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# 1           **Pharmacological characterization of the 3D MucilAir™ nasal model**

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31 **Abstract**

32           The preclinical evaluation of nasally administered drug candidates requires screening  
33 studies based on *in vitro* models of the nasal mucosa. The aim of this study was to evaluate  
34 the morpho-functional characteristics of the 3D MucilAir™ nasal model with a  
35 pharmacological focus on [ATP]-binding cassette (ABC) efflux transporters. We initially  
36 performed a phenotypic characterization of the MucilAir™ model and assessed its barrier  
37 properties by immunofluorescence (IF), protein mass spectrometry and examination of  
38 histological sections. We then focused on the functional expression of the ABC transporters  
39 P-glycoprotein (P-gp), multidrug resistance associated protein (MRP)1, MRP2 and breast  
40 cancer resistance protein (BCRP) in bidirectional transport experiments. The MucilAir™  
41 model comprises a tight, polarized, pseudo-stratified nasal epithelium composed of fully  
42 differentiated ciliated, goblet and basal cells. These ABC transporters were all expressed by  
43 the cell membranes. P-gp and BCRP were both functional and capable of actively effluxing  
44 substrates. The MucilAir™ model could consequently represent a potent tool for evaluating  
45 the interaction of nasally administered drugs with ABC transporters.

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56 **Keywords:** MucilAir™, *in vitro* model, nasal barrier, drug delivery, ABC transporters,  
57 bidirectional transport

## 58 **Introduction**

59 Nasal delivery represents a highly effective route of administration for drugs requiring a  
60 quick onset of action. Nasal drug delivery offers several advantages over systemic  
61 administration, including reduced side-effects, avoidance of hepatic first-pass metabolism and  
62 rapid local absorption of drugs owing to the abundant vascularization and high permeability  
63 of the sizeable nasal mucosa [1].

64 The introduction of intranasal drug candidates requires the development of pre-clinical  
65 screening experiments to evaluate their permeability through the nasal mucosa [2]. Currently,  
66 Caco-2 intestinal cell line is the only FDA-approved predictive *in vitro* model to evaluate the  
67 absorption of drugs [3]. Considering the morphological and physiological differences with the  
68 nasal barrier, new models of nasal mucosa must be developed and characterized to evaluate  
69 the absorption of nasal drugs. In this context, several *in vitro* cellular models have been  
70 developed with the aim of closely mimicking the biology of the nasal barrier. The use of  
71 immortalized nasal cell lines, such as the bovine turbinate (BT) [4], rat nasal squamous  
72 carcinoma (NAS 2BL) [5] and human nasal squamous carcinoma RPMI 2650 cell lines [6, 7]  
73 represents a widespread approach. Despite some advantages, including high proliferation  
74 capacity and genetic homogeneity, immortalized cell lines are far from the human nasal  
75 epithelium in terms of biophysiology due to their weak differentiation ability [8]. To  
76 overcome these limitations, various *in vitro* models have evolved over the years, becoming  
77 increasingly complex and developing from submerged monocultures to three-dimensional  
78 epithelia cultured at the air-liquid interface. These latest models, available under the brand  
79 names EpiAirway™ (MatTek Corporation) and MucilAir™ (Epithelix), are constituted from  
80 primary human epithelial cells freshly isolated from nasal or bronchial biopsies [9]. These  
81 models accurately reproduce the biophysiology of human airway epithelia including the  
82 presence of a functional mucociliary system and the secretion of mucus in a homeostatic state  
83 [10].

84 Nasally administered drugs permeate through the nasal epithelium principally via the  
85 transcellular route [11]. This route implicates transport of the drug substances across the  
86 lipophilic cell barrier which may involve specific interactions with ATP binding cassette  
87 (ABC) drug transporters [12]. These ATP-dependent active proteins participate in the efflux  
88 of xenobiotics from the cells [13], thereby greatly limiting the bioavailability of drugs  
89 intended for systemic circulation [14]. Functional expression of the main ABC transporters,

90 namely P-glycoprotein (P-gp), Multidrug Resistance associated Proteins (MRPs) and Breast  
91 Cancer Resistance Protein (BCRP) has already been widely demonstrated in several  
92 physiological barriers, including the blood-brain-barrier [15] and the intestinal barrier [16].  
93 The sparse data available concerning the human nasal epithelium reveal the expression of a  
94 wide range of ABC transporters [17, 18]. Identification of these transporters in *in vitro* models  
95 of the nasal epithelium is therefore essential in order to anticipate their involvement in the  
96 bioavailability of locally administered drugs [19].

97 In addition to the functional expression of ABC transporters, *in vitro* models must,  
98 regardless of their origin, exhibit critical barrier properties that should be carefully  
99 investigated to determine their relevance for drug transport studies. These properties include  
100 the establishment of an adequate transepithelial electrical resistance (TEER) and the  
101 expression of tight and adherens junction proteins limiting the paracellular permeability of  
102 hydrophilic compounds [6]. We recently demonstrated that the RPMI 2650 model is not  
103 suitable for evaluating the efflux of therapeutic compounds mediated by ABC transporters  
104 [20]. ~~Although the EpiAirway™ and MucilAir™ models have been used to investigate the~~  
105 ~~toxicity of inhaled compounds [21] and virus interactions [22]~~ Although the MucilAir™  
106 model have been used to investigate the inflammatory response to aerosolized pollen [21] or  
107 the protective properties of xyloglucan [22], to the best of our knowledge few data are  
108 available concerning its barrier properties for drug absorption and both the expression and  
109 functionality of ABC efflux transporters are still unknown. This study therefore focuses on  
110 the original pharmacological characterization of the MucilAir™ nasal model in terms of  
111 barrier properties extended to the functional expression of ABC efflux transporters.

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## 122 **Material and methods**

### 123 **Culture of MucilAir™ tissues**

124 The MucilAir™ nasal tissues were purchased from Epithelix (Geneva, Switzerland)  
125 and originated from a mixture of human nasal cells brushed from a pool of samples from 14  
126 healthy donors grown on 6.5 mm Transwell® Polyester membrane with 0.4 µm pore size  
127 (Costar 3470, Corning, New-York, USA). In our study, the MucilAir™ tissues were  
128 transferred on receipt into 24-well plates filled with 700 µL of pre-warmed MucilAir™  
129 (Epithelix) culture medium. The tissues were routinely cultured at 37°C in a saturated (>  
130 99%) humidity environment containing 5% CO<sub>2</sub>. The medium was renewed every two to  
131 three days. The transepithelial electrical resistance (TEER) was measured as a standard  
132 indicator of tissue integrity. Measurements were made every two days using an EVOM®  
133 resistance meter and STX 2 electrodes (World Precision Instruments, Sarasota, USA). Blank  
134 filter values were subtracted, and the corrected values were calculated according to the  
135 surface area of the inserts (0.33 cm<sup>2</sup>).

136

### 137 **Culture of Caco-2 cells**

138 Caco-2 cells were purchased from the American Type Culture Collection (Rockville,  
139 MD, USA) and used as a pharmacological control model for protein mass spectrometry  
140 experiments. Caco-2 cells were grown in 25 cm<sup>2</sup> flasks until passage 23 to 30. The cells were  
141 maintained in culture medium consisting of Dulbecco's modified Eagle medium (DMEM)  
142 supplemented with 10% fetal bovine serum (FBS), 1% non-essential amino acids, 100 U/mL  
143 penicillin G, 250 ng/mL amphotericin B and 100 µg/mL streptomycin in a 37°C, 95% relative  
144 humidity and 5% CO<sub>2</sub> atmosphere. Cells were seeded onto the membrane of the insert filters  
145 (Falcon®, translucent polyethylene terephthalate (PET) membrane, 0.4 µm pore size, high-  
146 density, with a surface area of 0.3 cm<sup>2</sup>) in 24-well companion plates (Dominique Dutscher,  
147 Strasbourg, France) at a density of 1 x 10<sup>4</sup> cells/well and cultured for 21 days. The culture  
148 medium was changed every 2–3 days.

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152 **Histological examination of MucilAir™ tissues**

153 The study of MucilAir™ tissues focused on their morphological characteristics and  
154 cell composition. For this purpose, freshly excised inserts were bisected to allow histological  
155 staining of paraffin-embedded sections. Fully differentiated tissue cultures were rinsed in  
156 phosphate-buffered saline (PBS) and fixed by **complete** immersion in 4% formaldehyde for  
157 20 min **at room temperature**. Fixed tissues were embedded in paraffin, sectioned and  
158 processed for staining with hematoxylin-eosin (HE) and alcian blue. **Alcian blue staining was**  
159 **performed during 30 min at room temperature with 1% alcian blue in 3% acid acetic at pH**  
160 **2.5**. Several sections were cut from paraffin blocks using a microtome (Leica Jung RM2035).  
161 The sections were then deposited on glass slides, observed by light microscopy (Microscope  
162 Leica DMRB) and digitalized with a Nanozoomer (Hamamatsu Photonics).

163

164 **MucilAir™ flow cytometric phenotypic analysis**

165 MucilAir™ tissues were dissociated **by incubating trypsin on both side of the inserts**  
166 **during 20 mins at room temperature** to obtain a cellular suspension, 100,000 cells being used  
167 for each staining procedure. The cell population was labelled with a specific anti-CLCA1.PE-  
168 Cyn5.5 polyclonal goat antibody (AC21-1575-16, Abcore) for goblet cells or with anti-β-  
169 tubulin.PE mouse monoclonal antibody (sc-5274.PE, Santa Cruz) for ciliated cells. Aliquots  
170 of 50,000 cells were analysed by flow cytometry. Sequential gating was performed. The  
171 FSC/SSC cytogram was used first to select ~~intact~~ **viable** cells, and second to distinguish  
172 specific cell populations. The gain setting was established by running unstained and isotype  
173 control cells (normal mouse IgG1.PE, sc-2866, Santa Cruz Biotechnology, and Lightning-link  
174 PE-Cyn5.5 tandem conjugation kit to goat IgG isotype control antibody, Innova Biosciences).  
175 Compensations were calculated by acquisition of fluorescent beads. Both percentage and  
176 geometric means of fluorescence were recorded. The results were expressed as the percentage  
177 of labelled positive cells. A FACS DiVa flow cytometer (BD Biosciences) equipped with an  
178 argon ion and He-Ne lasers was used. Data were analyzed using DiVa 5.03 software.

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## 182 **Immunofluorescence**

183 In this study, we used an IF technique applicable to flat-mounted human tissue initially  
184 developed for the study of endothelial and epithelial tissues [23, 24]. Briefly, MucilAir™  
185 inserts were fixed in pure methanol or 1% paraformaldehyde (PFA) **added on both sides** for  
186 30 min at room temperature (RT). PFA-fixed tissues were permeabilized with 1% Triton X-  
187 100 for 15 min at RT. ~~Tissues were rehydrated three times for 5 min in PBS at room~~  
188 ~~temperature (RT) for methanol-fixed inserts~~ **while methanol-fixed inserts were rehydrated**  
189 **three times for 5 min in PBS at room temperature.** Non-specific binding sites were then  
190 blocked for 1 h at 37°C in PBS containing 2% heat-inactivated goat serum and 2% bovine  
191 serum albumin. Following this blocking step, the inserts were cut into eight pie-shaped  
192 wedges and placed in 24-well plates. The primary antibodies (Table 1) were diluted 1/200 in  
193 the blocking buffer and incubated either for 1 h at 37 °C or overnight at 4°C. Nonspecific  
194 rabbit and mouse IgG were used as primary antibodies for the negative controls. The  
195 secondary antibodies were diluted 1/500 in the blocking buffer and incubated with the insert  
196 fragments for 45 min at 37 °C. These antibodies comprised Alexa Fluor 488 goat anti-mouse  
197 IgG2b (A-21141, Thermo Fischer Scientific [TFS]), Alexa Fluor 488 goat anti-mouse (A-  
198 11029, TFS), Alexa Fluor 555 goat anti-mouse 555 IgG1 (A-21127, TFS) or Alexa Fluor 555  
199 goat anti-rabbit (A-21429, TFS). The nuclei were finally counterstained with 0.1 µg/mL 4',6-  
200 diamidino-2-phenylindole (DAPI) in PBS at RT for 30 min. The samples were rinsed three  
201 times in PBS between all steps, except between the blocking step and incubation with the  
202 primary antibodies. The insert fragments were finally placed on glass slides, submerged in  
203 Vectashield Mounting Medium (H-1000, Vector Laboratories) and covered with glass  
204 coverslips. Evaluations of each marker were repeated at least twice. All biomarkers were  
205 imaged using an inverted epifluorescence microscope IX81 (Olympus, Tokyo, Japan)  
206 equipped with CellSens imaging software (Olympus, Munster, Germany). To highlight the  
207 spatial localization of tight cell junctions and ABC transporters in MucilAir™ tissue, a  
208 FLUOVIEW FV1200 laser scanning confocal microscope (Olympus, Tokyo, Japan) equipped  
209 with FV10-ASW4.1 imaging software was used.

210

## 211 **Paracellular permeability**

212 The paracellular permeability of MucilAir™ model was assessed using the hydrophilic  
213 compounds sodium fluorescein (**NaFlu**) and 4.4 kDa fluorescein isothiocyanate-dextran

214 (FITC-Dextran). The compounds were dissolved in Hank's balanced salt solution (HBSS)  
215 containing 1% HEPES (v/v) to a final concentration of 10 µg/mL and filled into the apical  
216 donor compartments, while HBSS containing 1% HEPES (v/v) alone was introduced into the  
217 basal receiver compartments. The inserts were then incubated for 2 h at 37°C and the amount  
218 of the fluorescent marker compound reaching the basal compartment was evaluated using a  
219 fluorometer (Fluoroskan Ascent™, Thermo Fisher Scientific) with wavelengths set at 485/535  
220 nm. The apparent permeability ( $P_{app}$ ) was calculated according to the equation:

$$221 \quad P_{app} = \frac{V}{C_i \times A} \times \frac{C_f}{\Delta t} \quad \text{Equation 1.}$$

222 where V is the volume of the acceptor compartment (in cm<sup>3</sup>), C<sub>i</sub> is the initial concentration of  
223 the test compound (in g/L or mol/L), A is the area of the insert (in cm<sup>2</sup>), C<sub>f</sub> is the final  
224 concentration of the compound in the acceptor compartment (in g/L or mol/L), and t is the  
225 duration of the experiment (in seconds).

226

### 227 **Bidirectional transport studies**

228 We investigated the involvement of P-gp, BCRP and MRP1-2 in the active efflux of  
229 known substrates in MucilAir™ tissues using bidirectional transport experiments. Only  
230 inserts displaying a TEER above 200 Ω.cm<sup>2</sup> were used. Rhodamine 123 (20 µM) was  
231 assessed as a P-gp substrate using verapamil (100 µM) as inhibitor. Chlorothiazide (100 µM)  
232 was assessed as a BCRP substrate using Ko143 (10 µM) as inhibitor. Methotrexate (100 µM)  
233 and probenecid (100 µM) were used as a broad-spectrum substrate and an inhibitor of MRPs,  
234 respectively.

235 All compounds were diluted either alone or with the associated inhibitor in HBSS  
236 transport buffer supplemented with 1% HEPES (v/v) and 1% DMSO (v/v). Prior to  
237 incubation, all solutions were pre-warmed to 37°C and the pH was adjusted to 7.4. Each  
238 condition was evaluated in triplicate. Bidirectional transport assays were performed from the  
239 apical to the basal compartment ( $P_{app\ A \rightarrow B}$ ) and from the basal to the apical compartment ( $P_{app\ B \rightarrow A}$ )  
240 for 2 h at 37 °C. Following incubation, the amounts of chlorothiazide and methotrexate  
241 that had permeated through the model in both compartments were quantified by liquid  
242 chromatography-mass spectrometry (LC-MS). Permeation of rhodamine 123 was quantified  
243 using a fluorometer at 485/535 nm. The bidirectional permeability was calculated according

244 to **equation 1**. Finally, to determine whether the test compound was actively effluxed by ABC  
245 transporters, its efflux ratio (ER) was computed using the equation:

246

$$247 \quad ER = \frac{P_{app}^{B \rightarrow A}}{P_{app}^{A \rightarrow B}} \text{ Equation 2.}$$

## 248 LC-MS analysis

249 Chlorothiazide and methotrexate were quantified using an Aquity UPLC system  
250 coupled with a Xevo TQ-D triple quadrupole mass spectrometer (Waters, Saint-Quentin-en-  
251 Yvelines, France). Compounds were detected by Multiple Reaction Monitoring (MRM).  
252 Negative ionization conditions were used for chlorothiazide ( $m/z$  293.98  $\rightarrow$  214.16) and  
253 positive ionization conditions for methotrexate ( $m/z$  455.19  $\rightarrow$  175.11). The internal standards  
254 (IS) were [ $^2\text{H}_6$ ]-salicylic acid (141.14  $\rightarrow$  97.10) and [ $^2\text{H}_3$ ]-methotrexate (458.25  $\rightarrow$  311.2) for  
255 chlorothiazide and methotrexate, respectively. The mobile phase was a mixture of (A) 0.1%  
256 formic acid in water and (B) 0.1% formic acid in acetonitrile. A gradient was applied to a  
257 BEH C18 column (50 mm  $\times$  2.1 mm  $\times$  1.7  $\mu\text{m}$ ) (Waters). The peak area ratios of the drugs  
258 and their respective IS were used to calculate drug concentrations.

259

## 260 Protein mass spectrometry

261 Protein mass spectrometry experiments were performed to investigate the relative  
262 abundance of phenotypic markers of nasal mucosa, tight junction proteins and ABC drug  
263 transporters in the nasal MucilAir<sup>TM</sup> model. The FDA-approved Caco-2 cell line was used as  
264 a pharmacological control as the only existing predictive *in vitro* model of intestinal drug  
265 absorption [3]. Briefly, cells were recovered from the insert filters by trypsinization and  
266 collected by centrifugation at 300 g for 5 min. The membrane protein fraction was extracted  
267 using the Mem-PER Plus membrane protein extraction kit (Thermo Fisher Scientific,  
268 Waltham, Massachusetts, USA) according to the manufacturer's protocol. Briefly, cell pellets  
269 were washed in the cell wash solution and re-suspended in the permeabilization buffer. After  
270 a 10 min incubation at 4°C with constant mixing, the cell lysates were centrifuged for 15 min  
271 at 16,000 g. The supernatant containing cytosolic proteins was removed and the pellets were  
272 re-suspended in the solubilization buffer. The homogenate was incubated for 30 min at 4°C  
273 with constant mixing and then centrifuged for 15 min at 16,000 g. The supernatant containing  
274 the membrane protein fraction was collected. Protein concentration was measured using the

275 Micro BCA protein assay kit (Thermo Fisher Scientific). The Pierce Mass Spec sample prep  
276 kit (Thermo Fisher Scientific) was used for in-solution tryptic digestion. Briefly, 100 µg of  
277 the membrane protein fraction were prepared in 100 µL of cell lysis buffer. The mixture was  
278 reduced with 10 mM dithiothreitol (DTT) for 45 min at 50°C and alkylated with 50 mM  
279 iodoacetamide (IAA) for 20 min at RT. The proteins were precipitated with acetone and then  
280 re-suspended in 100 µL of digestion buffer. The samples were digested with Lys-C (1:100) at  
281 37°C for 2 h then with trypsin (1:50) for 16 h at 37°C. Each sample was desalted using the  
282 Pierce Peptide desalting spin column according to the manufacturer's protocol.

283 The samples were analyzed using an Ultimate U3000 liquid chromatography (Thermo)  
284 system (at a flow rate of 300 nL/min) on an Easy-spray C18 column 2 µm, 0.075 mm ID x  
285 500 mm (Thermo Fisher Scientific) with a 150 min gradient. Mobile phase A was water with  
286 0.1% formic acid, and mobile phase B was 80% acetonitrile with 0.08% formic acid. Peptides  
287 were eluted by a gradient from 2.5% to 40% B over 123 min, followed by a short wash in  
288 90% mobile phase B before return to the starting conditions.

289 Mass spectrometry (MS) was performed using a Q-Exactive Plus spectrometer  
290 (ThermoFisher, San Jose, California, USA). After measurement of a precursor scan of intact  
291 peptides in the Orbitrap by scanning from m/z 375-1500 (with a resolution of 70,000), the 10  
292 most intensely multi-charged precursors were selected for HCD analysis in the C-trap (with a  
293 resolution of 17,500 and a normalized collision energy of 27). Automatic gain control (AGC)  
294 targets were  $3 \times 10^6$  ions for MS scans and  $1 \times 10^5$  ions for MS/MS scans. The maximum  
295 injection time was 100 ms and dynamic exclusion for 30 s was used to reduce repeated  
296 analyses of the same components.

297 Data concerning the identification and quantification of peptides and proteins were  
298 analyzed using Proteome Discoverer<sup>®</sup> software version 2.0 (Thermo Fisher Scientific). R  
299 software was used for statistical analysis and graphic outputs.

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## 305 **Results**

### 306 **Morphological and phenotypic characterization of the MucilAir™ nasal model**

307 We initially studied the morphology and cell composition of nasal MucilAir™ tissues  
308 (Fig. 1). Examination of alcian blue- and hematoxylin eosin (HE)-stained histological sections  
309 confirmed the pseudostratified organization of the tissues and the predominant presence of  
310 columnar ciliated cells bearing a differentiated apical cilium, organized in a clump extending  
311 into the lumen (Fig. 1A). The use of alcian blue allowed the staining of mucins and the  
312 subsequent visualization of elongated goblet cells enmeshed between ciliated cells with a large  
313 apical cup. Nuclei were tight and excluded at the basal pole. Goblet cells were distended by  
314 abundant blue secretory mucus granules into a typical cup-like shape. Basal progenitor cells  
315 were small, flattened, with a predominant nucleus and were in direct contact with the  
316 membrane of the insert. The thin and homogeneous fluorescent staining of  $\beta$ -IV tubulin, a  
317 major constituent of microtubules, confirmed the presence of apical cilia organized in clusters  
318 covering the major part of the epithelium (Fig. 1C). The ciliated and goblet cell populations  
319 were quantified by flow cytometry using the specific markers  $\beta$ -IV tubulin and CLCA1,  
320 respectively (Fig. 1B). Quantitative analysis showed  $12 \pm 3\%$  CLCA1-positive cells *versus*  $66$   
321  $\pm 17\%$   $\beta$ -IV tubulin-positive cells, corroborating the predominant presence of ciliated cells in  
322 the MucilAir™ model. Protein mass spectrometry analysis confirmed the expression of  $\beta$ -IV  
323 tubulin in MucilAir™ at the same level as in control Caco-2 cells (Fig. 5A). Interestingly, the  
324 abundance of the radial spoke head-like protein  $\beta$  4 (RSPH4) was approximately 10-fold  
325 higher in MucilAir™ than in Caco-2 cells, further testifying to the presence of ciliated cells in  
326 the nasal model. Gut specific mucin-13 was 10-fold more abundant in Caco-2 cells than in  
327 MucilAir™. Conversely, the airway-specific proteins mucin-5AC and mucin-5B displayed a  
328 100-fold and 10-fold greater abundance, respectively, in the nasal model than in Caco-2 cells.  
329 Finally, the basal cell marker aquaporin-3 was strongly detected in MucilAir™, but only  
330 weakly detectable in Caco-2 cells whereas integrin alpha-6 abundance was nearly identical in  
331 the two models. Overall, the MucilAir™ nasal model exhibited the main characteristics of the  
332 human nasal epithelium in terms of histology and cell type composition.

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## 336 **Barrier properties of the MucilAir™ nasal model**

337 In the second part of our study, we examined the barrier properties of the MucilAir™  
338 nasal model. In this context, we investigated the expression of the tight junction proteins  
339 zonula occludens 1 (ZO-1), occludin and claudin-1, and the adherens protein E-cadherin, by  
340 IF (Fig. 2A). Overall, the four proteins were found to be homogeneously expressed over the  
341 entire epithelium in a connecting network. A bright and homogeneous signal of ZO-1 was  
342 localized at the cell membrane. Confocal observations revealed a clear apical expression of  
343 the protein in the superficial cell layer. As an associated component of tight junction  
344 complexes, claudin-1 showed a distribution pattern similar to that of ZO-1, characterized by  
345 apicolateral membrane localization only in the superficial cell layer. A different expression  
346 pattern was observed for occludin, which was not only expressed on the apical side but was  
347 also localized on the lateral membranes of all cell layers. Finally, E-cadherin staining revealed  
348 a subcellular localization similar to that of occludin. The four proteins were detected in mass  
349 spectrometry with different abundances depending on the model used (Fig. 5B). Claudin-1  
350 showed a closely similar abundance in both models, whereas e-cadherin was detected to a  
351 slightly greater extent in Caco-2 cells. The greatest differences in abundance were observed  
352 for occludin and ZO-1, which both exhibited a 10-fold greater abundance in Caco-2 compared  
353 to MucilAir™. Claudin-3 and ZO-2 were detected at an identical level in both models while  
354 ZO-3 showed a slightly greater abundance in MucilAir™ than in Caco-2 cells. The average  
355 TEER of nasal MucilAir™ tissues ( $316 \pm 31 \Omega \cdot \text{cm}^2$ ) reflected the expression of tight junction  
356 complexes. Finally, the tightness of the MucilAir™ model was quantitatively evaluated using  
357 the hydrophilic compounds sodium fluoride (NaFlu) and 4.4 kDa Dextran (Fig. 2B). NaFlu  
358 showed an average permeability of  $5 \times 10^{-6} \text{ cm/s}$  whereas the permeability of 4.4 kDa Dextran  
359 was almost 10-fold lower ( $6 \times 10^{-7} \text{ cm/s}$ ).

360

## 361 **Expression of ABC efflux transporters**

362 We investigated the expression and subcellular localization of four ABC transporters,  
363 namely P-gp, MRP1, MRP2 and BCRP, in IF experiments using both epifluorescence and  
364 confocal microscopy (Fig. 3).

365 P-gp displayed a clear staining at the membrane of superficial cells with an expression  
366 characterized by bright multiple fluorescent spots covering the whole apical membrane of

367 most cells, although some cells remained unlabeled. BCRP exhibited a less intense signal  
368 than P-gp with a homogeneous expression characterized by thin and continuous apicolateral  
369 membrane staining in the superficial cell layer of the MucilAir™ tissues. The MRP1  
370 transporter showed an expression pattern nearly identical to that of P-gp with a distinct signal  
371 observed exclusively at the luminal side of the cells. Conversely, MRP2 exhibited a  
372 heterogeneous expression in cells, characterized by a subcellular localization throughout the  
373 cell membrane. All four transporters were detected in proteomic analyses with distinct  
374 abundance levels (Fig. 5C). Both P-gp and BCRP exhibited a 100-fold lower abundance in  
375 MucilAir™ than in the Caco-2 model. MRP2 was approximately 10 times as abundant in  
376 Caco-2 cells as in MucilAir™. Conversely, MRP1 displayed a greater abundance in  
377 MucilAir™ than in Caco-2. MRP3, MRP4 and MRP7 were detected at nearly the same level  
378 in both models.

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### 380 **Functionality of ABC efflux transporters**

381 We subsequently evaluated the functional activities of P-gp, BCRP and both MRPs by  
382 performing standard bidirectional transport experiments (Fig. 4).

383 The functional activity of P-gp was examined using rhodamine 123 as a substrate,  
384 associated with the P-gp inhibitor verapamil (Fig. 4A). Rhodamine 123 exhibited a  $P_{app (A \rightarrow B)}$   
385 of roughly  $2 \times 10^{-7}$  cm/s. The permeability of the compound in the basal to apical direction  
386 was found to be higher, around  $1.2 \times 10^{-6}$  cm/s, resulting in an efflux ratio of almost 6. The  
387 dissymmetric transport of rhodamine 123 was abolished in the presence of verapamil. Under  
388 these conditions, the  $P_{app (B \rightarrow A)}$  dropped to  $2 \times 10^{-7}$  cm/s whereas  $P_{app (A \rightarrow B)}$  remained  
389 unchanged and the ER was reduced by roughly 65% to nearly 2. P-gp was therefore  
390 functional in the MucilAir™ nasal model.

391 The functionality of BCRP was investigated using chlorothiazide and Ko143 as the  
392 substrate and inhibitor, respectively (Fig 4B). Chlorothiazide showed a differential transport  
393 through MucilAir™, characterized by a  $P_{app (B \rightarrow A)}$  169% higher than the  $P_{app (A \rightarrow B)}$ , leading to  
394 an ER of 2.7. The apical-to-basal permeability of chlorothiazide was not affected by the  
395 addition of Ko143 whereas the  $P_{app (B \rightarrow A)}$  was almost three times lower in the presence of this  
396 inhibitor, resulting in a halved ER. These results confirmed the involvement of BCRP in the

397 active efflux of chlorothiazide and demonstrated the functional activity of this transporter in  
398 the MucilAir™ nasal model.

399 Finally, the functional activity of the MRP transporters was evaluated using  
400 methotrexate as a broad-spectrum substrate coupled with the wide-range MRP inhibitor  
401 probenecid (Fig 4C). In contrast to rhodamine 123 and chlorothiazide, no dissymmetric  
402 transport was observed for methotrexate, which exhibited a nearly equally low permeability in  
403 both directions. The addition of probenecid did not change the bidirectional permeability of  
404 methotrexate and the consequent ER remained below 2. The MRPs tested were therefore not  
405 involved in the active efflux of methotrexate in the MucilAir™ model.

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## 421 Discussion

422 The efficacy of many drugs depends on their ability to cross tissues to reach their  
423 target. The efflux process mediated by ABC transporters plays a critical role in limiting the  
424 absorption and accumulation of exogenous compounds, which can lead to drug resistance.  
425 These membrane proteins are therefore key determinants of the pharmacokinetic and  
426 bioavailability profiles of locally administered drugs. At an early stage of drug development,  
427 *in vitro* models represent valuable tools for quickly assessing drug interactions with  
428 membrane transporters in pre-clinical studies [8, 25]. Our study focused on the morpho-  
429 functional characterization of the MucilAir™ nasal model based on its barrier properties with  
430 a pharmacological extension to the expression and functional activity of well-known ABC  
431 transporters.

432 We initially examined the morphological appearance and cell phenotype organization  
433 of MucilAir™ nasal tissues. The human nasal mucosa comprises a pseudostratified  
434 respiratory epithelium supported by a lamina propria. The nasal epithelium is composed of  
435 three types of cell including differentiated ciliated epithelial cells, goblet cells that produce  
436 mucus and basal cells involved in epithelium renewal. IF studies of  $\beta$ -IV tubulin, a major  
437 constituent of motile cilia [26], showed the presence of several cilia clusters sheathed in the  
438 apical membrane as previously described in the normal nasal mucosa [27]. Protein mass  
439 spectrometry was performed to investigate the abundance of specific phenotypic markers of  
440 nasal mucosa in the MucilAir™. Caco-2 intestinal model was used as a ~~negative~~ **positive**  
441 control for the validation of the proteomic method. Despite a preferential expression in cilia,  
442 the abundance of  $\beta$ -IV tubulin was similar in both MucilAir™ and Caco-2 models. This could  
443 be explained by the involvement of  $\beta$ -IV tubulin as one of the major constituents of  
444 ubiquitous cytoskeleton microtubules [28]. However, the greater abundance of RSPH4 in  
445 MucilAir™ than in Caco-2 cells was specifically related to the presence of ciliated cells. This  
446 protein is exclusively located in the head complex of cilia radial spokes involved in the  
447 transmission of regulatory signals in the ciliary beating process [29]. The presence of goblet  
448 cells was demonstrated by staining with alcian blue, a dye routinely used to stain mucins [30].  
449 As expected, the abundance of mucin-5B and mucin-5AC was greater in MucilAir™ than in  
450 Caco-2 cells, these proteins being the main gel-forming mucins secreted in the upper airway  
451 [31]. Also, as expected, mucin-13 was more abundant in Caco-2 cells than in MucilAir™, in  
452 line with its preferential expression in intestinal mucus [32]. The proportion of each cell type  
453 was in accordance with *in vivo* observations indicating up to 50-80% of ciliated cells [33] and

454 15% of goblet cells in the nasal epithelium [34]. Basal cells are expected to cover  
455 approximately 5-10% of the nasal epithelium [35]. The presence of basal cells in the  
456 MucilAir™ model was supported by the expression of aquaporin-3, Kreda et al. having  
457 shown that aquaporin-3 is exclusively expressed in basal nasal cells [36]. Overall, the  
458 MucilAir™ nasal model was close to the normal human nasal epithelium in terms of cell type  
459 composition and histology.

460 One of the main functions of nasal epithelium is to act as a physical barrier against  
461 pathogens, allergens and air pollutants [37]. The integrity of the nasal epithelium is principally  
462 ensured by the presence of both tight and adherens junctions [38]. Tight junction proteins  
463 form intercellular bridges between adjacent cells that modulate the paracellular passage of  
464 hydrophilic compounds [39], whereas adherens junctions are involved in the stabilization of  
465 cell–cell adhesion and polarity [40]. The MucilAir™ nasal tissues showed a typical apical  
466 expression of ZO-1, occludin, and claudin-1; three major constituents of tight junctions [41,  
467 42, 43] as well as the adherens junction protein e-cadherin [44]. The apical expression of  
468 occludin and claudin-1 has been demonstrated in excised nasal mucosa [45]. Moreover, Ong  
469 et al. recently observed the apical expression of ZO-1 and e-cadherin in primary nasal cells  
470 [46]. Caco-2 cell line provided a positive control of the abundance of tight junction proteins in  
471 proteomics experiment. Indeed, the Caco-2 model was shown to be a tight and polarized  
472 barrier with a strong expression of junctional proteins, a critical requirement for drug  
473 transport studies [47]. The greater abundance of occludin and ZO-1 in the Caco-2 cell line  
474 compared to MucilAir™ could be related to the cell composition of the two models. An  
475 ultrastructural study showed that tight junctions around nasal goblet cells were discontinuous  
476 and fragmented [48]. Similarly, tight junctions have been shown to be leakier between  
477 enterocytes and goblet cells than between enterocytes [49]. Considering that the Caco-2 cell  
478 line is homogenously composed of enterocytes, the lesser abundance of occludin and ZO-1 in  
479 MucilAir™ could be related to the presence of both goblet and ciliated cells. Proteomic  
480 analyses also revealed the presence of claudin-3 isoform, a constituent of tight junctions  
481 involved in the regulation of ion permeability [50], as well as ZO-2 and ZO-3, two tight  
482 junction-associated proteins [40]. Finally, the paracellular permeability of NaFlu through  
483 MucilAir™ was within the same range as that of excised human nasal mucosa [51]. As  
484 expected, 4.4 kDa dextran exhibited a lower permeability than that of NaFlu due to its higher  
485 molecular weight. Taken together, these results provide further evidence of the involvement  
486 and efficacy of tight junction complexes in selective regulation of the paracellular transport of  
487 hydrophilic compounds in the MucilAir™ nasal model. Moreover, a recent study described

488 the ability of this model to discriminate the permeability of compounds according to their  
489 physicochemical properties. Hydrophilic compounds typically exhibited lower permeability  
490 than lyophilic ones due to a preferential permeation through the more restrictive paracellular  
491 pathway [52].

492 The last step of the assessment of the barrier properties of MucilAir™ tissues led us to  
493 investigate the functional expression of ABC transporters P-gp, BCRP, MRP1 and MRP2.  
494 The Caco-2 model was used as a positive control of ABC transporters abundance in  
495 proteomics experiments. Indeed, Caco-2 model was previously validated for the *in vitro*  
496 evaluation of drugs as substrates or inhibitors of ABC transporters in pre-clinical screening  
497 studies [4, 53]. The functional activity of the selected transporters was subsequently assessed  
498 using the FDA-approved bidirectional transport protocol [4, 54].

499 P-gp is a glycoprotein widely expressed on the apical membrane of various tissues  
500 including the respiratory epithelium [55]. The MucilAir™ nasal model showed a homogenous  
501 and apical expression of P-gp. The same expression pattern has been previously described in  
502 normal nasal epithelium [17]. The relative abundance of P-gp was roughly 100 times lower in  
503 MucilAir™ than in the control Caco-2 model. This result was consistent with those of a  
504 previous study showing a weaker expression of P-gp in excised nasal mucosa compared to  
505 Caco-2 cells using the western blot technique [56]. Interestingly, two further studies have  
506 described a weak to moderate gene expression of P-gp in human nasal mucosa [18] and  
507 primary nasal cells [57]. The functional activity of this transporter was evaluated using  
508 rhodamine 123, a P-gp substrate previously shown to display an active efflux in intestinal  
509 Caco-2 cells [58]. We observed a dissymmetric transport of rhodamine 123 through  
510 MucilAir™, resulting in an ER of approximately 6 that was reduced by a factor of 3 in the  
511 presence of verapamil, a P-gp inhibitor [59]. As already reported, a compound may be  
512 considered as a substrate of ABC transporters if its ER is equal to or is above 2 and is at least  
513 halved in the presence of the corresponding selective inhibitor [4, 60]. Based on this  
514 observation, P-gp was functional in the MucilAir™ nasal model and acted as an apical pump  
515 that reduced drug absorption by extruding xenobiotics out of the cells [61].

516 As a member of the ABC transporter family, BCRP also performs a detoxifying  
517 function, manifesting broad substrate specificity [62]. We showed that the apical expression  
518 of BCRP in the MucilAir™ nasal model follows the same pattern as in bronchial Calu-3 cells  
519 [63]. The expression of BCRP in the nasal mucosa has been little investigated. Only a  
520 moderate gene expression was demonstrated in a recent study [18] and this finding could be  
521 consistent with the weaker detection of BCRP in MucilAir™ compared to the Caco-2 model.

522 Chlorothiazide was used as a substrate of BCRP in functional studies. This diuretic displayed  
523 an ER above 3 in the Caco-2 model [64] that was abolished by the known BCRP inhibitor  
524 Ko143 [65]. The bidirectional transport of chlorothiazide through MucilAir™ resulted in an  
525 ER of approximately 3. Addition of the inhibitor Ko143 halved the ER, thereby confirming  
526 the functional activity of BCRP in the nasal MucilAir™ model.

527 MRP1s are ABC efflux pumps involved in the excretion of metabolized xenobiotic  
528 compounds from cells [66]. We successfully demonstrated the homogenous apical expression  
529 of MRP1 in the MucilAir™ model as previously described in human nasal epithelium [17].  
530 The greater abundance of MRP1 in MucilAir™ compared to Caco-2 was in accordance with  
531 the results of a previous study reporting a much higher signal of MRP1 in excised nasal  
532 mucosa than in the Caco-2 cell line, using western blotting [67]. Moreover, MRP1 was found  
533 to be the most abundant isoform in human nasal mucosa [18] and primary nasal cells [57].  
534 MRP2 showed a faint and heterogeneous lateral signal at all plasma membranes in accordance  
535 with its weak gene expression in both nasal epithelium and primary nasal cells [18, 57]. A far  
536 weaker expression of MRP2 in the nasal mucosa than in the Caco-2 cell line was  
537 demonstrated using the western blot technique [67] strengthening the correlation between the  
538 MucilAir™ model and the nasal mucosa. Although both MRP1 and MRP2 were expressed in  
539 the MucilAir™ model, no active efflux of methotrexate was shown in functional studies. This  
540 could be explained by the opposite subcellular distribution of MRP1 and MRP2 at the apical  
541 and basolateral membrane, respectively. Considering that methotrexate is a broad-spectrum  
542 substrate of MRPs [68], the active efflux of this compound, mediated by MRP1 in the apical  
543 compartment, could be balanced by its excretion by MRP2 in the basal compartment, leading  
544 to the absence of a net active efflux. An alternative hypothesis refers to the simultaneous  
545 expression of MRP3, MRP4 and MRP7 in MucilAir™, these ABC transporters also being  
546 potentially involved in the active transport of methotrexate [69].

547 To the best of our knowledge, this study is the first to demonstrate the potent  
548 correlation between the MucilAir™ nasal model and the normal nasal epithelium, with regard  
549 to the histological characteristics, barrier properties and functional expression of ABC  
550 transporters. This model could be used to further evaluate the involvement of ABC  
551 transporters in the bioavailability of nasally administered drugs. However, care should be  
552 taken regarding its predictability of nasal drug absorption. The immortalized Caco-2 cell line  
553 is currently the gold-standard for the prediction of intestinal drug absorption due to strong *in*  
554 *vitro-in vivo* correlations [3]. We recently showed that the RPMI 2650 model may be a

555 potential candidate but failed to anticipate the active efflux of drugs mediated by ABC  
556 transporters [20]. Although we demonstrated that the primary MucilAir™ model was  
557 morphologically and physiologically closer to the human nasal mucosa than the RPMI 2650  
558 model, *in vitro-in vivo* correlations are still lacking to determine their predictability. Firstly,  
559 comparative studies with excised nasal mucosa focused on drug transporters expression and  
560 both passive permeability and active efflux of reference compounds should be performed to  
561 confirm the relevance of the *in vitro* permeability data. Ultimately, the relationship between  
562 the *in vitro* permeability data and *in vivo* nasal absorption rates of reference drugs in humans  
563 must be evaluated to determine the relevance of MucilAir™ to accurately predict nasal drug  
564 absorption in pre-clinical studies.

565

## 566 **Conclusion**

567 This study reports the first original pharmacological characterization of the  
568 MucilAir™ nasal model in terms of morphology, phenotype and expression of tight and  
569 adherens junction proteins, as well as the functionality of ABC drug transporters. The  
570 MucilAir™ nasal model matched the major features of a normal human nasal epithelium. The  
571 homogeneous expression of tight and adherens junction proteins over the entire apical surface  
572 of the epithelium demonstrated the ability of MucilAir™ to form a polarized and hermetically  
573 sealed barrier. The ABC transporters P-gp, MRP1, MRP2 and BCRP were all expressed at  
574 different levels and exhibited distinct IF patterns in accordance with their subcellular  
575 localizations. Bidirectional transport studies demonstrated the functional activities of P-gp and  
576 BCRP, these transporters being capable of actively effluxing their respective substrates.  
577 Finally, the MucilAir™ nasal model could be used as a relevant tool in preclinical screening  
578 studies for evaluating the involvement of ABC transporters in the bioavailability of nasally  
579 administered drug candidates.

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588

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592

593 **Conflict of interest**

594 C.M declare that S.C is the CEO of Epithelix SARL. S.C provided technical support and was  
595 not involved in the design of the study, the analysis of results and the writing of the article.

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801 **Figure captions**

802

803 **Fig. 1** Morphological and phenotypic characterization of the MucilAir™ nasal model.

804 **A.** Hematoxylin-eosin (HE) and alcian blue-stained histological section. **ci:** ciliated cells, **go:**  
805 goblet cells, **ba:** basal cells. **B.** Quantitative flow cytometry analysis of the cell population.  
806 Isotypic phycoerythrin (PE) and PE.Cyn5.5 control acquisitions versus PE and PE.Cyn5.5  
807 signals were performed for  $\beta$ -tubulin and chloride channel accessory 1 (CLCA1) markers,  
808 respectively. CLCA1 and  $\beta$ -tubulin immunostaining acquisitions were gated on the entire  
809 viable cell population; n=3 for each condition. **C.** Immunofluorescence staining of  $\beta$ -IV  
810 tubulin and actin. Observations were performed using confocal microscopy. Nuclei were  
811 counterstained using 4',6-diamidino-2-phenylindole (DAPI).

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813 **Fig. 2** Barrier properties of the MucilAir™ nasal model.

814 **A.** Immunofluorescence staining of the tight junction proteins zonula occludens 1 (ZO-1),  
815 occluding and claudin-1, and the adherens protein e-cadherin, in the MucilAir™ nasal model.  
816 Observations were performed using epifluorescence (left) and confocal microscopy (right).  
817 Nuclei were counterstained using 4',6-diamidino-2-phenylindole (DAPI). **B.** Transepithelial  
818 electrical resistance (TEER) of the MucilAir™ nasal model (n=6) and permeability of  
819 NaFlu/4.4 kDa dextran following 2 h of incubation (n=3). Data are expressed as the mean  $\pm$   
820 standard deviation.

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822 **Fig. 3** Immunofluorescence staining of [ATP]-binding cassette (ABC) efflux transporters P-  
823 glycoprotein (P-gp), multidrug resistance-associated protein (MRP1, MRP2) and breast  
824 cancer resistance protein (BCRP) in the MucilAir™ nasal model.

825 Observations were performed using epifluorescence (left) and confocal microscopy (right).  
826 Nuclei were counterstained in blue using 4',6-diamidino-2-phenylindole (DAPI).

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828 **Fig. 4** Bidirectional permeability and efflux ratio of rhodamine 123 (**A**), chlorothiazide (**B**)  
829 and methotrexate (**C**) through the MucilAir™ nasal model after 2 h of incubation.

830  $P_{app}$  bidirectional permeability, R. 123: rhodamine 123, CTZ: chlorothiazide, MTX:  
831 methotrexate; n=3 for each condition. Data are expressed as the mean  $\pm$  standard deviation.

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833 **Fig. 5** Label-free quantification of phenotypic markers (**A**), tight and adherens junction  
834 proteins (**B**) and ABC transporters (**C**) in the MucilAir™ nasal and Caco-2 models.

835 Whiskers indicate the first and third quartiles of the data, the horizontal bar within each box  
836 indicating the median value. Three biological replicates were examined for each model, each  
837 biological replicate being analyzed three times.

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855 **Table 1.** List of antibodies and reagents used for the immunostaining of  
 856 MucilAir™ nasal tissues

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Category	Target	Source	Supplier	Reference	Fixatives	Dilution	Incubation Time
Phenotyping	β-tubulin	mouse	Abcam	ab11315	Paraformaldehyde	1/200	60 min
	Actin	-	Abcam	ab176756	Paraformaldehyde	-	30 min
Junction proteins	ZO-1	rabbit	SantaCruz	sc-10804	Paraformaldehyde	1/200	60 min
	E-cadherin	rabbit	SantaCruz	sc-7870	Methanol	1/200	Overnight
	Occludin	rabbit	Abcam	ab31721	Methanol	1/200	Overnight
	Claudin-1	rabbit	Abcam	ab15098	Methanol	1/200	60 min
ABC drug transporters	P-gp	mouse	SantaCruz	sc-55510	Paraformaldehyde	1/200	60 min
	BCRP	mouse	SantaCruz	sc-58222	Methanol	1/200	Overnight
	MRP1	rabbit	Abcam	ab99531	Paraformaldehyde	1/200	60 min
	MRP2	rabbit	Abcam	ab172630	Paraformaldehyde	1/200	60 min

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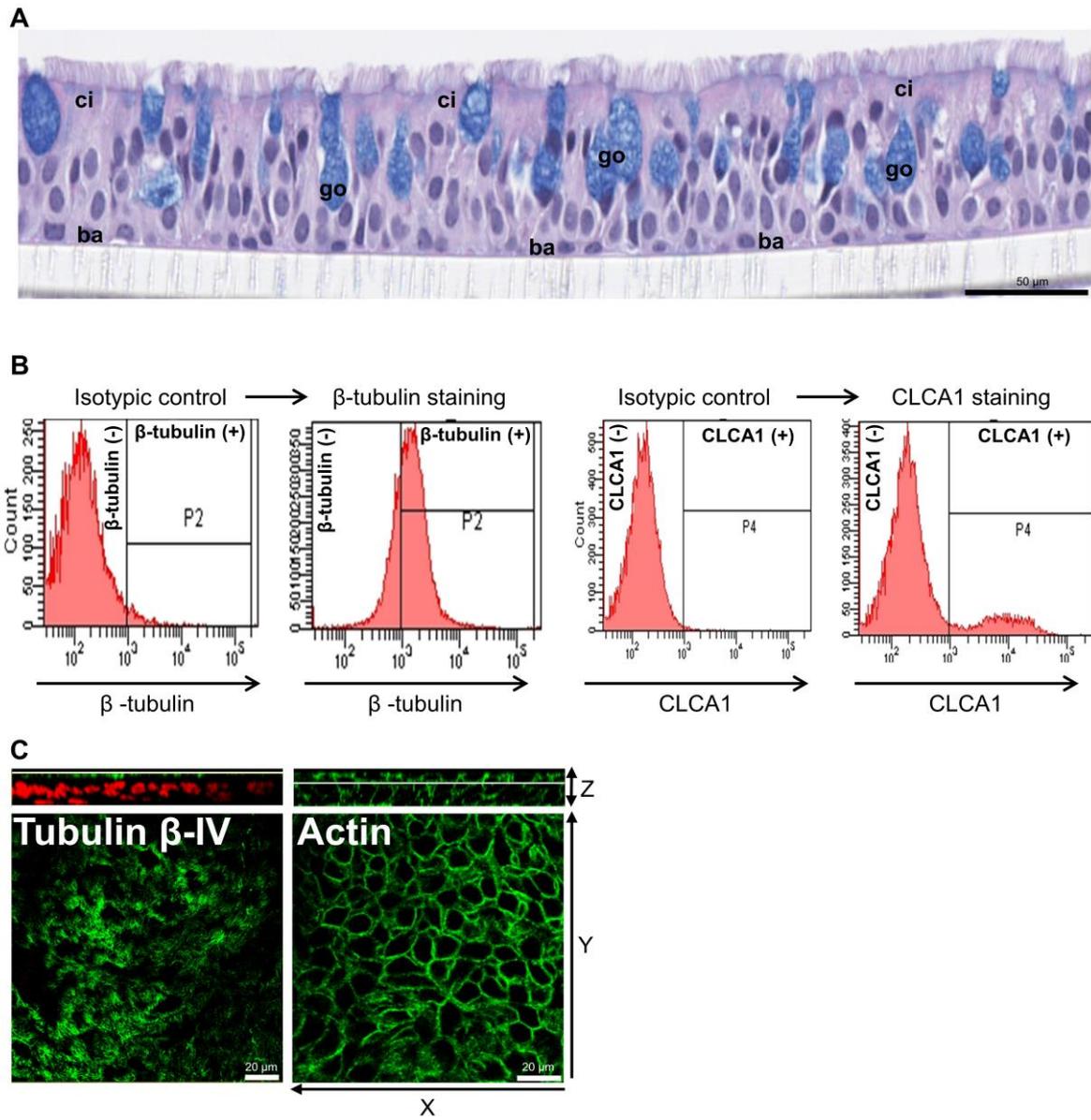
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**Figure 1**

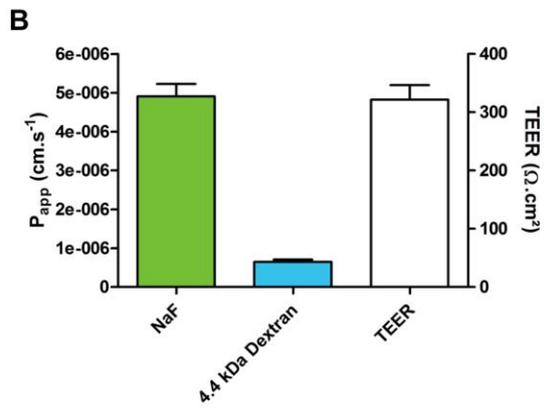
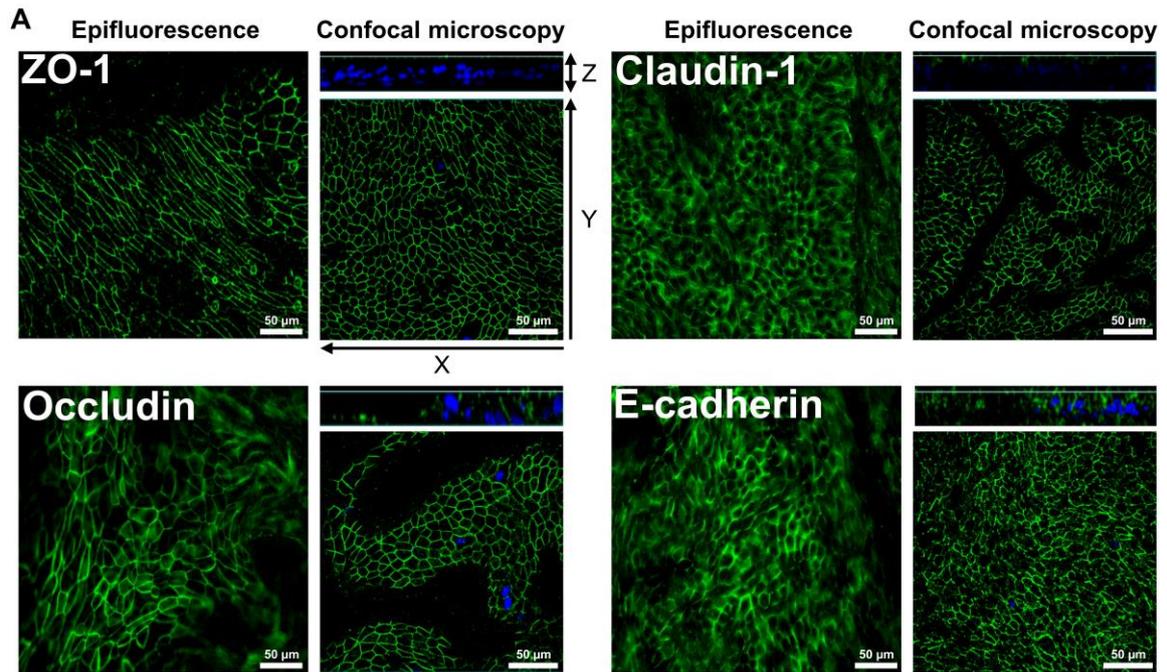


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Figure 2

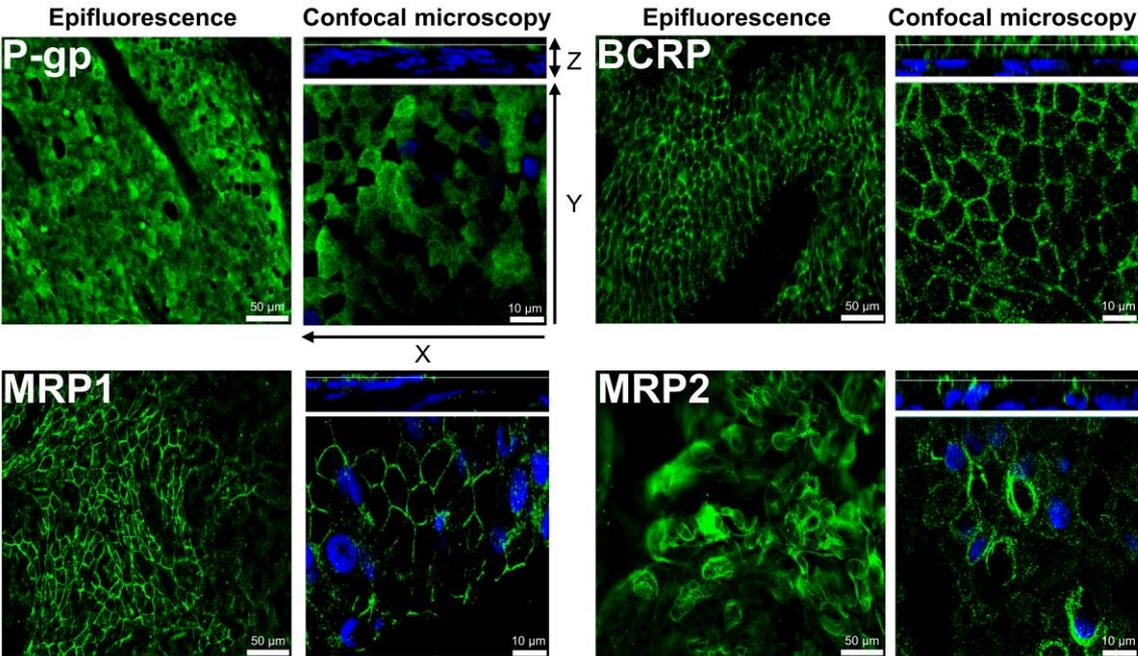


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**Figure 3**

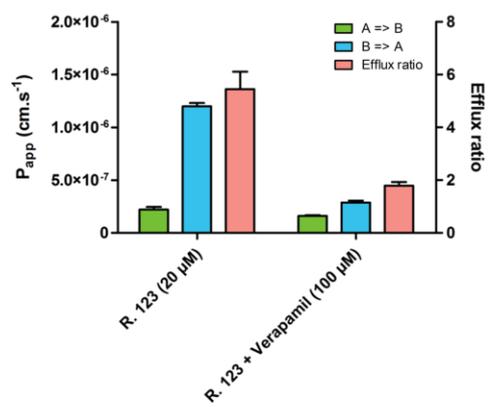


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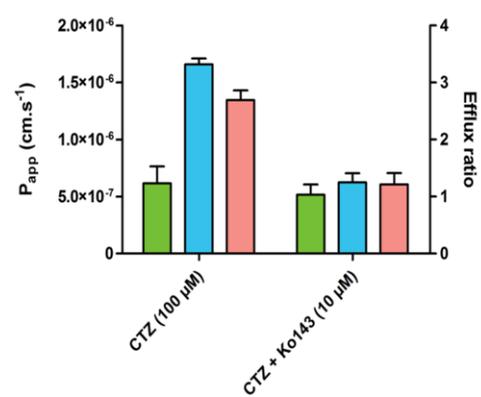
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# Figure 4

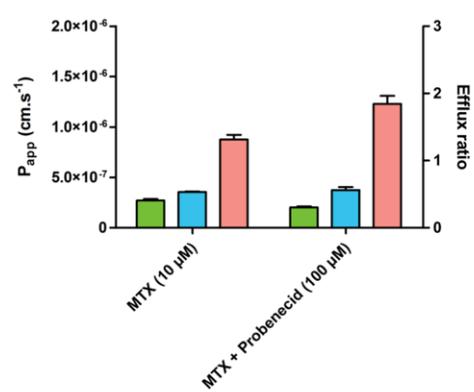
## A



## B



## C

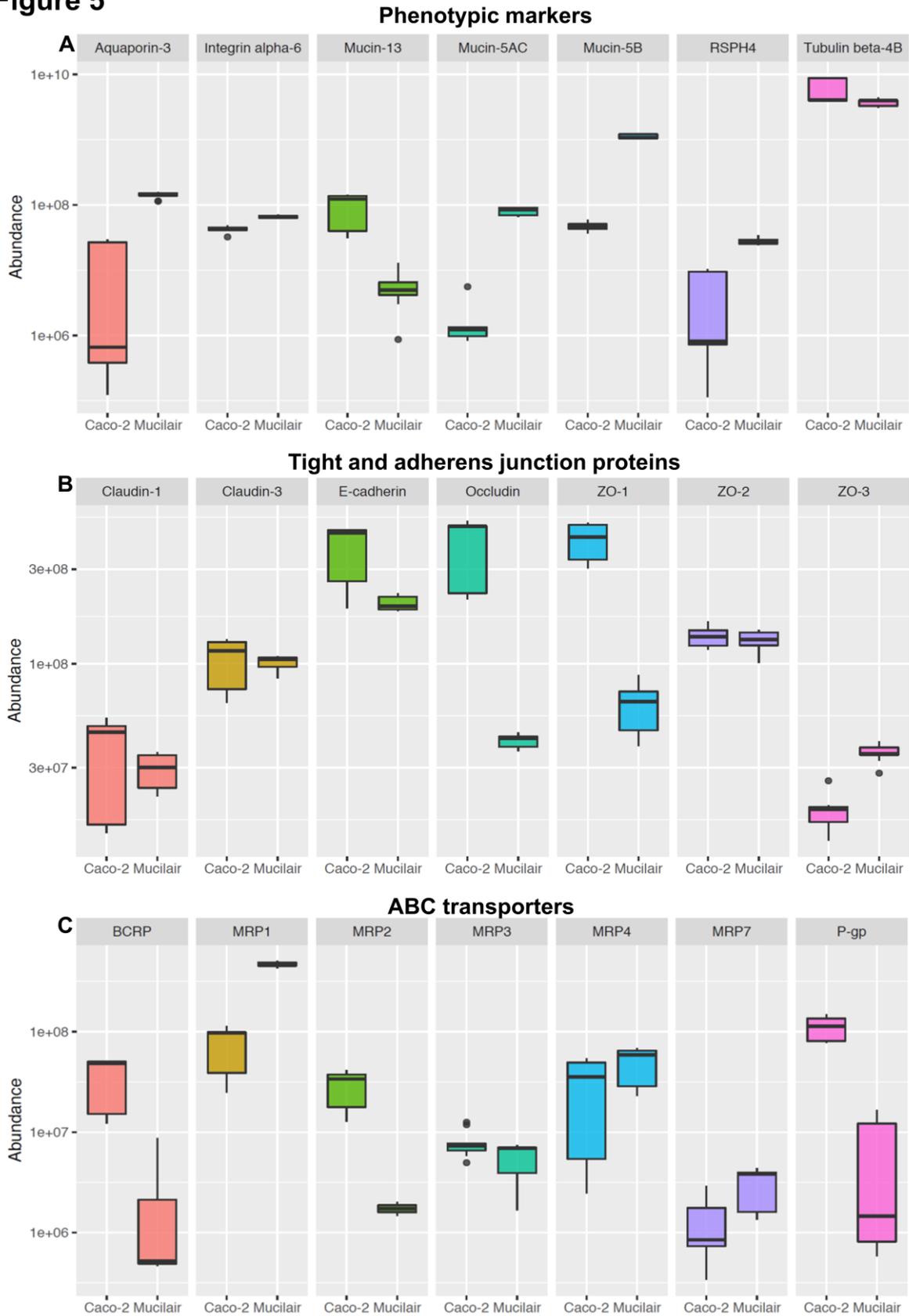


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**Figure 5**



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