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## **To cite this version:**

Djahid Kennouche, Eric Luneau, Thomas Lapole, Jérome Morel, Guillaume Millet, et al.. Bedside voluntary and evoked forces evaluation in intensive care unit patients: a narrative review. Critical Care, 2021, 25 (1),  $10.1186/s13054-021-03567-9$ . hal-03443149

# **HAL Id: hal-03443149 <https://hal.science/hal-03443149v1>**

Submitted on 24 Nov 2021

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## **REVIEW**

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# Bedside voluntary and evoked forces evaluation in intensive care unit patients: a narrative review

Djahid Kennouche<sup>1†</sup>, Eric Luneau<sup>1†</sup>, Thomas Lapole<sup>1</sup>, Jérome Morel<sup>1,2</sup>, Guillaume Y. Millet<sup>1,3†</sup> and Julien Gondin<sup>4\*[†](http://orcid.org/0000-0002-3108-605X)</sup>

### **Abstract**

Around one third of intensive care unit (ICU) patients will develop severe neuromuscular alterations, known as intensive care unit-acquired weakness (ICUAW), during their stay. The diagnosis of ICUAW is difficult and often delayed as a result of sedation or delirium. Indeed, the clinical evaluation of both Medical Research Council score and maximal voluntary force (e.g., using handgrip and/or handheld dynamometers), two independent predictors of mortality, can be performed only in awake and cooperative patients. Transcutaneous electrical/magnetic stimulation applied over motor nerves combined with the development of dedicated ergometer have recently been introduced in ICU patients in order to propose an early and non-invasive measurement of evoked force. The aim of this narrative review is to summarize the diferent tools allowing bedside force evaluation in ICU patients and the related experimental protocols. We suggest that non-invasive electrical and/or magnetic evoked force measurements could be a relevant strategy to characterize muscle weakness in the early phase of ICU and diagnose ICUAW.

**Keywords:** Intensive care unit-acquired weakness, Skeletal muscle function, Electrical stimulation, Magnetic stimulation, Ergometers

#### **Introduction**

Around one third of ICU patients will develop severe neuromuscular alterations, known as intensive care unit-acquired weakness (ICUAW), during their stay [1]. ICUAW, defned as "*a syndrome of generalized limb weakness that develops while the patient is critically ill and for which there is no alternative explanation other than the critical illness itself*" [2], is the most related disease acquired in ICU. Both persistent reduction of force production and atrophy are involved in the

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poor health-related quality of life  $[3]$ . There is so far no efective treatment to counteract the long-term deleterious effects of ICUAW  $[4]$ . This is mainly due to the difculties of making an early diagnosis which further limit our knowledge of the underlying pathophysiological mechanisms of ICUAW [5]. ICUAW can be caused by (i) a critical illness polyneuropathy (CIP) which has been described as a distal axonal sensory-motor polyneuropathy affecting limb and respiratory muscles  $[6]$ ; (ii) a critical illness myopathy (CIM) which is considered as a primary myopathy that is not related to muscle denervation [7]; (iii) a combination of both also referred to as critical illness polyneuromyopathy (CIPNM) [8].

ICUAW diagnosis currently relies on manual muscle testing using the Medical Research Council (MRC) score  $[9]$ . This method is easy to perform as it does not require any special equipment. Handgrip (HG) [10] and



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handheld (HHD) [11] dynamometers have been used to provide quantitative values of the patient's maximal strength. However, both MRC score and voluntary force measurements can be obtained only in awake and fully cooperative patients so that ICUAW diagnosis is inevitably delayed.

To overcome these limitations, non-volitional techniques combining electrical [12] or magnetic [13] stimulation applied to a motor nerve or over a muscle belly [14] with force measurements on a dedicated bedside ergometer have emerged in the field of ICU. This allows to record evoked-force in fully sedated patients, so that measurement can be performed early after ICU admission (*i.e.* within 24 h of ICU admission [15]).

The aim of this narrative review is to summarize the diferent tools and related experimental protocols allowing bedside force evaluation of limb muscles in ICU patients. We will exclude the tools used to assess respiratory muscle function since it has been described in details elsewhere [5, 16]. After a brief presentation of the gold-standard method for ICUAW diagnosis (*i.e.* MRC scale), we will present for each existing dynamometers and ergometers: (i) intra- and inter-investigators reliability, (ii) their interests and limitations for quantitative voluntary and evoked-force measurements at the bedside, (iii) an overview of the cross-sectional studies in which force production was compared between ICU patients and healthy controls as well as longitudinal approaches in which the time course of changes in force was assessed throughout an ICU stay. The search strategy is described in Additional File 1.

#### **MRC scale**

#### **Defnition**

MRC is currently the gold-standard diagnostic method of ICUAW. This scale includes the measurements of 6 muscle groups (shoulder abductors, elbow fexors, wrist extensors, hip fexors, knee extensors and ankle dorsifexors) on each side, ranking them between 0 (no visible contraction) and 5 (normal force on complete range of motion). The MRC scale is an ordinal scale which gives a sum-score (*i.e.* sum of each individual muscle score) ranging from 0 (paralysis) to 60 (normal force).

#### **Reliability of MRC sum‑score**

Intra-investigator and inter-investigator reliability was considered as a test–retest performed by the same investigator on diferent occasions and measurements performed by diferent investigators on the same day, respectively. MRC reliability has mainly been assessed by intraclass correlation coefficients (ICCs), ranging between 0 (no agreement) and 1 (excellent agreement). So far, intra-investigator reliability of MRC has never been reported in ICU patients, even though good to excellent ICC values were observed in other pathologies [17, 18]. Inter-investigator reliability of the MRC sumscore was found to be good to excellent in ICU patients [19–23] (Table 1). However, lower ICC values (*i.e.* ranging from 0.29 to 0.75) were reported when considering individual muscle groups  $[20]$ , indicating that MRC is less reliable to assess force from a single muscle group. High inter-investigator reliability was also reported for the four-point scale (ICCs= $0.90-0.94$ ) on a small cohort of ICU patients [24].

#### **Diagnostic approach**

An MRC sum-score below 48 has been arbitrarily used for ICUAW diagnosis [25] and a score below 36 indicates severe muscle weakness [19] (Fig. 1). A four-point ordinal scale has been recently introduced but remains to be validated on a large cohort of patients [26]. An MRC sumscore<40 has been proposed as a modality to specifcally diagnose patients with CIPNM [27]. However, this study suffers from several limitations such as highly selective inclusion criteria (*i.e.* only septic patients), a small sample size (*i.e.* only 50 patients), a lack of information regarding the electrophysiological investigations and the day of assessment. Interestingly, it has been recently demonstrated that even a slight reduction in MRC sum-score (*i.e.*≤55) at ICU discharge may identify patients with poor long-term outcomes (*i.e.* mortality, strength, functional capacity and physical function) [28]. Further studies are needed to determine whether and to what extent this specifc cut-of MRC sum-score at ICU discharge is infuenced by the etiology of ICUAW (*i.e.* CIP, CIM or CIPNM).

#### **Limitations**

The first important limitation of MRC is that the grade  $\leq$  3 only uses gravity as reference whereas grade > 3 refers to muscle contraction against non-standardized and subjective resistance so that it is difficult to

**Table 1** Inter-investigator reliability measurements of MRC sumscore

References	Number of patients	Number of investigators	ICC (95% CI-range)	
Hermans et al. [19]	75	2	$0.95(0.92 - 0.97)$	
Hough et al. [20]	30	2	$0.83(0.67 - 0.93)$	
Kleyweg et al. [21]	60	2	$0.97(0.96 - 0.98)$	
Fan et al. [22]	10	19	$0.99(0.98 - 1.00)$	
Connolly et al. [23]	20		$0.94(0.85 - 0.98)$	

Intraclass Correlation Coefficients (ICC) and their 95% Confidence Interval (CI) are reported





diferentiate grade 4 (subnormal strength) and grade 5 (normal strength). MRC is further limited by a ceiling efect that precludes accurate measurements of strength. Although MRC sum-score is a good predictor of both hospital [29] and long-term [28] mortality, patients have to be awake and fully cooperative so that the diagnostic is inevitably delayed and can be further complicated by pain, edema or limitation on range of motion [30].

#### **Voluntary force measurements**

#### **Existing ergometers and associated protocols**

HG dynamometer (Fig. 2a) has been used to provide quantitative strength values in ICU patients who are sufficiently cooperative and have an MRC score  $\geq 3$  in at least four of six muscle groups being tested [11]. Different experimental protocols have been used to quantify voluntary strength by HG, *i.e.* measurements are not fully standardized among studies in ICU patients [31]. A majority of studies followed the recommendations of the American Society of Hand Therapists by performing testing in a seated position [10, 19, 27, 32– 37] while other investigations used a supine position to

take into account the patients' inability to maintain a stable vertical position [11, 24, 38–41]. Both shoulder and forearm were in neutral/rotation position when testing in seated position while the elbow joint angle varied from 90° of flexion to full extension when testing in supine position.

HHD (Fig. 2b) have been used to assess voluntary strength in several muscle groups from awakening to ICU discharge. Voluntary force measurements can be performed in both lower and upper limb muscle groups (*i.e.* wrist extensors, elbow flexors and extensors, shoulder extensors, abductors and rotators, hip fexors and extensors, knee extensors, ankle dorsifexors) in less than 15 min  $[42]$ . As for HG, HHD does not require any complex training for the physician/investigator. The protocol is carried out in a supine position to avoid measurement errors due to gravity and to consider the inability of ICU patients to remain seated at the edge of the bed [39, 43]. Knee extension force measurements have been performed with either the test leg positioned over a bolster [39, 40] or at 30° [38] to 90° [11] of knee fexion. Considering these diferences in testing position,



methodological guidelines have been provided to standardize HG and HHD force measurements in ICU patients [11, 19, 39].

#### **Reliability**

Intra-investigator reliability of HG measurements has been reported to be excellent in ICU patients  $(ICC=0.86-0.92)$ , although lower than that observed in healthy subjects  $(ICC=0.97-0.99)$  [39]. Inter-investigator reliability was also good to excellent for HG in ICU patients (Table 2), as illustrated by the ICCs ranging from 0.88 to 0.97 [19, 24, 39]. Again, higher ICCs were found in healthy subjects (0.96 and 0.97) as compared to ICU patients (0.89 and 0.92) [39].

Excellent intra-investigator reliability of HHD measurements was obtained in all muscles but the left elbow





Intraclass Correlation Coefficients (and their 95% Confidence Interval) are reported

*W* women, *M* men, *R* right, *L* left

flexors (ICC =  $0.42$ ). This later finding could be explained by the presence of radial arterial lines during the initial measurements [39]. Inter-investigator reliability of HHD was good to excellent [11, 39] (except for the elbow fexors, Table 2). However, Vanpee et al. [11] reported higher ICCs for elbow flexion and knee extension as compared with those measured by Baldwin et al. [39]. This could be related to several methodological diferences between the two studies, such as the defnition of awakening, the testing position, the use of visual feedback during force measurements, the age of the patients, the length of stay at the frst force assessment and the experimental design.

#### **Voluntary force in ICU patients: cross‑sectional, longitudinal and diagnostic approaches** *Cross‑sectional approach*

Absolute HG forces largely varied between studies and ranged from 3 to 20 kg during the first week of admission [32, 36, 44] and from 6 to 16 kg [19, 24, 32, 39–41] over the second and third week (Table 3). Absolute HHD forces ranged from 8 to 12 kg for knee extension and elbow extension after a median ICU stay of 13–16 days [39, 40]. Several factors can explain the large differences among studies. Both age and the proportion of men could infuence absolute force values [24, 45]. Older patients (>80 years old) had lower HG absolute force values than their younger counterparts after ICU discharge [45]. It has also been reported that women had a median HG score of 0 kg while men obtained a median score of 20 kg when measurements were performed around 9 days after awakening  $[24]$ . In addition, the longer the mechanical ventilation, the lower the absolute grip force values (Table 3) [32]. Severity of illness (*i.e.* APACHE III) was also higher and HG force was lower in patients with ICUAW as compared with patients without ICUAW [10].

To take into account these diferences, HG and HHD force has been normalized to age- and sex-matched values recorded in healthy controls to obtain relative/predictive values, *i.e.* values that patients should get if they had no ICUAW. Relative HG force values ranged from 12 to 37% of predicted values during the frst week of ICU stay [32, 36, 44] (Fig. 1). This heterogeneity can also be due to diferences in duration of MV and ICU stay and disease severity. Surprisingly, the lowest relative force values (12% of predicted values) were observed in a specifc cohort of patients admitted to surgical ICU and having a very short MV (median of 3 days) and ICU stay (median of 5 days) duration  $[44]$ . This unexpected result could be related, at least in part, to the fact that 55% of the patients had HG force of 0 kg  $[44]$ .

HG, elbow flexion and knee extension relative force values ranged from 25 to 39% of predicted values (Fig. 1) and from 51 to 54% in the late phase of ICU admission (12–16 days) [32, 40] and at hospital discharge [33, 35, 36], respectively. Interestingly, patients with septic shock displayed lower predictive values than patients with only severe sepsis [33], illustrating the impact of disease severity on force production. Despite the use of relative/predictive values, diferences in the clinical status of patients and in the normative database [46–48] clearly limit the comparison of voluntary force measurements among studies in ICU patients.

#### *Longitudinal approach*

To circumvent the aforementioned issues, longitudinal voluntary force measurements have been performed with both HG and HHD during ICU stay [41, 49]. HG force remained unchanged from day 1 to day 5 of awakening (*i.e.* the initial strength measurements were performed at a median ICU stay of 3 days) [36] or declined throughout the ICU stay (*i.e.* -0.34 lb-force per additional day of MV ventilation, especially in older women) [41]. Force recorded by HHD was reduced by 10–13% from day 3 to day 7 of ICU stay [49]. Altogether, these fndings indicate that force does not recover within the frst days of awakening.

Changes in voluntary force production between ICU and hospital discharge are still unclear. Indeed, knee extension force remained unchanged [38] while higher HG force values were reported at hospital discharge as compared with ICU discharge, although no statistical analysis was performed between the two measurements [35, 50]. ICUAW patients were always weaker than patients without ICUAW at both ICU and hospital discharge [35]. Further longitudinal studies are needed to determine the time course of voluntary force production from awakening to hospital discharge.

#### *Diagnostic approach*

The ability of HG to diagnose ICUAW has been investigated and cut-off values of less than 11 kg in men and less than 7 kg in women (Fig. 1) allowed to discriminate ICUAW with a sensitivity of 0.81 and a specifcity of 0.83 [10]. In addition, MRC scores were positively correlated with HG force values. The use of HG as a surrogate to MRC to diagnose ICUAW was further confrmed by Parry et al. [24] with a sensitivity of 0.88 and a specificity of 0.80. However, the specifcity was lower in women (0.45–0.55) than in men (0.88–0.92), despite a perfect sensitivity for women  $(i.e. 1.0)$ . The lower specificity in women was explained by a very large number of women (14 out of 16) with a grip strength of 0 kg. Finally, the cut-off values of Ali et al.  $[10]$  were further confirmed in another population of ICU patients [34]. Lower cutoff values (*i.e.* 7 kg for men and 4 kg for women) were reported in septic patients diagnosed with CIPNM [27].







However, these results should be interpreted with caution considering the above-mentioned methodological limitations of this study [27]. Surprisingly, no study has investigated if HHD could be used to diagnose ICUAW despite its good to excellent reliability (Table 2 and Fig. 1).

#### **Limitations**

Normative database of voluntary force vary among studies which limits the interpretation of cross-sectional studies. In addition, patients must be sufficiently awake/ cooperative to be able to develop a voluntary force and should have an MRC score higher than 3 in elbow fexion and wrist extension [19]. However, criteria used to defne awakening state have not been standardized between studies [11, 39]. In addition, HG force measurements had a significant floor effect with  $\sim$  25–55% of patients having a score of 0 kg  $[24, 44, 51]$ . This could be related to the diagnosis of ICUAW [24], lack of alertness or motivation as well as fatigue and pain associated with the disease. Finally, the frst voluntary force measurements are usually performed after a median ICU stay ranging from 3  $[36, 44, 49]$  to 16 days  $[40]$ . In this context, non-volitional force measurements could be an attractive alternative to HG/HHD in order to provide an earlier characterization of neuromuscular function in sedated patients (Fig. 1).

#### **Evoked force**

#### **Existing ergometers and associated protocols**

Non-volitional force measurements can be obtained in sedated patient using an ergometer consisting of a force transducer and an adjustable platform combined with supramaximal stimuli applied either over a motor nerve or a muscle belly  $[52]$ . The most used technique is electrical stimulation  $(ES)$  [53] that usually allows to spatially recruit all motor units. Magnetic stimulation (MS), which consists in applying a magnetic feld over a motor nerve through an ergonomic coil to depolarize motor axons, has been introduced as an alternative to ES [54] to limit discomfort. The main advantages of evoked force either with ES or MS rely on the possibility to assess muscle force in sedated patients in the very early phase of ICU admission (*i.e.* within 24 h of ICU admission, [15]). Evoked force can be obtained in response to single twitch (Tw), paired pulse and/or trains of stimulations [52]. So far, diferent ergometers have been developed allowing to record evoked force in response to ES and/or MS in ICU patients on three muscle groups (Fig. 2c–e): adductor pollicis  $[12, 13, 55]$ , ankle dorsifiexors  $[15, 56]$  and quadriceps [14, 57, 58].

#### *Adductor pollicis (AP)*

The first ergometer to assess AP force in ICU patients was inspired by a device (Fig. 2c) previously developed by Merton [59]. Forearm and hand are immobilized in supinated position in an arm board. An adjustable metal loop connected to a strain gauge is positioned around the proximal phalanx of the thumb to record evoked force in response to stimulation applied over the ulnar nerve. The thumb is abducted and the metacarpophalangeal and interphalangeal joints are fully extended.

#### *Ankle dorsifexors*

The ergometer used to assess the ankle dorsiflexors force in response to peroneal nerve stimulation (Fig. 2d) combines a boot fxed on an adjustable footplate with a strain gauge to record the evoked force [15, 56, 60]. The system can be adjusted to fit the patient's leg that is frmly maintained using non-elastic straps. The patient is lying in bed, with the leg fully extended, the other one being maintained to avoid unwanted motion during the stimulation.

#### *Quadriceps*

Three different ergometers have been developed so far (one of them is shown on Fig. 2e), to record quadriceps force production in response to stimuli applied either over the femoral nerve  $[58, 61]$  or the muscle belly  $[14]$ . The ergometers have been designed to optimize knee and hip angle joint angles when patient is in supine position. The tested leg is positioned on a support and a strain gauge is attached next to the malleolus perpendicularly to the leg axis.

#### **Reliability**

Reliability of evoked-force measurements has been scarcely investigated in ICU patients. No studies have measured intra- or inter-investigator ICC values and only a few investigations have reported coefficient of variations (CV) between two measurements. Intrainvestigator reliability of magnetically-evoked Tw forces was found to be good in AP muscle (CV of 7.8% [3–9%]) [13]. Data extraction from Laghi's et al. study [58] indicated an excellent intra-investigator reliability of quadriceps evoked force recorded in response Tw and paired pulse MS stimulations in ICU patients (CV of 1.9% [0.6–7.7%] and 1.5% [0.2–3.4%], respectively). In the same way, a good reliability of quadriceps Tw measurements in response to MS was also suggested on the basis of Bland–Altman comparison of values recorded in sedated and awake patients [61]. Only one study investigated the reliability of evoked force using ES and reported an excellent intra-investigator variability in ICU patients (*i.e.*  $CV = 6\%$ ) [56].

#### **Evoked force in ICU patients: cross‑sectional and longitudinal approaches** *Cross‑sectional approach*

AP Tw force production in response to MS was 40% lower in ICU patients (at a length of stay: ∼18.5 days) as compared with healthy subjects (*i.e.* 4.2 N [2.2–6.7 N] vs. 7 N [4.4–9.8 N], respectively) [13]. Electrically-evoked force recorded (within 24 h of inclusion) on the AP muscle in response to a 30 Hz stimulation train was 69% lower in ICU patients (mean MV duration: $\sim$  14 days) than in healthy subjects after a 2-week immobilization period to mimic disuse associated with ICU (*i.e.*  $20 \pm 16$ *vs*  $65 \pm 19$  N, respectively) [55]. This suggests that factors other than immobilization are involved in muscle weakness. Ankle dorsifexors evoked force in response to ES was reduced by  $\sim$  20% for Tw and by  $\sim$  40% for trains of stimuli after one week of ventilation and ICU stay as compared to healthy volunteers [56].

Quadriceps evoked Tw force in response to MS was four times lower in ICU after a mean stay of 7 days than in healthy subjects  $[58, 61]$ . When considering quadriceps force in response to paired pulse MS stimulations, values were $\sim$  54% lower in ICU patients (MV duration: $\sim$ 10 days) as compared with healthy subjects  $(i.e. 10.2 \text{ vs. } 22.1 \text{ kg, respectively})$  [58]. Finally, the ratio between the force evoked by a tetanic stimulation at 10 Hz to the force evoked by a tetanic stimulation at 50 Hz has been found to be higher in ICU patients with sepsis than in controls  $[12]$ . The clinical relevance of this index is unclear and no information on the magnitude of muscle weakness was provided in this study. In summary, although the clinical conditions varied between these studies, ICU patients showed large reduction in evoked force in both upper and lower limb muscles (Table 4 and Fig. 3).

#### *Longitudinal approach*

There is a paucity of studies that assessed the time-course of changes in evoked force in ICU patients. In a small cohort of 8 patients, seven of them showed a gradual decrease in electrically-evoked ankle dorsifexor force during the ICU stay  $[60]$ . Interestingly, force significantly recovered after weaning of MV in ICU survivors but continued to decrease in the two patients who eventually died. In addition, ankle dorsifexor force recorded within the 24 h of admission was already lower than that recorded on similarly aged healthy controls, suggesting that muscle weakness may be related to the infuence of both critical illness and the presence of associated comorbidity [15]. In this study, muscle weakness was

**Table 4** Main outcomes from studies measuring evoked force in ICU patients

References	Muscle	Stimulation technique	Number of patients (controls)	Duration of ICU stay or MV <sup>5</sup> (days [range])	Main results
Finn et al. [12]	<b>Adductor Pollicis</b>	FS	44 (26)	$9.5$ [0-38]	F10/F50 <sup>*</sup> ratio was higher in patients than in controls
Harris et al. [13]		ES & MS	12(38)	$18.5$ [1-89]	Force was 40% lower in patients as compared with controls
Eikermann et al. [55]		ES	13(7)	13.5 $[5-23]$ <sup>\$</sup>	Force was 69% lower in patients as compared with controls
Connolly et al. [15]		ES	21	$13 [9 - 25]$	Force was lower within the 24 h of admission in patients as compared with control values obtained in healthy subjects Force remained unchanged when recorded 7 days after the initial measurements
Ginz et al. [56]	Ankle Dorsiflexors	ES	19(20)	$7$ [N/A]	Force was 20-40% lower in patients as compared with controls
Ginz et al. [60]		ES	8	$5 [2 - 10]$	Force decreased during the ICU stay and recovered after weaning of MV in ICU survivors
Silva et al. [14]	Quadriceps	$ES^{\#}$	30(30)	$23$ [15-26]	Force decreased by $\sim$ 25 and $\sim$ 36% after 14 days of MV
Laghi et al. [58]		<b>MS</b>	12(50)	9.9 $[1-22]^{5}$	Force was 54% lower in patients as compared with controls
Vivodtzev et al. [61]		<b>MS</b>	13(8)	$7$ [N/A]	Force was 75% lower in patients as compared with controls

\* F10/F50: ratio between the forces produced by a 10 Hz stimulation train to the force produced by a 50 Hz stimulation train

Electrical stimulation was applied over the quadriceps muscle belly; ES: electrical stimulation; MS: magnetic stimulation; MV: mechanical ventilation; N/A: Not available



not further exacerbated when force was recorded 7 days after the initial testing. On the contrary, quadriceps electrically-evoked force decreased by  $\sim$  25% and by  $\sim$  36% at day 7 and day 14 of ICU stay [14], respectively.

#### **Limitations**

Although both ES and MS techniques seem to be reliable to record evoked-force in ICU patients, these results have been obtained on small cohorts of patients (*i.e.*  $n < 15$  patients). There is so far no-commercially available ergometer allowing for evoked-force measurements at the beside and these investigations require specialized expertise. Discomfort associated to ES may prevent longitudinal force measurements in ICU patients after awakening  $[12, 56]$ . The level of discomfort is lower when using MS but the conditions of stimulation supramaximality with MS may not be met in overweight/obese patients [62] or in patients with edema which represent a large proportion of ICU patients. It is unclear whether and to what extent force measurements on a single muscle group may be representative for generalized muscle weakness.

#### **Conclusions and perspectives**

Over the last decade, force evaluation at patient bedside evolved from subjective to objective/quantitative measurements. Non-invasive electrical and/or magnetic evoked force measurements could be a relevant strategy to characterize muscle weakness in the early phase of ICU (*i.e.* in sedated patients). However, there is still a paucity of ergometers adapted to routine clinical practice and the reliability of evoked force measurements remains to be carefully investigated. Only a few longitudinal studies have characterized changes in evoked force from admission to awakening and/or to hospital discharge. Moreover, unlike with voluntary force measurements, the link between evoked force measurements and the diagnosis of ICUAW remains to be established. Overall, prospective multicenter ICU cohort studies are needed to determine whether and to what extent (e.g. cutoff values) evoked force measurements can be used as a valid surrogate of MRC for ICUAW diagnosis. This would allow to identify ICU patients most at risk early and will subsequently enable tailored interventional strategies, which can be delivered in the critical period to try to minimize the related alterations of neuromuscular function. Bedside ergometers could also be used to provide a comprehensive characterization of skeletal neuromuscular function in fully cooperative patients in order to get information on maximal voluntary force (as usually assessed by HHD), voluntary activation using superimposed stimuli on a maximal voluntary contraction (to evaluate whether and to what extent neural drive is impaired in ICU patients) and Tw properties (an index of muscle function) (Fig. 1) [52]. Evoked force measurements should also be combined with surface electromyography and ultrasound analyses, that can be easily performed at the bedside in sedated patients, in order to get a clear picture of the deleterious consequences of an ICU stay on the neuromuscular system and to improve our knowledge of the pathophysiology of ICUAW. The application of ES over the muscle belly (also refers to as neuromuscular ES) has been considered as a potential strategy for limiting/preventing muscle weakness/ atrophy in ICU patients. However, its efectiveness is still equivocal in ICU patients [14, 63], one reason likely being methodological limitations. Indeed, the force produced in response to the stimulation, known as the main determinant of neuromuscular ES efectiveness [64], has never been accurately quantified in ICU patients. Therefore, the use of bedside ergometers could also allow to objectively quantify the individual contractile response to neuromuscular ES and identify potential responders to neuromuscular ES.

#### **Supplementary Information**

The online version contains supplementary material available at [https://doi.](https://doi.org/10.1186/s13054-021-03567-9) [org/10.1186/s13054-021-03567-9](https://doi.org/10.1186/s13054-021-03567-9).

**Additional fle 1**: Search strategy used for the review

**Acknowledgements** We thank Isabelle Millet for drawing Fig. 2.

#### **Authors' contributions**

DK, EL, GYM and JG contributed to the conception and design of this review. DK and EL extracted the data. DK, EL, GYM and JG interpreted and synthesized the data. DK, EL, GYM and JG wrote the draft manuscript. All authors contributed to and revised the fnal manuscript. All authors read and approved the final manuscript.

#### **Funding**

This work was funded by an Idex Fellowship (to GYM).

#### **Availability of data and materials**

Not applicable.

#### **Declarations**

**Ethics approval and consent to participate** Not applicable.

#### **Consent for publication**

Not applicable.

#### **Competing interests**

The author(s) declared no potential conficts of interest with respect to the research, authorship, and/or publication of this article.

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# Received: 3 February 2021 Accepted: 5 April 2021

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