



HAL
open science

Towards a seamless experimental protocol for human arm impedance estimation in an interactive dynamic task

Vincent Fortineau, Maria Makarov, Pedro Rodriguez-Ayerbe, Isabelle A Siegler

► To cite this version:

Vincent Fortineau, Maria Makarov, Pedro Rodriguez-Ayerbe, Isabelle A Siegler. Towards a seamless experimental protocol for human arm impedance estimation in an interactive dynamic task. 2021. hal-03254516v1

HAL Id: hal-03254516

<https://hal.science/hal-03254516v1>

Preprint submitted on 8 Jun 2021 (v1), last revised 24 Aug 2021 (v2)

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

Towards a seamless experimental protocol for human arm impedance estimation in an interactive dynamic task

Vincent Fortineau^{1,2}, Maria Makarov¹, Pedro Rodriguez-Ayerbe¹, Isabelle A. Siegler²

Abstract—The estimation of the human endpoint impedance interacting with a physical environment provides modelling insights both for the field of human movement science and for the design of innovative controllers for collaborative robotics based on physical human-robot interaction. Most of the existing human impedance estimation methods described in the literature rely on controlled environments closer to a laboratory than to an industrial setting. In this paper, a force perturbation method is proposed without any specific requirements on neither the force nor the position trajectories and without additional sensors placed on the human. The method is illustrated through an experimental study on a benchmark interaction task. The task was selected to be sufficiently variable for preventing the use of average trajectories and the perturbations used for the estimations are sufficiently low amplitude and short to not deteriorate the human performance in the task. The obtained impedance model parameters are in adequacy with the ones found in the literature, suggesting the validity of the proposed approach. The low constraints on the experimental settings make it applicable even out of the lab, for example, in human-robot collaboration in manufacturing environments, to adjust the robot behaviour to changes in the state of the operator (fatigue, stress) or to adjust to a variety of human operators with different interaction strategies.

I. INTRODUCTION

Humans are capable of tailoring their limbs' dynamic properties [23] to improve the performance during the exploration of a new task [6] and achieve stable behaviour with a wide range of environments. Understanding and reproducing some properties of the humans' interactions during various tasks is thus relevant for the design of innovative robot control strategies.

The mechanical impedance of human limbs has been studied for decades under the control prism [17] and is still an active research topic [10], [18]. The notion of impedance relates kinematics to forces, allowing the modelling of human movements during physical interactions. Elementary models, such as mass (M or I for inertia) - spring (K) - damper (B , hence the acronym KBM or KBI) or Hill-type muscle models, have been shown to approach human behaviour [20], [23].

The mechanical impedance cannot be directly measured and requires perturbing the limbs for estimations. Thus, the environment often has to be very well mastered to identify the impedance parameters. Two configurations can be easily distinguished: on one hand, static or isometric tasks [8], [10],

[12], where the unperturbed pose is well known and on the other hand, dynamic tasks, where ongoing movements make the estimation of the unperturbed trajectory more complicated.

The choice of the perturbations nature, either force or position, is often dictated by kinematics knowledge. When the trajectory can be estimated online [5], position perturbations enable stiffness identification alone. The introduction of force perturbations requires prior information on neither the movement nor the force shape. Moreover, using a dedicated apparatus for the force introduction [1] can help to control the force perturbation dynamics. In [9], hand impedance estimations were conducted among welders, which brightly allowed the knowledge of the unperturbed trajectories. In other situations where the trajectory could not be perfectly known beforehand [1], [4], [5], the movement's repeatability allowed imperfect but sufficient knowledge on the unperturbed trajectories.

Another family of methods proposed in the literature relies on measurements of muscle activity using electromyographic sensors. Impedance estimations based on such measurements are, for instance, reported in an isometric task [24] or right after its completion [7]. Dynamic tasks make it more complicated to differentiate impedance from the task muscles activation.

In previous work at the intersection of robotics, control and human movement sciences [3], [19], the authors studied the human central nervous system during cyclic movements in a simulated benchmark task. They were able to reproduce human-like performances using a Central Pattern Generator based control structure. An experimental test-bed was designed for impedance measurements using interactive robotics [11]. The present paper aims to complete the kinematic aspects of previous work by adding an impedance model of the human arm during the task. Dynamic considerations should allow finer modelling of human behaviour during a cyclic task, notably by observing possible impedance variations within a cycle or across individuals with different strategies. Such an examination provides insights for the human-robot collaboration as well as for control strategies design for robot interacting with various physical environments.

This paper proposes a new methodology to identify the human endpoint impedance through an interactive robot [11], in conditions where both the restitution force and position (the differential between unperturbed and perturbed) can neither be measured, nor estimated with sufficient precision from average trajectories only. The optimisation-based estimation of the unperturbed force trajectory proposed in this paper significantly improves the impedance parameter estimation.

¹ Université Paris-Saclay, CNRS, CentraleSupélec, Laboratoire des signaux et systèmes, 91190, Gif-sur-Yvette, France
vincent.fortineau@centralesupelec.fr

² CIAMS, Université Paris-Saclay, 91405, Orsay, France, & Université d'Orléans, 45067, Orléans, France

Experimental validation shows that the identified parameters are consistent with previously documented values (Section V-B.3). Thus, the proposed estimation method allows less constrained experimental conditions and can be more easily replicated outside a laboratory for impedance estimation in a dynamic task.

The experimental test-bed is outlined in Section II, with the experimental data sets conditions. The issue of force trajectory estimation raised in [11] is then addressed in Section III. The impedance identification methodology is described in Section IV. Finally, the results using this implementation are presented in Section V.

II. EXPERIMENT

The experiment is briefly recalled in this section. For further details, please confer to previous work, [3], [11] for the ball bouncing task and [11] for the interactive robot control and a first approach of impedance estimation based on spline virtual trajectories.

A. Interactive rhythmic task

A user is manipulating an admittance controlled robot, manoeuvring its endpoint as a physical interface, to control a paddle simulated in a virtual environment. A 5-DOF KUKA™ youBot arm is used. The motion of the robot arm is restricted to the vertical plane and is performed using three actuated joints. To yield a rhythmic dynamic behaviour, the user has to move the paddle to bounce a virtual ball subject to gravity and moving along the vertical axis, to a target height simulated in the digital environment. When the ball hits the paddle, force feedback f_i is provided by the robot to the human to simulate the impact of the ball on the paddle [14].

To allow impedance estimation during the task, pulse force perturbations are introduced using the robot, in both directions of the uni-dimensional task. Both timing and direction are stochastic. These perturbations are generated at the motor torque level and are consequently filtered by the robot dynamics before reaching the endpoint. In order to have a negligible influence on the task, the perturbations force effects have a duration under 60 ms and a rather low amplitude, below 5 N. Perturbations are pseudo-randomly introduced at three different phases of the cyclic behaviour. A cycle is defined here as the time frame between two consecutive ball impacts on the paddle. In the considered task, the mean cycle time is of 1.18 s. According to the onset time in the cycle, the three perturbations categories are denoted (c_1) 25 %, (c_2) 50 %, (c_3) 75 %. A minimal non-perturbed interval of 2 s is imposed to ensure a nominal behaviour at the perturbation time.

B. Data sets

Both the endpoint position and force of the physical interaction between the human and robot arms are acquired with external sensors to obtain unbiased data. Interaction force is measured using an ATI™ mini45 force sensor also used in the robot admittance control and the endpoint position is measured using an Optitrack™ V120:Trio motion capture

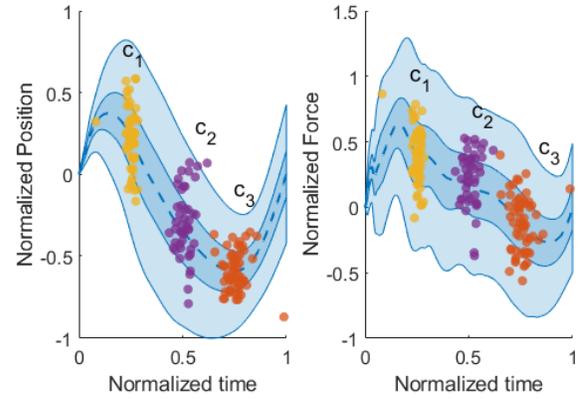


Fig. 1: normalised cycles of the data set d_3 ; perturbations are indicated with circles, the dotted lines represent the average normalised cycles while the coloured areas represent 1 and 3 standard deviations from the average cycle. The time normalisation was done using interpolations on the average cycle duration.

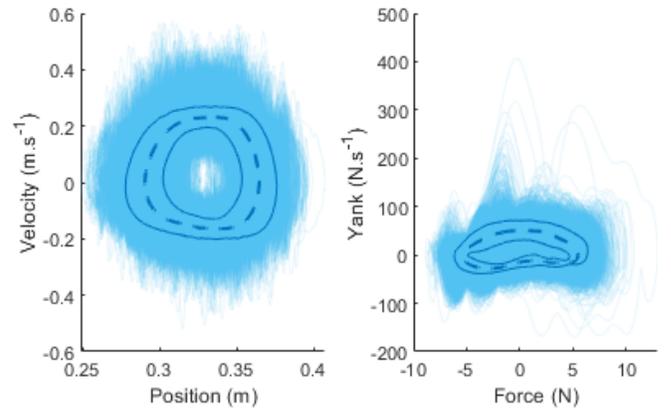


Fig. 2: Phase diagrams; for the kinematic and dynamic variables on data set d_2 . The deep blue ocean lines indicate both average (dotted) and standard deviations (solid).

system. For more information about the apparatus, please refer to [11].

A single user conducted a total of 28 physical interactions of approximately 5 min each with the experimental test-bed, in the absence of random perturbations. During half of those experiments, referred later as data set d_1 , force feedback representing ball impacts were introduced as described in Section II-A. The other half remained unsullied and is referred to as d_2 .

A third data set, d_3 , was collected by the same user. During a total of 7 manipulations of less than 2 min on average, 165 perturbed trajectories were recorded and classified according to the onset time of the force perturbation in the cycle (Section II-B). Eight of those perturbed trajectories could not be clearly classified because they occurred in unsteady cycles and were discarded. The distribution of onset time of the force perturbation is presented in Fig. 1. The three categories c_1 , c_2 and c_3 are not exactly equally represented since their generation was pseudo-random, they have respectively 60 (+28/-32), 51 (+25/-26) and 46 (+29/-17) elements each. Each of these three categories contains positive and negative

perturbations (numbers indicated previously in parentheses).

III. VIRTUAL TRAJECTORIES ESTIMATION

This section depicts the new methodology proposed to estimate unperturbed trajectories, previously called *virtual trajectories* in [22].

Most impedance estimation methods rely on the fact that deviations δf (force) and δx (position) from virtual trajectories (see Section IV for the impedance model relating motion to restitution force) can be introduced either by force or position perturbations. At least one is by essence unknown and needs to be reconstructed, while the other one can be perfectly mastered when the perturbation system allows it. In the literature, the averaged previous unperturbed trajectories were used in [4], with the assumption of sufficient reproducibility in the movements. A prediction algorithm with an unbiased error estimation, smaller than 1 cm after 200 ms, was proposed in [5]. We could not reach better result than those with cubic splines [11] while replicating those methods, that were not designed for force trajectories with high variability, as is the case for the benchmark task considered in this study. The variability of position and force profiles is illustrated in Fig. 1 and 2. For example, along 568 cycles (Fig. 1) of set d_3 , achieved by one of the authors, during seven sessions, the deviation observed on the normalised cyclic data reached up to respectively 22% and 26% of the normalised amplitude of the position and the force.

A. Preliminary remarks for signal analysis

The estimation of the position and force virtual trajectories is first validated using the unperturbed data set d_2 (Section II-B). The position virtual trajectory estimation was well approximated with cubic splines in [11]. Accordingly, this part focuses on force trajectories, cubic splines cannot approximate with sufficient precision due to more complex dynamics.

1) *Temporal analysis*: As seen from Fig. 2 to 3, the force signals shape varies significantly across cycles, even in the absence of perturbations. While the positions follow roughly a sinusoidal profile (Fig. 1a), forces (Fig. 1b) are affected by higher frequency oscillations inside the cycle. These oscillations should not be considered as perturbations, and their origin can be related to the human-robot physical interaction and the admittance control tuning (while the stability of this control was experimentally verified, strict passivity was not ensured). This situation is not exceptional, all the more if several human subjects operate the same robot and employ different interaction patterns. These intra-cycle oscillations can not be simply filtered out and should be taken into account for an efficient virtual trajectory estimation.

2) *Frequency analysis*: In the Fourier transform of the data sets d_1 and d_2 , the main frequency is observed, as expected, around 0.9 Hz, that is the frequency imposed by the ball bouncing task. While looking at the spectral analysis of both case scenario (with and without force feedback), the main differences occur after 5 Hz in both position and force signals. Those differences are more pronounced in the force spectral density, since the perturbations have more impacts on the

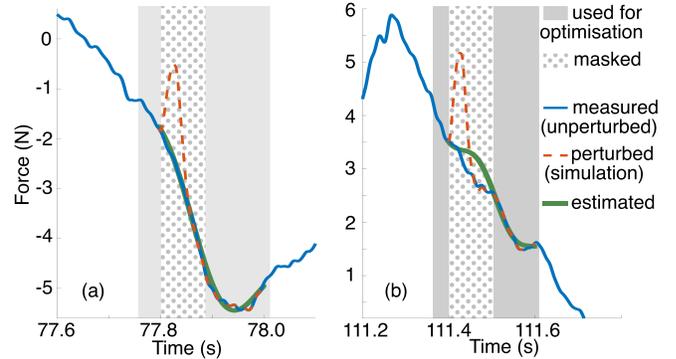


Fig. 3: Two examples of force trajectory estimations, with the measured unperturbed force (solid blue), the simulated perturbations (dashed orange) and estimated unperturbed force (green). Figure (a) depicts a successful estimation, while figure (b) shows a failed estimation that leads to an underestimated restitution force with oscillations.

force trajectory. Therefore, it can be deduced that most of the perturbed behaviour dynamics modify the trajectories, both in force and position, within a window of 200 ms. It also is worth noticing that the force spectral density is larger, in a broader frequency band than the position, confirming that this signal is less filtered and richer in frequency content.

B. Force virtual trajectory estimation

The estimation of the virtual force using cubic spline interpolations [11] raised the issue of sensitivity to the landing point. Indeed, as advanced in Section III-A.2, the force signal has higher power intensities, notably in higher frequencies. This makes the application of spline interpolation less reliable than for the position. In [1], the cyclic patterns of previous unperturbed data were fitted to a sinusoidal expression to predict the virtual position. A sum of sines is proposed to approach the virtual force in an offline resolution in a similar spirit. The general form is explicitly expressed in (1), with n being the number of sines and A_i , f_i and ϕ_i the parameters of each sine. Linear components a and b were added, with a boolean l . Hereinafter, this general form is adapted to the considered case through optimisations, and statistical analysis is performed.

$$f_z(t) = l(at + b) + \sum_{i=1}^n A_i \sin(2\pi f_i t + \phi_i) \quad (1)$$

1) *Optimisation*: From (1), the tested subset of functions corresponds to $2 \leq n \leq 5$, which amounts to a total of 8 possible combinations, if we consider $l = 0$ or 1. To identify the parameters of these functions, an optimisation problem is defined to minimise the nonlinear quadratic error, $\min_x \|f(x = \{A_i, f_i, \phi_i, a, b\})\|_2^2$, with a Levenberg-Marquardt algorithm [16]. Thereagainst [1], [5], the previous unperturbed cycle is not used to solve the virtual trajectory, but only data within a cycle shortly before and after the perturbation; this is only possible since the estimation is proceeded offline (see Fig. 3). A chunk of the signal is selected with a masked window, corresponding to the perturbed force. The masked interval is chosen to be 100 ms long and will

not be used to minimise the quadratic errors. 40 ms before the perturbation and 110 ms after the mask are used for the optimisation definition, as shown in Fig. 3.

This optimal problem is susceptible to the initial values provided. Therefore, two options are put forward using d_2 : i) for each of the 14 sessions, the optimisation for the first cycle in the session is performed with 250 starting points and the parameters obtained from this optimisation are then used as initial values for the next cycles, ii) 50 starting points are used for every cycle. One of the multiple starting points, x_0 , is manually fed; the other ones are randomly set within the boundaries specified in the Table I deduced from both temporal and spectral analysis. These two initialisation methods double the number of candidates to 16.

	A_i (N)	f_i (Hz)	ϕ_i (rad s ⁻¹)	a (N s ⁻¹)	b (N)
b_l	0	0	$-\pi/2$	-100	-100
x_0	1	$0.9(2i-1)$	0	1e-3	1e-3
b_u	10	10	$\pi/2$	100	100

TABLE I: Lower (b_l) and upper (b_u) boundaries and manually fed initial conditions (x_0)

2) *Evaluation*: In order to evaluate the proposed method, the estimated virtual trajectories need to be compared to a ground truth, unavailable in perturbed measurements. To that purpose, the sessions d_2 conducted without perturbations nor force feedback described in Section III-A are used. A total of 3144 evaluations are performed on the rhythmic force trajectories. If the optimised parameters are capable of approximating well the 100 ms masked t_{mask} as well as the next 100 ms t_{next} , then we consider that this methodology is capable of estimating a sufficient portion of the virtual force trajectory, for the impedance estimation, as explained in Section IV.

The comparison between the different models is then done using the Akaike criterion (AIC) [2] to favour the accuracy of the model and penalise the number of parameters and, therefore, potential overfitting. The model with three sines ($n = 3$), no linear components ($l = 0$) and systematic multi-starts (option *ii*) reached the lowest AIC value and was therefore retained. This model has an average adjusted coefficient of determination [21] (R_{adj}^2) of $91.0\% \pm 10.0\%$ on $t_{mask} + t_{next}$ interval and $95.1\% \pm 5.3\%$ on t_{mask} interval, after removing outliers outside five scaled median absolute deviations (sMAD). The histogram (Fig. 4) summarises the distribution of the errors, that are Gaussian-like centred close to zero, with average errors of respectively 12 mN and 6 mN, for the two conditions. The figure shows that most of the errors occurred in the interval t_{mask} .

IV. IMPEDANCE IDENTIFICATION METHODOLOGY

This section describes the methodology proposed for the identification of the impedance parameters.

This paper does not intend to differentiate the contribution of reflexes from the intrinsic properties of the human arm, like it was done in [13], but rather try to observe the arm's endpoint behaviour along the uni-dimensional task. A simple viscoelastic 2nd order model of impedance is used (2), in a comparable manner as [9], with M , B and $K \in \mathbb{R}^{n_c \times n_c}$,

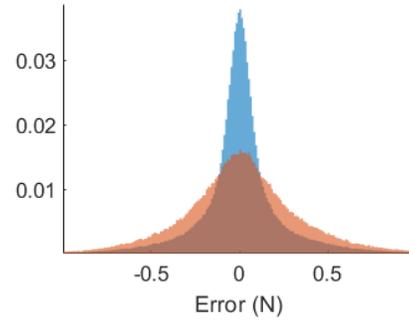


Fig. 4: Errors for the selected force estimation method, on the t_{mask} interval only (orange) and on the $t_{mask} + t_{next}$ (blue). The histogram ordinate indicates the probability of each 10 mN bin.

respectively the matrices of mass, damping and stiffness in the n_c Cartesian dimensions. For the studied uni-dimensional ball bouncing task, only the components along the vertical z axis are considered, $n_c = 1$.

$$\delta \mathbf{f} = \mathbf{M} \delta \ddot{\mathbf{x}} + \mathbf{B} \delta \dot{\mathbf{x}} + \mathbf{K} \delta \mathbf{x} \quad (2)$$

A. Auto Regressive model

1) *Delay*: Once the virtual trajectories have been computed from experimental data (see Section III), the differential estimated behaviour δf_z and δx_z can be exposed. Fig. 5 shows isolated perturbed behaviour of those trajectories. As expected from Section II-A, the main dynamics of the force perturbation happens in the first 60 ms, with a maximum reached around 33 ms. There is an apparent latency δ_t to notice in the positioning behaviour compared to the force differential. The figure does not allow an accurate evaluation of that delay; it can solely be bounded safely between 5 and 15 ms. This delay is studied in Section V-A. A possible origin would be that the motion capture system, used for the position acquisition, has a sampling rate of 8.3 ms, while position measurements were next interpolated at 1 kHz. A delay of about 8 ms can therefore be expected.

2) *Identification model*: The following discrete-time difference equation is considered for the identification of the second-order system (2) sampled with a zero-order hold and taking into account the previously mentioned pure delay:

$$(1 + a_1 q^{-1} + a_0 q^{-2}) \delta x_z [T_k] = (b_1 + b_0 q^{-1}) \delta f_z (T_k - \delta_t) + e(T_k) \quad (3)$$

with q the delay operator, a_i and b_j the model coefficients related to K , B and M , δ_t a pure delay and e white noise. The time window used for the identification is discussed in Section V-B.1.

The eigenvalues $\lambda_{1,2}$ of the second-order impedance model can easily be discretised to fit those of the discrete model (3) in (4), with a sampling time T . Two equations are therefore provided using the poles of the system.

$$e^{\lambda_{1,2} T} = e^{\frac{-B \pm \sqrt{B^2 + 4MK}}{2M} T} = \frac{-a_1 \pm \sqrt{a_1^2 - 4a_0}}{2} \quad (4)$$

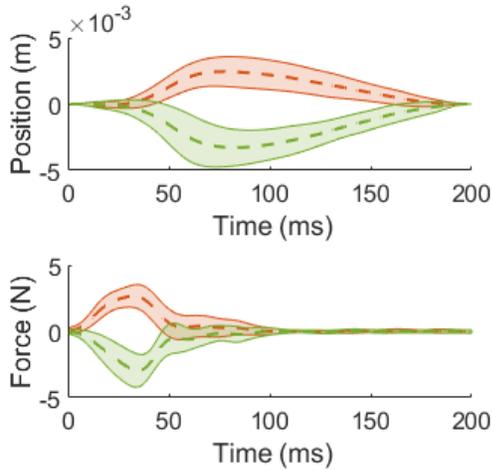


Fig. 5: Isolated typical effects of the perturbations on both the position and force. The average behaviours are shown with dotted lines, while the coloured areas represent the standard deviation. Positive (green) and negative (orange) perturbations are differentiated by their colour.

The last equation to completely identify the impedance parameters from the discrete coefficient of the proposed model (3) can be obtained using the final value theorem (5) or with the discretised coefficient b_1 .

$$K = \frac{1 + a_1 + a_0}{b_1 + b_0} \quad (5)$$

Identifying the impedance parameters K , B and M using this ARX model is more robust than with a straight temporal least square identification technique based on velocities and accelerations. Indeed, this way, the kinematic derivatives are not required, either using sensors or using numerical derivation.

B. Model evaluation

1) *Sensitivity*: A local sensitivity analysis of the impedance parameters to the coefficients of (3), evaluated for typical coefficients (see Section V-B.3) giving the impedance values $(K, B, M) = (200 \text{ N m}^{-1}, 10 \text{ N s m}^{-1}, 1 \text{ kg})$ reveals on Fig. 6 that all parameters are more sensitive to the sum of the numerator coefficients. Moreover, it is essential to underline that the stiffness K has the greatest sensitivity value (more than ten times the sensitivity of the damping B). Therefore the stiffness will be the more sensible to erroneous data, either coming from wrong virtual trajectories or poor ARX identification.

2) *Simulation*: A simulation was used to validate both the presented virtual trajectory estimation and impedance parameters identification methods. In an over-simplistic spirit, the model for the arm movements was assumed to be the same as the one for the impedance behaviour. For the sake of veracity, empirical force data was injected into the arm model. Force perturbations were generated with a step signal filtered by a second-order, chosen to have a 70 ms pseudo-period with a 5 N amplitude to resemble the experimental ones. Those perturbations were injected in an impedance model with known parameters and summed to the simulated

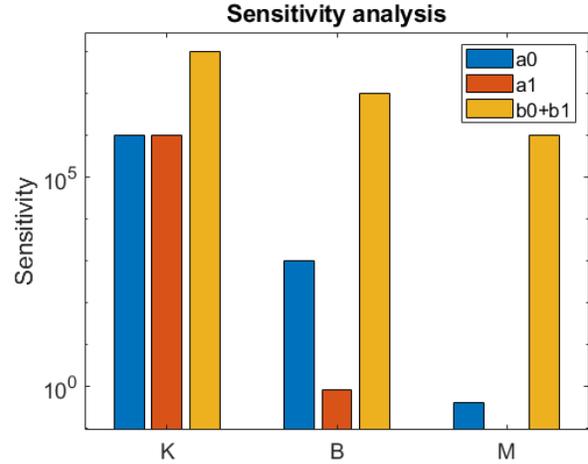


Fig. 6: Local sensitivity analysis $\left. \frac{\partial X_i}{\partial Y_i} \right|_{y_0}$, on a logarithmic scale, with X_i the impedance parameters and Y_i the discrete coefficients.

arm movement. For a simulated impedance behaviour with $K = 200$, $B = 10$ and $M = 0.5$ on 104 estimations, an average R_{adj}^2 of $99\% \pm 1\%$ was reached to reconstruct of the position with the identified parameters after removing outliers (5 sMAD). The parameters were identified with the characteristics provided in Table II with the subscript 1. Another example is also provided in the table. As expected from Section IV-B.1, stiffness was the parameter with the highest volatility. The threshold for outliers was reduced from five to the usual three sMAD, to abide by the increase in abnormal data.

	\hat{K}_1	\hat{B}_1	\hat{M}_1	\hat{K}_2	\hat{B}_2	\hat{M}_2
mean	258 N m ⁻¹	12.5 N s m ⁻¹	523 g	378 N m ⁻¹	15.9 N s m ⁻¹	487 g
std ⁽¹⁾	116 N m ⁻¹	6.81 N s m ⁻¹	110 g	166 N m ⁻¹	5.89 N s m ⁻¹	63 g
re ⁽²⁾	29%	25%	5%	5.4%	6.0%	2.5%

(1) standard deviation, (2) relative mean error

TABLE II: Parameters estimation in simulation.

It is relevant to notice that, with perfect knowledge of the virtual trajectory, the parameters were estimated with relative errors of about 0.05%, which means that the estimation errors mainly originate in the errors of virtual trajectory estimation.

V. RESULTS

This section presents results using the experimental protocol previously described in [11], with force feedback and controlled timing force perturbations. The data set d_3 , described in Section II-B, is used. For the data processing, variance analysis (ANOVA) will be conducted with a threshold fixed at 5% for significance levels. Both the degrees of freedom and the F value will be indicated in parenthesis (DOF, F) for the ANOVAs.

A. Delay

The delay δ_t unveiled in Section IV-A.1 was determined by running several estimations with varying delay. To evaluate the quality of estimated parameters, the measured position was compared to its reconstruction using the identified parameters and the estimated input force. Fig. 7 depicts the variations

of R_{adj}^2 for the reconstructed position. A one-way ANOVA showed a significant main effect of the delay on R_{adj}^2 (10, 14.75). The highest adjusted coefficient of determination reached a score of $95.1\% \pm 5.5\%$ for 12 ms (5 sMAD); this delay is therefore used for the impedance estimations. Although it is important to stress that a posthoc analysis (Tukey's HSD) revealed that no significant differences were observed between the 12 ms delay and all the delays comprised between 8 ms to 14 ms.

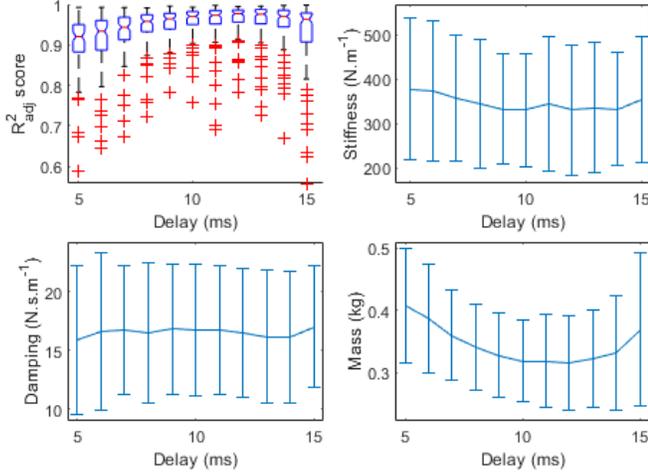


Fig. 7: Variations of R_{adj}^2 and impedance parameters against the delay for the identification ii with all perturbations classes indistinctly regrouped. The standard deviations are used as confidence intervals.

B. Impedance parameters

1) *Time window*: As mentioned in [9], voluntary reactions need to be discarded because linear impedance models cannot correctly model them. Voluntary reactions can be observed as soon as 100 ms after a perturbation [15]. Yet, at a 1 kHz rate, [9] found that using only 100 ms of data after the perturbation did not bring satisfying results. Therefore, they assumed that voluntary actions were not dominant in the first 200 ms and used that time window for the evaluation. To confirm that observation, impedance estimations were conducted with a data range varying from 50 ms to 200 ms. The adjusted coefficients of determination of the reconstructed position, and the impedance parameters identified, are compared in Fig. 8.

Fig. 8 shows the average estimated stiffness, damping and mass values as functions of the estimation time window length. Convergence is observed for respectively 153, 128 and 146 ms. However, the standard deviation of each of the parameter seems to reach a steady-state before, for about 80 ms, without significant reductions after that milestone. At the final stage, for 200 ms, the stiffness still has a standard deviation that represents 44.8% of its average value, the damping 34.2% and the mass 42.9%. This variability might be explained by the non-differentiation of the different perturbation categories. This result tends to show that an identification on a time window of 150 ms at 1 kHz might be enough. The paper will study both the identified parameters using 150 ms (subscript i) and 200 ms (subscript ii) to carry this investigation.

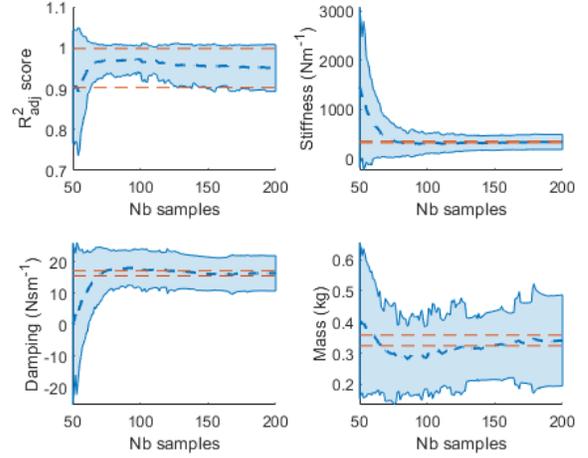


Fig. 8: Influence of the number of samples used for the ARX identification, the blue dotted line represents the average, and the light blue area represents one standard deviation from the average. The orange dotted lines show the 5% boundaries of the final values.

2) *Outliers*: The impedance estimations were separated into several groups according to the cyclic phase and the perturbation direction to isolate possible sources of variability. For both identifications, most of the outliers happened in a single class c_2+ . For the identification ii , six negative values amongst 7 R_{adj}^2 inferior to 50% were observed on 25 estimations, while no other negative values could be monitored for the other classes (Fig. 9). Moreover, six last values were considered abnormal, even with coefficients of determination above 50%, since their stiffness values were outside 5 sMAD. Therefore, among the 157 classified recordings, a total of 14 values were not considered (8.9%). Similar results were found for the identification i , but with a total of 17 outliers, which represent 10.8% of the data.

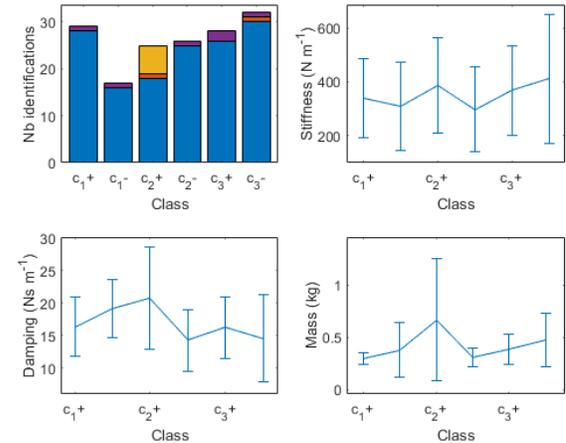


Fig. 9: The bar stacked chart shows in blue the kept data, in orange the R_{adj}^2 less than 50% and in purple the stiffnesses outside 5 sMAD and in yellow the outliers that belong to both categories. The others charts indicate the average and standard deviation for all impedance parameters estimated, using 200 ms (ii).

3) *Estimated parameters:* In [8], [9], [17], [23], Cartesian stiffnesses were found within a magnitude ranging in 40 N m^{-1} to 700 N m^{-1} , under static and moving configurations, with and without load for the human arm. Moreover [8], [9], [23] found damping parameters ranging between 8 N s m^{-1} to 44 N s m^{-1} and masses between 0.6 kg to 2.5 kg . The results presented here (Table III) are within those ranges but for the estimated masses that are slightly below.

4) *Variance analysis:* Considering the results from the identifications using 150 ms , an analysis of variance showed a significant effect of the phase on the adjusted coefficients of determination (5, 15.12). However, a posthoc analysis revealed that differences between positive and negative perturbations were only significant within c_2 . Only one significant difference could be observed between the classes c_1 and c_3 , for the specific case of c_1^- and positive c_3^+ . Taking into account the impedance parameters, neither the mean variations of stiffness nor damping observed during the different phases were significant (5, 1.59), (5, 2.37). Meaningful mean variations between the phases were found for the mass (5, 5.22). A posthoc analysis showed that this result was caused by the class c_2^+ that has greater a variance. A glance at Fig. 9 and Table III corroborate this finding for both identifications, which might indicate less reliable data.

Similar results were found for the identifications done with 200 ms . The only noticeable discrepancy was about the damping identified, which were found significantly different (5, 4.34), solely because of group c_2^+ . Finally, comparing the two different identifications, in first hand, if regrouping all classes, significant differences could only be found for R_{adj}^2 (1, 12.03) with an increase of 4% in average for the second identification and non-meaningful mean variations of the impedance parameters between 1% and 5%. On the other hand, if comparing separated classes in both identification, (eg. $i c_1^+$ with $ii c_1^+$), significant differences were found neither for the adjusted coefficient of determination nor the impedance parameters. However, the mean variation observed consistently in the same direction concerning R_{adj}^2 , a mean improvement of 4.3% on average, with the maximum being observed for the class c_2^+ (8.6%) and the minimum for class c_2^- (0.9%). Interestingly, the most considerable average variations for mass and damping were also in class c_2^+ , but for stiffness, it was in class c_3^+ .

VI. CONCLUSIONS

The identification method proposed here with the experimental test-bed design described in [11], offers a low constraint methodology for the impedance identification in the absence of knowledge on both force and position virtual trajectories during a dynamic task. A general study on the human movement brought sufficient estimation identifying of endpoint impedance parameters within the range of what is provided in the literature. However, the identification being sensitive to errors in the virtual trajectories as well as non-linear phenomena (voluntary movements, non-linear reflexes), the method still requires numerous estimations for reliable results. The results in this paper tend to show that using a time

window of only 150 ms for the identification was sufficient to bring result non significantly different from those with a 200 ms time window.

No significant stiffness variations were observed in the three cyclic phases chosen. Most of the significant variations were concentrated in class c_2^+ . However it might indicate that either the methodology or the experimental test-bed was less reliable in that phase. Compared to previous work, using an ARX methodology improved the repeatability in the estimation of both the damping and mass. Using the new force trajectory estimation method drastically reduced the errors in virtual trajectories and improved the estimation of the stiffness, for perturbation below 5 N inducing typical movements deviations δx less than 3 cm . It made the perturbations hardly distinguishable from the task force feedback without disrupting the task.

Further experiments will be conducted to evaluate the inter and intra-individual variability of end-point impedance parameters in interactive tasks. Obtained parameter values can be used for the analysis and design of feedback control strategies in interactive robotics.

REFERENCES

- [1] M. O. Abe and N. Yamada, 'Modulation of elbow joint stiffness in a vertical plane during cyclic movement at lower or higher frequencies than natural frequency', *Exp Brain Res*, vol. 153, no. 3, pp. 394–399, 2003.
- [2] Akaike H. (1998) Information Theory and an Extension of the Maximum Likelihood Principle. In: Parzen E., Tanabe K., Kitagawa G. (eds) Selected Papers of Hirotugu Akaike. Springer Series in Statistics (Perspectives in Statistics). Springer, New York, NY.
- [3] G. Avrin, et al., 'The self-organization of ball bouncing', *Biol. Cybern. (modelling)*, Springer Verlag, 2018.
- [4] D. J. Bennett, et al., 'Time-varying stiffness of human elbow joint during cyclic voluntary movement', *Exp Brain Res*, vol. 88, no. 2, pp. 433–442, 1992.
- [5] E. Burdet, et al., 'A method for measuring endpoint stiffness during multi-joint arm movements', *J. Biomech.*, vol. 33, no. 12, pp. 1705–1709, 2000.
- [6] E. Burdet, et al., 'The central nervous system stabilizes unstable dynamics by learning optimal impedance', *Nature*, vol. 414, no. 6862, pp. 446–449, 2001.
- [7] C. Castellini, A. Arquer and J. Artigas, "sEMG-based estimation of human stiffness: Towards impedance-controlled rehabilitation," 5th IEEE RAS/EMBS International Conference on Biomedical Robotics and Biomechanics, Sao Paulo, Brazil, 2014, pp. 604-609.
- [8] J. M. Dolan, M. B. Friedman and M. L. Nagurka, 'Dynamic and loaded impedance components in the maintenance of human arm posture', *IEEE Trans. Syst., Man, Cybern. Syst.*, vol. 23, no. 3, pp. 698–709, 1993.
- [9] M. S. Erden and A. Billard, "Hand Impedance Measurements During Interactive Manual Welding With a Robot," in *IEEE Transactions on Robotics*, vol. 31, no. 1, pp. 168-179, Feb. 2015.
- [10] C. Fang, A. Ajoudani, A. Bicchi and N. G. Tsagarakis, "Online Model Based Estimation of Complete Joint Stiffness of Human Arm," in *IEEE Robotics and Automation Letters*, vol. 3, no. 1, pp. 84-91, Jan. 2018.
- [11] V. Fortineau, M. Makarov, P. Rodriguez-Ayerbe and I. A. Siegler, "Interactive robotics for human impedance estimation in a rhythmic task," 2020 IEEE 16th International Conference on Automation Science and Engineering (CASE), Hong Kong, China, 2020, pp. 1043-1048.
- [12] D. L. Guarin and R. E. Kearney, "Time-varying identification of ankle dynamic joint stiffness during movement with constant muscle activation," 2015 37th Annual International Conference of the IEEE EMBC, Milan, Italy, 2015, pp. 6740-6743.
- [13] D. L. Guarin and R. E. Kearney, 'Unbiased Estimation of Human Joint Intrinsic Mechanical Properties During Movement', *IEEE Trans. Neural Syst. Rehabil. Eng.*, vol. 26, no. 10, pp. 1975–1984, 2018.

	c_1^+	c_1^-	c_2^+	c_2^-	c_3^+	c_3^-	+	-
${}_iK$	338 ± 158	319 ± 151	408 ± 227	294 ± 173	308 ± 133	397 ± 221	345 ± 172	343 ± 193
${}_iB$	16.7 ± 5.2	18.5 ± 4.2	17.8 ± 12.0	13.7 ± 4.4	15.6 ± 6.6	13.2 ± 5.4	16.6 ± 7.8	14.6 ± 5.2
${}_iM$	0.288 ± 0.061	0.369 ± 0.235	0.756 ± 0.788	0.293 ± 0.071	0.354 ± 0.123	0.484 ± 0.393	0.430 ± 0.441	0.391 ± 0.291
${}_iR_{adj}^2$	83.5 ± 4.6	88.7 ± 3.9	73.6 ± 14.0	93.0 ± 2.9	81.6 ± 9.8	82.6 ± 6.9	80.3 ± 10.2	87.6 ± 6.9
${}_{ii}K$	340 ± 147	310 ± 164	387 ± 177	298 ± 159	368 ± 167	411 ± 241	362 ± 160	348 ± 203
${}_{ii}B$	16.3 ± 4.5	19.1 ± 4.5	20.7 ± 7.9	14.2 ± 4.7	16.2 ± 4.8	14.5 ± 6.7	17.4 ± 5.9	15.4 ± 5.9
${}_{ii}M$	0.294 ± 0.057	0.378 ± 0.259	0.664 ± 0.581	0.305 ± 0.088	0.381 ± 0.147	0.471 ± 0.253	0.418 ± 0.334	0.392 ± 0.222
${}_{ii}R_{adj}^2$	88.1 ± 3.6	91.6 ± 3.0	80.5 ± 11.4	94.0 ± 7.5	86.4 ± 7.0	84.7 ± 6.8	80.4 ± 10.7	85.6 ± 10.4

TABLE III: Results: standard deviation are indicated in as confidence intervals.

- [14] Kawazoe, Y. Dynamics of the Ball-Racket Impact in Tennis: Contact Force, Contact Time, Coefficient of Restitution and Deformation, Proceedings of ACM, 2002, pp. 286-293.
- [15] B. Libet, "Unconscious cerebral initiative and the role of conscious will in voluntary action", Behavioral and Brain Sciences, vol. 8, n4, p. 529-539, déc. 1985, doi: 10.1017/S0140525X00044903.
- [16] Moré J.J. (1978) The Levenberg-Marquardt algorithm: Implementation and theory. In: Watson G.A. (eds) Numerical Analysis. Lecture Notes in Mathematics, vol 630. Springer, Berlin, Heidelberg.
- [17] F. A. Mussa-Ivaldi, N. Hogan and E. Bizzi, 'Neural, mechanical and geometric factors subserving arm posture in humans', J. Neurosci., vol. 5, no. 10, pp. 2732-2743, 1985.
- [18] G.-H. Phan, C. Hansen, P. Tommasino, A. Budhota, D. M. Mohan, A. Hussain, E. Burdet and D. Campolo, "Estimating Human Wrist Stiffness during a Tooling Task," Sensors, vol. 20, no. 11, p. 3260, Jun. 2020.
- [19] I. A. Siegler, B. G. Bardy and W. H. Warren, 'Passive vs. active control of rhythmic ball bouncing: The role of visual information', J. Exp. Psychol. Hum. Percept. Perform., 36(3), 729-750, 2010.
- [20] Tee, K., Burdet, E., Chew, C. et al. A model of force and impedance in human arm movements. Biol. Cybern. 90, 368-375 (2004). <https://doi.org/10.1007/s00422-004-0484-4>
- [21] H. Theil, et al., 'Economic Forecasts and Policy', Holland, Amsterdam: North, pp. 213, 1961.
- [22] T. Tsuji, 'Human Arm Impedance in Multi-Joint Movements', in Advances in Psychology, vol. 119, P. Morasso and V. Sanguineti, Eds. North-Holland, 1997, pp. 357-381.
- [23] T. Tsuji and Y. Tanaka, 'Bio-mimetic impedance control of robotic manipulator for dynamic contact tasks', Robotics and Autonomous Systems, vol. 56, no. 4, pp. 306-316, 2008.
- [24] C. Wang, L. Jiang, C. Guo, Q. Huang, B. Yang and H. Liu, "sEMG-based estimation of human arm force using regression model," 2017 IEEE International Conference on Robotics and Biomimetics (ROBIO), Macau, 2017, pp. 1044-1049.