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Combining fluorescence fluctuations and photobleaching to quantify surface density

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Abstract

We establish a self-calibrated method, called *pbFFS* for *photobleaching Fluctuation* Fluorescence Spectroscopy, which aims at characterizing molecules or particles labelled with an unknown distribution of fluorophores. Using photobleaching as a control parameter, pbFFS provides information on the distribution of fluorescent labels and a more reliable estimation of the absolute density or concentration of these molecules. We present a complete theoretical derivation of the pbFFS approach and experimentally apply it to measure the surface density of a monolayer of fluorescently tagged streptavidin molecules that can be used as a base platform for biomimetic systems. The surface density measured by pbFFS is consistent with the results of spectroscopic ellipsometry, a standard surface technique. However, pbFFS has two main advantages: it enables in situ characterization (no dedicated substrates are required) and is applicable to low masses of adsorbed molecules, as demonstrated here by quantifying the

density of biotin-Atto molecules that bind to the streptavidin layer. Besides molecules immobilized on surfaces, we also applied pbFFS to molecules diffusing in solution, to confirm the distribution of fluorescent labels found on surfaces. Hence, pbFFS provides a set of tools to investigate molecules labelled with a variable number of fluorophores, with the aim to quantify either the number of molecules or the distribution of fluorescent labels, the latter case being especially relevant for oligomerization studies.

Introduction

Biomimetic approaches are popular in medical applications and cellular studies. As the extracellular matrix (ECM) plays a complex role on cell response to drugs, growth factors and morphological cues, ¹ it is advantageous to design biomaterials mimicking the natural environment of cells in the body for enhancing the efficiency of biomedical products. Moreover these biomaterials can bring a deeper understanding of the influence of selected components of the ECM on cellular processes such as proliferation, migration and differentiation. ² Developing these platforms requires a precise control of the immobilized compounds. Standard surface techniques include spectroscopic ellipsometry and quartz crystal microbalance with dissipation monitoring (QCM-D). ^{3,4} However, these techniques are *ex situ* since the platforms have to be built on auxiliary substrates, which may affect the functionalization process. Moreover, low masses of adsorbed molecules cannot be detected by the above techniques. Fluorescence-based methods would, in principle, allow *in situ* characterization (i.e. with the substrates used for cellular studies), as well as detection of small surface densities of adsorbed molecules.

Using fluorescently-labelled molecules, a simple image provides relative information on molecular density through its intensity, but estimating the absolute value of the number of molecules requires additional and fragile calibrations.⁵ There are alternative approaches based on single molecule strategies, but they are adapted only for very low surface densities.⁶ On the other hand, Fluorescence Fluctuation Spectroscopy (FFS) techniques,⁷ and

more specifically Image Correlation Spectroscopy (ICS) which is suited to the characterization of immobile molecules, are intended for absolute quantification. These methods derive historically from Fluorescence Correlation Spectroscopy (FCS) and are based on the notion that signal originating from a submicrometric region within the sample, corresponding to the Point Spread Function (PSF) of the microscope, exhibits statistical fluctuations, since this PSF region does not always include the same number of molecules. The relative amplitude of these fluctuations provides an estimation of the average number of molecules in the PSF region and hence the concentration or density. Molecules cross the PSF either by spontaneous motion, as in the case of FCS, or by scanning the excitation laser (as in confocal microscopy), as in the case of ICS. ICS has been used to assess oligomerization, or qualitatively detect the presence of aggregates through an increase of brightness or a corresponding decrease of number density. 9,10

In fact, standard FFS techniques can only provide reliable quantitative information if all molecules have the same brightness (or if the distribution of brightness is known). Yet commercially available large proteins are rarely all labelled with the same number of fluorophores, so that they present a distribution of brightness. In this case, the number density of fluorescent entities (molecules or particles) estimated by conventional FFS is underestimated: indeed, part of the measured fluctuations would be due to variations in brightness and not only in number of entities, as usually assumed in FFS. More precisely, if the brightness distribution is characterized by a mean value, $\bar{\epsilon}$ and a standard deviation, σ_{ϵ} , it can be shown (following ^{9,11}) that the mean number of entities in the PSF volume or area, as measured by FFS, is related to the true number of entities, N, by:

$$N_{FFS} = \frac{N}{1 + (\sigma_{\epsilon}/\bar{\epsilon})^2} \tag{1}$$

Consequently, the wider the brightness distribution, the more pronounced the underestimation of the number density. The same bias affects the estimation of average brightness (which tends to be overestimated). Using only standard FFS methods, there is no way to evaluate this bias.

The present work aims at using photobleaching as a control parameter to measure accurately the density of surfaces coated with multiply-labelled entities. The combination of FFS and photobleaching has been proposed previously and used to estimate the degree of fluorescent labelling, ¹² the size of oligomers ^{13,14} or the surface density of molecules. ¹⁵ However the practical implementations were either limited to the specific case of a Poisson distribution of brightness, ^{12,15} or failed to decipher the real parameters that could be deduced from the photobleaching decay. ^{13,14} We present here a complete theoretical description of a method combining ICS to photobleaching, which is not specific to ICS and can be extended to other FFS techniques (for instance FCS, as in ¹²): we name it *pbFFS* for *photobleaching FFS*. Compared to previous work, we present a more in-depth theoretical derivation. We show that the measured brightness always decays linearly with photobleaching, whatever the distribution of fluorescent labels, and hence exactly two outputs can be extracted from this decay: (i) the brightness of a single fluorescent label, (ii) a factor depending on the mean and variance of the number of fluorescent labels per entity. We stress the fact that the presented method has the advantage to be *calibration free*.

The pbFFS method is experimentally validated on substrates covered with monolayers of streptavidin molecules via a linker, used as a platform to build biomimetic surfaces step by step by adsorbing biotinylated molecules on top of it. ^{3,16} We applied pbFFS to streptavidin (SAv), fluorescently tagged with Alexa (SAv-Alex). Thanks to an additional assumption about the fluorescent labelling, we could bracket the mean number of fluorescent labels per SAv and, hence, estimate the absolute number density of SAv molecules covering the substrate. The resulting densities have been validated by independent spectroscopic ellipsometry measurements. We show that pbFFS is capable of measuring SAv surface densities that span over two orders of magnitude. Then, pbFFS was used to quantify the number of biotinylated fluorescent molecules (Atto labelled biotin, bAtto) that attach to a streptavidin base layer.

In this case, the mass of adsorbed molecules was too low to be measured with accuracy by QCM-D or ellipsometry (since the mass of bAtto is only 1 kDa as compared to SAv which is 55 kDa). Interestingly, we also found by performing control photobleaching-FCS experiments that bAtto molecules are prone to aggregation in solutions, which potentially impacts the way they bind to the SAv base layer.

Principles of photobleaching Fluctuation Fluorescence Spectroscopy

As illustrated in Fig. 1A and D, a pbFFS experiment consists in alternating photobleaching phases, where a high laser power is sent into the sample to bleach a fraction of the fluorescent labels (e.g. Alexa) borne by the entities (e.g. streptavidin) and measurement phases at a reduced laser power. During the latter, the fluorescence signal, F, the mean number of entities, N_{FFS} and the brightness, defined as $B_{FFS} = F/N_{FFS}$, are measured. As more fluorescent labels are photobleached, the image intensity (in ICS, Fig. 1B) or the photon count rate (in FCS, Fig. 1C) decreases, while the autocorrelation amplitude increases, denoting a reduction of the number of entities N_{FFS} in the PSF submicrometric region.

We consider a sample consisting of entities labelled with multiple fluorophores of identical brightness, ϵ . The distribution of the number of these labels per entity before photobleaching is characterized by its mean and its standard deviation, named respectively m and σ . It can be shown (see Section S1 of the Supporting Information (SI)) that the measured brightness B_{FFS} is an affine function of the photobleaching stage p, defined as the fluorescence signal normalized to its initial value, i.e. p = F/F(1):

$$B_{FFS}(p) = \epsilon (1 + S_{\sigma m} p) \tag{2}$$

where $S_{\sigma m}$ is the slope normalized by the single label brightness. It is related to the standard

deviation and mean value of the distribution according to:

$$S_{\sigma m} = \sigma^2/m + m - 1 \tag{3}$$

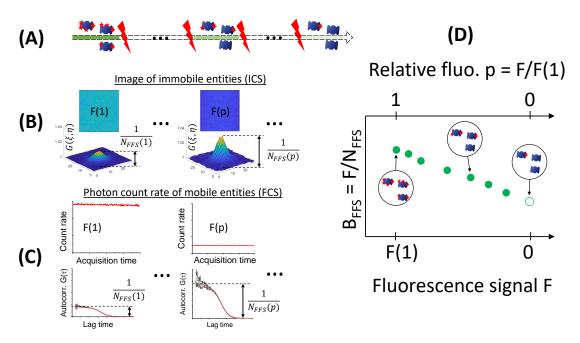


Figure 1: Principle of a pbFFS experiment. Part (A) shows, along the dashed arrow, the photobleaching phases (red flashes) that alternate with the measurement phases (green sections of decreasing intensities). During the latter, the number of unbleached fluorescent labels borne by the entities decreases. The fluorescence signal, F, corresponds to the mean image intensity of immobilized fluorescent entities measured by ICS (B), or to the mean photon count rate of mobile fluorescent entities measured by FCS (C). The number of entities measured by FFS, N_{FFS} , also decreases as can be seen by the increased amplitude of the spatial autocorrelation in ICS, $G(\xi, \eta)$, or temporal autocorrelation in FCS, $G(\tau)$. Part (D) shows that the brightness measured during the successive phases, defined as $B_{FFS} = F/N_{FFS}$, plotted vs the fluorescence signal, monotonously decreases upon photobleaching and tends towards that of a single fluorescent label.

The true total number of entities is then given by:

$$N = F(1)/m\epsilon \tag{4}$$

The linear decay of the measured brightness versus the fluorescence signal is valid for any

distribution of fluorescent labels, assuming that all fluorescent labels have the same brightness, ϵ and a constant probability to bleach, whatever their number in the entities. A straightforward result of any pbFFS experiment is the single label brightness, ϵ . This is an interesting output since, using Eq. 4, one can derive the total number of fluorescent labels, $Nm = F(1)/\epsilon$. The exploitation of the slope, $S_{\sigma m}$, is more complex, because we see from Eq. 3 that, in the general case, it is impossible to independently determine the mean value, m and the standard deviation, σ , of the number of fluorescent labels per entity. However, specific fluorescent label distribution add constraints such that, in practice, the m values are reduced to some range (For details see Section S2 in SI). This is the case for the SAv monolayer, as discussed in the next section.

Implementation of the analysis method

Effect of background

When performing pbFFS experiment we sometimes observe, both on surface and in solution, photobleaching decays that do not exhibit a linear behavior (as the red line in the schematic Fig. 2A), but drop down to lower values of the brightness when the fluorescence signal gets small (green curve). This is due to an uncorrelated background, BG, that contributes to the detected signal, thus making the relative fluctuations smaller and consequently the apparent number of entities larger, hence a lower brightness, as described in. ¹⁷ It is nevertheless possible to incorporate the background as a free parameter in the photobleaching decay analysis by rewriting Eq. 2 as:

$$B_{FFS}(p) = \epsilon \left(1 - \frac{r_{BG}}{p} \right) \left(1 + S_{\sigma m} \frac{p - r_{BG}}{1 - r_{BG}} \right) \tag{5}$$

where $r_{BG} = BG/F(1)$ stands for the background normalized to the total initial signal (i.e. including the background itself). Correspondingly, p becomes the relative total signal,

including the background. The latter originates, either from light scattering (due to the glass substrate or to the walls of the PDMS microwells), or from some bulk fluorescence that would be not properly filtered out by the confocal detection. This effect appeared to be especially pronounced and difficult to mitigate in solutions. The fit of the photobleaching decay shown in Fig. 2A thus gives the parameters ϵ , $S_{\sigma m}$ (and BG, if relevant).

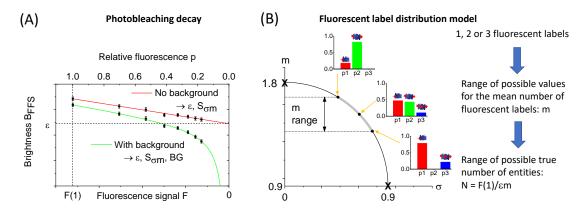


Figure 2: Schematics of the implementation of the brightness decay analysis: (A) Upon photobleaching, the brightness, B_{FFS} , decreases linearly versus the fluorescence signal, F or p (red solid line), thus providing the output parameters ϵ and $S_{\sigma m}$; in case of background (green solid line) an additional parameter, BG, can be estimated by fitting the decay (see text for details). (B) By combining the relation between m and σ corresponding to the measured value of $S_{\sigma m}$ and the constraints deriving from three non-nil probabilities (p_1, p_2 and p_3 for 1, 2 or 3 fluorescent labels), the possible m values are restricted to a limited range; three examples of distributions of probabilities corresponding to the minimum, maximum and central values of m are depicted for $S_{\sigma m} = 0.8$. Finally, this analysis provides a value of the mean number of fluorescent labels, m, which combined with the initial fluorescence signal, F(1) and the parameter ϵ , leads to an estimation of the true number of entities, N.

Taking into account the fluorescent label distribution

The degree of fluorescent labelling of SAv-Alex given by the manufacturer being 2, we take this number as an approximate value and consider that each SAv protein can bear 1, 2 or 3 Alexa labels, with probabilities p_1 , p_2 and p_3 . The key point is that this discrete distribution of probabilities has only 2 independent degrees of freedom (since, once the probabilities p_1 and p_2 are known, the last one, p_3 , automatically follows). Additionally, we show in SI, Section S1, that, due to Eq. 3, the σ , m values are constrained along a circle. Combined

with the properties of the distribution, this leads to a limited range of possible mean number of fluorescent labels. In our current situation, it can be shown (see SI, Section S2, Eq. S11 to S15 and Fig. S1) that if $S_{\sigma m} \leq 1$, then $\frac{3}{3-S_{\sigma m}} \leq m \leq \frac{2}{2-S_{\sigma m}}$, while if $1 < S_{\sigma m} \leq 2$, then $\frac{3}{3-S_{\sigma m}} \leq m \leq \frac{6}{4-S_{\sigma m}}$ (we never measured $S_{\sigma m} > 2$). Fig. 2B schematically shows a few examples of distributions of probabilities (p_1, p_2, p_3) , which correspond to the value $S_{\sigma m} = 0.8$ that is often found for SAv-Alex, spanning from the narrowest distribution (minimum value of σ), with the largest mean value, m, to the widest one, with the smallest m. Clearly, the latter distribution is unrealistic, as it would correspond to SAv proteins that never bear 2 fluorescent labels, while most of them bear 1 fluorescent label and some 3! It can be shown (SI, Section S2) that the condition to have a probability to bear 3 fluorescent labels smaller than that for 2 implies $m > \frac{1}{1-\frac{3}{8}S_{\sigma m}}$.

Interestingly, if we had hypothesised that SAv proteins could bear 2, 3 or 4 Alexa labels, this would lead to, either no solution when $S_{\sigma m} < 1$ or, for the few cases where we measured $1 \le S_{\sigma m} \le 1.5$, to a vast majority of SAv molecules bearing 2 Alexa labels and almost none bearing 3 or 4, which is consistent with the model retained throughout this work (see Section S2 of SI, Eq. S16).

Concerning the biotinylated fluorescent molecules, it is clear from the bAtto formula (given in the product specification) that they correspond to one single Atto dye. However, as already noted above, as a SAv protein of the base layer exposes from 1 to 3 free biotin binding sites, several bAtto molecules can colocalize on a single SAv protein. Therefore, we also assume that biotinylated entities can bear 1, 2 and 3 fluorescent labels.

To conclude, from the analysis of the brightness decay, we obtain a range of values for m, and hence a range of values for the true number of fluorescent entities, $N = F(1)/m\epsilon$, which in turn leads to the final surface density given by $N/\pi w_r^2$.

Experimental results

Streptavidin layers are densely packed

Photobleaching ICS experiments have been performed on SAv layers with different percentages of fluorescently labelled SAv (SAv-Alex) of 1%, 10%, 50% and 100%. Since ICS usually performs better for relatively low surface densities, these dilutions aimed at testing the robustness of our method in a range of densities relevant for biomimetic surfaces. See Section S4 of SI about sample preparation, acquisition protocol and data analysis.

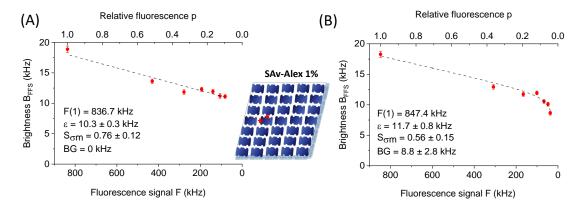


Figure 3: Characteristic brightness decay versus the fluorescence signal for a SAv layer prepared with 1% dilution of SAv-Alex. (A) Example without background (i.e. fixed to 0), showing the linear decay and the fit (dashed black line) with the ϵ and $S_{\sigma m}$ outputs corresponding to the measured (red) points; the errors bars are the standard errors of the mean calculated from 8×8 sub-images; (B) In presence of background, the corresponding parameter, BG, can be fitted (it represents about 1% the initial fluorescence signal, F(1)), while the other outputs, ϵ and $S_{\sigma m}$, are consistent with the results of the background-free case.

We see in Fig. 3A a plot of a characteristic brightness decay versus the fluorescence signal obtained for 1% dilution of SAv-Alex. The parameters estimated from the fit, $\epsilon = 10.3$ kHz and $S_{\sigma m} = 0.76$, correspond to an initial brightness, given by $B_{FFS}(1) = \epsilon(1 + S_{\sigma m})$, that is about 1.8 times larger than the single fluorescent label brightness. Consequently, if the distribution of the number of fluorescent labels per molecule was single-valued, one would be close to the situation of 2 Alexa dyes per SAv, which corresponds to the manufacturer specifications. However, using the theory presented in Section S2 of SI, we can estimate

the range of m values compatible with both the possible numbers of fluorescent labels and the estimated value of $S_{\sigma m}$ at [1.40, 1.61] (see SI, Section S2, Fig. S1 and Eq. S14). This corresponds to a surface density of fluorescently labelled SAv, at 1% dilution, in the range of 316-363 molecules per μm^2 (using $w_r = 0.22 \mu m$ for this data set). We also show, in Fig. 3B, another result obtained with the same dilution of SAv-Alex, but exemplifying the consequence of a background on the brightness decay. Although the background accounts only for about 1% of the total initial signal, the deformation from linearity of the brightness decay is very pronounced at the end of the process. However, the decay can still be well fitted using one additional parameter, BG, while the other parameters remain consistent with their values estimated without background.

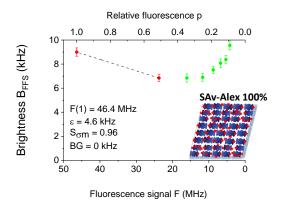


Figure 4: Example of the dramatic consequence, for the brightness decay, of the fluorescence quenching between Alexa555 fluorophores of a streptavidin layer prepared with 100% of SAv-Alex. Note that the single fluorescent label brightness, ϵ , is more than twice smaller than its value at high dilution (see Fig. 3), while the $S_{\sigma m}$ parameter, estimated from the 2 first points, stays consistent.

A physically different situation occurs at high surface densities of fluorescently labelled SAv, as shown in Fig. 4 for a layer containing 100% of SAv-Alex. This curve exhibits a dramatic brightness recovery after an initial decay. By fitting the first part of the brightness variation, assumed to be linear, we estimated the $S_{\sigma m}$ parameter at a value, 0.96, reasonably close to the one measured at 1% dilution. Conversely, the single fluorescent label brightness, $\epsilon = 4.6$ kHz, is found to be more than 2 times lower than the value measured at high

dilutions of SAv-Alex (see Fig. 3). We suggest that fluorescence quenching between identical fluorophores can explain this behavior: at 100% concentration, the mean distance between the Alexa555 dyes is of the order of the size of the streptavidin molecules, that is ≈ 5 nm. At such short distances, the reduction of the fluorescence quantum yield can be very pronounced. 18 When photobleaching occurs, the mean distance between intact fluorescent labels increases, thereby reducing self-quenching so that the brightness tends towards its normal value. Because this is not within the scope of the present work, we did not study further the exact shape of the brightness curve, but we tentatively made use of the 100% concentration results to estimate the surface density of SAv. Using the waist size found for this 100% SAv-Alex case, $w_r = 0.25 \mu m$ and m = 1.7 (middle of the range corresponding to $S_{\sigma m}=0.96$), we estimate 30330 streptavidin molecules per μm^2 . First, this number is close to 100 times the surface density measured at 1% dilution. Second, it corresponds to a mean distance of 5.7 nm between streptavidins, which is consistent with the assumption of a densely packed layer, given the size of a streptavidin molecule. 19 Therefore, although based solely on the first 2 points, the results obtained for 100% of fluorescently labelled SAv are compatible with the lower-density case. Experiments have also been performed with 10% and 50% dilutions, the results of which are reported and synthesized in Table 1. Overall, our SAv-Alex results are consistent with each other, with a clear trend towards more fluorescent quenching as the surface density of SAv-Alex increases.

Streptavidin in solution has the same fluorescent label distribution

In order to get an independent estimation of the fluorescent label distribution, we also applied our method to SAv-Alex molecules freely diffusing in solution. We found a value of $S_{\sigma m}$ very consistent with the estimations on surfaces (around 0.8), as illustrated in Fig. 5A. As a control case, Fig. 5B shows that Sulforhodamine B sodium salt (SRB) solutions lead to a constant brightness when photobleaching, as expected for a single dye molecule.

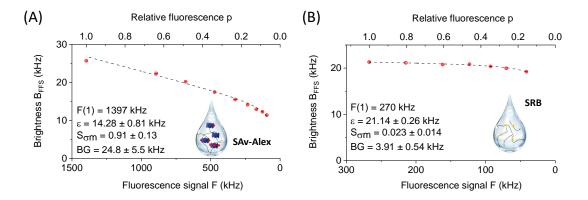


Figure 5: Examples of brightness decays measured by FCS, for solutions confined in PDMS microwells. (A) SAv-Alex molecules, where the normalised slope, $S_{\sigma m}$, is close to its value found on surfaces (see Fig. 3); (B) SRB in HEPES, clearly showing an almost constant brightness, in agreement with the expected behavior of a single dye molecule. For both cases a background of up to 2% is estimated. Note that the error bars are smaller than the point size.

Biotinylated molecules bind to about 10% of the streptavidin base layer

Next we investigated the surface density of biotinylated molecules deposited on top of SAv layers, in order to show the potential of pbFFS as a characterization tool for developing biomimetic surfaces. Fluorescent bAtto molecules bound on a streptavidin base layer were observed. The brightness decay, as shown in Fig. 6A, exhibits a normalized slope, $S_{\sigma m} = 0.21$, which is significantly smaller than the one observed for a SAv-Alex layer. This means that this case is close to the one of a single fluorescent label per labelled SAv. Assuming the same type of distribution (i.e. over 1, 2 or 3 fluorescent labels), the range of m values that corresponds to $S_{\sigma m} = 0.21$ is estimated to [1.08, 1.12] (see SI, Fig. S1 and Eq. S14). Two quantities can be estimated from these measurements: the surface density of bAtto molecules given by $F(1)/\epsilon \pi w_r^2$, which is 3708 molecules per μm^2 and the density of fluorescently labelled SAv given by $F(1)/(m\epsilon \pi w_r^2)$ with m = 1.1, center of the range estimated above, which is approximately $3370/\mu m^2$. Since we found previously ~ 30330 SAv per μm^2 in the base layer, this implies that about 1 in 10 SAv molecules can carry a bAtto molecule. Note that the areal

mass density reported, from different experiments, in Table 1 is that of bAtto molecules.

Each SAv has 4 biotin binding sites: at least one of these is used to bind to the PLL-g-PEGbiotin base layer, so that the *a priori* number of available sites for bAtto is between 0 and 3. Our data indicate that many SAv molecules could not bind any bAtto, presumably due to steric hindrance. More precisely, using $m \sim 1.1$, we can deduce that among the *fluorescently labelled* SAv, about 90% of SAv bound only one bAtto (see Eq. S12 in SI), leaving 10% that carry more than one bAtto. Two mechanisms can lead to this distribution: either bAtto bind to SAv as single molecules, in which case a few SAv have more than one occupied biotin-binding pocket, or bAtto preexist as dimers, trimers, etc. in the solution used for incubation, in which case, SAv may present only one pocket occupied by a bAtto complex. Indeed, the fact that Atto dyes are moderately hydrophilic 20 could favor aggregation.

To assess bAtto aggregation in solution, we performed pbFFS experiments with bAtto solutions (FCS), as reported in the next paragraph.

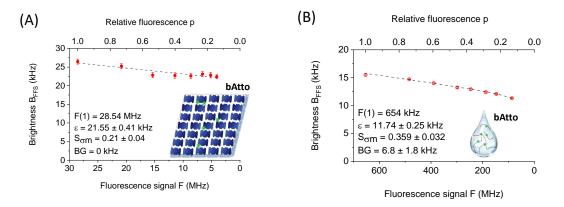


Figure 6: Brightness decay of biotinylated fluorescent molecules (bAtto), measured on surface and in solution. (A) ICS measurements for bAtto bound to a streptavidin base layer, exemplifying the lower normalised slope value, $S_{\sigma m} = 0.21$, compared to SAv-Alex (the fact that bAtto exhibits a single fluorescent label brightness different from that of Alexa555 labelled SAv is only due to the photophysical properties of these dyes); (B) FCS measurements for bAtto freely diffusing in solution. Note that the error bars are smaller than the point size.

Biotinylated molecules slightly aggregate in solution

We show in Fig. 6B an example of a photobleaching experiments with bAtto in solution. Globally, we recovered values of the normalised slope close to those found on surface (i.e. $S_{\sigma m} \approx 0.2-0.3$), which is clearly distinct from the single molecule case of SRB in solution shown in Fig. 5B. This range of values for $S_{\sigma m}$ corresponds (see SI, Fig. S1) to a mean number of fluorescent labels per diffusing entity, m, between 1 and 1.2, as summarized in Table 1. Since one bAtto molecule definitively corresponds to a single Atto dye, we conclude that unspecific aggregation occurs between bAtto molecules in solution, despite the moderate concentration ($< \mu$ M). As a consequence, although the concentrations used to incubate the SAv base layer with bAtto are much lower than those used for FCS experiments (which should mitigate the aggregation trend), we cannot exclude that each SAv has only one bAtto binding site occupied by an aggregate. In this case, the number of available biotin binding sites on the SAv layer is not that of the number of bound bAtto molecules (i.e. $3708 / \mu m^2$) but rather that of the number of SAv molecules labelled with bAtto (i.e. $3370 / \mu m^2$).

Note that the difference in brightness between bAtto in solution and on a SAv layer, shown in Fig. 6, is not relevant, as the ICS and FCS experiments are performed on surface and in bulk, respectively (with different microscopy setups). The same remark stands for SAv results shown in Fig. 5A and Fig. 3.

Table 1: Degree of fluorescent labelling (m values) and areal mass density (when applicable) measured with pbFFS for different molecules, on surface and in solution. For SAv-Alex molecules diluted at 50, 10 and 1%, the estimated areal mass density is linearly extrapolated to 100% SAv. Values are given as mean \pm SD

Molecule	Sample	Fluo. Label.	Density (ng/cm^2)
SAv-Alex	Surface 100%	1.79 ± 0.39	239 ± 34
SAv-Alex	Surface 50%	1.22 ± 0.05	303 ± 50
SAv-Alex	Surface 10%	1.94 ± 0.22	293 ± 69
SAv-Alex	Surface 1%	1.74 ± 0.36	284 ± 70
SAv-Alex	Solution	1.58 ± 0.18	n/a
bAtto	Surface	1.13 ± 0.09	0.82 ± 0.23
bAtto	Solution	1.125 ± 0.057	n/a
SRB	Solution	1.013 ± 0.011	n/a

pbFFS results agree with spectroscopic ellipsometry

We present in Table 1 the degree of fluorescent labelling (m) corresponding to different molecules, SAv-Alex, bAtto and SRB, in solution and on surfaces. For each case, the lower and upper values of the m ranges estimated for the different experiments were pooled altogether to give a mean and a standard deviation (SD) of m. When applicable, these values were then used to derive the areal mass density of SAv molecules. Although the photobleaching decay curves of 100% SAv-Alex have a limited number of exploitable points (due to the above mentioned quenching effect), the corresponding pbFFS estimation of the density is in fairly good agreement with the spectroscopic ellipsometry result that gives $246 \pm 36 \ ng/cm^2$. The linear extrapolation to 100% SAv of the SAv-Alex molecules diluted at 1, 10 and 50% tends to show a higher areal mass density, but this effect may be related to the uncertainty of dilutions. We also stress the fact that, although the degree of labelling found for 50% dilution differs from the other cases, the corresponding areal mass density stays consistent with the other results.

Concerning bAtto, the reported areal mass density of $0.82 \pm 0.23 \ ng/cm^2$ is that of the total number of bAtto molecules bound to the SAv base layer. This value holds whatever the distribution of bAtto on SAv molecules. Note that such low density could not be measured by ellipsometry, so that no comparison can be made.

Discussion

We have presented a method, named pbFFS, which aims at estimating the number density of entities of non uniform brightness. We have shown its potential for more reliable quantification of surface density in the context of biomimetic layer characterization. Hereafter, we discuss two limiting situations.

In this work, we have measured surface densities spanning two orders of magnitude, from ~ 300 to ~ 30000 molecules per μ m². This latter value is probably close to the highest

density that can be measured using ICS. Indeed, at high concentration/density of molecules, the relative intensity fluctuations and thus, the autocorrelation amplitude, are very small and may be hidden behind unwanted variations (non-uniformity of the imaging system or the sample). Therefore, it is quite important to properly flatten images, check stability of solutions, etc. High densities can also induce some detrimental photophysical effects, such as quenching. However, we experimentally showed that this does not prevent correct results, provided the biased data points are taken off from the analysis.

The streptavidin molecules studied here were labelled by 1 to 3 fluorophores, so the degree of fluorescent labelling was rather low. One may wonder whether pbFFS would also be suitable for studying entities with a higher degree of fluorescent labelling (several tens of fluorophores or more). In this case, the photobleaching process starts with entities that are initially very bright and must be carried out till only single fluorescent labels are left, which requires a high dynamic range of detection. Using fluorescent nanospheres we could check that, in principle, our framework also applies in such situations, as shown in SI, Section S3.

Besides number density quantification, some applications may benefit from the ability of pbFFS to provide information on the degree of fluorescent labelling (or number of fluorophores per entity). This would be the case of oligomerization studies. Oligomerization is an ubiquitous phenomenon that plays an important role in numerous biological processes. The size of oligomers is usually estimated using fluorescence fluctuation methods (FCS, ICS) by comparing the measured brightness to the one found on a sample containing only monomers, in the same experimental conditions. Such methods suffer from two drawbacks: first, a reference sample with only monomers may not be easily available; second, if all the oligomers do not have the same size, the result is biased resulting in an overestimation of the oligomer size. More advanced techniques have been proposed, such as SpIDA, 22 FIF 23 or eN&B 24 but still rely on the monomer brightness. The pbFFS method does not require a separate measurement on monomers, since the monomer brightness (ϵ) is provided by the fit: it is self-calibrated, which is a significant advantage. Moreover, some information on

the distribution of oligomer size can be obtained, although, as shown in this work, the exact distribution can only be resolved if the number of degrees of freedom is reduced by additional assumptions (e.g. only few possible oligomers). This strategy would work not only on fixed samples, but also in living cells. Photobleaching has been proposed in live cell, outside of the oligomerization context, to retrieve molecular brightness and to turn confocal images into concentration maps.²⁵ However this method cannot be used in cases when the studied protein forms homo-oligomers, contrarily to the present work.

Finally, we point out that, while our method contrasts with standard semi-quantitative fluorescence approaches that cannot deal with a distribution of brightness, it can be compared with some single molecules techniques based on stepwise photobleaching. ^{6,26} For instance, Madl et al. performed a combination of photobleaching and brightness analysis to measure the subunit composition of membrane proteins. ²⁷ In a recent work, Stein et al. have combined FCS with single-molecule localization microscopy to provide the number of docking strands in spatially well-separated origami nanostructures. ²⁸ However, single molecules techniques obviously require extremely low surface density of immobilized molecules, while pbFFS works in much higher density regimes, which are more relevant for most biomimetic and biological samples.

Conclusion

In this paper we presented a method, combining fluctuations analysis and photobleaching, that aims at characterizing molecules or particles fluorescently labelled with an unknown distribution of fluorophores. pbFFS can be used both on surfaces or in volume, with immobilized or moving molecules (either in flow or freely diffusing), observed in confocal or TIRF microscopy performed in photon counting mode. It provides the single fluorescent label brightness, as well as a parameter depending on the mean and variance of the distribution of fluorescent labels. If additional assumptions can be used to restrict the number of degrees

of freedom of this distribution, the degree of fluorescent labelling and an unbiased value of the concentration or density can be deduced.

The pbFFS method has been demonstrated on a SAv base layer of biomimetic samples to estimate the surface density of SAv, and its propensity to bind a top layer of bAtto molecules. For the base layer density, the density estimated with pbFFS is in agreement with ellipsometry measurements. However, compared to this latter technique or QCM-D, pbFFS has the advantage of allowing *in situ* characterization, since it does not require dedicated substrates, and allows the quantification of low mass of adsorbed molecules (as in the case of bAtto), out of reach of the other techniques, thanks to the intrinsic sensitivity of fluorescence measurements.

We believe pbFFS can provide a powerful framework to attain more reliable fluorescence fluctuations analysis: indeed, standard FFS techniques are completely unable to assess whether their results are biased by a dispersion of brightness values (or number of fluorescent labels), whereas, using pbFFS, the linear decay of the brightness during photobleaching is a simple checkpoint, which contributes to making the measurements more trustworthy.

In addition to number density estimations, the capability of pbFFS to evaluate the number of fluorophores per entity should make it particularly useful for oligomerization studies, as estimating protein oligomerization is essential to understand numerous cellular functions.

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Supporting Information Available

Section S1 - Theoretical derivation of the brightness decay and exploitation of the measurements; Section S2 - Theoretical derivation of occupancy probabilities and m value ranges; Section S3 - Results and analysis of experiments with 20 nm fluorescent beads; Section S4 - Materials and methods (PDF).

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TOC Graphic

