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The ictal signature of thalamus and basal ganglia in focal epilepsy: An SEEG study

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ACCEPTED

Abstract

Objective: To determine the involvement of subcortical regions in human epilepsy by analyzing direct recordings from these regions during epileptic seizures using stereoelectroencephalography (SEEG) **Methods:** we studied the SEEG recordings of a large series of patients (74 patients, 157 seizures) with an electrode sampling the thalamus and in some cases also the basal ganglia (caudate nucleus -22 patients- and putamen – 4 patients). We applied visual analysis and signal quantification methods (Epileptogenicity Index, EI) to their ictal recordings and compared electrophysiological with clinical data. **Results:** We found that in 86% of patients thalamus was involved during seizures (visual analysis) and that 20% showed high values of epileptogenicity ($EI > 0.3$). Basal ganglia may also disclose high values of epileptogenicity (9% in caudate nucleus) but to a lesser degree than thalamus ($p < 0.01$). We observed different seizure onset patterns including low voltage high frequency activities. We found high values of thalamic epileptogenicity in different epilepsy localisations, including opercular and motor epilepsies. We found no difference between epilepsy aetiologies (cryptogenic vs malformation of cortical development, $p = 0.77$). Thalamic epileptogenicity was correlated with the extension of epileptogenic networks ($p = 0.03$, $\rho 0.32$). We found a significant effect ($p < 0.05$) of thalamic epileptogenicity regarding the post-surgical outcome (higher thalamic EI corresponding to higher probability of surgical failure) **Conclusions:** Thalamic involvement during seizures is common in different seizure types. The degree of thalamic epileptogenicity is a possible marker of the epileptogenic network extension and of post-surgical prognosis.

Introduction

Focal epilepsy is traditionally considered as the epitome of a cortical disease. However Henri Gastaut in the 1970s discussed the idea of focal epilepsy as a cortico-subcortical disease, in which subcortical structures could be responsible for the seizures' initiation ¹. Even earlier, Jasper wrote about a "cortico-thalamic rhythmic system" that could be activated by a focal discharge. ² Still, the involvement of subcortical structures in the epileptic network was long ignored. The scant literature on intracerebral recordings, mainly on temporal lobe epilepsy, showed that subcortical structures, such as the thalamus ³⁻⁶, caudate nucleus ⁷ or other basal ganglia ⁸ are involved in seizure dynamics. Studies from non-human primates also demonstrated the participation of subcortical nuclei in ictal networks ^{9,10,11}.

Recently, the role of subcortical structures in epilepsy gained renewed interest. Some neuroimaging studies ¹²⁻¹⁷ evidenced the participation of the thalamus in epileptic networks suggesting that its involvement is related to post-surgical prognosis ^{4,18}. Moreover, subcortical-cortical connectivity was shown to be altered in different epilepsy types. ^{19, 20}

When surgery is contraindicated or unsuccessful, deep brain stimulation (DBS) targeting thalamic nuclei can be an option (for a review see ²¹) but the mechanisms of cortico-subcortical interactions during seizures are mostly unknown and it is unclear which type of epilepsy is best suited to such a treatment.

The aims of this work were to evaluate thalamic and other subcortical nuclei participation in epileptogenic networks and to estimate the correlation of thalamic activity with clinical data and post-surgical outcome.

Methods

Patient selection

We selected patients who underwent SEEG exploration from January 2001 to May 2018 and who had at least one intracranial electrode implanted in the thalamus. Some of the patients had also an electrode reaching other subcortical structures (caudate nucleus or putamen). At the time of the SEEG recording, all patients had a comprehensive evaluation including detailed clinical history, neurological examination, neuropsychological testing, routine MRI and surface electroencephalography (EEG). SEEG exploration was carried out during long-term video-EEG monitoring, as part of normal patient clinical care. Clinical data, SEEG recordings including recorded epileptic seizures were collected and analysed. The Engel class surgical outcome classification was used to assess post-surgical outcome.

Standard Protocol Approvals, Registrations, and Patient Consents

The institutional review board of the French Institute of Health (IRB15226) approved this study and a written patient consent was obtained from all included patients.

SEEG recordings and montage selection

Recordings were performed using intracerebral multiple contact electrodes (10–15 contacts, length: 2mm, diameter: 0.8mm, 1.5mm apart) placed intracerebrally according to Talairach's stereotactic method. The anatomical targeting of electrodes was established, independently of this study, in each patient according to information available after the non-invasive study and clinical hypotheses about the localization of the epileptogenic zone. The number of electrodes ranged from 6 to 22 electrodes, with more recent implantation having an higher number of electrodes.

A post-operative computerized tomography (CT) scan and/or MRI were used to verify the absence of bleeding and the position of electrodes. Video-EEG recording was performed as long as necessary (1 to 3 weeks) to record several of the patient's habitual seizures. Finally, CT-scan/MRI data fusion was performed when all data were available to accurately check the anatomical location of each contact along the electrode trajectory. For this purpose we used our in-house software GARDEL - <http://meg.univ-amu.fr/wiki/GARDEL:presentation> - ²². In patients explored before 2008, imaging data were in some cases lacking and we used the description of electrode position that was available for all patients. We included these patients since the aim of the study was to evaluate thalamic participation during seizures, while a detailed anatomical description of electrode position was beyond the scope of this study. An exploration of the thalamus targeting the pulvinar medialis has become customary in our department whenever a posterior temporal electrode exploring the planum temporale (PT) has to be implanted for the definition of the epileptogenic zone. Indeed, it is technically easy and safe to insert an orthogonally implanted electrode slightly deeper at the level of PT and thus reach the pulvinar medialis with the most medial contacts. A division between the thalamic contacts located in the pulvinar versus those not reaching the pulvinar, but other thalamic subnuclei (anterior, median and lateral), was computed. Regarding basal ganglia, the electrode used to explore the frontal operculum for clinical reasons was also sampling the head of the caudate nucleus. The putamen could also be explored by an opercular electrode or an oblique insular electrode.

Signals were recorded on a Natus system sampled at 256, 512 or 1024 Hz with 16 bits resolution. Two hardware filters were present in the acquisition procedure. The first is a high-pass filter (cut-off frequency equal to 0.16 Hz) used to remove very slow variations that could contaminate the baseline. The second is an anti-aliasing low-pass filter (cut-off frequency

dependent on sampling frequency: equal to 97 Hz at 256Hz, 170 Hz at 512 Hz and 340 Hz at 1024 Hz).

In each patient, to analyse data, a SEEG bipolar montage was created and applied to all selected seizures. The SEEG montage included all subcortical channels, as well as all grey matter channels. Channels showing artefacts were excluded from analysis. All signal analysis was performed with the AnyWave software (available at <http://meg.univ-amu.fr/wiki/AnyWave:Download>)²³.

Ictal recordings: visual analysis and computation of the Epileptogenicity Index (EI)

Seizure were collected (with a maximum of 3 seizures per patient) and two types of analysis were done: visual and quantified.

Visual analysis was done with the help of normalized time frequency analysis (nTF)²⁴. In particular, we characterised seizure onset patterns (SOP)²⁵ in the thalamus and basal ganglia. The pattern in the subcortical structures was analysed only if it was present during the first 15 seconds from cortical seizure onset. Specific subcortical SOP were defined as low voltage fast activity (LVFA) associated or not with DC shift, rhythmic spikes or rhythmic spikes and wave discharges from alpha to higher frequency band (RS), and theta band discharge (theta). Discharges involving several frequency bands could be found in thalamus at the same time. In this case we selected the one with the highest normalised power as the main discharge. Discharges at other frequencies that were simultaneously present were also analysed. If a LVFA was present in any seizure for the patient, it was considered as the main pattern. With the RS pattern we included all patterns that did not show a clear fast discharge in the nTF but not even only a theta propagation pattern. Heterogeneous patterns could be recorded, ranging from spikes in the beta frequency to oscillations in the alpha band and a mixture of different activities.

To perform quantified analysis, we computed the EI for all selected seizures by using our in-house plugin ²⁶, implemented in the AnyWave software ²³. The EI is a method applied to SEEG signal aiming at quantifying the epileptogenicity of brain structures. The EI methodology has been described extensively in previous works ²⁷. Briefly, the EI allows to quantify the epileptogenicity of a brain region by considering both 1) the capacity of this region to generate fast activity at the beginning of the seizure, changing from the slower background activity preceding the seizure to faster frequencies and 2) the velocity of this change during the seizure course; in other words the time in which this change take place. High EI values (> 0.3) are characteristic of regions in which we can record a fast epileptic discharge at the beginning of a seizure (generally the very firsts seconds).

When computation of EI was not possible, *e.g.* in absence of a fast discharge or fast spiking activity or in presence of a noisy signal, the patient was excluded from subsequent analysis. If the thalamus ipsilateral to the seizure onset side was not explored, the patient was excluded. Structures involved at seizure onset as detected by EI analysis were then compared to visual analysis to verify concordance between the two analyses. A value of EI for each sampled brain region was calculated, with a threshold of 0.3 to define a channel as epileptogenic²⁷. The same threshold was used for other subcortical structures.

Data analysis

The number of patients and seizures with a high epileptogenicity in the thalamus or in another subcortical structure were calculated, as well as the number of patients showing an ictal discharge in the time course and nTF analysis. Values of thalamic epileptogenicity (one per patient - the maximum EI value across all seizures) were grouped according to clinical data as epilepsy aetiology and epilepsy type.

The primary goal of this study was to examine the relationship between epileptogenicity of the thalamus and epilepsy severity. To answer this question, we first computed the Spearman correlation between thalamic epileptogenicity and i) number (or percentage) of brain regions with high epileptogenicity ($EI \geq 0.3$) and ii) epilepsy duration. Secondly, we investigated whether thalamic epileptogenicity is higher in patients with poor post-surgical outcome compared to those with good outcome (Engel class I and II vs Engel class III and IV) using a multivariate probit regression and taking the number of brain regions with $EI \geq 0.3$ and its interaction with thalamic epileptogenicity as control variables. For the regression, we used standardized variables (i.e. we transformed the variables so that the mean and standard deviation equal zero and one respectively) to handle more homogeneous variables. We finally controlled for multiple testing using the False-Discovery Rate procedure²⁸; only adjusted p-values are reported unless stated otherwise.

The secondary aim of this study is to describe the repartition in percentage of different clinical characteristics (i.e. aetiology, epilepsy type, seizure onset type) in this patient cohort, and the differences of i) epileptogenicity of the explored subcortical structures (thalamus, caudate nucleus, putamen) and ii) thalamic epileptogenicity between different groups of aetiology and type of epilepsy. The comparison was only done when a minimum of twelve observations were available per group. This number was arbitrarily chosen as the minimum amount to have meaningful statistics. We report the common language effect size of the Wilcoxon rank sum test (i.e. the U statistic divided by the product of the number of elements of each variable) and its 95-percent confidence interval²⁹ for the comparison between different variables. The percentages and their 95-percent confidence intervals, calculated with continuity correction, are written when the number of elements is above five (minimum amount for the confidence interval validity). The statistical analysis was done using MATLAB (The Mathworks Inc.,

Natick, MA, U.S.A.), and the R-package `asht` for the confidence interval of the Wilcoxon rank sum test.

Data Availability

Full access to data is possible upon reasonable request.

Results

Population characteristics

In our cohort, a total of 83 patients had at least one electrode in a thalamic nucleus. Eight patients were excluded due to the impossibility of computing EI (absence of fast discharges (5) signal too noisy (3)). One patient was excluded because the thalamus was explored in the hemisphere contralateral to the seizure onset. Finally, 74 patients were included (43 women). Twenty-two patients had an electrode in the caudate nucleus and 4 had one electrode exploring the putamen. Mean age at SEEG recording was 30.5 (range 5-61 SD 12.9), mean epilepsy duration was 18.3 (range 4-33 SD 11.4) and mean age of epilepsy onset was 12.2 (range 4 months-28 SD 9.4). One hundred and fifty-seven seizures were analysed.

The aetiology was: 31 (42%, [30-54%]) cryptogenic, 22 (30%, [19-41%]) malformation of cortical development (MCD), 8 (11%, [3-19%]) hippocampal sclerosis, 4 infectious disease, 9 (12%, [4-20%]) other aetiologies (including 3 post-stroke, 3 tumour, 2 head trauma, 1 cavernoma). The epilepsy type was: 36 (49%, [37-61%]) temporal lobe epilepsy (TLE) (23 mesial TLE, 7 lateral TLE, 6 mesio-lateral TLE), 11 (15%, [6-24%]) bitemporal epilepsy, 10 (13%, [5-22%]) temporal plus epilepsy, 3 opercular epilepsy, 8 (11%, [3-19%]) epilepsy of motor-premotor system, 6 (8%, [1.2-15%]) posterior epilepsy.

Thirty-nine patients (53 %, [41-65%]) had subsequent surgery, among which eleven had a follow up <12 months (15%, [6.1-24%]). The mean follow-up duration was 61 months (range 2-198 months).

Finally, 14/28 (50 %, [30-70%]) had good surgical outcome (12 Engel I - 2 Engel II) and 14 (50 %, [30-70%]) had poor outcome (9 Engel III, 5 Engel IV). Thirty-five (47%, [35-59%]) did not have surgery after SEEG. In 24 (32%, [21-44%]) surgery was contraindicated. The reasons of contraindication were a widespread network (18 – 24%, [14-35%]) or overlap of the epileptogenic zone with eloquent cortices (6 - 8%, [1.2-15%]). Six patients are waiting for surgery (8%, [1.2-15%]), three had good response to thermocoagulation, one patient died, and one was lost to follow up/refused surgery.

Seizure onset patterns in thalamus

Visual analysis revealed that the thalamus participated in seizures in the great majority of patients (86 % [77-95%] in the first 15 seconds). Different and particular patterns were observed: low voltage fast activity (LVFA, 31 %, [20-42%]), rhythmic spikes (RS, 38%, [26-50%]) or theta activity (theta, 18%, [8.2-27%]) possibly with some fast activities. The distribution of SOP across epilepsy type is illustrated in Fig. 1. The main frequency of thalamic discharge as calculated by nTF was 20 Hz (range: 4 - 160 Hz). It should be noted that in 16 patients, other frequencies of ictal discharges accompanied the main one (mean 50 Hz, range: 10 - 190 Hz). In summary a total of 4 patients presented ictal discharges above 80 Hz. Some examples of thalamic discharges are illustrated in Fig. 2 (A-D).

Basal ganglia can participate in seizure genesis and propagation

High epileptogenicity values, as evaluated with quantified analysis (EI), were also recorded from caudate nucleus and putamen (Fig. 3). Twenty-two patients had an exploration of caudate nucleus (CN) and in two patients it was included in the EZ according to EI values.

Regarding putamen, this was sampled in four patients, being in one part of the EZ (Table 1). Regarding SOP, in CN we observed in 7 patients a pattern classified as RS characterized by a discharge around 8-10 Hz with intermingled spikes; in 3 patients we observed a LVFA pattern (Fig 1E), in 4 patients a theta discharge and in 7 patients no participation in the first 15 seconds of the seizure was observed. In the putamen we observed a RS pattern in 2 patients (Fig. 2f), in one patient a theta activity and in one patient no ictal activity.

Epileptogenicity of thalamus and basal ganglia and correlation with clinical data

In fifteen patients (15/74, 20%, [10-30%]) the thalamus was included in the EZ in at least one seizure (21 seizures). The pulvinar was the explored nucleus in 42/74 patients, location of the others contacts in the thalamus was in the median nuclei (8/74), in the lateral nuclei (16/74) and in 8 patients it was not possible to reconstruct it retrospectively. In two patients (2/22) the caudate nucleus was included in the EZ as was the putamen in one patient (1/4) (Fig. 3). When comparing epileptogenicity in thalamus and caudate nucleus we found a large difference (Wilcoxon rank sum test: uncorrected $p < 0.01$, effect size: 0.259 [0.158 0.401]), with higher values in thalamus. Two examples of seizures with high subcortical epileptogenicity are reported in Fig. 4.1 (thalamus) and Fig. 4.2 (caudate nucleus). The relationship between thalamic epileptogenicity and different types of epilepsy and aetiology of epilepsy are shown in Fig. 5.

The highest values of thalamic epileptogenicity were found in infectious disorders and cryptogenic epilepsies. No difference was found in thalamic epileptogenicity across the more represented aetiologies as the confidence interval of the effect size is large and centred near 0.5 (crypto vs MCD, Wilcoxon rank sum test: uncorrected $p = 0.77$, effect size: 0.531 [0.377 0.678]). As far as localisation/type is concerned, the highest thalamic epileptogenicity was found in opercular and bitemporal epilepsies, but no statistical analysis was possible due to

the insufficient number of observations per group. A significant correlation was found between the extension of the epileptogenic network (% brain region with $EI > 0.3$ - $p = 0.0379$, $\rho = 0.32$ [0.10 0.52]- and number of regions with $EI > 0.3$ - $p = 0.0195$, $\rho = 0.27$ [0.044 0.47]) and thalamic epileptogenicity (Fig. 6). No significant correlation of thalamic epileptogenicity and epilepsy duration was found ($\rho = -0.00020755$, [-0.22 0.22], $p = 0.9986$).

Thalamic epileptogenicity and surgical outcome

To compare thalamic epileptogenicity and surgical outcome we included patients with a follow up of more than 12 months (28: 14 Engel I or II). We found using the probit regression (Table 2) a significant effect ($p < 0.05$) of the thalamic epileptogenicity regarding the post-surgical outcome while controlling for the number of brain regions with high epileptogenicity and its interaction. In fact, the confidence interval of the coefficient of the extent of the SOZ is large and does not permit to draw any conclusion concerning its relationship with the outcome.

Discussion

The present results demonstrate, in a large cohort of patients, that the thalamus is involved in focal seizures in the vast majority of patients (86%) according to visual analysis. In a subset of patients (20%) the thalamus was involved early in seizure generation, as shown by a high value of epileptogenicity measured by a quantified ictal analysis (EI). EI evaluate the rapidity of a brain region to generate fast activity at the beginning of the seizure, and thus indicates that a given region is involved at the very start of the seizure. We found a significant correlation between the number of regions with a high degree of epileptogenicity and thalamic epileptogenicity. We also showed that thalamic epileptogenicity has a significant effect regarding the post-surgical outcome. Taken together, these findings suggest that thalamic

involvement in focal seizures could be a marker of extension of the epileptogenic network and may influence the surgical outcome.

Past research has mainly focused on thalamus in mesial temporal lobe epilepsy. According to Rosenberg and colleagues³ and Guye and colleagues⁴ a large percentage of MTLE showed thalamic involvement (80%), with an effect on clinical presentation if thalamus was involved⁴. Regarding seizure onset patterns, we found similar patterns to those described by Rosenberg, especially a prevalence of RS in MTLE (Fig. 1), but we also observed high frequency discharges in some cases, reaching a maximum of 190 Hz.

Here we showed that thalamic involvement is possible in all focal epilepsies independently of the lobar localisation or aetiology (Fig. 5). The possible connections of the different thalamic nuclei with the neocortex are reported in some tractography studies^{30,31}. The pulvinar is reported to be extensively connected to large parts of the cortex from the mesial temporal lobe to the parietal cortex. Interestingly, a resting state functional connectivity study proposed pulvinar nuclei as a key reflection of symptom-related functional deficits in mTLE³² and evidenced a connectivity of this nucleus with the orbitofrontal region. In our cohort, we found the highest values of thalamic epileptogenicity in bitemporal, insulo-opercular and motor system epilepsies. The high thalamic epileptogenicity in insulo-opercular epilepsy seems consistent with SEEG cortical evoked potentials, reported in Rosenberg's study³³, in which these two regions appeared highly connected (90% response rate) and with recent data on MRI insulo-thalamic connectivity³⁴. Regarding motor-premotor epilepsy and thalamic epileptogenicity, the relationship is intriguing and could be related to the "higher order connections" of the pulvinar³⁵. Patients with motor-premotor and insulo-opercular (in the dominant hemisphere) epilepsies are often contraindicated for surgery because of functional reasons. Recent data from our group³⁶ demonstrated that pulvinar stimulation could be efficient in improving seizure termination and could potentially reduce degree of impaired

consciousness. In this context our results suggest that DBS targeting the pulvinar could be an interesting option in some cases. Nevertheless, because of the limited number of patients with these epilepsies in our cohort, these data should be considered as preliminary observations and need to be confirmed by future studies.

Thalamic involvement in our study correlated with network extension. More complex epilepsies seem to more frequently involve thalamic participation in their epileptogenic network. Nevertheless, calculating network extension in patients with different SEEG implantations (number of electrodes) and different surgery outcome or contraindication to surgery (considering that some important brain regions could have missed in the implantation scheme) represent a limitation of the study.

Thalamic epileptogenicity was found to have a significant effect regarding seizure outcome, confirming the prognostic value of thalamic implication. Our results are in agreement with recent fMRI connectivity data showing that patients with TLE who showed higher presurgical levels of functional synchronization between the thalamus and other extratemporal regions had less favourable surgical outcome¹⁸. Thalamic involvement could also be a possible marker of the “synchronisability” of the network, and thus related to surgical outcome^{4,37}.

Regarding basal ganglia, namely caudate nucleus and putamen, we found that they could also be involved in focal seizures as already reported with neurophysiological³⁸ and MRI data³⁹. In our cohort caudate nucleus showed high epileptogenicity in only 9% (2/22) of patients compared to the 20% (15/74) with high thalamic epileptogenicity and when comparing EI values on both structures we found a significant difference. However it could be possible that in a different cohort of patients, for example with a higher number of patients affected by frontal lobe epilepsies, caudate nucleus involvement would be more frequent^{10,11}. Previous work on temporal lobe epilepsy showed a minor role of basal ganglia in the seizure network

⁴⁰. Recently, cortico-striatal synchronisation was reported using SEEG ⁷ during focal seizures, especially at the end of seizures, supporting a role of these nuclei in seizure termination as previously reported by our group regarding thalamus ⁶. A hypothesis about a role in inhibiting seizure spread was also proposed by other authors ⁴⁰: according to this theory basal ganglia may influence cortical oscillatory processes related to control of seizures via their feedback pathways to the cortex.

Recently, indications for intracranial presurgical investigation including SEEG have been evolving, tending to include more “complex network” epilepsies and/or MRI-negative epilepsies⁴¹. Wider SEEG indications are also related to the possibility of proposing palliative options in complex extended cases based on SEEG-guided radiofrequency thermocoagulation ^{42,43}. Moreover, SEEG has been revealed to be useful in epilepsies with widespread networks related to post-stroke aetiology, in order to guide surgical disconnection⁴⁴. Finally, some genetic epilepsies, as the case of tuberous sclerosis complex epilepsies, could also benefit from intracerebral explorations ⁴⁵. Actually in a large percentage of patients (24/74 39% in our cohort and 69/246 28% in the Cuello et al. study ⁴⁶) surgery was contraindicated, evidencing an important need for other therapeutic options.

Our results indicate that the vision of "focal" epilepsy should change. In addition to the important notion of an epileptogenic network ^{47,48}, we showed that epilepsies are cortical-subcortical diseases in which epileptogenicity can affect subcortical structures, particularly the thalamus. In the future, therapies aimed at modifying network activity on a personalized scale will have to take these modifications into account. In this sense, the development of effective thalamus stimulation paradigms in DBS aimed at desynchronizing the network ⁵ or elective modulation techniques of certain nodes through new stimulation ^{49,50} offer particularly encouraging prospects.

Fig. 1: Percentage of different SOP in thalamus across epilepsy type.

Legend: biT – bitemporal epilepsy; T plus –temporal plus epilepsy; TLE,MTLE – mesio temporal lobe; TLE,MLTLE – mesio-lateral temporal lobe epilepsy; epilepsy TLE,LTLE – lateral temporal lobe epilepsy; PE- posterior epilepsy; Op – insulo-opercular epilepsy; Mot – motor-premotor epilepsy.

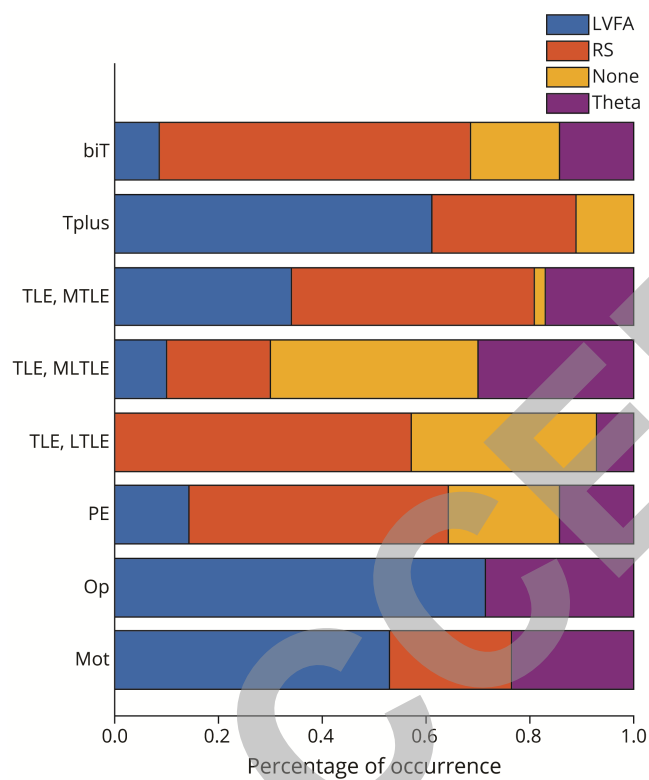


Fig. 2: Examples of subcortical ictal discharges represented in their time course and nTF analysis. In the thalamus: LVFA pattern (A and B), RS (C) and theta (D). Different frequencies may be present in each pattern. In D, a high frequency component is visible, without a clear discharge (D). SOP in the caudate nucleus (E) and in the putamen (F).

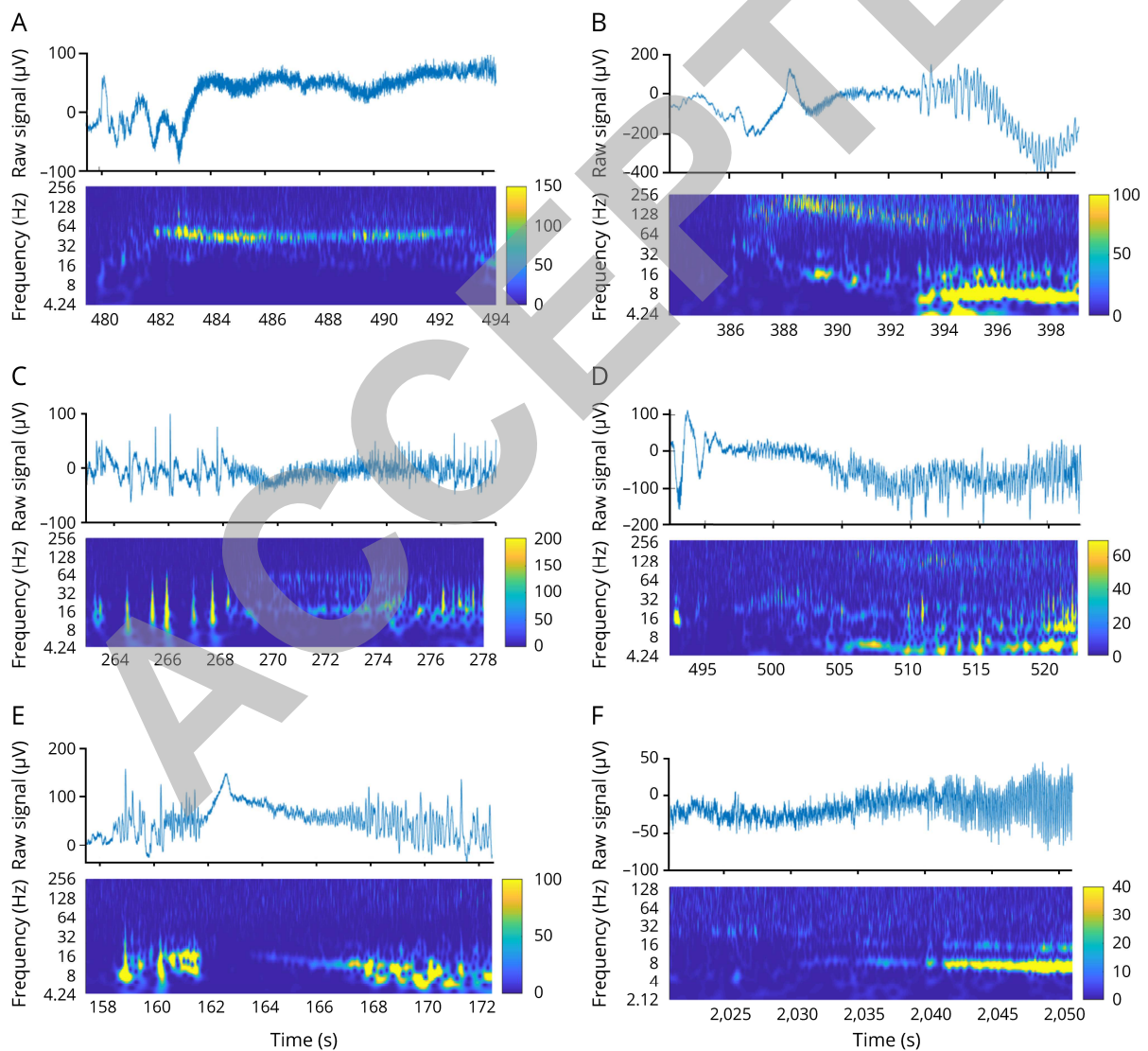


Fig. 3: EI values (max EI value per patient) in the different subcortical structures.

(Thalamus vs Caudate nucleus Wilcoxon rank sum test $p < 0.01$)

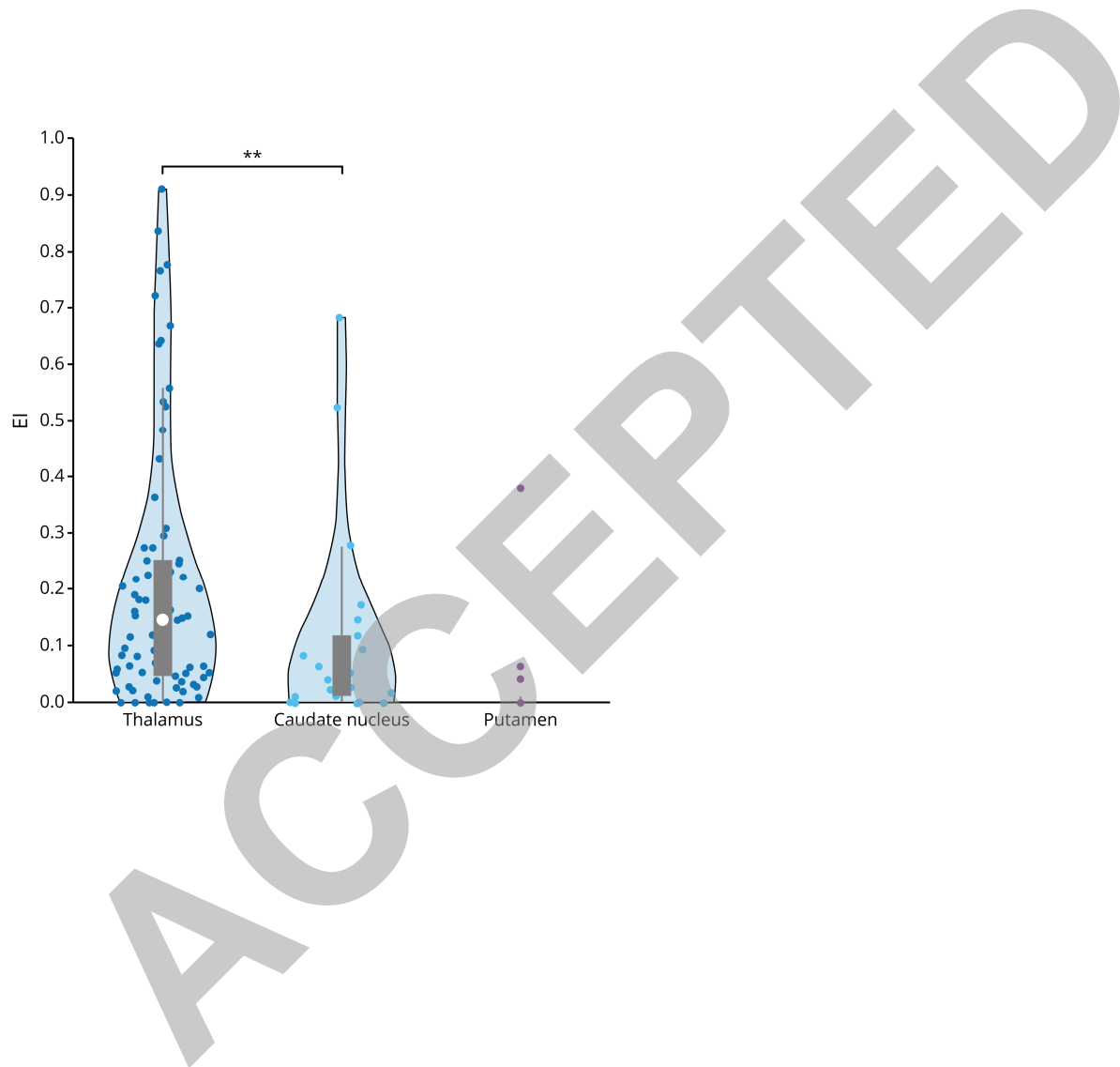


Fig. 4: Focal seizures involving thalamus (4.1, patient 64) and caudate nucleus (4.2, patient 52)

a. SEEG at seizure onset: large epileptogenic network; note the fast discharge in thalamus (Th, 1a) and caudate nucleus (CN, 2a)

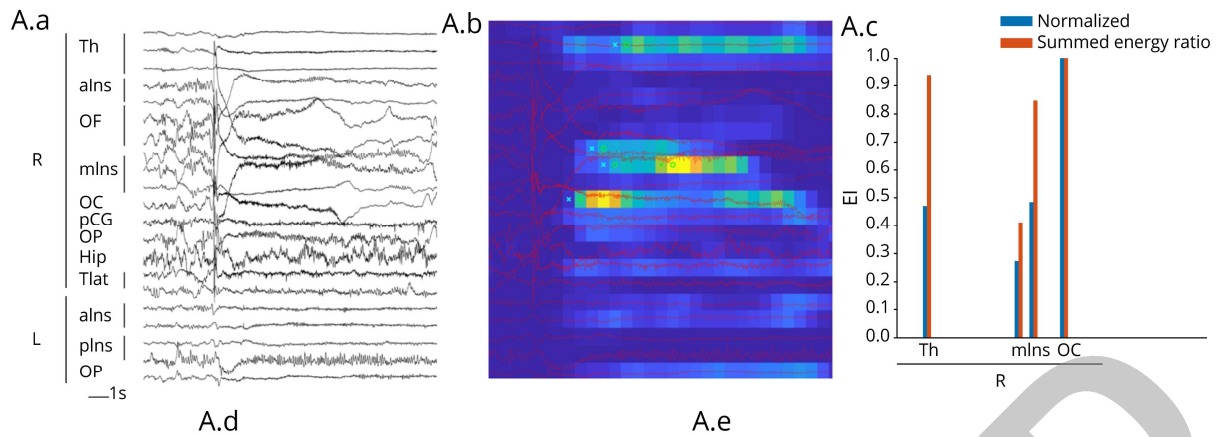
b. Epileptogenicity Index map showing the increase in energy ratio (in blue to yellow scale) and the time of detection (circle – alarm time- and cross – detection time >27)²⁷ in each selected SEEG channel. Notably in the map of fig 4.1 a detection cross at the level of channel Th (thalamus) is evident at the very beginning of the seizure given rise to the high epileptogenicity value in thalamus. To be noted, the first detection (cross) is not at Th level but in the OC channel that show the maximum value of EI (as shown in c). Comparatively, in fig 4.2 an early cross is visible in the CN (caudate nucleus) but the maximum of energy ratio is evident at the level of OR that shows the highest EI value (shown in c).

c. Results of the epileptogenicity index (in blue normalized EI, in red summed energy ratio)²⁷

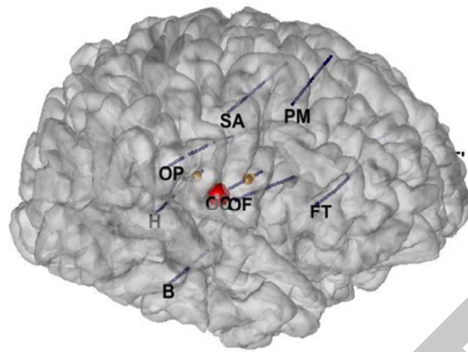
d. 3D representation of the SEEG exploration; the balloons indicate the EI detections. Balloon colour (from yellow to red) and dimension correspond to the EI value

e. MRI (T1 sequence) - CT data fusion: to be noted electrode H (see flash) sampling from thalamus (1e) and electrode OF' (see flash) sampling from caudate nucleus (2e)

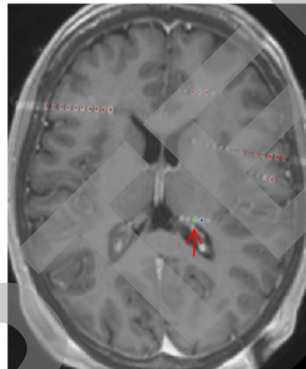
Legend: aCG- anterior cingulated cortex; aIns –anterior insula ; BT-basotemporal; Hip-hippocampus; Ins- insula; L- left; mIns- middle insula; OC- central operculum; OF – frontal operculum; OP- parietal operculum; OR- orbitofrontal cortex; pCG- posterior cingulated gyrus; pIns- posterior insula; R-right; Th - thalamus; T lat – temporo-lateral



A.d



A.e



B.a

B.b

B.c

B.d

B.e

Fig. 5: Thalamic epileptogenicity across different epilepsy type and aetiologies. Each point represents the maximum EI value in the thalamus for each patient according to the type of epilepsy and aetiologies respectively (crypto vs MCD, Wilcoxon rank sum test: uncorrected $p = 0.77$, effect size: 0.531 [0.377 0.678]).

Legend: Mot – motor-premotor epilepsy; Op – insulo-opercular epilepsy; PE- posterior epilepsy; TLE,LTLE – lateral temporal lobe epilepsy; TLE,MLTLE – mesio-lateral temporal lobe epilepsy; TLE,MTLE – mesio temporal lobe epilepsy; T plus –temporal plus epilepsy; biT – bitemporal epilepsy; HS – hippocampal sclerosis; Inf – post -infectious; MCD- malformation of cortical development; crypto – cryptogenic; other includes: cavernoma, post stroke epilepsy, post-traumatic epilepsy

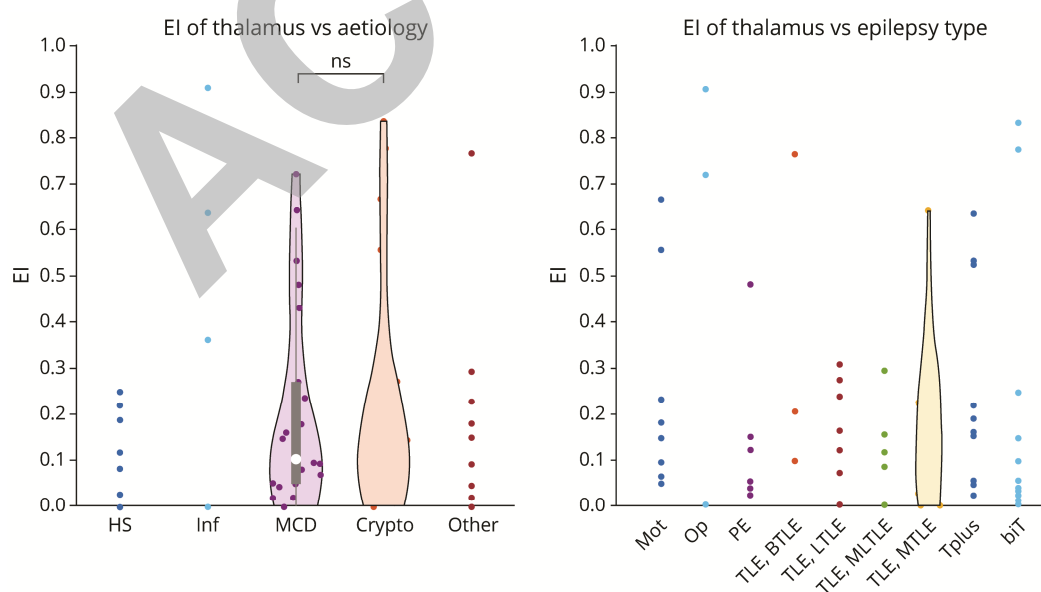


Fig. 6: Thalamic EI values correlation with the percentage of brain regions with a high EI value. A significant correlation was found ($p = 0.03$, $\rho 0.32$) suggesting the thalamus as a possible marker of the extension of the epileptogenic network

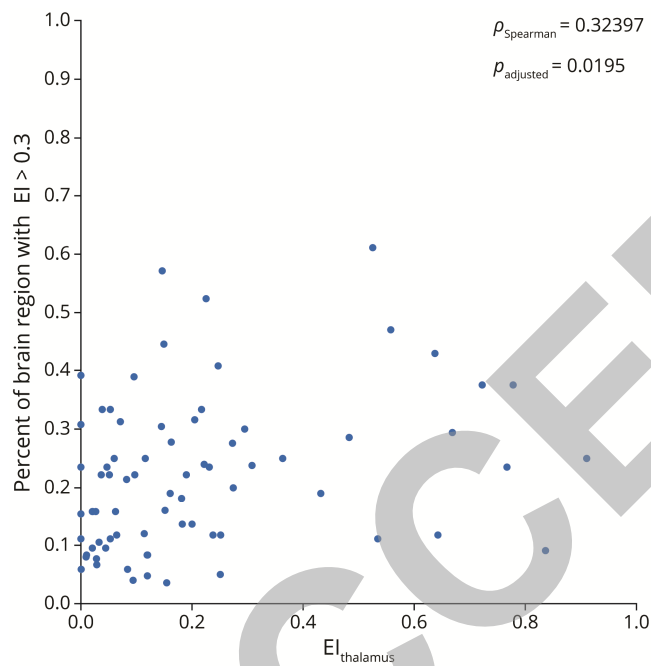


Table 1: Patient characteristics

n	sex	age at SEEG	n of seizures	epilepsy type	aetiology	SOP in TH	other subcortical/SOP	epilepsy onset	duration	after SEEG: type of surgery/contraindication: reason	Engel class	follow up (months)
1	M	15	2	TLE, MLTLE	MCD	rTheta		6	9	L T lobectomy	3	198
2	F	44	1	TLE, MTLE	HS	none		8	36	L T lobectomy	1	144
3	M	37	2	Mot	post stroke	rTheta		23	14	L F cortectomy	2	46
4	M	43	2	Tplus	MCD	RSW		25	18	R T lobectomy	3	120
5	M	24	1	TLE, MTLE	tumor	LVFA	CN: LVFA	1	23	L T lobectomy + lesionectomy	4	195
6	M	43	2	TLE, LTLE	crypto	RSW	CN: RSW	10	33	R latero-T cortectomy	1	72
7	F	17	3	Mot	MCD	RSW	CN: rTheta	0	17	L F cortectomy	3	132
8	M	22	2	biT	tumor	RSW		16	6	R T lobectomy	1	168
9	M	22	1	TLE, LTLE	MCD	none		15	7	R STG cortectomy	1	120
10	F	35	2	TLE, MLTLE	HS	none	CN: none	1	34	R T lobectomy	1	36
11	M	32	2	biT	crypto	RSW		18	14	C: bilateral		
12	F	35	1	TLE, MLTLE	tumor	LVFA		3	32	R TI lobectomy	2	132
13	M	31	2	TLE, MTLE	HS	LVFA	CN: none	4	27	L T lobectomy	3	72
14	F	54	3	TLE, MTLE	Inf	LVFA		1	53	L T lobectomy	3	42
15	F	13	3	TLE, MTLE	HS	RSW		2	11	L T lobectomy	1	42

16	M	25	2	Op	Inf	rTheta		15	10	OP gamma knife	3	24
17	F	61	2	TLE, MTLE	crypto	RSW		28	33	R T lobectomy	3	36
18	F	45	3	PE	crypto	none		16	29	C: bilateral		
19	M	42	1	TLE, MTLE	HS	rTheta		6	36	R T lobectomy	1	54
20	F	16	1	TLE, LTLE	MCD	rTheta		13	3	C: function		
21	F	46	3	biT	crypto	none		12	34	C: bilateral		
22	F	26	2	PE	crypto	LVFA	CN: none	7	19	L TO cortectomy	4	132
23	M	15	3	PE	MCD	RSW	CN: none	4	11	lesionectomy	4	150
24	F	19	2	Tplus	MCD	RSW		12	7	C: function		
25	F	48	2	biT	crypto	RSW		14	34	C: bilateral		
26	M	29	3	Mot	crypto	LVFA		5	24	lost FU		
27	F	15	3	TLE, LTLE	MCD	RSW		11	4	L T lobectomy	1	94
28	F	16	1	Mot	post stroke	RSW		3	13	C: extended		
29	F	27	2	TLE, MTLE	crypto	RSW	CN and Put: RSW	17	10	R T lobectomy	1	18
30	M	12	3	Op	MCD	LVFA	CN: LVFA Put: RSW	6	6	thalamic stimulation	4	140
31	F	25	2	PE	MCD	RSW		5	20	TO disconnection	3	19
32	M	28	1	TLE, MTLE	MCD	LVFA		10	18	C: function		
33	F	30	3	biT	MCD	RSW		21	9	C: bilateral		
34	M	52	1	TLE, MTLE	crypto	LVFA	CN: RSW	35	17	dead		
35	M	19	2	Tplus	crypto	LVFA	CN: RSW	10	9	C: extended		
36	F	22	1	Tplus	crypto	RSW		18	4	RT lobectomy, after VNS	4	41
37	F	39	3	TLE, MTLE	crypto	LVFA		20	19	C: function		

38	F	29	3	TLE, MTLE	MCD	RSW		8	21	R T cortectomy	1	17
39	F	23	2	TLE, LTLE	MCD	none		15	8	C: function		
40	F	23	3	biT	crypto	LVFA		5	18	C: bilateral		
41	M	29	3	Tplus	Inf	LVFA	CN: RSW	0	29	C: extended		
42	F	45	1	Tplus	HS	LVFA		1	44	C: extended		
43	F	42	3	TLE, MTLE	TC	RSW		24	18	in program		
44	M	45	2	TLE, MTLE	crypto	rTheta		17	28	C: extended		
45	M	35	2	Mot	crypto	rTheta		1	34	C: extended		
46	M	21	1	TLE, LTLE	crypto	none		15	6	R ant T lobectomy (extension to T1)		FU<12m
47	F	42	2	TLE, MTLE	MCD	RSW		33	9	Good, thermocoagulation		
48	M	21	2	PE	MCD	RSW		0	21	in program		
49	M	60	2	TLE, MTLE	crypto	rTheta		36	24	R T lobectomy	3	19
50	F	29	3	biT	MCD	none		20	9	C: bilateral		
51	M	15	1	Mot	crypto	LVFA		3	12	C: extended		
52	M	29	3	TLE, MLTLE	crypto	rTheta	CN: LVFA	7	22	L T resection (extended)		FU<12m
53	F	42	3	TLE, MTLE	crypto	RSW		24	18	L Tl lobectomy		FU<12m
54	F	35	2	PE	MCD	rTheta		12	23	in program		
55	M	33	2	biT	crypto	rTheta	CN: tTheta	11	22	C: bilateral		
56	F	47	2	TLE, MTLE	crypto	RSW	CN: RSW	38	9	LT lobectomy (posterior hipp included)		FU<12m
57	F	38	2	Tplus	crypto	LVFA	CN: RSW	19	19	C: extended		
58	M	36	2	Tplus	cavernoma	LVFA	Put: rTheta	23	13	Good, thermocoagulation		
59	M	26	2	TLE, MTLE	HS	RSW		5	21	L ant T lobectomy		FU<12m

60	F	25	2	TLE, MLTLE	crypto	none	CN and Put: none	11	14	in program		
61	M	10	3	TLE, MTLE	crypto	rTheta		3	7	L T lobectomy	1	18
62	M	7	3	TLE, MTLE	MCD	RSW		1,5	6	LT lobectomy		FU<12m
63	F	26	3	TLE, MTLE	MCD	LVFA		23	3	lesionectomy plus parahipp	1	18
64	F	38	2	Op	Inf	LVFA	CN: none	3	35	C: bilateral		
65	F	17	3	Mot	crypto	LVFA		15	2	C: function		
66	F	22	3	TLE, LTLE	crypto	RSW		13	9	RT lobectomy plus STG		FU<12m
67	F	7	2	Mot	post stroke	LVFA		2	5	L F lobectomy, SMA		FU<12m
68	M	47	1	Tplus	TC	LVFA	CN: rTheta	22	25	RT lobectomy		FU<12m
69	F	20	1	TLE, MTLE	HS	RSW		8	12	in program		
70	F	48	2	TLE, MTLE	MCD	LVFA	CN: RSW	11	37	Good, thermocoagulation		
71	F	37	3	biT	crypto	RSW		21	16	C: bilateral		
72	F	32	1	biT	crypto	rTheta	CN: rTheta	24	8	RT lobectomy		FU<12m
73	F	48	2	Tplus	MCD	none	CN: none	8	40	in program		
74	M	5	3	biT	crypto	RSW		0	5	R T lobectomy		FU<12m

Legend: F – female; M male; Mot – motor-premotor epilepsy; Op – insulo-opercular epilepsy; PE- posterior epilepsy; TLE,LTLE – lateral temporal lobe epilepsy; TLE,MLTLE – mesio-lateral temporal lobe epilepsy; TLE,MTLE – mesio temporal lobe epilepsy; T plus –temporal plus epilepsy; biT – bitemporal epilepsy. HS – hippocampal sclerosis; Inf – post -infectious; MCD- malformation of cortical development; crypto – cryptogenic; other includes: cavernoma, post stroke epilepsy, post-traumatic epilepsy. RS- rhythmic spikes; LVF- low voltage fast activity; R - right; L - left; T- temporal, F – frontal, ant- anterior, STG- superior temporal gyrus; SMA- supplementary motor area. C- contraindication.

In bold values of EI > 0.3 for subcortical structures.

Table 2: Multivariate probit regression

	Coefficient estimate	95% - confidence interval of the coefficient		Adjusted p-value
		Lower bound	Upper bound	
Constant	0.126	-0.422	0.675	NA
Thalamic EI	0.682	0.0520	1.312	0.0451*
Number of regions with EI > 0.3	0.602	-0.124	1.328	NA
Interactions	-0.423	-1.164	0.318	NA

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References

1. Broughton R, Gastaut H. Epileptic Seizures. 1972.
2. Jasper HH. Electrical signs of epileptic discharge. *Electroencephalogr Clin Neurophysiol*. Epub 1949.:11–18.
3. Rosenberg DS, Mauguière F, Demarquay G, et al. Involvement of medial pulvinar thalamic nucleus in human temporal lobe seizures. *Epilepsia*. 2006;47:98–107.
4. Guye M, Régis J, Tamura M, et al. The role of corticothalamic coupling in human temporal lobe epilepsy. *Brain*. 2006;129:1917–1928.
5. Yu T, Wang X, Li Y, et al. High-frequency stimulation of anterior nucleus of thalamus desynchronizes epileptic network in humans. *Brain*. 2018;141:2631–2643.
6. Evangelista E, Bénar C, Bonini F, et al. Does the thalamo-cortical synchrony play a role in seizure termination? *Front Neurol*. 2015;6.
7. Aupy J, Wendling F, Taylor K, Bulacio J, Gonzalez-martinez J, Chauvel P. Cortico-striatal synchronization in human focal seizures. *Brain*. Epub 2019.:1–14.
8. Rektor I, Kuba R, Brázdil M. Interictal and ictal EEG activity in the basal ganglia: An SIEEG study in patients with temporal lobe epilepsy. *Epilepsia*. 2002;43:253–262.
9. Sherdil A, Coizet V, Pernet-Gallay K, David O, Chabardès S, Piallat B. Implication of Anterior Nucleus of the Thalamus in Mesial Temporal Lobe Seizures. *Neuroscience* [online serial]. Elsevier Ltd on behalf of IBRO; Epub 2019. Accessed at: <https://linkinghub.elsevier.com/retrieve/pii/S0306452219304245>.

10. Devergnas A, Piallat B, Prabhu S, et al. The subcortical hidden side of focal motor seizures: Evidence from micro-recordings and local field potentials. *Brain*. 2012;135:2263–2276.
11. Vuong J, Devergnas A. The role of the basal ganglia in the control of seizure. *J Neural Transm*. Springer Vienna; Epub 2017.
12. Keller SS, Richardson MP, Schoene-Bake JC, et al. Thalamotemporal alteration and postoperative seizures in temporal lobe epilepsy. *Ann Neurol*. 2015;77:760–774.
13. Whelan CD, Altmann A, Botía JA, et al. Structural brain abnormalities in the common epilepsies assessed in a worldwide ENIGMA study. *Brain*. 2018;141:391–408.
14. Rektor I, Tomčík J, Mikl M, Mareček R, Brázdil M, Rektorová I. Association between the basal ganglia and large-scale brain networks in epilepsy. *Brain Topogr*. 2013;26:355–362.
15. Morgan VL, Rogers BP, Abou-khalil B. Segmentation of the Thalamus Based on BOLD Frequencies affected in Temporal Lobe Epilepsy. 2016;56:1819–1827.
16. Chassoux F, Artiges E, Semah F, et al. Determinants of brain metabolism changes in mesial temporal lobe epilepsy. *Epilepsia*. 2016;57:907–919.
17. He X, Chaitanya G, Asma B, et al. Disrupted basal ganglia—thalamocortical loops in focal to bilateral tonic-clonic seizures. *Brain*. 2020;143:175–190.
18. He X, Doucet GE, Pustina D, Sperling MR, Sharan AD, Tracy JI. Presurgical thalamic “hubness” predicts surgical outcome in temporal lobe epilepsy. *Neurology* [online serial]. 2017;88:2285–2293. Accessed at: <http://dx.doi.org/10.1212/WNL.0000000000004035>.

19. Výtvarová E, Mareček R, Fousek J, Strýček O, Rektor I. Large-scale cortico-subcortical functional networks in focal epilepsies: The role of the basal ganglia. *NeuroImage Clin.* 2017;14:28–36.
20. Park KM, Lee BI, Shin KJ, et al. Pivotal Role of Subcortical Structures as a Network Hub in Focal Epilepsy : Evidence from Graph Theoretical Analysis Based on Diffusion-Tensor Imaging. 2019;15:68–76.
21. Fisher RS, Velasco AL. Electrical brain stimulation for epilepsy. *Nat Rev Neurol* [online serial]. Nature Publishing Group; 2014;10:261–270. Accessed at: <http://dx.doi.org/10.1038/nrneurol.2014.59>.
22. Medina Villalon S, Paz R, Roehri N, et al. EpiTools, A software suite for presurgical brain mapping in epilepsy: Intracerebral EEG. *J Neurosci Methods.* Elsevier B.V.; 2018;303:7–15.
23. Colombet B, Woodman M, Badier JM, Bénar C-G. AnyWave: A cross-platform and modular software for visualizing and processing electrophysiological signals. *J Neurosci Methods.* Elsevier B.V.; 2015;242:118–126.
24. Roehri N, Lina J, Mosher JC, Bartolomei F, Benar CG. Time-frequency strategies for increasing high frequency oscillation detectability in intracerebral EEG. 2016;2:1–12.
25. Lagarde S, Bonini F, McGonigal A, et al. Seizure-onset patterns in focal cortical dysplasia and neurodevelopmental tumors: Relationship with surgical prognosis and neuropathologic subtypes. *Epilepsia.* Epub 2016.:1–10.
26. Roehri N, Pizzo F, Lagarde S, et al. High-frequency oscillations are not better biomarkers of epileptogenic tissues than spikes. *Ann Neurol.* 2018;83:84–97.

27. Bartolomei F, Chauvel P, Wendling F. Epileptogenicity of brain structures in human temporal lobe epilepsy: A quantified study from intracerebral EEG. *Brain*. 2008;131:1818–1830.
28. Benjamini Y, Hochberg Y. Controlling the False Discovery Rate: A Practical and Powerful Approach to Multiple Testing. *J. R. Stat. Soc.* 1995. p. 289–300.
29. Fay MP, Malinovsky Y. Confidence intervals of the Mann-Whitney parameter that are compatible with the Wilcoxon-Mann-Whitney test. *Stat Med*. 2018;37:3991–4006.
30. Behrens TEJ, Johansen-Berg H, Woolrich MW, et al. Non-invasive mapping of connections between human thalamus and cortex using diffusion imaging. *Nat Neurosci*. 2003;6:750–757.
31. Song Y, Jiayang Z. Discriminating preictal and interictal brain states in intracranial EEG.pdf. *J. Neurosci. Methods* 2016. p. 45–54.
32. Jo HJ, Kenny-Jung DL, Balzekas I, et al. Nuclei-specific thalamic connectivity predicts seizure frequency in drug-resistant medial temporal lobe epilepsy. *NeuroImage Clin* [online serial]. Elsevier; 2019;21:101671. Accessed at: <https://doi.org/10.1016/j.nicl.2019.101671>.
33. Rosenberg DS, Mauguière F, Catenoix H, Faillenot I, Magnin M. Reciprocal thalamocortical connectivity of the medial pulvinar: A depth stimulation and evoked potential study in human brain. *Cereb Cortex*. 2009;19:1462–1473.
34. Ghaziri J, Tucholka A, Girard G, et al. The Corticocortical Structural Connectivity of the Human Insula. *Cereb Cortex*. 2017;27:1216–1228.
35. Sherman SM. Thalamic relays and cortical functioning. *Prog Brain Res*.

- 2005;149:107–126.
36. Filipescu C, Lagarde S, Lambert I, et al. The effect of medial pulvinar stimulation on temporal lobe seizures. *Epilepsia*. Epub 2019.:1–6.
 37. Kini LG, Bernabei JM, Mikhail F, et al. Virtual resection predicts surgical outcome for drug resistant epilepsy. *Brain*. Epub 2019.:1–14.
 38. Rektor I, Kuba R, Brázdil M, Halánek J, Jurák P. Ictal and peri-ictal oscillations in the human basal ganglia in temporal lobe epilepsy. *Epilepsy Behav* [online serial]. Elsevier Inc.; 2011;20:512–517. Accessed at: <http://linkinghub.elsevier.com/retrieve/pii/S1525505011000059>.
 39. Dreifuss S, Vingerhoets FJG, Lazeyras F, et al. Volumetric measurements of subcortical nuclei in patients with temporal lobe epilepsy. *Neurology*. 2001;57:1636–1641.
 40. Rektor I, Kuba R, Brázdil M, Chrastina J. Do the basal ganglia inhibit seizure activity in temporal lobe epilepsy? *Epilepsy Behav* [online serial]. Elsevier Inc.; 2012;25:56–59. Accessed at: <http://linkinghub.elsevier.com/retrieve/pii/S1525505012003332>.
 41. Cloppenborg T, May TW, Blümcke I, et al. Trends in epilepsy surgery: Stable surgical numbers despite increasing presurgical volumes. *J Neurol Neurosurg Psychiatry*. 2016;87:1322–1329.
 42. Isnard J, Taussig D, Bartolomei F, et al. French guidelines on stereoelectroencephalography (SEEG). *Neurophysiol Clin*. Elsevier Masson SAS; Epub 2017.
 43. Cossu M, Fuschillo D, Casaceli G, et al. Stereoelectroencephalography-guided

- radiofrequency thermocoagulation in the epileptogenic zone: a retrospective study on 89 cases. *J Neurosurg.* 2015;123:1358–1367.
44. Marchi A, Pennaroli D, Lagarde S, et al. Epileptogenicity and surgical outcome in post stroke drug resistant epilepsy in children and adults. *Epilepsy Res.* 2019;155:106155.
 45. Neal A, Ostrowsky-Coste K, Jung J, et al. Epileptogenicity in tuberous sclerosis complex: A stereoelectroencephalographic study. *Epilepsia.* Epub 2019.:81–95.
 46. Cuello Oderiz C, von Ellenrieder N, Dubeau F, et al. Association of Cortical Stimulation–Induced Seizure With Surgical Outcome in Patients With Focal Drug-Resistant Epilepsy. *JAMA Neurol.* Epub 2019.:1–9.
 47. Bartolomei F, Lagarde S, Wendling F, et al. Defining epileptogenic networks : Contribution of SEEG and signal analysis. *Epilepsia.* Epub 2017.:1–17.
 48. Malinowska U, Badier J, Gavaret M, Bartolomei F, Chauvel P, Bénar CG. Interictal Networks in Magnetoencephalography. *Hum Brain Mapp.* 2014;35:2789–2805.
 49. An S, Bartolomei F, Guye M, Jirsa V. Optimization of surgical intervention outside the epileptogenic zone in the Virtual Epileptic Patient (VEP). *PLoS Comput Biol* 15(6). 2019;15:1–25.
 50. Olmi S, Petkoski S, Guye M, Bartolomei F, Jirsa V. Controlling seizure propagation in large-scale brain networks. *PLoS Comput Biol.* 2019;15:1–23.