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Decision support in removing fractured endodontic instruments: a patient-specific approach

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Abstract: Aim: Instrumental fracture is a common endodontic complication that is treated by surgical or non-surgical removal approaches. However, no tool exists to help the clinician to choose between available strategies, and decision-making is mostly based on clinical judgment. Digital solutions, such as Finite Element Analysis (FEA) and Virtual Treatment Planning (VTP), were recently proposed in maxillofacial surgery to help in this regard. The aim of the present paper is to present a digital tool to choose between non-surgical and surgical strategies in a clinical situation of fractured instrument (FI). Material and methods: Patient tooth data were recorded using cone beam computed tomography (CBCT). VTP was conducted using an application suited for medical images to segment and plan the procedure. FEA has been carried out using the Abaqus software according to published material properties. Five models have been created: the initial state of the patient, two non-surgical removal strategies using a low or high root canal enlargement, and two surgical removal strategies using a 3- or 6-mm apicoectomy. Results: Results of the VTP found a risk of perforation for the non-surgical strategies and a sinus proximity for surgical ones. FEA identified the lowest mechanical risk for the 3-mm apicoectomy strategy. A 3-mm apicoectomy approach was finally chosen and performed. Conclusion: This digital approach could offer a decision tool for the instrument removal by planning the treatment and predicting the mechanical impact of each strategy.

Keywords: Finite Element Analysis; Virtual treatment planning; Endodontics; Apicoectomy; Instrument removal; Decision-making
Introduction

The fracture of an endodontic instrument within the root canal is a common complication of endodontic treatments (0.25 to 7.41%), most fractures occurring in the apical third of the root \(^1,2\). This fracture can affect tooth prognosis and several instrument removal strategies have been reported to complete the endodontic treatment \(^3,4\). A non-surgical strategy was proposed using ultrasonic tips to loosen the fractured instrument, but this procedure can lead to canal over enlargement or root perforation \(^5,6\). A surgical strategy was also reported to remove the instrument after performing an apicoectomy \(^7\), but it induces a reduction of the crown-to-root ratio \(^8,9\). Both strategies thus mechanically impact the tooth and the success of the endodontic retreatment \(^10,11\). Nowadays, there is no tool to guide the clinician in choosing between these strategies, and decision-making is mostly based on clinical judgment instead of scientific evidence \(^3\).

Digital approaches have been used for many years; for instance, Virtual Treatment Planning (VTP) has been used to improve the reconstruction accuracy and outcome in the maxillofacial field \(^12,13\). Similarly, patient-specific Finite Element Analysis (FEA) was reported to provide better predictions on bone fracture than what experienced clinicians predict in orthopedic practice \(^14\). In endodontics, FEA has been used to evaluate the influence of the instrument position and the resection length on the root stress distribution \(^15–17\). However, these studies used standard anatomic dimensions to create finite element (FE) models while the success rate mainly depends on patient-specific parameters such as bone loss and canal anatomy \(^6,9,18\). A recent study proposed to combine VTP and FEA for computer-aided decision-making, with the aim to predict the mechanical behavior of different maxillofacial surgeries and choose the most adapted solution for the patient \(^19\). Herein, we report a case of an endodontic instrument fracture and the application of a digital approach combining VTP and FEA to help decide between surgical and non-surgical strategies for its removal.
Case report

Case presentation

A 26-year-old female patient was addressed to the department of endodontics of the Lyon University Hospital with a instrument fractured (FI) in the root canal of her right second maxillary premolar. The 8 mm-long instrument was fractured during an initial endodontic treatment of irreversible pulpitis, one week earlier. The patient reported no pain since the fracture occurred. Clinical examination of the premolar crown indicated presence of four dental walls and a recent temporary restoration on the occlusal face. The tooth presented no cold response, no percussion or palpation tenderness, and physiological mobility. The intraoral periapical radiograph confirmed the transfixed position of the instrument, close to the sinus, and the absence of periapical radiolucency or local swelling of the sinus membrane. The patient tooth was scanned before any intervention to evaluate the instrument position using cone beam computed tomography (CBCT; Planmeca ProMax 3D, Helsinki, Finland) operating at 120 kV, 100 mAs, with a slice thickness of 0.75 mm. The data were recorded under the Digital Imaging and Communication in Medicine (DICOM) format and analyzed. Two non-surgical and surgical strategies emerged from the discussions of the healthcare team, but no consensus was reached on the treatment that could ensure the best outcome. A digital approach, combining VTP and FEA 19, was then implemented to visualize the planned treatment and predict the mechanical impact of the two removal strategies (Fig 1).

Virtual treatment planning

The different anatomical structures were segmented using DESK, an application suited for medical images 20. The semi-automatic segmentation is based on the attribution of pixel labels, “seeds”, inside each anatomical structure and a growing region algorithm. Four labels were generated according to the structures of “air”, “tooth”, “bone”, and “intra-root canal material”
to produce a multi-label 3D image. This initial 3D image was then modified to simulate the procedures of the different removal strategies.

Five clinical situations were considered by the healthcare team: the initial state of the patient, two simulated non-surgical removal strategies using a low or high root canal enlargement, and two simulated surgical removal strategies using a 3- or 6-mm apicoectomy.

An ultrasonic tip (ET25; Satelec, Bordeaux, France) was modelled by a conical cylinder 0.5 mm in diameter and a 4% taper, and recorded under STL format for VTP of non-surgical approaches. The surface of the tip was then superimposed along one third of the instrument either on the distal side of the instrument to simulate a low root canal enlargement, or on the distal and vestibular sides of the instrument to simulate a high root canal enlargement. VTP of surgical approaches was conducted with a 3- or 6-mm root shortening (Fig 2A).

The different virtual removal strategies were analyzed on the 3D modified image. The latter offers the operator the possibility to add or suppress masks of bone, ultrasonic tip or instrument to plan his procedure. For non-surgical strategies, the high enlargement was associated to a long perforation. VTP of surgical strategies were also informative on the reduction of the crown-root ratio (Fig. 2A). The 3D modified image could also be used to simulate the clinical point of view of the dental practitioner. For non-surgical strategies, the location of the instrument and the long perforation were difficult to perceive on the simulated clinical view. The clinical view of surgical strategies also enables to plan the possible access ways that avoid sinus perforation (Fig. 2B).

*Finite element modelling and mechanical analysis*

Modified 3D images were then meshed with tetrahedral elements using the Computational Geometry Algorithms Library (CGAL) meshing library 20 imported in the FEA software Abaqus (Dassault Systèmes, Vélizy-Villacoublay, France; Fig. 3). The periodontal ligament
could not be detected on the DICOM and was simulated around the root surface with a thickness of 250 μm \(^{21}\). The attributed material properties (Table 1) were referenced from the literature \(^{21-23}\). All materials were supposed homogeneous, linear and elastic, and there was a perfect bonding between each component \(^{16}\). The occlusal faces were not modelled due to x-ray artefacts. A vertical load of 150 N was distributed on the top surface of the root and the nodes of the base, and lateral faces of the bone were constrained to prevent displacement \(^{16}\). A static explicit analysis was conducted to calculate principal strains and Von Mises stresses for all FE models. The mechanical behavior of the tooth was evaluated by comparing the Von Mises stress distribution and the maximal Von Mises stress (fracture criterion) \(^{24}\) between all FE models. Each FE model was verified using a convergence test \(^{25}\) and the Zhu-Zienkiewicz error estimator \(^{26}\) (Table 2).

The apicoectomy models presented a lower fracture criterion than enlargement models and the model of the initial state of the patient. The 3-mm apicoectomy model presented the lowest stress value, whereas the high enlargement model presented the highest fracture criterion of all models (Table 3). Regarding stress distribution, high values around the instrument were found in the initial model; high values around the perforation were found in the enlargement models; and high values on the resected surface were found in apicoectomy models (Fig 3). The error indicator was considered as acceptable \(^{27,28}\) for all models, indicating that this method provides valuable models for FEA.

*Management of the fractured instrument*

After having informed the patient about the possible treatments, a 3-mm apicoectomy strategy was decided in accordance with her. First, the orthograde root canal treatment up to the fractured instrument and the tooth restoration were completed. One week later, the micro apical surgery was conducted following a 3-mm apicoectomy. The root end and the instrument were removed as a single entity to avoid risk of instrument projection into the sinus \(^{29}\) and the root end was
inspected under high magnification. The root canal was treated in a minimally invasive way using only a 3-mm ultrasonic retro-tip and the quality of the obturation was controlled on a periapical radiograph. The patient returned to her referent practitioner for the prosthetic rehabilitation, and the tooth remained asymptomatic at six weeks follow-up. The periapical radiograph at six months showed bone healing and absence of periapical radiolucency (Fig 4).

Discussion

This is the first work to report the use of digital technologies as decision support between non-surgical and surgical strategies of removal of a fractured endodontic instrument. In the present case, the digital approach allowed to visualize and anticipate the patient-specific root and sinus perforation, and to predict the mechanical impact of four removal strategies.

Studies reported that clinicians have difficulties to orient themselves in space from CBCT slices during their surgical procedure. Herein, VTP was used to simulate the procedures using a multi-label 3D image and to predict the iatrogenicity of the procedure. Increased risks of perforation and complications were reported for removal of apically fractured instruments. The 3D image enabled to precisely evaluate the presence of perforation and the position of the sinus using the clinical view. It is of note that the use of a printed guide increases the accuracy and reduces the risk of sinus perforation during endodontic microsurgery. However, this was not used in the case presented herein owing to the risk of instrument projection into the sinus.

In the current case, surgical strategies present a more favorable stress distribution than non-surgical ones, which supports herein the apicoectomy. This conclusion was also recommended by a previous narrative review promoting a surgical approach in cases of a separated instrument in the apical part of the root. Regarding the resection level, a 3-mm apicoectomy presents lower stress values than a 6-mm apicoectomy, which is in accordance with previous FEA.
studies. However, if a short resection is not sufficient to remove the instrument, increasing the resection level appears herein mechanically more acceptable than non-surgical strategies.

Despite the apparent value of the presented strategy, several limitations are to be highlighted. The main one is that the accuracy of CBCT is questionable in the occlusal part due to artifacts, whereas it is known that occlusal morphology influences the stress distribution in FEA. Recent technologies such as micro CBCT and the use of an intraoral scanner avoiding x-ray artefacts could improve future simulations. FEA results should also be carefully interpreted due to the technical impossibility to identify patient-specific parameters such as force intensity or for ligament modeling. Both VTP and FEA also required supplementary software and operator skills, which makes their use in routine clinical practice complex. The development of an intuitive software, marked as a medical device, will be necessary in the future to allow a wide dissemination of this technique among dental practitioners.

**Conclusion**

The case presented in this report illustrates some benefits of computer-aided solutions for decision-making in the removal of fractured endodontic instruments, by planning the treatment and predicting the mechanical impact induced by non-surgical and surgical strategies. Further investigations are required to confirm the relevance of this digital approach and improve the current software for routine clinical practice.
Acknowledgements

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References


<table>
<thead>
<tr>
<th>Material</th>
<th>Young’s modulus (GPa)</th>
<th>Poisson’s ratio</th>
<th>Reference</th>
</tr>
</thead>
<tbody>
<tr>
<td>Dentine</td>
<td>18.6</td>
<td>0.31</td>
<td>21</td>
</tr>
<tr>
<td>Ligament</td>
<td>0.069</td>
<td>0.45</td>
<td>21</td>
</tr>
<tr>
<td>Trabecular bone</td>
<td>1.3</td>
<td>0.3</td>
<td>21</td>
</tr>
<tr>
<td>Gutta percha</td>
<td>0.069</td>
<td>0.45</td>
<td>21</td>
</tr>
<tr>
<td>Root-end filling (modified zinc-oxyde eygenol)</td>
<td>0.1</td>
<td>0.31</td>
<td>23</td>
</tr>
<tr>
<td>Instrument (ProTaper Gold®)</td>
<td>50</td>
<td>0.26</td>
<td>22</td>
</tr>
</tbody>
</table>
Table 2 Number of elements, nodes, and error indicator according to the finite element model considered.

<table>
<thead>
<tr>
<th>Model</th>
<th>Number of elements</th>
<th>Number of nodes</th>
<th>Zhu-Zienkiewicz error indicator</th>
<th>Mean coronal strain</th>
</tr>
</thead>
<tbody>
<tr>
<td>Initial State</td>
<td>202636</td>
<td>29742</td>
<td>9.1 %</td>
<td>2.4 $10^{-4}$</td>
</tr>
<tr>
<td>Low enlargement</td>
<td>202462</td>
<td>29637</td>
<td>9.2 %</td>
<td>2.4 $10^{-4}$</td>
</tr>
<tr>
<td>High enlargement</td>
<td>202027</td>
<td>29614</td>
<td>9.3 %</td>
<td>2.4 $10^{-4}$</td>
</tr>
<tr>
<td>3-mm apicoectomy</td>
<td>201714</td>
<td>29855</td>
<td>8.9 %</td>
<td>2.4 $10^{-4}$</td>
</tr>
<tr>
<td>6-mm apicoectomy</td>
<td>207250</td>
<td>31126</td>
<td>9.2 %</td>
<td>3.2 $10^{-4}$</td>
</tr>
</tbody>
</table>
Table 3 Patient-specific analysis based on the 3D image and maximal Von Mises stress of the different removal strategies.

<table>
<thead>
<tr>
<th>Analysis of the 3D image</th>
<th>High stress location</th>
<th>Fracture criterion</th>
</tr>
</thead>
<tbody>
<tr>
<td>Initial state</td>
<td>No</td>
<td>Around the instrument</td>
</tr>
</tbody>
</table>

**Removal strategy**

<table>
<thead>
<tr>
<th>Removal strategy</th>
<th>High stress location</th>
<th>Fracture criterion</th>
</tr>
</thead>
<tbody>
<tr>
<td>Low enlargement</td>
<td>Apical perforation</td>
<td>Around the perforation</td>
</tr>
<tr>
<td>High enlargement</td>
<td>Lateral perforation</td>
<td>Around the perforation</td>
</tr>
<tr>
<td>3-mm apicoectomy</td>
<td>Decrease of the crown-root ratio</td>
<td>Resected apex</td>
</tr>
<tr>
<td>6-mm apicoectomy</td>
<td>Decrease of the crown-root ratio</td>
<td>Resected apex</td>
</tr>
</tbody>
</table>
Process for a patient-specific therapeutics analysis

**Fig 1** Process for a patient-specific biomechanical analysis and detailed steps for virtual treatment planning and finite element analysis: (A) axial view of Cone Beam Computed Tomography, (B) attribution of pixel labels, “seeds”, inside each anatomical structure, (C) segmentation based on a growing region algorithm, (D) transformation of the initial 3D image to simulate a 3-mm apicoectomy, (E) analysis of the 3D simulated treatment, and (F) meshing of the 3D transformed image to get a finite element model, and application of boundary conditions.
Fig 2 3D images for each situation of the virtual treatment planning. (A) Superimposition on the initial 3D image of the surfaces of the ultrasonic tip for enlargement strategies and osteotomy for apicoectomy strategies. (B) Simulated clinical views of the initial 3D image and of the modified 3D images for each removal strategy.
Fig 3 Cut views for each mesh and buccal views of Von Mises root stress represented by color, from blue (low values) to red (high values), for each finite element model. (A) Initial model representing the initial state, (B) low enlargement model, (C) high enlargement model, (D) 3-mm apicoectomy model, and (E) 6-mm apicoectomy model.
Fig 4 Micro apical surgery of the maxillary premolar. (A) Initial radiograph after instrument fracture, (B) size of the resected apex and of the removed instrument, and (C) postoperative radiograph at six months.