether the UV treatment itself had an effect on surface topography, a control 230 sample was prepared with non-grafted-ozonized PET under UV irradiation for 30 min without monomer. No major difference between this UV control (Figure 3A) and the non-231 232 grafted-ozonized control (Figure 2A) were observed. To the contrary, a smoother surface 233 was observed on UV grafted PET with patches particularly striking in the adhesion image 234 (Figure 3B). The patch shown in Figure 3C is \sim 1.5 nm thick (red line) and with reduced adhesion (Figure 3D). An average thickness of the patches can be deduced from multiple 235 236 measurements of different patches (\sim 1.2 nm, n = 5, Figure S5). Taking into account the 237 surface covered by the patches (~ 8% of the total area, Figure S5) the thickness averaged overall the whole area is ~0.09 nm (8% x 1.2 nm), consistent with the XPS results (~0.05 nm, 238 239 see above and Figure S2) suggesting that those patches are indeed composed of PNaSS.



240

Figure 3. AFM images of UV grafted PET (A) Control sample (ozonized PET under UV irradiation without monomer), (B) UV grafted PET, (C) Particular Cross-section by red line, and (D) Adhesion force distribution (flat surface, patches); scan size 500 nm x 500 nm, 256 points/line, scan rate 1 Hz, PF-QNM

245

246 4. Discussion

The combination of the XPS, surface tension and AFM images suggest the following picture of the grafted surfaces. The thermal grafting results indicate a low grafting (XPS results, Figure 1A) on PET. This correlates with the surface tension measurements where we do not observe significant changes from the unmodified surfaces (Figure 1B). The AFM images of those surfaces in dry air may not allow visualization of the PNaSS in the case of thermal grafting. The absence of detectable change in the case of thermal grafting is probably due to a combination of low grafting (as indicated by XPS and surface tension) and of the fact that the non-grafted-ozonized PET surface is already rough making it harder to detect small changes.

In the case of thermal grafting in the presence of Mohr's salt, XPS and surface tension measurements correlate and both point to an increased functionalization. The AFM images show an increased roughness (Figure 2 and Figure S6) but this increase cannot be attributed to PNaSS because we know from the XPS results that on average the PNaSS layer is only of the order of ~ 0.02 nm suggesting a low coverage of thin patches (Figure S2). Instead, the increase of the surface roughness is probably caused by surface degradation in the presence of Mohr's salt redox initiator as previously reported [40].

263 In the case of photoinitiated radical polymerization (UV grafting), again XPS and surface 264 tension measurements correlate (Figure 1). Compared to Mohr's salt, they point to an 265 increased PNaSS surface density for PET. In the AFM images we observe ~1 nm thick patches 266 covering 8% of the surface and with markedly reduced adhesion. We interpret those patches as being PNaSS patches since they correspond to the average thickness estimated 267 by XPS. We note that the rest of the surface show a different (smoother) structure 268 compared to the control. We used an ozonized PET under UV irradiation in distilled water to 269 270 evaluate if changes to surface topology could have been caused by the UV irradiation treatment but that does not seem to be the case. Further investigations will be needed to 271 272 determine what causes the smoothening of the PET surface during PNaSS grafting by UV irradiation. Another limitation of our interpretation of the results is that those unexplained 273 topography changes could have contributed to the variations of contact angle 274 275 independently of PNaSS coverage.

276

277 **5. Conclusion**

PNaSS was successfully immobilized by ozonation activation and thermal grafting or UV grafting. The results provide insights into the morphology of PNaSS grafted on polyethylene terephthalate that is commonly used in biomedical engineering by harnessing a combination of AFM-Peakforce Quantitative Nanomechanical properties with XPS and contact angle measurements. Average thicknesses in the nm or sub-nm range determined

by XPS indicate a low PNaSS coverage. In the case of UV grafting 1 nm thick discrete patches 283 284 covering ~ 8% of the surface were observed. Some surface reconstruction happening during 285 PNaSS grafting will need to be explored in further work. As said in the introduction, the 286 reported findings would allow precising how the pNaSS molecules can interact with specific proteins as fibronectin and by this with cells. A lot of in vitro and in vivo biological results 287 were obtained and published on pNaSS grafted PET and this precise and fine view in the 288 structure of the grafted molecules will be a perfect tool to perfect the elucidation of the 289 mechanism of the biological activity of such surfaces. 290

291

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295

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414 **Declaration of interests**

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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418 Author Contributions

Tuan Ngoc Nguyen: principal technical contributor, conception, design and conduct of the
experiments, acquisition, analysis, interpretation of data, initial draft the work. Raphaël
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acquisition, analysis, interpretation of data. Véronique Migonney: supervisor, project
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