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Anticancer boron-containing prodrugs responsive to oxidative stress from the tumor microenvironment

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- 10

11 **ABSTRACT**

12

13 Boronic acid (and ester) prodrugs targeting the overexpressed level of reactive oxygen species 14 within tumor microenvironment represent a promising area for the discovery of new selective anticancer chemotherapy. This strategy that emerged only ten years ago is exponentially 15 growing and could demonstrate its clinical usefulness in the near future. Herein, the previously 16 17 described small-molecule and macromolecular anticancer prodrugs activated by carbon-boron oxidation are gathered. This review reports on the most interesting derivatives mentioned in 18 the literature based on the in vitro and in vivo activity when available. Eventually, the 19 20 pharmacological applicability of this strategy is discussed, in particular, the kinetic aspect of the prodrug oxidation and the selectivity of this reaction towards certain ROS from the tumor 21 22 microenvironment are specified.

23 24

25 **1. Introduction**

26

The prodrug strategy was initially introduced by Albert in 1958.[1] Prodrugs are activity-masked 27 molecules designed to be activated in vivo by an enzymatic or a chemical reaction. In most 28 cases, these molecules are covalent assemblies made of the active drug linked to a temporary 29 molety. The latter chemical unit confers new physicochemical properties to the entire entity 30 optimizing its absorption, distribution, metabolism, excretion and toxicity (ADMET).[2-4] The 31 32 prodrug strategy used in anticancer chemotherapy intends to deliver the active drug only at 33 the tumor site in order to avoid deleterious side effects on normal tissues. Indeed, chemotherapies used in medical oncology are mostly cytotoxic agents and these drugs 34 indifferently target both healthy and cancer cells. In this case, the temporary moiety must: (i) 35 strongly impede the activity of a given antitumor agent; (ii) be specifically cleaved in cancer 36 37 tissues to permit cancer-targeted drug delivery.[5-7]

Cancer cells are markedly different to cells from healthy tissues. The biologic singularities of cancer cells is therefore exploited in anticancer prodrug strategy in order to localize the delivery of the active drug at the tumor site. Abnormalities of the tumor environment has led to distinct strategies in cancer-responsive prodrug research. First, certain enzymes such as cathepsins are overexpressed in cancer cells and specific prodrugs were developed to target this

characteristic.[8-10] Prodrugs capitalizing on the hypoxia of cancer cells inside solid tumors 43 are also the object of intensive research.[11-13] Antitumor targeted-prodrugs responsive to 44 the pronounced oxidative stress in cancer cells have been recently developed.[14,15] Indeed, 45 biological studies of tumors have revealed that cancer cells have a higher degree of oxidative 46 stress compared to healthy cells.[16] This stress is produced by deregulated and enhanced 47 mitochondrial functions and cellular metabolism. Oxidative stress stimulates the tumor 48 progression processes such as cell proliferation and angiogenesis. Cancer cells migration and 49 50 neovascularization will ultimately lead to the dissemination and growth of cancer cells in metastatic sites. Macrophages have been described to promote the generation of oxidative 51 stress of cancer cells through the secretion of molecular mediators.[17] These immune cells 52 53 are primarily present around the tumor cells in order to eradicate them by phagocytosis and production of oxygen-containing reactive molecules. Nonetheless, they will indirectly contribute 54 55 to cancer progression.[18] These cellular events provide an increase of the oxygenated 56 reactive molecules level in the tumor microenvironment.

These highly reactive molecules are composed of reactive oxygen species (ROS) and reactive 57 nitrogen oxide species (RNOS).[16] Among ROS, superoxide anion (O2.) is engendered from 58 59 O_2 via NADPH oxidase action and mitochondrial metabolism. O_2 is subsequently converted to hydrogen peroxide (H₂O₂) by superoxide dismutase (SOD) catalysis. H₂O₂ further evolves 60 into hypochlorous acid (HOCI) and hydroxyl radical (HO \cdot). Among RNOS, nitric oxide (NO \cdot) is 61 produced by reaction of molecular oxygen and L-arginine catalyzed by nitric oxide synthases 62 (NOSs). NO- spontaneously reacts with O2- to form peroxynitrite/peroxinitrous acid (ONOO 63 /ONOOH). The latter species is unstable and generate hydroxyl radical and nitrogen dioxide 64 radical (NO₂·). 65

Boronic acids and their corresponding esters have been developed as temporary masking 66 groups for drugs or probes specifically triggered by oxygen-containing reactive molecules.[19-67 68 23] In biological aqueous media, boronate esters are rapidly hydrolyzed into boronic acid.[24] Among the different reactive species, hydrogen peroxide, hypochlorite anion (CIO-) and 69 peroxynitrite were shown to react with boronic acids and esters to further oxidize the carbon-70 boron bond to form an alcohol group.[25] In biological conditions, hypochlorite anion will almost 71 exclusively react with cellular amines and thiols since the latter reactions will be faster than the 72 73 oxidation of carbon-boron bonds. Nucleophilic oxygen of the reactive species will be able to attack the empty p orbital of the boron atom (Scheme 1).[26,27] Carbon migration to oxygen 74 75 further gives a borate that will be hydrolyzed to afford the corresponding alcohol and non-toxic boric acid.[28] At physiological pH, conversion by peroxinitrite is 10⁶ times faster than the 76 hydrogen peroxide-mediated oxidation likely due to the anionic form of peroxinitrite in 77

78 comparison to neutral H₂O₂.[25]



Scheme 1. Mechanism of boronic acid oxidation into alcohol by either hydrogen peroxyde or
 peroxynitrite.

82

79

The boronic/boronates functionalities were used as temporary moieties to either mask aliphatic 84 alcohols, [25, 29] enols [30, 31] or aryl-alcohols. [19, 23] The active effector can be connected to 85 the boronic/boronates groups directly or via self-immolative spacers.[32,33] The use of these 86 spacers allows the bounding of different effectors through either their alcohol or amine 87 functions generating ether, carbonate or carbamate bonds. The volume added by the spacer 88 to the final entity contributes to a better masking of the biological activity. Oxidation of such 89 spacer lead to the formation of an aryl-alcohol motif that will undergo spontaneous elimination 90 leading to the release of an effector (Scheme 2). 91

Boronic/boronate prodrug



94 95

Scheme 2. Release of the active drug from boron-containing prodrug by either direct C-B bond oxidation or by oxidation and subsequent self-immolative process.

98

The strategy of boronic acid/boronate oxidation has been widely used for the emergence of many probes for tumor imaging and/or prodrugs with tumor targeting properties leading to the release of the parent drug. Herein, we comprehensively review the ROS responsive boronate prodrugs that were developed and evaluated as anticancer agents. In the next section, we gathered the different platforms used to construct the prodrug of interest: a majority of small molecules were found but a non-negligible amount of drug delivery-based polymeric matrix and nanoparticles were also described.

106

2. Small-molecule and macromolecular prodrugs

108

109 Precursors of selective estrogen receptor modulators (SERM)

The selective estrogen receptor modulators have been developed to treat breast cancer tumors presenting the estrogen receptor.[34] Antiestrogens, such as tamoxifen 1, bind to the hormone receptor and block the proliferation of the cancer cells. Moreover, tamoxifen 1 is a prodrug converted to both 4-hydroxytamoxifen 2 and endoxifen 4 by cytochrome P450

- enzymes. The Wang group has therefore synthesized and evaluated boron-based prodrugs of
- 4-hydroxytamoxifen **2** and endoxifen **4** as potential anticancer agents (Scheme 3).[35–37]



Scheme 3. Structures of 4-hydroxytamoxifen and endoxifen (oxidative metabolites of tamoxifen) and theirs prodrugs.

119

This strategy is indeed meaningful since these two active metabolites would be similarly 120 obtained by oxidative cleavage of the boronic acid function of 3 and 5 in the tumor environment. 121 In vitro cytotoxic activity of 3 and 5 was determined against MCF-7 and T47D, two breast 122 cancer cell lines expressing the estrogen receptor. The prodrug 3 and its active metabolite 4-123 hydroxytamoxifen 2 were as active against a given cell line. 80% conversion of prodrug 3 to 4-124 hydroxitamoxifen 2 was observed in cell culture media and the cellular uptake of 3 was 4 times 125 higher than 4-hydroxytamoxifen 2 in MCF-7 culture. Comparable in vitro observations were 126 made for the prodrug/drug couple: 5/endoxifen 4. Growth inhibition of MCF-7 cancer 127 xenografts in mice was similar for the prodrug 5 and the active metabolite endoxifen 4 at the 128 optimal dose of 1 mg/kg. Metabolism and pharmacokinetic studies in mice showed that the 129 plasma concentration of boronic prodrugs 3 and 5 were 40-fold higher than their respective 130 active ingredients or the other parent prodrug tamoxifen 1 administrated at the same dose. 131 Noteworthy, the conversion of both prodrugs was due to the oxidation of the boronic acid 132 functions by cytochrome P450 enzyme rather than the ROS/RNOS overexpressed by cancer 133 cells. The enhanced bioavailability from the prodrugs 3 and 5 is therefore due to the prolonged 134 release of the phenol counterparts. Hence, rapid excretion of 4-hydroxytamoxifen 2 and 135 136 endoxifen 4 is observed when these molecules are directly injected and this was attributed to the glucuronidation of the hydroxy groups during phase II metabolism. 137

138

139 Precursor of epigenetic regulators

140 Histone deacetylase (HDAC) inhibitors

Histone deacetylases (HDACs) remove acetyl groups from histone and other nonhistone
 targets. HDACs control the transcription of oncogenes leading to the production of proteins
 involved in cancer induction and proliferation and HDAC inhibitors were developed to prevent

the progression of cancer cells.[38] Interestingly, two hydroxamate molecules: vorinostat 6 and 144 belinostat 8, FDA-approved drugs for the treatment of cutaneous T-cell lymphoma, were the 145 basis for the preparation of prodrugs (Scheme 4).[39,40] Indeed, these pharmaceuticals are 146 good candidates for prodrug development since they present important drawbacks such as 147 toxicity and weak bioavailability due to both the lack of hydroxamic acid stability and to rapid 148 excretion by sulfation and glucuronidation. Liao et al.[39] proposed the prodrug 7 of vorinostat 149 6 targeting the acute myeloid leukemia owing to the high level of ROS produced by these tumor 150 151 cells.[41]



152 153

Scheme 4. Prodrugs of vorinostat and belinostat.

154

Here, the drug was linked to a self-immolative benzene boronic acid moiety to afford the prodrug **7**. The viability of two leukemia cell lines, U937 and MV4-11, treated by **7** and vorinostat **6** was determined in vitro and showed a partial recovery (~ 20%) of the drug activity after incubation.

Furthermore, Wang and colleagues prepared a prodrug 9 made of a benzene boronate nucleus 159 160 branched to the hydroxamic acid moiety of belinostat 8 for the chemotherapy of solid tumors.[40] Belinostat 8 and 9 were tested in vitro against four cancer cell lines: A549 (lung 161 carcinoma), HeLa (cervical cancer) and, MDA-MB-231 and MCF-7 (breast adenocarcinoma). 162 Again, around 25% of the parent drug activity was recovered after incubation except for the 163 MCF-7 cells where prodrug 9 displayed only 5% of the corresponding drug activity. Conversion 164 of the prodrug 9 into belinostat 8 in MDA-MB-231 culture cell media was ~ 10% after 24h of 165 166 incubation. The HDAC inhibitory activity of the prodrug 9 was then measured and was ten times lower than that of belinostat 8. Altogether, these observations account for the noticeable 167 difference of cancer cells viability between the drug and the prodrug. In vivo activity of prodrug 168 9 was compared to belinostat 8 in a MCF-7 xenograft model in mice at the dose of 10 169 mg/kg/day, a slight increase of efficacy was observed for 9 toward the free drug. The belinostat 170 171 8 concentration was twice higher in tumor tissue after prodrug 9 subcutaneous injection in contrast with the same injected dose of the parent drug. The higher efficacy of the prodrug is 172 explained by the increased bioavailability of the benzene boronate precursor 9. The plasmatic 173 174 concentration in mice was quantified for both belinostat 8 and its prodrug 9: 10 mg/kg were independently injected and after 3h, the concentration of belinostat 8 was 7-fold higher when 175 using the prodrug 9.[42] Moreover, study of 9 metabolism in liver S9 fraction clearly brought to 176 light the role of the enzymatic metabolism (via cytochrome P450) in the conversion of the 177 boronic acid function into the corresponding phenol leading to belinostat 8 through self-178 179 immolation.

181 Lysine-specific histone demethylase inhibitor

Among histone post-translational modifications, lysine methylation of histone governs the structure of chromatin and the methylation degree of histones is involved in cancer formation.[43] Lysine-specific histone demethylase inhibitor are not currently used in clinic but these molecules are studied for the development of anticancer epigenetic drugs. Engel et al.[44] have prepared a benzene boronate prodrug **11** of the promising histone demethylase inhibitor *trans*-2-phenylcyclopropylamine **10** (Scheme 5).



188 189

Scheme 5. Prodrug of *trans*-2-phenylcyclopropylamine.

190

Prodrug **11** was tested in vitro against glioblastoma U87 cells and primary glioblastoma cells, and healthy astrocytes. No activity was observed up to 300 μ M on healthy astrocytes while primary glioblastoma and U87 cells were impacted at 10 μ M and 1 μ M respectively. The authors also showed the impact of the quinone methide (formed from the benzene boronate promoiety) which reacts covalently with gluthatione in cells reducing the intracellular concentration of this antioxidant (vide infra).

197

198 **Precursor of tyrosine kinase inhibitors**

199 Crizotinib **12** is a tyrosine kinase inhibitor developed to treat non-small cell lung cancers.[45] 200 This drug however presents important side effects such as hepatoxicity and neutropenia. 201 These drawbacks prompted the Kowol group to prepare a benzene boronate prodrug **13** of 202 this molecule in an attempt to selectively reach the cancer cells (Scheme 6).[45]



203

Scheme 6. Benzyloxycarbonyl prodrug of crizotinib and non-immolated metabolite **14**.

205

Three non-small cell lung cancer cell lines (H1993, RUMH and H2228) known to respond to 206 207 crizotinib 12 were evaluated toward their production of ROS by flow cytometry using 2',7'-208 dichlorofluorescein diacetate. The in vitro ROS production of the H1993 cells was found to be twice as much as the two other cell lines. In vitro cytotoxicity assays showed that approximately 209 50% of free crizotinib **12** (IC₅₀ ~ 3-15 μ M) activity was found with the prodrug **13**. Addition of 210 H₂O₂ prior to incubation with the different cell lines completely restored the activity of the 211 original drug, except when in contact with H1993 cells where the activity remains surprisingly 212 lower. The authors also observed that a stable non-immolated metabolite 14, a p-213

- 214 hydroxybenzyl adduct of crizotinib was as active as the free drug against all the tested cell
- lines pointing out that benzyl moiety is not sufficient to mask the drug activity in this case.
- 216

217 Precursors of antimetabolite drugs

- 218 Methotrexate (MTX) 15, a potent inhibitor of the dihydrofolate reductase implied in the purine
- and pyrimidine synthesis, is used in clinic to treat cancer and autoimmune diseases. The
- 220 Clausen group has described several benzene boronate prodrugs of methotrexate **15** originally
- developed for the treatment of rheumatoid arthritis (Scheme 7).[46,47]



- 222
- 223

Scheme 7. Prodrugs of MTX, 5-FU and gemcitabin.

224

Recently, the in vitro activity of the prodrug **16** (Scheme 7) was reported on HL-60 (human leukemia cancer cell line), HeLa cancer cell line and HEK293 (human embryonic kidney cell line).⁴⁷ The HL-60 cells were shown to produce around ten times more ROS in vitro than of the HEK293 cells. However, prodrug **16** displayed close in vitro activity against the two latter cell lines (IC₅₀ ~ 0.05 μ M), a growth inhibition decreased by a factor 2-4 in comparison with the free methotrexate **15**.

The antimetabolite 5-fluorouracil (5-FU) **17**, a widely used antitumor drug, presents several side effects such as myelosuppression and neurotoxicity. In order to reduce these drawbacks, the Xue group has developed the benzene boronate prodrug of 5-fluorouracil (Scheme 7).[48] Boronate prodrug **18** and its corresponding boronic acid were tested in vitro against the 60 cancer cell lines from the National Cancer Institute. Prodrug **18** was more active against all cell lines than its boronic acid counterpart which is guite surprising since boronate esters are hydrolyzed into boronic acid in aqueous media (vide supra). Then, the authors particularly compared breast cancer cells MCF-7 to immortalized mouse embryonic epicardial cells MEC1. 5-Fluorouracil **17** was cytotoxic against two cell lines with an IC₅₀ around 1 μ M whereas **18** had no effect against MEC1 up to a concentration of 100 μ M and was slightly active on the MCF-7 cancer cells (IC₅₀ = 10-50 μ M). Aside from that, prodrug **18** showed a better drug safety profile than 5-fluorouracil **17** on wild-type C57BL/6 male mice.

Another nucleotide analog used in clinic, gemcitabin 19, was linked to a benzene boronate 243 244 moiety to build the prodrug **20** (Scheme 7).[49] Gemcitabin **19** and prodrug **20** were evaluated in vitro against pancreatic cell lines: cancerous (PSN1 and BxPC3) and normal (NPEC). The 245 H₂O₂ level produced by each cell line was measured using the ROS-Glo[™] assay which 246 demonstrated a weakly higher production of ROS by the cancer cells. Gemcitabin **19** displayed 247 an IC₅₀ of 0.005-0.015 µM against the three cell lines and prodrug **20** was around 20 times 248 less active in each case. Nonetheless, prodrug 20 was able to retrieve the activity of gemcitabin 249 250 19 when ROS were artificially produced by the cancer cell lines via preliminary addition of 2deoxy-D-glucose. In vivo activity was determined using PSN1 xenograft model in mice and 251 showed a similar activity of both gemcitabin **19** and prodrug **20**. However, myelosuppression 252 253 was lowered in mice treated with the prodrug 20 and the authors showed that concentration of the resulting gemcitabin 19 in bone marrow was reduced in comparison with the gemcitabin-254 255 treated group.

256

257 **Precursors of cytotoxic drugs**

258 Campthotecin 21

Campthotecin **21** is a strongly cytotoxic natural product as a result of its topoisomerase I inhibitory activity. The 10-hydroxycampthotecin known as SN-38 **22**, is the toxic hydrolytic metabolite of the commercialized prodrug irinotecan **23**.[50] Thus, Lei et al.[51] prepared the oxidative prodrug **24** of SN-38 **22** by replacing the original phenol group into a boronic acid function (Scheme 8).



265

Scheme 8. Prodrugs of camptothecin.

266

267 Prodrug 24 and the corresponding active metabolite SN-38 22 were tested in vitro against six cancer cell lines: colon cancer cells HCT-15 and HT-29, breast cancer cells MCF-7 and MDA-268 MB-231 and, glioblastoma cells U87MG and U251. The activity of SN-38 22 was fully restored 269 upon incubation of 24 with the different cell lines (IC₅₀ ranging from 0.01 to 5 μ M). The authors 270 observed that the conversion of 24 into SN-38 22 in MCF-7 culture cell media was around 40% 271 272 after 48h of incubation. Moreover, the topoisomerase I inhibitory evaluation of 24 showed that the boronic acid derivative was as potent as SN-38 22. These two latter observations therefore 273 account for the good in vitro activity of 24 against this panel of cancer cells. Prodrug 24 was 274 275 evaluated in vivo using U87MG cancer xenograft in mice and displayed a modest efficacy at 2 276 mg/kg in comparison with the reference irinotecan 23 (antitumor effect of 8% T/C with irinotecan vs. 28% T/C with 24). 277

278 Theranostic boronate-based prodrugs of campthotecin were also prepared. In cancer chemotherapy, this approach combining therapy and diagnosis allows the visualization of the 279 drug by imaging its localization within the organism. The Kim group prepared a prodrug 25[52] 280 281 able to release a fluorophore (a coumarin) and SN-38 22 whereas the Shabat group developed a precursor 26 liberating a near-infrared cyanine fluorophore and campthotecin 21 (Scheme 282 8).[53] Prodrug 25 and SN-38 22 were evaluated in vitro against melanoma cells B16F10 and 283 284 cervical cancer cells Hela. The prodrug 25 was able to restore around 60% of the SN-38 22 activity on both cancer cells and a complete recovery was obtained when adding 100 µM of 285 286 H_2O_2 . This latter observation was made at 100 μ M of tested compounds, a concentration way beyond the IC₅₀ of SN-38 22. The authors treated a B16F10 melanoma xenograft in mice with 287

25 at 0.25 mg/kg or with a saline solution. Again, a relatively limited efficacy was observed with 288 a slightly prolonged survival time (1-6 days) of the treated mice over the non-treated group. 289 Regrettably, irinotecan 23 or the active ingredient SN-38 22 were not evaluated in this in vivo 290 study. In regards to the cyanine prodrug 26, the activity against U87MG cells was first 291 determined in vitro: the authors observed an IC₅₀ of 0.25 µM for the prodrug 26 whereas 292 campthotecin **21** was ten times more active ($IC_{50} = 0.02 \mu M$). Nonetheless, the pre-incubation 293 of H_2O_2 with **26** lead to the full release of campthotecin **21** and therefore the original IC₅₀ of 294 295 this free drug was re-established. In vivo imaging of the prodrug 26 using U87MG cancer xenograft in mice showed a precisely localized activation within the tumor after intratumoral 296 administration. The fluorescence appeared only one minute after prodrug injection and the 297 298 cyanine dye was still observable 6 hours after administration to the mice.

299

300 Doxorubicin 27

301 Doxorubicin **27** is a cytotoxic natural product acting as DNA intercalating agent and 302 topoisomerase II inhibitor (Scheme 9). Although used in clinic as antitumor drug, important 303 side effects such as cardiotoxicity were described.[54] Our group therefore prepared 304 arylboronate-based prodrugs of doxorubicin by branching the free amine function of this 305 drug.[55]





306 307

First, using an arylboronate profluorescent probe of coumarin, we determined the most efficient 309 cell line at converting the probe into free coumarin among a panel of six cancers from different 310 organs (breast cancer MCF-7 and the resistant counterpart MCF-7 MDR, hepatocellular 311 carcinoma Hep G2, lung adenocarcinoma A549, glioblastoma U87, pancreatic cancer cell line 312 MiaPaCa-2). Hep G2 and MiaPaCa-2 were the most ROS-producing cell lines but the 313 cytotoxicity of the prodrugs was nonetheless evaluated on the different cell lines. Prodrug 28 314 was the most interesting since it displayed an IC₅₀ of 0.3 μ M corresponding to 67% of the total 315 effect obtained with the same concentration of doxorubicin 27 ($IC_{50} = 0.2 \mu M$). Using MiaPaCa-316 2 pancreatic tumor in ovo xenograft via the HET-CAM (Hen's Egg Test-Chorioallantoïc 317 Membrane) assay, 28 induced the same tumor regression as doxorubicin 27 intratumorally 318 319 injected at the same dose. Ye et al. [56] have efficiently entrapped the prodrug 28 in polymeric nanoparticles of polyethylene glycol conjugated to niacin (PEG-NAM, Scheme 9). The ROS 320 generator β-lapachone was co-encapsulated within the micelles in order to enhance the 321 322 release of free doxorubicin. The authors observed that β -lapachone was first liberated and was then able to amplify the conversion of 28 into doxorubicin 27. The loaded nanoparticles 323 together with doxorubicin 27, β-lapachone and 28 were evaluated in vitro against three breast 324 cancer cell lines (4T1, MCF-7 and MCF-7 ADR, i.e resistant to doxorubicin) and against 325 NIH/3T3 fibroblasts. Prodrug 28 was less active than doxorubicin 27 showing weak in vitro 326 327 conversion of 28 into free drug against the four cell lines. Furthermore, the IC₅₀s of doxorubicine 27, β-lapachone and the loaded nanoparticles obtained were equals in every 328 cases except with the resistant MCF-7 cells where the micelles and β-lapachone were 4-5 329 times more active. This last observation highlight the particular efficacy of the latter molecules 330 against doxorubicin resistant cancer cells. In vivo pharmacokinetics assays showed that both 331 bioavailability and tumor concentration of doxorubicin 27 is improved when the doxorubicin-332 333 containing polymeric micelles are injected to mice in comparison with the administration of free drug at the same dose. The different molecules were tested on a MCF-7 ADR tumor xenograft 334 model by intravenous injections at 5 mg/kg. An important tumor regression was observed (~ 335 336 90%) when treated with doxorubicin 27 loaded nanoparticles which was higher than the free doxorubicin 27 (~ 50%) and prodrug 28 (~ 30%). 337

A theranostic prodrug **29** of doxorubicin was built based on a central benzenic self-immolative spacer able to release simultaneously the free drug and a fluorophore, a tetraphenylethene with aggregation-induced emission properties (Scheme 9).[57] The construct **29** was evaluated in vitro on Hela cells that were first treated with 1-phorbol-12-myristate-13-acetate (PMA), an agent inducing the ROS production in cells. After incubation, fluorescence and cytotoxicity ($IC_{50} \sim 2 \mu M$) were observed in PMA-treated cells whereas no effect was detected on the PMAfree cells.

345 Organo-silica nanoparticles 30 displaying phenyl boronic moiety at their surface were prepared by the Shi group.[58] Doxorubicin was then covalently linked via its cis diol part to generate a 346 347 boronate ester bond leading to nanoparticles covered with the drug (Scheme 9). These 348 nanoparticles were designed to specifically release the doxorubicin within a tumor by ROSmediated oxidation or by acidic cleavage of the boronate ester bond (due to particularly acidic 349 pH in cancer cells). Hyaluronic acid was also coated at the surface of the nanoparticles in order 350 to specifically target the CD44 receptor which is overexpressed at the surface of certain cancer 351 cells. Efficient in vitro release of doxorubicin 27 was first demonstrated in presence of H₂O₂ 352 353 and then the particles were evaluated against Hep G2 cancer cells (CD44+++) and NIH/3T3 fibroblasts (CD44+). Nanoparticles 30 bearing hyaluronic acid and doxorubicin were: (i) more 354 toxic against Hep G2 (IC₅₀ ~ 0.5 μ M) than their hyaluronic acid free counterparts (IC₅₀ = 2 μ M) 355 356 and (ii) more active against Hep G2 than NIH/3T3 (IC₅₀ ~ 2 μ M).

358 Paclitaxel **31**

Paclitaxel is an antitumor drug inhibiting microtubules depolymerization therefore blocking the mechanism of mitosis.[59] This form of the drug presently used suffers from several side effects and a micellar prodrug **32** built from conjugates "polyethylene glycol-benzene boronatepaclitaxel (Scheme 10) was developed by Dong et al.[60]



363

364

Scheme 10. Prodrug of paclitaxel.

365

Prodrug **32** was evaluated in vitro against breast cancer MCF-7 and U251 human glioma cells. 366 the latter cell being less sensible to paclitaxel. Interestingly, prodrug 32 was three times more 367 active than paclitaxel 31 against U251 cells when pre-incubation with PMA, the ROS inductor, 368 was applied. A non-activatable analog of micellar prodrug 32 devoid of the boron trigger was 369 also tested and showed significant cytotoxicity decreased by only a factor 5 in comparison with 370 371 free paclitaxel 31. This highlights the uncertain ability of the temporary promoiety, although very bulky, to clearly impair the paclitaxel activity. In vivo, a similar trend was observed on a 372 MCF-7 xenograft tumor model in mice. Micelles 32 displayed the best activity with almost 90% 373 374 of tumor inhibition attributable to its advantageous pharmacokinetics compared to paclitaxel 31 (~ 70% inhibition). Noticeably, the non-activatable prodrug was almost as active as 375 376 paclitaxel 31 (~ 60% inhibition).

377

378 **Precursor of nitric oxide**

In cells, nitric oxide is an endogenous signaling molecule involved in several metabolic pathways. High concentration of nitric oxide usually lead to elevated formation of cytostatic peroxinitrite (vide infra). The Chakrapani group has prepared a theranostic precursor **33** of nitric oxide based on a self-immolative coumarin core linked to a nitrosohydroxylamine (Scheme 11).[61] The release of the latter moiety will spontaneously generate two molecules of nitric oxide.



Scheme 11. Theranostic prodrug of nitric oxide.

Theranostic prodrug **33** was evaluated in vitro against MRC5 fibroblasts and three cancer cell lines: A549, HeLa, MDA-MB-231. Incubation with the cancer cells, in particular with A549, showed greater conversion of **33** into turned-on coumarin and nitric oxide using fluorescence microscopy experiment. A similar activity was observed against all three cell lines ($IC_{50} \sim 10$ μ M) and a lower effect was noted on the MRC5 cells ($IC_{50} \sim 25 \mu$ M).

393

394 Precursors of DNA alkylating agents

395 Nitrogen mustards

Nitrogen mustards are cytotoxic drugs reacting with DNA to form interstrand cross-links (ICLs).

The Peng group designed and synthesized benzene boronate prodrugs of chlormethine **34** since this drug is weakly selective of cancer cells (Scheme 12).[62]



399 400

Scheme 12. Prodrugs of chlormethine.

401

402 When linked to benzene boronate, chlormethine is not able to form the electrophilic aziridinium 403 cycle strongly reacting with DNA. In vitro, prodrug 35 showed efficient ability to alkylate DNA in presence of H₂O₂ and **35** was further evaluated against four cancer cells: leukemia cells SR, 404 405 lung cancer cells NCI-H460, renal cancer cells SN12C and CAKI-1, and healthy lymphocytes. Prodrug 35 (with no added H₂O₂) was especially active against SR and NCI-H460 cells with 406 85-90% of growth inhibition at 10 µM while no activity was detected at this concentration on 407 the normal lymphocytes. Rationally, the same activity for 35 and its corresponding free boronic 408 acid was found in vitro against all cell lines. This benzene boronate prodrug of chlormethine 409 **34** was further bonded to a polymeric assembly of poly(fluorene-co-phenylene) by Li et al.[63] 410 The polymeric prodrug **36** (Scheme 12) can be considered as theranostic since the polymer 411 backbone is fluorescent and was visualized into cells by imaging. The polymeric prodrug 36 412 was tested on HeLa and A549 cells, and globally, 36 displayed a similar level of cytotoxicy as 413 prodrug **35** (i.e 80% of growth inhibition at 10 μ M). 414

Using a closely related strategy as earlier, Peng and co-workers prepared boronate prodrugs of aromatic nitrogen mustards where the electron-withdrawing boronate function was either directly linked to the effector (**38** and **39**) or via a benzyl self-immolative spacer (**37**) (Scheme 13).[64,65]



419

420 **Scheme 13.** Structures of chlorambucil, melphalan and the prodrugs of aromatic nitrogen 421 mustard.

422

Amongst the synthesized prodrugs, prodrug 37 and 38 were the most active at forming ICLs 423 and at inhibiting the panel of 60 cancer cells from the NCI. In particular, IC₅₀s of both prodrugs 424 37 and 38 were obtained below 1 µM against SR and NCI-H460 cells. Analogs of prodrugs 38 425 426 bearing a substituent were synthesized to further optimize the antitumor activity of this 427 series.[66] Prodrug **39** displaying a cysteinyl methyl ester motif was shown to enhance the water solubility and cell permeability. Moreover, 39 was more effective in vitro against MDA-428 MB-468 than 38 and the reference drugs chlorambucil and melphalan. Prodrug 39 was 429 evaluated in vivo using MDA-MB-468 cancer xenograft in mice and displayed significantly 430 reduced tumor growth compared to the vehicle with no side effects. 431

432

433 Quinone methides as alkylating agents

The Peng group also envisioned the generation of quinone methides as Michael acceptor for DNA strand (Scheme 14).[67–69] Among several benzene boronate precursors, prodrug **41** was the most interesting of their series.



438

Scheme 14. Prodrug of quinone methide as Michael acceptor.

439

440 Prodrug **41** was able to form ICLs in presence of H_2O_2 and its cytotoxicity was evaluated 441 against the NCI cancer cells panel. IC₅₀s of **41** against several cancer cells was about 10-20 442 μ M which was significantly more active than chlorambucil and melphalan.

443

444 Precursors of ROS/RNOS amplifier/accumulator for oxidation therapy

445 Aminoferrocene

Over the last decade, the group of Mokhir has developed benzene boronate precursors of aminoferrocene.[70–79] These precursor were conceived to increase drastically ROS concentrations inside cancer cells leading ultimately to cell death, i.e oxidation therapy.[80] The released aminoferrocene **42** reacts with hydrogen peroxide or oxygen to afford both cytotoxic hydroxyl radical and ferrocenium ion **43** (Scheme 15). These ROS are usually detoxified by antioxidants such as glutathione but in this strategy, electrophilic quinone methide is also formed and acts as glutathione scavenger blocking this protective mechanism.



453

454 **Scheme 15.** Cycle for ROS amplification within tumor environment initiated by the presence 455 of free aminoferrocene.

From a first series of aminoferrocene prodrugs,[70] the authors found that the prodrug **44** (Scheme 16) was the most efficient at both penetrating and amplifying ROS within HL-60 leukemia cells. This is attributable to the greater stability of the liberated *N*benzylaminoferrocene and **44** was indeed the most cytotoxic prodrug against HL-60 (IC₅₀ = 9 μ M) whereas no activity was found against healthy fibroblasts (IC₅₀ > 100 μ M).



464

The authors further showed that the cytotoxicity was decreased when the ferrocene part was 465 partly constituted of a cyclopentadiene carboxylic acid moiety.[71] Modification of the N-benzyl 466 group by either introducing ortho- or para-substitutent or replacement of the benzene ring by 467 a pyridine nucleus was also counterproductive to the cytotoxicity on HL-60 cells.[71,72] 468 Prodrug 44 was therefore selected for in vivo studies. [72,73] First, 44 was not toxic on healthy 469 mice up to 6 mg/kg and 44 was further evaluated on L1210 leukemia xenografted mice. Six 470 471 injections per day at 26 µg/kg led to the extension of survival time (+ 30%) of the mice. The authors noted an increased oxidative stress in L1210 cancer cells recovered from treated 472 animal.[72] Prodrug 44 was also evaluated on xenografts of human prostate adenocarcinoma 473 in CBA mice in view of the high in vitro ROS production observed from prostate cancer cell 474 lines. However, this latter in vivo assay showed a modest tumor mass reduction for the cohort 475 treated with 44.[73] Prodrug 44 was however described to aggregate in aqueous solution and 476 new analogs were therefore designed in order to reduce this property. A N-propargyl prodrug 477 45 displaying lower hydrophobicity was indeed less susceptible to aggregation and was also 478 shown to display in vitro cytotoxicity similar to that of 44. Growth inhibiton of Guerin's 479 carcinoma in rat was observed when 45 was administrated intraperitoneally at a single dose 480 of 30 mg/kg seven days after tumor transplantation.[74] 481

482 Aminoferrocene theranostic prodrugs (Scheme 16) were then developed by branching 483 benzene boronate precursors of aminoferrocene to a [¹⁸F]-fluoroglucose for positron emission 484 tomography (PET).[75] Theranostic prodrug **46** had an in vitro cytotoxicity close to that of the 485 reference prodrug **44** (e.g. against HL-60, IC₅₀(**46**) = 26 μ M compared to IC₅₀(**44**) ~ 10 μ M). 486 The corresponding free boronic acid of **46** was injected in mice bearing two tumors: PC3 (human prostate cancer) and AR42J (rat pancreatic cancer). PET analysis showed a moderate
 localization of the tracer in both tumors but the measured radioactivity remain relatively stable
 in the tumors for 60 minutes in comparison with the healthy organs of the mice.

An organic moiety able to target the lysosome was alternatively added on the benzene 490 boronate precursors of aminoferrocene.[76] The piperidine prodrug 47 (Scheme 16) was 491 prepared in order to obtain an ammonium form at physiological pH leading to lysosome 492 trapping and accumulation. Biophysical properties of 47 were compared to the reference 493 494 prodrug 44 and were shown significantly improved. In particular, the hydroxyl radical formation was more efficient from prodrug 47 and this was transcribed with the higher in vitro cytotoxicity 495 496 observed for 47 than for 44 against several cancer cell lines (6 to 8 folds more active). The ability of prodrug 47 to disrupt lysosomal function was confirmed by a fluorescence imaging 497 experiment. Prodrug 47 was evaluated in Nemeth-Kellner lymphoma xenograft mice model by 498 intraperitoneal injection of eight doses of 40 mg/kg every two days for 15 days. The tumor 499 weight of treated animals was reduced in comparison with the untreated cohort but the results 500 were very contrasted. 501

- 502 These aminoferrocene precursors were further complexified by the increment of a platinum-
- 503 based antineoplastic prodrug moiety (48, 51 and 52) (Scheme 16 and 17).[77–79]



504 505

Scheme 17. Bis "aminoferrocene-platinum" prodrugs.

506

The bis "aminoferrocene-cisplatin" prodrug **51** was shown to effectively release cisplatin **49** after addition of H_2O_2 , indeed, the free aminoferrocenes generated are able to transfer one electron that both reduces the metal complex into cisplatin and forms the activated ferrocenium. **51** was evaluated against normal fibroblasts HDFa, ovarian carcinoma cell line A2780 and the cisplatin resistant counterpart A2780cis cell line. Prodrug **51** was not toxic

against the healthy fibroblasts while activity of free cisplatin 49 was fully recovered when A2780 512 cells were treated with 51 (IC₅₀ ~ 2 μ M). Interestingly, the resistant A2780cis cells behaved 513 differently: activity of prodrug **51** (IC₅₀ = 6 μ M) was twice greater than cisplatin **49** (IC₅₀ = 13 514 μ M). The authors revealed that prodrug **51** was not generating an aminoferrocene which 515 strongly produces ROS but the activity of prodrug 51 was mostly due to the release of cisplatin 516 50 rather than the generally modest activity provided by ferrocenium. The oxaliplatin prodrug 517 52 was built with the same scaffold used for cisplatin prodrug 51 (Scheme 17).[78] In construct 518 519 **52**, the spacer between the ferrocene and the platinum-based drug was truncated (C_4 in lieu of C_5) in order to facilitate the intramolecular electron transfer within these two moieties. 520 Prodrug 52 was indeed more active than 51 against both ovarian cancer cell lines in vitro : IC₅₀ 521 522 $(A2780) = 0.4 \mu M$ and $IC_{50} (A2780 cis) = 0.7 \mu M$. Analog 52 followed the trend described for prodrug 51 in view of the stronger activity (over free cisplatin 49) displayed by the free drug 523 oxaliplatin 50 : IC₅₀ (A2780) = 0.9 μ M and IC₅₀ (A2780cis) = 3 μ M. The authors further 524 synthesized a mono-"carboplatin-aminoferrocene" prodrug 48 (Scheme 16).[79] Accumulation 525 of 48 in the mitochondria of A2780 cancer cells was demonstrated using the mitochondrial 526 tracker rhodamine R123 and it was assumed that this uptake was due to the release of a 527 delocalized lipophilic cation: the generated ferrocenium. In vitro activity of 48 was then 528 determined against the three aforementioned cell lines and adopted the tendency observed 529 530 for cisplatin prodrug 51 but to a weaker extent.

531

532 Diethyldithiocarbamate 54

533 Diethyldithiocarbamate **54** is a metabolite of disulfiram **56**, a drug used in clinic to treat chronic 534 alcoholism and recently, copper complex of diethyldithiocarbamate **53** was shown to have 535 anticancer activity.[81] The formation of this complex **53** generates ROS in the cancer cells 536 and the Pu group prepared a prodrug **55** capitalizing on the ROS amplification due to both 537 formation of the latter complex and a quinone methide (Scheme 18).[82]



538 539

Scheme 18. Structures of disulfiram and the prodrug of diethyldithiocarbamate.

540

Prodrug 55 was tested against 4T1 breast cancer cells in vitro : In the presence of the nontoxic 541 concentration of copper (1 μ M), activity was six times more potent on cancer cells (IC₅₀ = 1 542 μ M) than on normal fibroblasts NIH3T3 (IC₅₀ = 6 μ M). This difference of activity could be 543 explained by the high ROS production of 4T1 which was essentially due to the 544 diethyldithiocarbamate copper complex formation and minimally as a result of quinone methide 545 546 generation. In vivo testing was made on a 4T1 xenograft mice and the most potent result was obtained using a co-injection of copper gluconate at 1.5 mg/kg with 55 at 37 mg/kg. Applying 547 this protocol, a decrease of 80% of the tumors volume was observed in comparison to the 548 inactive vehicle or copper gluconate alone. 549

551 Cinnamaldehyde 57

552 Cinnamaldehyde **57** is a natural product found in cinnamon essential oil and used as food 553 flavoring. This aldehyde was shown to amplify ROS in cancer cells but this action is very limited 554 on healthy cells. Poor bioavailability of cinnamaldehyde **57** has prevented its application in 555 clinic and therefore this compound was a good candidate for prodrug development. Thus, the 556 Lee group has prepared a benzene boronate prodrug of cinnamaldehyde **58** (Scheme 19).[83]



557

Scheme 19. Prodrug of cinnamaldehyde.

- 558
- 559

Under oxidative conditions, this prodrug 58 will generate a guinone methide able to covalently 560 trap antioxidants leading to ROS accumulation in cells. Moreover, a molecule of 561 cinnamaldehyde 57 will be released under acidic conditions found in cancer cells and then 562 enhanced the already high level of ROS. The authors first evaluated the ability of 58 to lower 563 the glutathione level in three cell lines: prostate cancer DU145, colon cancer SW620 and 564 fibroblasts NIH3T3. Only the DU145 cells were responsive to 58 and presented a reduction of 565 566 around 50% of intracellular glutathione concentration. Cytotoxicity of prodrug 58 was weak against the three cell lines and DU145 cells were more affected (IC₅₀ = 48 μ M) than the NIH3T3 567 fibroblasts (IC₅₀ = 182 μ M). A tumor xenograft mouse model of DU145 cells was used to 568 569 evaluate the in vivo antitumor effect of 58 and campthotecin 21 as reference drug. Seven injections every 3 days of either 58 or campthotecin 21 at 2 mg/kg showed the same tumor 570 volume reduction (~ 75 %). Prodrug 58 was more active than control compound 571 cinnamaldehyde 57 or a quinone methide generator alone. 572

573

574 Glucose oxidase

575 The glucose oxidase enzyme catalyze the reaction of glucose and oxygen into gluconolactone

and hydrogen peroxide. This enzyme can therefore generate ROS from two compounds

577 naturally abundant in cells. To capitalize on this, Li et al.[84] have prepared nanocapsules **59**

able to entrap glucose oxidase (Scheme 20).



580 **Scheme 20.** Nanocapsules loaded with glucose oxidase for the amplification of ROS within 581 the tumor microenvironment.

582

583 The shell of the capsule was made of a diblock copolymer of PEG and polymethacrylate grafted with benzene boronate and piperidine moieties. Protonation of piperidine in the acidic 584 585 tumor environment increases the permeability of the nanocapsule and allows the entry of glucose which lead to the strong production of H_2O_2 . This enhanced level of hydrogen peroxide 586 further reinforces the oxidation of the benzene boronate part into glutathione scavenger 587 588 quinone methide. The authors verified that this dual acting nanoconstruct was operational in vitro by measuring H₂O₂ production and guinone methide formation. Mice bearing lung 589 carcinoma A549 were treated with nanocapsule 59 and showed complete inhibition of tumor 590 591 growth in comparison with either glucose oxidase or empty nanocapsule alone.

592

3. Pharmacological relevance

594

595 In this section, the strategy of boron-containing prodrugs responsive to oxidative stress is 596 discussed in regards to its potential to reach the market as effective cancer treatment. Indeed, 597 boronic acid/boronate prodrug have been largely evaluated in animal models but no clinical 598 trials have been started with any of these molecules so far.

599 Nonetheless, the potential of these constructs is strong considering that several drugs containing a boronic acid function, are already on the market.[28,85] Moreover, the 600 development of boron-containing classical drug remains a dynamic area of research.[86] In 601 602 terms of drug delivery, the boronic acid function is particularly relevant since it allows facilitated internalization in cancer cells.[87.88] The reversible formation of ester bonds between boronic 603 acid and the diol of saccharides ensure this membrane crossing. Precisely, high affinity 604 between boronic acids and the glycocalix of cancer cells lead to the selective uptake of the 605 molecules bearing this moiety. 606

607 Furthermore, to improve the strategy of the small-molecule prodrugs, the kinetic of prodrug 608 conversion must be considered. At the tumor site, activation of boron-containing prodrugs by ROS can either occur extra- or intracellularly. As the system is not closed, the liberated drug 609 will then freely diffuse around the tumor (~10⁻³ mm³; a mass of around 1,000 cancer cells) and 610 that will influence the concentration profile of the drug. Scission of the prodrugs should arise 611 locally to preserve an efficient dose of the liberated drugs within the tumor. In view of the 612 diffusion coefficient of small molecules (10⁻¹⁰ m².s⁻¹) and considering the aforementioned tumor 613 volume, oxidation of precursors into drugs should last approximately 2 minutes in order to 614 maintain the concentration of the free drugs equal to that of the corresponding prodrugs. When 615 the prodrug conversion implies an additional self-immolative step, the complete process must 616 not exceed the latter duration. 617

The reaction of boron-containing prodrug with the ROS species is bimolecular and the rate will therefore depend on the concentration of both reactants: v = k[prodrug][ROS]. The concentration of the prodrug is mostly guided by the dose injected to the biologic system but levels of peroxinitrite and hydrogen peroxide is dictated by the living organism. Specific activation in the tumor microenvironment can occur since the concentrations of peroxinitrite and hydrogen peroxide are strongly increased in comparison with healthy tissues. Cellular concentration of peroxinitrite can reach 50-100 μ M in pathological conditions whereas a basal

concentration of 0.1-1 µM was estimated in healthy cells.[89,90] Physiological hydrogen 625 peroxide is produced at a steady-state concentration of 0.1-1 µM which rises to 10-100 µM in 626 malignant organs.[91,92] 627

628 In this activation strategy, two parameters must be taken into account: the half-life of each 629 ROS in vivo and the rate constant associated to a ROS and a particular prodrug structure.

As mentioned earlier, at physiological pH, oxidation of the carbon-boron bond by peroxinitrite 630 is 10⁶ faster than that obtained with hydrogen peroxide: e.g. conversion of phenylboronic acid 631 to phenol occurred with rate constant of $1 \times 10^6 \text{ M}^{-1} \cdot \text{s}^{-1}$ with peroxinitrite and approximatively 632 1-2 M^{-1} .s⁻¹ with hydrogen peroxide.²⁵ In vivo, peroxinitrite has a half-life of ~ 10 ms and reacts 633 preponderantly but reversibly with carbon dioxide (1-2 mM) to form nitrosoperoxocarbonate 634 anion (ONOOCO₂⁻) at a rate constant of 0.5 x 10⁵ M⁻¹.s⁻¹. As opposed to hypochlorite anion 635 which react faster with biomolecules than boronate/boronic acid in vivo, peroxinitrite is able to 636 oxidize the carbon-boron bond due to the rapid kinetic of this reaction over the addition of 637 carbon dioxide. 638

639 In biological systems, hydrogen peroxide also reacts with biomolecules such as amino acids and metals (free or inside metallo-enzymes). Consequently, its half-life in cells is ~ 1 ms. The 640 reaction with the thiol group of cysteine residues was described as the fastest physiological 641 transformation of hydrogen peroxide with a rate constant up to 10⁶ M⁻¹.s⁻¹.[93,94] 642

Given the differences of reactivity of both involved oxidative species, peroxynitrite is likely to 643 be the main actor for the conversion of these prodrugs into the corresponding free drugs. In 644 645 view of the short half-life of oxidative species, increasing the rate constant of this oxidation reaction should result to a greater number of available peroxynitrite molecules that can react 646 with the boronic acid prodrug. This would lead to a better yield of prodrug transformation at the 647 tumor site and then improve the chance of treatment efficacy. Notably, the structure of the 648 prodrug will also greatly affect the kinetic of oxidation in regards of the ROS involved in the 649 reaction. The possibility of modulating the prodrug scaffold in favor of a faster reactivity toward 650 ROS is crucial and can be operated by medicinal chemists. 651

652 In term of structure-kinetic studies of boronic acids conversion into alcohols, we noted that aliphatic boronic acids are 10 times slower than benzene boronic acids (Scheme 21).[25] 653



- 654
- 655

Scheme 21. Relative rate of C-B bonds oxidation of alkyl, benzyl and vinyl boronic acid derivatives. 656

657

The oxidation kinetic of benzene boronic acids is dependent of the substitutions of the aromatic 658 nucleus.[24,30] Adding a strongly electron-withdrawing substituent such as a nitro group at the 659 para position of the ring increased the oxidation rate by 20-fold whereas an electron-donating 660 methoxy group at the same position divided this rate by a factor of three. Although electron-661 withdrawing group substitution of the benzenic ring lead to a faster formation of the quinone 662

663 methide intermediate, this latter modification also cause a dramatic reduction of the kinetic of 664 the following self-immolation step.[32] Therefore, no substitution of benzene boronate nucleus 665 as self-immolative promoiety can be envisioned to increase the global rate of the 666 oxidation/disassembly steps of such constructs.

667 The vinyl boronic acid group was also shown to release an effector through oxidation and 668 subsquent self-immolation process.[30,31,95] The oxidation of the vinyl boronic acid motif was 20 times more rapid than that of the equivalent unsubstituted benzene boronic acid group.[30] 669 This difference of reactivity could be attributed to a faster self-immolation step since the π 670 671 electrons of the double bond are not delocalized within a benzene nucleus and therefore available for the elimination reaction. Moreover, the empty p-orbital of the boron in vinyl boronic 672 acid motif is less hindered than in the benzenic equivalent leading to an easiest access of the 673 674 nucleophilic oxidative species. Eventually, this motif could be further engineered to potentially 675 increase the global rate of effector release.

With the condition that an average drug concentration of 10 µM is required within the tumor of 676 677 around 10⁻³ mm³, the rate of the reaction (v = k[prodrug][ROS]) should not fall belowc 10 μ M per 2 minutes which is about 0.1 µM.s⁻¹ (total conversion inside the tumor). Given the 678 concentration of peroxinitrite (~ 10 µM; the most reactive ROS) in cancer cells, only prodrugs 679 680 oxidized at rate constant (k) higher than $10^3 \,\mathrm{M}^{-1}$.s⁻¹ would be effective. Nonetheless, due to the short half-life of peroxinitrite (~10 ms), we estimate that the reaction of the latter oxidant with 681 a particular boronic acid prodrug should react at a rate constant superior to 10⁷ M⁻¹.s⁻¹ in order 682 to afford 10 µM of drug localized at the tumor site. In light of this short physiological half-life, 683 targeting mitochondria is a relevant strategy in order to efficiently reach the cellular ROS. Such 684 vectorized prodrug containing a delocalized lipophilic cation was already developed by the 685 686 Mokhir group.[79]

687 In regards of the aforementioned boronic acid promoieties, we noticed that the quinone methide species generated from benzene boronates were not strongly cytotoxic but very 688 689 efficient at scavenging antioxidants.[44,70,83,84] Remarkably, it was occasionally reported that the boronic promoiety was not completely masking the pharmacological activity of the 690 branched drug.^{45,60} This suggests that the attachment of a benzene boronic acid promoiety to 691 a drug do not provoke the automatic discontinuation of the bioactivity. Furthermore, the 692 nominal boronic acid function is often used in this reviewed prodrug strategy and it was recently 693 proposed that the latter function could be used as a bioisoster of a hydroxyl group. Some 694 successful drug analogs were indeed developed by the Wang group[96-98] that formerly 695 developed boronic acid-containing prodrugs (vide supra). 696

697 The same group showed that boronic acid prodrug were also activated by the cytochromes P450.[42] Thus, the benzene boronic promoiety could even be employed for the development 698 of several types of prodrug allowing the prolonged release of any drug for the treatment of any 699 700 disease.[99] Consequently, this activation could compete with the expected oxidation by the ROS of cancer-targeting boronic acid prodrugs within the tumor microenvironment. It is 701 important to note, however, that unlike a direct chemical reaction between an oxidant and a 702 703 boronic acid molecule, the reaction of the latter function with the cytochromes P450 is an enzymatic reaction. This implies the entrance of the prodrug into the active site before oxidation 704 of the C-B bond. In order to develop boronic acid prodrugs specifically targeting tumors, their 705 oxidation by cytochromes P450 should be evaluated. In case of unwanted interaction, 706 modulation of the structural core of the boronic acid promoiety should be therefore considered 707 708 to impede the prodrug access to the catalytic sites of the cytochromes P450.

710 **4. Conclusion**

711

This review reports on the different small-molecule, polymeric and nanoparticle-based 712 713 prodrugs activated through oxidation of intrinsic carbon-boron bonds by ROS from tumor environment. The literature reveals several constructs with interesting activity and until now, 714 none of these prodrugs have entered into clinical trial. In view of the in vivo data, this prodrug 715 716 strategy is promising for the treatment of several tumors such as leukemia, breast and pancreatic cancers which produce high concentrations of ROS. Chemical system leading to 717 both ROS amplification and anticancer agent delivery were particularly effective. In order to 718 obtain a ROS-activated boronic acid prodrug with a great therapeutic potential, it would be 719 720 beneficial to develop a structure which could both intensify the ROS level within cancer cells 721 and ensure rapid release of a drug by virtue of a rapid C-B oxidation.

722

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