

Phase Synchrony Neurofeedback? BEWARE!

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▶ To cite this version:

Côme Le Breton, Théodore Papadopoulo, Maureen Clerc. Phase Synchrony Neurofeedback? BE-WARE!. NEC 2021 - Neuroergonomics Conference, Sep 2021, München, Germany. hal-03538875

HAL Id: hal-03538875 https://hal.science/hal-03538875

Submitted on 21 Jan2022

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Background

Phase synchrony estimation in EEG signals is subject to a number of pitfalls, which makes neurofeedback protocols rare, despite their potential in health care applications (epilepsy syndromes, attention deficit hyperactivity disorder..).

Phase synchrony measures the consistency of a relationship between the phase of two signals. It requires in the first place the determination of a phase (or phase difference), and in a second place the quantification of this consistency.

EEG signals are the combination at the scalp of the activity of the neurons of the cortex, plus possibly external noises.

A simple, but likely generic assumption (especially in the framework of **phase synchrony**), is to assimilate **EEG signals** to locally stationary weighted sums of sinusoids.

Methodology

A] From the fundamentally equivalent methods to extract the phase from **EEG signals**, we retained the **Morlet Wavelet Transform**. We derive analytically the convolution of a **Morlet wavelet** with a sinusoid and extend the derivation to the weighted sums of locally stationary sinusoids. Additionally we propose an approximation of the former derivation with **loose constraints**.

The behavior of the **weights** for **varying width** and **frequencies** is analyzed.

We present two cases of **false synchrony**, one of **missed synchrony**, and one of **spurious synchrony**.

B] The correlation coefficients of two δt distant Morlet wavelet **coefficients** is computed

C] We set up an **experiment** to assess the correlation between common phase synchrony measures. A subject underwent 13 recordings of 275 seconds, alternating between 20s of **Eyes Open** Fixation of the screen (Baseline) and 20s of Eyes Closed Relaxation, interleaving 5 seconds of rest between each event.

Results

A] The wavelet transform is an accurate estimation of the argument of a sine wave for $\Omega > 2$.

The benefit of increasing the width of the wavelet (Ω) to values higher than 30 is minimal, and at the expanse of reducing the temporal accuracy of the transform.

The higher the frequency of interest (v_w) is, the more mixing **between frequency** components (v_s) around that frequency (respecting the uncertainty principle).

The **amplitude ratio** between components **matters** in the phase estimation, but **lightly** in comparison to the distance ratio between v_w and v_s .

This **phase** between **two pairs of sinusoids** oscillating in the vicinity of the wavelet frequency (v_{w}) is almost zero for two different pairs of sinusoids (i.e. $v_{a0} = 9.5$, $v_{a1} = 11.5$; $v_{b0} = 10$, $v_{b1} = 11$). It means that the **phase is not unique** : several combinations of different frequencies produce the same phase.

B] The derivation of the correlation between two close coefficients show that they are not independent.

C] Some synchrony measures are strongly correlated and thus redundant : PLI and ImCoh or PLV and Coh are strongly correlated, on the other hand **PLI and PLV** are **complementary**, and would benefit from being analyzed altogether when assessing synchrony.

Conclusion

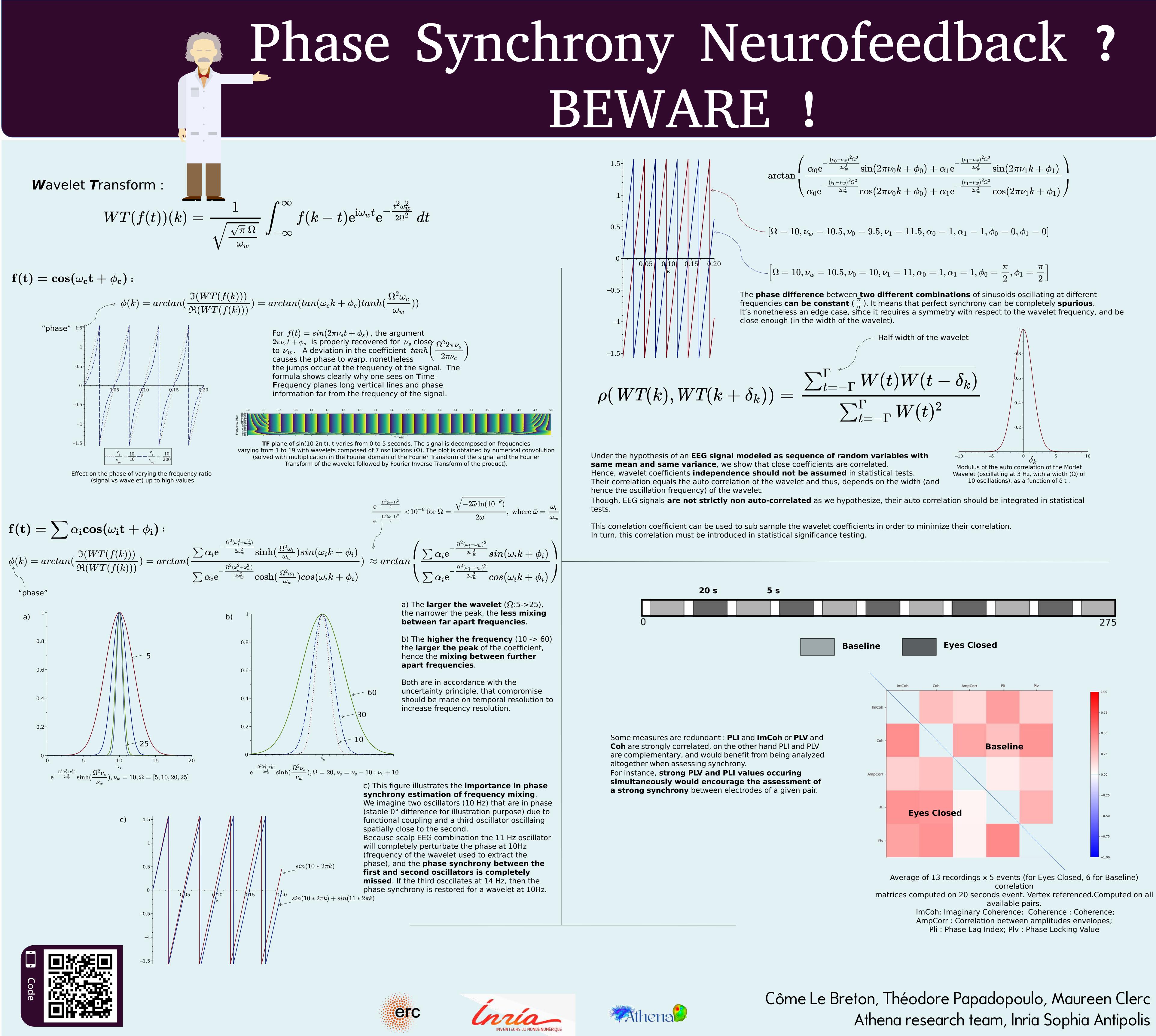
Assessing properly phase synchrony is a real challenge, even for offline analysis.

It has mostly to do with the volume conduction / volume leakage mixing, the uncertainty principle and the redundancy of the wavelet coefficients.

One or more of these issues are often neglected.

We provide a framework for better understanding and interpreting phase extraction with the Morlet Wavelet Transform to show that errors are made when extracting phase information and must be accounted for.

Before attempting to blindly use phase synchrony measures in Neurofeedback, there *a fortiori* a need for a proper and efficient estimation of the statistical significance of the measures calculated on the fly.



$$2=10,
u_w=10.5,
u_0=10,
u_1=11, lpha_0=1, lpha_1=1, \phi_0=rac{\pi}{2}, \phi_1=rac{\pi}{2}$$

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