Correlative joint definition for motion analysis and animation
Nicolas Pronost, Anders Sandholm, Daniel Thalmann

To cite this version:
Nicolas Pronost, Anders Sandholm, Daniel Thalmann. Correlative joint definition for motion analysis and animation. Computer Animation and Social Agents (CASA), May 2010, Saint-Malo, France. hal-03542801

HAL Id: hal-03542801
https://hal.science/hal-03542801
Submitted on 25 Jan 2022

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L’archive ouverte pluridisciplinaire HAL, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d’enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.
Correlative joint definition
for motion analysis and animation

Nicolas Pronost, Anders Sandholm and Daniel Thalmann
Ecole Polytechnique Federale de Lausanne
Virtual Reality Laboratory

Abstract
In this paper we address the problem of creating accurate joint models from real motions while allowing scalability. We propose an automatic method to model, scale and simulate non-idealized joints from the external motion of markers. We demonstrate the method on the human knee joint modeling for musculoskeletal analysis and for character animation. The resulting joints, called correlative joints, are character and motion independent and rely on linear combinations of degrees of freedom calculated from multiple regression laws. We show that by using such models, inverse kinematics solvers find better solutions when tracking motions and solving constraints. Importing correlative joints into new models involves only minimal requirements on landmarks locations and no costly additional computations.

Keywords: Virtual Human, Motion Analysis and Modeling, Biomechanics, Animation

1 Introduction
Accurate track of human joint kinematics is instrumental for investigation of biomechanical mechanisms and motion simulation. Designing the mechanical behavior of a joint relies partially on the minimization of the modeling errors while retaining controllability. To be useful in simulation, a kinematic model has to be a good compromise between generality and accuracy. Indeed, both in biomechanics and animation, generality is required to allow the models to be scalable to any subjects or virtual characters. Different levels of accuracy may therefore be required, from a natural looking to biomechanically validated motion.

Generality is usually provided by the possibility of matching data of a model to an experimental one. Hence, to model joint kinematics amounts to study scaled properties of a generic model. And then to ensure enough generality without loss of accuracy becomes a challenging problem.

In this paper we present a method to model accurate joint kinematics from real motions while allowing to be easily reused on any subject or virtual character. We can describe it as a functional method to compute joint kinematics which produces generic models. We demonstrate the method on the human knee, hence creating a highly correlative joint. We show that using this model, inverse kinematics (IK) solvers find better solutions. Results are presented both on the subject used to create the model and on several others where the model is scaled to match their morphologies. Improving IK tracking is crucial as it is a fundamental step of a biomechanical motion analysis and is one of the most used technique in animation to imposes postures and constraints.

2 Related work
Joint kinematics and its measurement during a movement is an important requirement in the orthopedic and rehabilitation fields [1] as much as in animation [2]. In many laboratories, mo-
tion analysis systems can accurately measure 3D rotation of joints, and especially the knee joint [3, 4] which is intensively studied for its preponderant role in our daily activities.

For quantifying joint motion, the International Society of Biomechanics recommends the calculation proposed by Grood and Suntay [5]. Regarding angular displacements, their model needs as input the relative orientation between the Cartesian bone-embedded anatomical frames (BAFs). Several calibration procedures were proposed to transform 3D positions of markers as measured by standard motion capture systems into BAFs orientation [6, 7].

The most commonly used method to describe rotations of a joint is the Eulerian or Cardanic description, which decomposes the position of a limb with regard to its parent (or vice versa) into three sequential rotations along three pre-defined axes named flexion/extension, abduction/adduction and internal/external axial rotation [5]. These three pre-defined axes are also known as anatomical axes and can be defined by palpation of external anatomical landmarks [6]. Due to localisation errors leading to misorientation and overestimation of angular trajectories [8], researchers proposed different methods to measure joint kinematics. Methods which use both anatomical and functional calibration [9] are reported to be more repeatable than methods based only on anatomical calibration. And as Reinschmidt et al. [10] showed, the agreement between skin and bone markers based kinematics for ab/adduction and internal/external knee rotation ranged from good to virtually no agreement, and in some subjects, the errors exceed the actual motion. In these latter experiments, joint kinematics are very accurately tracked but on the other hand, using bicortical pins or in vivo medical imaging [11] to create models requires equipment, invasive procedure and time that one can most of the time not afford. Moreover, such methods can not be applied on animated virtual humans.

Musculoskeletal models including different joint descriptions have already been proposed and validated in literature [12]. For instance, Yamaguchi and Zajac [13] proposed a planar static model of the knee joint. A pathway for the instantaneous center of rotation was chosen that gives realistic orientations of the femur relative to the tibia. Techniques to model joints from surfaces have also been developed [14, 15].

We demonstrate the whole process on the human knee (section 3) by creating a joint consisting of three rotational DoF and three correlative translational DoF. The three translations defining the position of the joint center are thereby moving along with the posture. The objective is to automatically determine these relationships. The input data are 3D positions of reflective markers from mocap which are fixed to the skin of real subjects (section 3.1). Multiple linear regression laws are then applied to model the correlative DoFs of the knee joint (section 3.2). Even knowing the artifact issue raised above, we show the robustness of our method on tracking results during an IK operation (section 3.3). We have embedded multiple linear relationships between DoFs in the biomechanics platform OpenSim [12] and ran simulations (section 4.1). The procedure to benefit from our models to animate virtual characters is presented in section 4.2 and more examples on creating correlative joints from motion data are showed in section 4.3.

3 Correlative knee joint creation procedure

3.1 Experimental set-up

In an articulated mechanical system, a six-component structure describes the transformation to go from a local body reference frame to the next one. In animated and biomechanical systems, the three translational components are often constants, defining an idealized joint. Unfortunately some joints can not reasonably be modeled with such approximation, they have to integrate moving centers of rotation to better represent the kinematics. As seen in section 2, knee joints greatly benefit from non-idealized kinematics. In this paper we demonstrate the procedure on the human knee by modeling the posture-dependent position of the knee joint center (KJC). The procedure is generic and
may be applied to any body part and any joint of a mechanical system as soon as external markers can be located and tracked.

To develop the knee model, we used seven skin markers placed on anatomical landmarks (see Figure 1): RGT (great trochanter), RLFE (lateral femur epicondyle), RMFE (medial femur epicondyle), RTT (tibial tuberosity), RFH (fibula head), RMEDMAL (medial malleolus) and RLA TMAL (lateral malleolus). The local reference frame which defines also the three rotational DoF, is defined as follows (see right of Figure 1):
- Z: The line parallel to a line connecting RMFE and RLFE, pointing to the right;
- Y: The line parallel to a line lying in the plane defined by the two RFE’s and RGT, orthogonal to the Z-axis, pointing cranially;
- X: The line perpendicular to Y and Z, pointing anteriorly.

We captured different kinds of motions in order to study the influence of the movement on the kinematics of the knee joint and on the generality of our models. Regular gaits and crouch motions have been captured. We divided the crouch motions into 6 sub-motions: with 0° between the feet, with 30°, 60°, 90°, 120° and finally almost 180° (as much as possible for the subject). We captured six subjects performing 10 gaits and 5 crouches of each kind. This leads to more than 30,000 frames (i.e. elements of relationship) per subject. Moreover, we captured one standing motion for each subject for scaling purpose and for determining the rotation axes as previously described. Crouch motions have been chosen as they involve a large range of knee bending, thus we will be able to evaluate our method over this large range.

3.2 Method

The first step consists in calculating the elements of the relationships from the motions. The procedure is depicted in Figure 2. Firstly, the standing motion of the subject is used to define the local coordinate system of the knee. A free joint (six DoF) is then placed at the knee. The three rotations are defined around these three local axis and the three translations are defined along the three local axis of the parent joint, the hip. Finally, we run an IK solver driven by the positions of the seven markers over time. For this task, we used the IK tool of OpenSim [12] where the same weight is used for the seven markers. As a result, we get for each frame, the local KJC positions and the three local angular trajectories. We obtain for each subject 10 datasets of gait and 6 × 5 datasets of crouch motion.

The second step consists in modeling these independent sequences by multiple variable functions. If linear relationships exist, the following equations will describe the three dimensional position \( (T_x, T_y, T_z) \) of the KJC according to the three angular values \( (\alpha_1, \alpha_2, \alpha_3) \) around \((\vec{x}, \vec{y}, \vec{z})\) such that:

\[
\begin{align*}
T_x &= c_1x \times \alpha_1 + c_2x \times \alpha_2 + c_3x \times \alpha_3 + c_4x \\
T_y &= c_1y \times \alpha_1 + c_2y \times \alpha_2 + c_3y \times \alpha_3 + c_4y \\
T_z &= c_1z \times \alpha_1 + c_2z \times \alpha_2 + c_3z \times \alpha_3 + c_4z
\end{align*}
\]

(1)

To determine the three sets of coefficients \( (c_1, c_2, c_3, c_4) \), we calculate multiple linear regression laws on the datasets. Multiple regression solves for the unknown coefficients by minimizing the sum of the squares of the deviations of the data (angular trajectories) from the model (KJC positions) using a least-squares fit. The algorithm is as follows:

1. create the column matrix of experimental data \( E \):
   \[
   E = T_x(f), f \in [1 \cdots F] \text{ (respectively } T_y \text{ and } T_z \text{) where } F \text{ is the number of frames of the motion}
   \]

2. create the 3 column matrices
of angular trajectories
\[ \alpha_1(f), \alpha_2(f), \alpha_3(f), f \in [1 \ldots F] \]

3. create the design matrix \( M \):
\[
M = \begin{pmatrix}
1 & \alpha_1(1) & \alpha_2(1) & \alpha_3(1) \\
\vdots & \vdots & \vdots & \vdots \\
1 & \alpha_1(F) & \alpha_2(F) & \alpha_3(F)
\end{pmatrix}
\]

4. solve the equation:
\[
C = M \setminus E
\]
where \( C = [c_4, c_1, c_2, c_3] \) (respectively \( y \) and \( z \))

5. validate the result
\[
\text{valid} = (\max(|M \times C - E|) < |\min(E)|)
\]

In our study, all the resulting regression laws were validated: the maximums of the absolute values of the deviation of the data were always smaller than the minimums of the data values. This certifies that the model accurately follows the data and that linear functions are enough to model such joints. Mathematical justifications to solve the equation of item 4 can be found in the Matlab’s backslash operator documentation.

Table 1 presents the coefficients computed from the crouch motions. We do not show the coefficients specific to the sub-motions (different degrees between the feet), but the section 3.3 presents the modeling variations using a global-based law and a sub-motion-based law.

We can notice here the importance of the \( c_4 \) values which represent the constant components of the KJC position. These values are strongly related to the morphology of the subject. The taller the subject, the larger the \( c_4 \) value. This property shows already that the laws are subject-specific, \( i.e. \) one cannot directly use a correlative joint on any subject/virtual character. Nevertheless, this information can be used to develop simpler models. Indeed, the constant terms \( c_4 \) are definitely a good guess for setting a three DoF idealized joint. The following section presents evaluations of the laws regarding to sub-motions and simulation results of the kinematics of the leg.

### 3.3 Evaluation

In the first part of this section we present the accuracy induced by modeling the knee joint by multiple linear functions. Table 2 shows the average deviation between the KJC positions from IK and the positions estimated from the linear functions described from equation 1. The mean deviation is about 1.55 mm for gait motions and 1.32 mm for crouch motions. If we use a sub-motion specific function (\( i.e. \) using coefficients generated with the corresponding angles between the feet), the mean deviation decreases to 0.98 mm (\( \sim 26\% \) less). That indicates that as expected, the sub-motion models are more accurate as they are more specific and that the benefit is not negligible. It will certainly also be the case for other subsets of motion such as for locomotion consisting of gait (speed-dependent), run, jump, side-walk, etc.

In Figure 3, we propose visualizations of the deviations in the crouch models. The three axes define the 3D space of the knee joint orientation. The color represents the deviation, from blue (minimal deviation in the subject dataset) to red (maximal deviation). We can notice that the deviation is mainly homogeneously distributed. All postures are equally well modeled. The angular trajectories are closed to each others for a given subject, facilitating the linear relation-
Table 1: Multiple regression coefficients for the crouch motions

<table>
<thead>
<tr>
<th></th>
<th>Subject1</th>
<th>Subject2</th>
<th>Subject3</th>
<th>Subject4</th>
<th>Subject5</th>
<th>Subject6</th>
</tr>
</thead>
<tbody>
<tr>
<td>$T_x$ c1x</td>
<td>0.0573</td>
<td>0.1142</td>
<td>0.0496</td>
<td>0.0322</td>
<td>-0.0007</td>
<td>0.0404</td>
</tr>
<tr>
<td>c2x</td>
<td>0.0361</td>
<td>0.0340</td>
<td>0.0470</td>
<td>0.0328</td>
<td>0.0348</td>
<td>0.0351</td>
</tr>
<tr>
<td>c3x</td>
<td>0.0582</td>
<td>0.3426</td>
<td>0.0788</td>
<td>0.1105</td>
<td>-0.0297</td>
<td>0.0203</td>
</tr>
<tr>
<td>c4x</td>
<td>0.0748</td>
<td>0.0691</td>
<td>0.0783</td>
<td>0.0637</td>
<td>0.0713</td>
<td>0.0878</td>
</tr>
<tr>
<td>$T_y$ c1y</td>
<td>0.0306</td>
<td>0.0501</td>
<td>0.0657</td>
<td>0.0613</td>
<td>0.1460</td>
<td>0.1001</td>
</tr>
<tr>
<td>c2y</td>
<td>-0.0442</td>
<td>-0.0366</td>
<td>-0.0364</td>
<td>-0.0143</td>
<td>-0.0260</td>
<td>-0.0585</td>
</tr>
<tr>
<td>c3y</td>
<td>-0.1055</td>
<td>-0.1093</td>
<td>0.0330</td>
<td>0.0044</td>
<td>0.1869</td>
<td>0.2011</td>
</tr>
<tr>
<td>c4y</td>
<td>-0.5035</td>
<td>-0.4274</td>
<td>-0.4920</td>
<td>-0.4662</td>
<td>-0.5105</td>
<td>-0.5310</td>
</tr>
<tr>
<td>$T_z$ c1z</td>
<td>-0.0199</td>
<td>-0.0100</td>
<td>0.0362</td>
<td>-0.0536</td>
<td>0.0000</td>
<td>-0.0586</td>
</tr>
<tr>
<td>c2z</td>
<td>0.0210</td>
<td>0.0515</td>
<td>0.0116</td>
<td>0.0376</td>
<td>0.0148</td>
<td>0.0277</td>
</tr>
<tr>
<td>c3z</td>
<td>-0.2218</td>
<td>-0.1856</td>
<td>0.0142</td>
<td>-0.2319</td>
<td>-0.0292</td>
<td>-0.3299</td>
</tr>
<tr>
<td>c4z</td>
<td>0.0346</td>
<td>0.0414</td>
<td>0.0318</td>
<td>0.0260</td>
<td>0.0292</td>
<td>0.0347</td>
</tr>
</tbody>
</table>

Table 2: Average deviation (mm) between the positions of KJC from IK and the correlative positions from the regression laws (motion specific / sub-motion specific).

<table>
<thead>
<tr>
<th></th>
<th>Subject1</th>
<th>Subject2</th>
<th>Subject3</th>
<th>Subject4</th>
<th>Subject5</th>
<th>Subject6</th>
</tr>
</thead>
<tbody>
<tr>
<td>Crouch</td>
<td>1.3 / 1.1</td>
<td>2.0 / 1.4</td>
<td>0.9 / 0.7</td>
<td>1.1 / 0.9</td>
<td>1.6 / 1.0</td>
<td>1.0 / 0.8</td>
</tr>
<tr>
<td>Gait</td>
<td>1.1 / -</td>
<td>0.9 / -</td>
<td>1.5 / -</td>
<td>1.7 / -</td>
<td>3.1 / -</td>
<td>1.0 / -</td>
</tr>
</tbody>
</table>

4 Results

4.1 Integration and simulation in OpenSim

In order to demonstrate the capabilities of the method, we present in this section quantitative results on motion analysis. We want to show improvements in the tracking of captured motions, using the IK tool embedded in OpenSim. Results proposed in this section are obtained with the Interior Point Optimizer method (IPOPT), but equivalent results have been calculated with Feasible Sequential Quadratic Programming (FSQP) [16] and a Jacobian-based method. To evaluate the tracking, we use the sum of the frame-by-frame RMS distance between the experimental markers and the virtual markers (attached to the model and moved by the IK solution).

To take into account our new joint description, we have implemented a new kind of constraint in OpenSim. This constraint describes the linear relationship between one DoF and others (no limitation on the number and the kinship).

Let us consider the correlative DoF $X$ which depends on the values of $n$ other DoFs $Y_1...n$:

$$X = \left( \sum_{i=1}^{n} c_i \times Y_i \right) + c_{n+1}$$  \hspace{1cm} (2)

where $c_1...n+1$ are scalars.

We do not require these DoFs to be all different but each of them has to be different from $X$. This new feature enables us to directly deal with multiple linear relationships. Then for instance to model the crouch-specific knee, $c_1...n+1$ are set to the values of table 1.

We proceed several simulations with this feature. Firstly, we compared three models of the knee joint. One that we call 3DOF, is made of two translational and one rotational DoF. Its rotation axis was determined by a planar static model and the two translations depend on the ro-
A second, called 1DOF is made of only one rotational DoF, around the same axis than the previous model. The last one is ours (3+DOF) made of three rotational and three correlative translational DoF: The location of the KJC of the 1DOF model is set to the default position from the 3DOF model which has been biomechanically validated. We did not use the $c_4$ values to place this KJC as we indeed want to compare our model to validated literature models.

In table 3, we present average values of IK errors during the track of mocap data using these three models. Errors were obtained on 10 gaits and 10 crouches that are different from the motions used to create our models. The reported RMS errors are not normalized by neither the number of frames nor the number of markers. The error differences between the gaits and the crouches mainly come from the number of frames (a complete crouch takes more time to perform than a gait cycle). As expected, we observe that the 3DOF error is lower than the 1DOF error and that the 3+DOF error is lower than both of them. We present error values only for one subject, but the same experiment was done on the others. Results show that IK errors are reduced by:

- $44(\pm 8)\%$ between 3+DOF and 1DOF for gait motions
- $31(\pm 5)\%$ between 3+DOF and 3DOF for gait motions
- 71(±9)% between 3+DOF and 1DOF for crouch motions
- 66(±6)% between 3+DOF and 3DOF for crouch motions

This demonstrates the benefit induced by our model. Indeed, such large improvements of IK tracking have a direct influence on the motion analysis accuracy and on the naturalness of animated motions.

<table>
<thead>
<tr>
<th>Subject</th>
<th>1DOF</th>
<th>3DOF</th>
<th>3+DOF</th>
</tr>
</thead>
<tbody>
<tr>
<td>Gait</td>
<td>3.02</td>
<td>2.48</td>
<td>1.19</td>
</tr>
<tr>
<td>Crouch</td>
<td>272.94</td>
<td>261.46</td>
<td>76.34</td>
</tr>
</tbody>
</table>

Table 3: Average values of RMS distances (m).

The previous results were obtained by applying the knee model to the corresponding subject and motion. Now, we study what happens if a specific knee model is used to simulate another subject or the same subject but on another kind of motion. We therefore set up two experiments.

In the experiment 1, we scale the model of subject 2 to subject 1 (denoted model1 from 2) and track gaits and crouches of subject 1. To scale the model, we update the coefficients as follows:

\[
c_{id}^{\text{scaled}} = \frac{c_{id}(s_1 + s_2)}{2}, \quad i \in [1, 2, 3, 4], \quad d \in [x, y, z]
\]

with

\[
s_1 = \frac{\vec{RGT}_{model1} \vec{RLFE}_{model1}}{\vec{RGT}_{model2} \vec{RLFE}_{model2}}
\]

\[
s_2 = \frac{\vec{RMFE}_{model1} \vec{RLFE}_{model1}}{\vec{RMFE}_{model2} \vec{RLFE}_{model2}}
\]

This scaling method is based on the same approach that classical methods in the literature [12] where such linear scaling function has been validated over the range of human bodies.

We then compare both tracking results of model1 from 2 and the specific model of subject 1 (denoted model1). The table 4 shows the resulting errors from 10 gaits and 10 crouches. We first see that the error using a scaled model is, as expected, larger than the error using our specific model. We also notice that the scaled error is much lower than the error of the 3DOF model. That implies that one can use a generic 3+DOF model to perform analysis on another subject.

IK results will still be better than a scaled 3DOF model from literature. This property was verified by carrying out the same experiment on the other models/subjects/motions, not detailed here.

<table>
<thead>
<tr>
<th>Subject</th>
<th>model1</th>
<th>model1 from 2</th>
</tr>
</thead>
<tbody>
<tr>
<td>Gait</td>
<td>76.34</td>
<td>87.35</td>
</tr>
<tr>
<td>Crouch</td>
<td>1.19</td>
<td>2.10</td>
</tr>
</tbody>
</table>

Table 4: Experiment 1 : tracking errors (m) of model1 and model1 from 2.

In the experiment 2, we use the 3+DOF model defined from gait motions to track crouch motions and vice versa. The results on subject 1 are presented in table 5. The error induced by a model defined from a different kind of motion is about 40% for gait and 70% for crouch. On the other hand, the errors are still lower than the error from the 3DOF model, thus showing the benefit of our models. Gaits are better tracked in the experiments as there is less angular trajectories to extrapolate from a crouch model than the opposite.

<table>
<thead>
<tr>
<th>Subject</th>
<th>3+DOF gait</th>
<th>3+DOF crouch</th>
</tr>
</thead>
<tbody>
<tr>
<td>Gait</td>
<td>1.19</td>
<td>1.68</td>
</tr>
<tr>
<td>Crouch</td>
<td>130.34</td>
<td>76.34</td>
</tr>
</tbody>
</table>

Table 5: Experiment 2 : tracking errors (m) of motion specific models.

4.2 Application to virtual character animation

In this section we give information about how to use our correlative joints in virtual character animation. We denote modelcorr the model on which we have created correlative joints and modelanim the model of the virtual character we want to animate.

Firstly, the correlative joints from modelcorr have to be defined with the same orientation than modelanim as follows:

1. To choose three anatomical markers on the parent body of the joint on modelcorr (for example RGT, RMFE and RLFE for the knee);
2. To place three virtual markers on \( \text{model}_{\text{anim}} \) on the equivalent landmarks (see left of Figure 4);

3. To scale the coefficients of the relationships according to the respective markers distances (as in equation (3));

4. To create the local coordinate system from the markers for both models (as in section 3.1 for the knee);

5. To apply the two successive transformations to compute the local joint orientation in \( \text{model}_{\text{anim}} \).

The proper behavior of the joint will depend on the accuracy of the markers positioning. This issue, which is also shared by motion analysis setups, could become tricky for not-really-human characters.

Secondly, the animation engine has to be able to evaluate equation 1 when the value of a DoF involved in a correlative joint changes. The implementation of this ability depends on the engine, but most of them provide script programming which can be used for this purpose. As a consequence, when editing a motion, either from mocap or keyframing, inverse and direct kinematics solvers will benefit from the correlative joint feature (see Figure 4).

While creating or editing a new motion involving a correlative joint, the animator does not require necessarily to create a motion specific model as described in this paper. Indeed, as soon as the model has been created on a sufficient range of value, the model is valid for any motion within this range (see experiment 2). Then assuming that correlative models have been created from biomechanical datasets and accurate motion analysis (for instance using bicortical pins), the development of realistic virtual character animations is straight forward and without additional cost.

4.3 More correlative joints from motion

We have demonstrated the method on the human knee joint. This joint is mechanically complex and a high-degree model (3 rotations and 3 correlative translations) was necessary to represent its kinematics. Our method can also be used to model simpler joints. The Figure 5 illustrates three of our experiments in retrieving lower and higher pair joints from the motion of external markers placed over the different body parts.

![Figure 5: Lower and higher pair mechanisms modeled with correlative joints.](image)

An helical joint is a one rotational DoF lower pair mechanism providing a single-axis translation. The typical illustration is the screw-bolt system (Figure 5(a)). The translation is gener-
These examples show the ability of the method to retrieve and simulate as well simple kinematic models. We can also notice that even if the model is defined in a particular coordinate system, there is no need to know in advance the respective direction of the translations and rotations involved in the relationships. The user has only to decide the DoFs that will be in control and the correlative ones.

5 Conclusion

In this paper we have presented a method to create an accurate and scalable model of a joint from the motion of external markers. The computed joint can be reused on any real subject or virtual character with only minimal requirements on anatomical landmarks. To perform direct and inverse computational approaches, no costly additional algorithm is involved. Only the evaluation of equation 1 has be added, composed of few additions and multiplications.

Many complex biological joints can be modeled using our technique. We demonstrated that the human knee joint can be modeled using a correlative joint. And we believe that most of human joints, even complex as the shoulder, will benefit from such mechanical description.

We showed that by using our model, inverse kinematics solvers find better solutions both on the subject used to create the model (error reduced by 53 up to 80%) and on others subjects where the relationships were scaled to match the new morphologies (error reduced by 25 up to 41%). Biomechanical simulations will better match the experimental data allowing more accurate estimation of forces, muscle activations etc. And character animation will benefit in more natural motions with no major cost.

Finally, we remind the good performances of our model compared to 1DOF and 3DOF models of literature. We believe that this work contributes to the development of reliable methods of simulation for animation and biomechanical analysis.

Acknowledgements

This work is supported by the European Marie Curie Program under the 3D ANATOMICAL HUMAN project (MRTN-CT-2006-035763).
References

the ankle joint complex: Application of
a combined dual-orthogonal fluoroscopic
and magnetic resonance imaging tech-
nique. Journal of Orthopaedic Research,

ber. Simulating humans: computer graph-
ics animation and control. Oxford Uni-
versity Press, Inc., New York, NY, USA,
1993.

C.D. Papageorgiou, A. Mitsou,
and N. Stergiou. Three-dimensional
tibiofemoral kinematics of the anterior
cruciate ligament-deficient and recon-
structed knee during walking. American
Journal of Sports Medicine, 31(1):75–79,
2003.

[4] U. Della Croce, V. Camomilla, A. Lear-
dini, and A. Cappozzo. Femoral anatom-
ical frame: assessment of various defini-
tions. Medical Engineering & Physics,

[5] E.S. Grood and W.J. Suntay. A joint co-
ordinate system for the clinical description
of three-dimensional motions: Application
to the knee. Journal of Biomechanical En-

[6] A. Cappozzo, F. Catani, U. Della Croce,
and A. Learndini. Position and orienta-
tion in space of bones during movement:
anatomical frame definition and determi-
nation. Clinical Biomechanics, 10(4):171

Putte, N. St-Onge, N. Duval, and J. de
Guise. A reproducible method for studying
three-dimensional knee kinematics. Journal
of Biomechanics, 38(9):1926 – 1931,
2005.

[8] U. Della Croce, A. Cappozzo, and D.C.
Kerrigan. Pelvis and lower limb anatom-
ical landmark calibration precision and its
propagation to bone geometry and joint an-
gles. Medical and Biological Engineering

oreux. Defining the knee joint flexion-
extension axis for purposes of quantita-
tive gait analysis: An evaluation of methods.

[10] C. Reinschmidt, A.J. Van den Bogert,
A. Lundberg, B.M. Nigg, N. Murphy,
A. Stacoff, and A. Stano. Tibiofemoral and
tibiocalcaneal motion during walking: ex-
ternal vs. skeletal markers. Gait & Posture,

age matching method for determining in-
vivo tka kinematics with a dual-orthogonal
fluoroscopic imaging system. Journal of
Biomechanical Engineering, 128(4):588–
595, 2006.

E.L. Topp, and J.M. Rosen. An interac-
tive graphics-based model of the lower ex-
tremity to study orthopaedic surgical pro-
cedures. IEEE Transactions on Biomedical

nar model of the knee joint to characterize
the knee extensor mechanism. Journal of

[14] W. Shao and V. Ng-Throw-Hing. A generic
joint component framework for realistic ar-
ticulation in human characters. In ACM
Symposium on Interactive 3-D Graphics,

for multibody dynamics. ACM Trans. Graph.,

[16] C.T. Lawrence and A.L. Tits. Nonlin-
ear equality constraints in feasible sequen-
tial quadratic programming. Optimization