

Comparison of efficiency and activity recovery coefficients of Compton and Anger cameras in Nuclear Medicine

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Ane Etxebeste, Enrique Muñoz, Denis Dauvergne, J M Letang, M. Borja-Lloret, et al.. Comparison of efficiency and activity recovery coefficients of Compton and Anger cameras in Nuclear Medicine. IEEE Nuclear Science Symposium and Medical Imaging Conference (IEEE NSS MIC) 2021, Oct 2021, Virtual Yokohama, Japan, Oct 2021, Yokohama (virtual), Japan. hal-03473005

HAL Id: hal-03473005 https://hal.science/hal-03473005

Submitted on 9 Dec 2021

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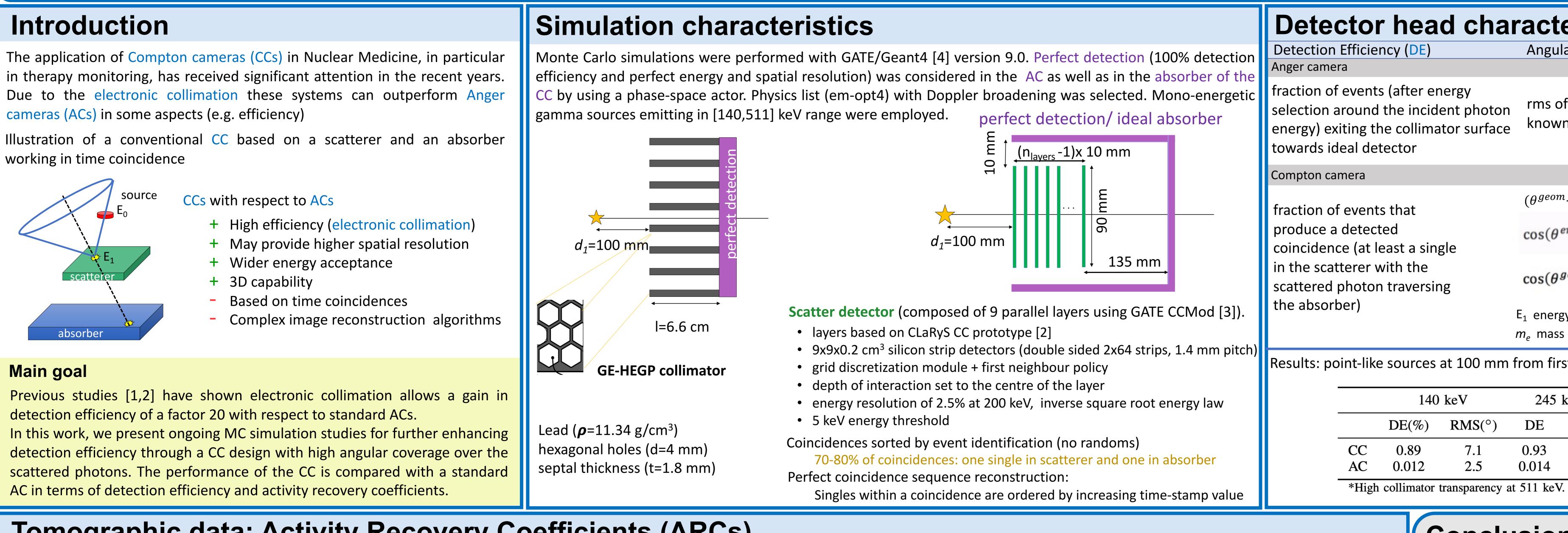
Comparison of efficiency and activity recovery coefficients of Comp cameras in Nuclear Medicine



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cameras (ACs) in some aspects (e.g. efficiency)

working in time coincidence



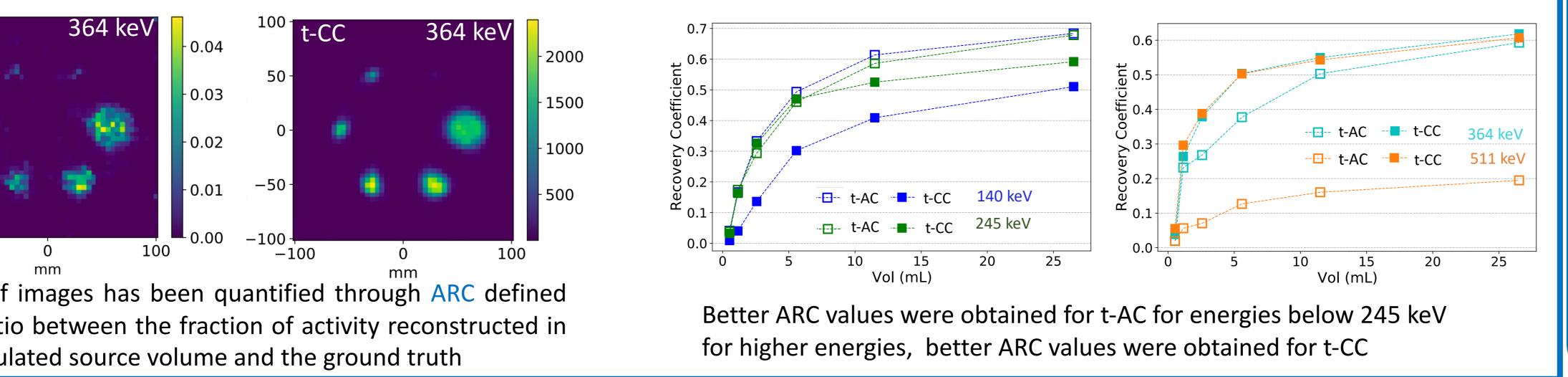
Tomographic data: Activity Recovery Coefficients (ARCs)

180 views, step of 2 degrees100 t-AC0.5 s/view at 100 mm from rotation center50Source distribution (NEMA IEC body phantom config):506 spheres of 10/13/17/22/28/37 mm diameters0distributed along a circumference of D=114.4 mm0Constant activity concentration: 20.5 kBq/mL-50mono-energetic gamma sources [140, 245, 364, 511] keV-100Reconstruction, ML-EM algorithm :100 t-ACRTK toolkit [5] for t-ACQuality of		
0.5 s/view at 100 mm from rotation center100 t-ACSource distribution (NEMA IEC body phantom config): 6 spheres of 10/13/17/22/28/37 mm diameters distributed along a circumference of D=114.4 mm Constant activity concentration: 20.5 kBq/mL mono-energetic gamma sources [140, 245, 364, 511] keV100 -50 -100 -100Reconstruction, ML-EM algorithm : RTK toolkit [5] for t-AC in-house code [6] for t-CC FoV 46×46×46 voxels of 4.4 mm³Quality of as the ratio each simulation		Reconsti
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FoV 46×46×46 voxels of 4.4 mm ³ each simula		Quality of i
		as the ratio
[1] L. Han et al., Phys. Med. Biol., vol. 53, no. 24, p. 7029, 2008 [3] A. Etxebeste et al		[3] A. Etxebeste et al.

[1] L. Han et al., Phys. Wed. Biol., Vol. 53, no. 24, p. 7029, 2008 [2] M. Fontana et al., Phys. Med. Biol, vol. 63, no. 23, p. 8794, 2017. [4] Jan et al., Phys. Med. Biol., vol. 56, no. 4, p. 881, 2011

[3] A. Etxebeste et al., Phys. Med. Biol., vol. 65, no. 5, p. 55004, 2020

tructed transversal central slice for t-AC and t-CC



[5] S. Rit et al 2014 J. Phys. Conf. Ser. 489(1) [6] V. Maxim et al 2016 Phys. Med. Biol. 61 p. 243

ARCs (t-CC and t-AC) as a function of the sphere volume for different energies.

Acknowledgements

This work was performed within the framework of the Labex PRIMES (ANR-11-LABX-0063). This project has received funding from PIC 2018 programme under the reference CSIC 2018FR0032 and CNRS PICS08272

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	n) of er	nergy sel	ected ev	vents		
$(heta^{geon})$	$\theta^{n} - \theta^{energ}$	^y) distri			\vec{g}_{10}	
$\cos(\theta^{energy}) = 1 - \frac{m_e c^2 E_1}{E_0 (E_0 - E_1)}$ E ₁ source						
$\cos(\theta^{geom}) = \frac{\dot{g}_{10} \cdot \dot{g}_{21}}{ \vec{g}_{10} \vec{g}_{21} } \qquad $						
E_1 energy deposited in the Compton scattering E_2						
m_e mass of the electron						
m from first scatterer layer (CC) / collimator surface (AC)						
245	keV	364	keV	511 1	xeV*	
DE	RMS	DE	RMS	DE	RMS	
0.93	5.2	0.88	4.3	0.82	4.0	
0.014	3.8	0.018	9.8 (0.067	21.1	

Conclusions

Results showed an increase of the detection efficiency of CC up to a factor 74 in the studied energy range as compared to standard AC. For energies above 245 keV, a better angular resolution and ARC were obtained for t-CC, whereas for energies below 245 keV the quality of the reconstructed image in terms of ARC, under the studied conditions, was better for t-AC.

Future work

In the future, we plan to include realistic conditions in absorber detectors and compare the performance of this CC design with commercial SPECT AC system designs.

In addition, we plan to evaluate in more detail the quality of the different types of coincidences detected in the CC system.

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