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Ultrasound-induced Coalescence of Free Gas Microbubbles

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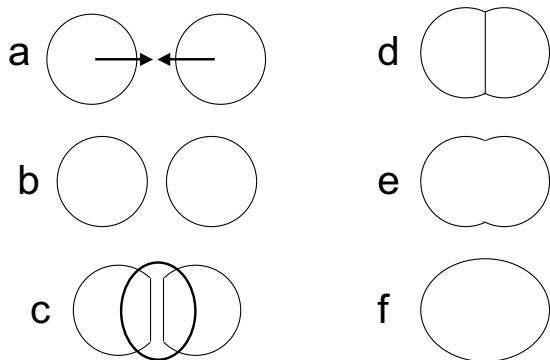


Fig. 1. Schematic representation of colliding bubbles or droplets: approach (a–b), flattening of the interposed film (c), drainage to a critical thickness (d), film rupture (e), and formation of a single bubble (f).

Abstract—When gas bubbles collide, the following stages of bubble coalescence have been reported: flattening of the opposing bubble surfaces prior to contact, drainage of the interposed liquid film toward a critical minimal thickness, rupture of the liquid film, and formation of a single bubble. During insonification, expanding contrast agent microbubbles may collide with each other, resulting in coalescence or bounce.

In this study, we investigate the validity of the film drainage formalism for expanding free bubbles, by subjecting rigid-shelled contrast agent microbubbles to ultrasound, in order to release gas, and photograph the coalescence of these free gas bubbles. As with colliding bubbles, bubble surface flattening is related to the Weber number. Only inertial film drainage between free interfaces explains the observed coalescence times. In accordance with theory, smaller bubble fragments coalesce on very small time scales, while larger bubbles bounce off each other.

I. INTRODUCTION

When two gas bubbles collide or are driven into each other, coalescence into a single bubble may result. The following stages of bubble coalescence have been identified (*cf.* Figure 1): flattening of the opposing bubble surfaces prior to contact, drainage of the interposed liquid film toward a critical minimal thickness, rupture of the liquid film, and formation of a single bubble. If the critical thickness is not reached during collision, the bubbles bounce off each other instead.

Free gas bubble coalescence after collision has been studied

extensively [1], [2], [3], [4], [5], [6]. With ultrasound contrast agents, microbubble coalescence has been observed during ultrasound insonification, when expanding microbubbles come into contact with each other [7], [8], [9]. With the aid of high-speed photography, we previously investigated the coalescence times of insonified soft-shelled microbubbles. We compared observed coalescence times to calculated film drainage times, based on the Reynolds equation [10] for no-slip interfaces and on the drainage equation for free interfaces. We concluded that the bubbles behaved as if they had free interfaces like free gas bubbles [8]. However, to support this conclusion, we should investigate the validity of the drainage equations for expanding bubbles. In this study we do so, by subjecting rigid-shelled contrast agent microbubbles to ultrasound, in order to release gas, and investigate the coalescence of these free gas bubbles. We compare these times to the computations.

Previously, we reported on ultrasound-induced gas release from contrast agent microbubbles [7]. This so-called *sonic cracking* has been observed with microbubbles with rigid encapsulations.

II. THEORY

Flattening of the opposing bubble surfaces occurs in case of colliding bubbles with constant volumes, if the bubble system has a Weber number $We \gtrsim 0.5$ [5]. If $We \lesssim 0.5$, the bubbles will coalesce without the prior formation of an interposed film. The Weber number for a fluid containing two bubbles with radii R_1 and R_2 , respectively, is given by the inertial force relative to the surface tension force:

$$We = \rho u^2 \left/ \frac{\sigma}{R_m} \right., \quad (1)$$

where u is the relative approach velocity, ρ is the fluid density, σ is the surface tension, and R_m is the mean bubble radius for which holds:

$$\frac{2}{R_m} = \frac{1}{R_1} + \frac{1}{R_2}. \quad (2)$$

We propose to extend this criterium to approaching walls of expanding bubbles. Because the radius and with it the approach velocity of oscillating bubbles change during a cycle, so does the Weber number. The approach velocity for

expanding bubbles with a constant center-to-center distance is

$$u = \dot{R}_1 + \dot{R}_2. \quad (3)$$

If the Weber number is low, bubble coalescence will always occur, without flattening of the adjacent surfaces prior to contact [5]. In the high Weber number regimen, coalescence is determined by a second step, after flattening: film drainage. When the expansion time is less than the time needed for film drainage, the bubbles bounce off [11].

The radial velocity of the liquid in the film is a combination of a plug flow driven by the motion of the interfaces, and a laminar velocity profile (analogous to Poiseuille flow) driven by the radial pressure gradient [12], [13]. If the bubble surfaces consist of a high concentration of surfactant, on our working scales the interfaces are to be considered immobile (no-slip) [14]. In the case of no-slip interfaces, the interfacial tangential velocity is zero, so the plug flow contribution is zero [12]. In the case of free interfaces, the Poiseuille contribution to the drainage flow becomes negligible [14], [12]. The film drainage time for free radial surfaces is approximated by the equation [15], [16]:

$$\tau_d \approx R_f \sqrt{\frac{\rho}{8p}} \log\left(\frac{h_i}{h_c}\right), \quad (4)$$

where η is the viscosity of the fluid, ρ is the density of the fluid, R_f is the film radius, h_i is the initial thickness, h_c is the critical film thickness, at which the film ruptures, p and is the pressure difference between film and surrounding fluid which is taken

$$p = \sigma \left(\frac{1}{R_1} + \frac{1}{R_2} \right). \quad (5)$$

In our computations, we take

$$\begin{aligned} \eta &= 0.001 \text{ Pa s}, \\ \rho &= 998 \text{ kg m}^{-3}, \\ \sigma &= 0.072 \text{ N m}^{-1}, \text{ and} \\ h_c &= 10 \text{ nm}. \end{aligned} \quad (6)$$

Flattening takes place when:

$$\dot{R}_1 + \dot{R}_2 \gg \frac{dh}{dt}, \quad (7)$$

whereas the flat film drainage happens in the next stage, when

$$\dot{R}_1 \approx \dot{R}_2 \approx 0. \quad (8)$$

Thus, during drainage, on our timescales, we may take p and R_f constant over time [8].

Repeated coalescence and fragmentation has been reported [8]. Fragmentation is the fission of a bubble into smaller bubbles. It occurs around peak contraction, when the bubble collapse is driven by inertial forces, since the inward acceleration continues to increase as the bubble approaches its minimum radius and suddenly changes sign as the bubble begins a rebound [17]. The number of fragments into which a bubble breaks up has been related to the dominant spherical harmonic oscillation mode n [18], [9]. The estimated number of fragments N is

$$N \approx n^3. \quad (9)$$

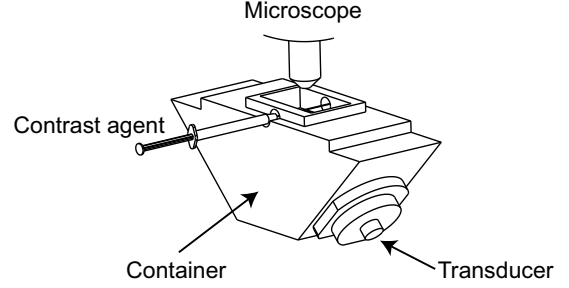


Fig. 2. Overview of the experimental bubble-system.

III. EXPERIMENTAL METHODS

Our experimental setups for taking pictures of insonified contrast bubbles were as described in [19] and in [20]. An overview of the bubble-system is shown in Fig. 2. A $\varnothing 200 \mu\text{m}$ capillary tube, through which contrast agent was flowing, was fixed in the focal area of a v389-SU 500 kHz or a v397-SU 2.25 MHz single-element transducer (Panametrics Inc., Waltham, MA). The optical observations of the insonified ultrasound contrast agent were recorded with the Brandaris-128 system, operating at speeds up to 15 MHz.

The free gas bubbles were released from PB127 (POINT Biomedical Corporation, San Carlos, CA). PB127 consists of bilayered microspheres encapsulating nitrogen bubbles with a mean diameter of $4 \mu\text{m}$. The outermost layer is albumin and the inner layer is composed of a biodegradable polymer. The content of a PB127 vial was resuspended in 5 ml of deionized water, and shaken gently for 20 seconds before further dilution. Diluted PB127 was inserted through the capillary tube using a syringe pressed by hand. It was insonified by 6 or 8 cycles of 500 kHz (period $T_p=2 \mu\text{s}$), or by 8 cycles of 1.7 MHz ($T_p=0.6 \mu\text{s}$) ultrasound at acoustic pressures corresponding to mechanical indices between 0.3 and 1.9.

IV. RESULTS AND DISCUSSION

The same stages of coalescence described for colliding bubbles could be distinctly observed with expanding free gas microbubbles and soft-shelled microbubbles. Examples of soft-shelled microbubble coalescence were shown in [7], [8], [21].

As with encapsulated bubbles, coalescence and bounce were regularly observed. For the interacting free gas microbubbles with flattened interfaces observed in the optical images, $We \gtrsim 1$. We obtained 9 image sequences where free bubble coalescence times and the bubble dimensions could be measured. The times between flattening of the free bubble surfaces and coalescence are less than $0.3 \mu\text{s}$, for expanded gas bubbles with diameters between 3 and $5 \mu\text{m}$.

Figure 3 shows an example of gas release from a PB127 bubble. Each frame corresponds to a $23 \times 23 \mu\text{m}^2$ area. Four PB127 bubbles are in the field of view. After ultrasound arrival (frame 13) the bubbles contract. During expansion, gas escapes from the $\varnothing 3 \mu\text{m}$ upper bubble (16–19). The free gas is seen detached in frame 21. It expands (22–25) and starts to contract (26). Close to its minimum, the free gas bubble

splits up into multiple fragments (27). During expansion, the fragments appear to have coalesced into two separate bubbles (28–29). These bubbles collide during expansion (30). The Weber number, calculated from the bubble wall velocity (29–30) $u \simeq \frac{2 \mu\text{m}}{0.1 \mu\text{s}}$, is $We > 20 \gg 0.5$, which agrees with the flattening of the bubble surfaces. Computing equation (4) with $R_1 = 3.9 \mu\text{m}$, $R_2 = 3.4 \mu\text{m}$, and $R_f = 2.1 \mu\text{m}$ yields

$$\tau_d = 0.6 \mu\text{s} \approx T_p. \quad (10)$$

This long drainage time accounts for the observed bounce (30–32). Close to maximal contraction (33), the two bubbles fragment. During expansion, the fragments are seen to coalesce (35–37) into two bubbles of perpendicular orientation. Again, these bubbles bounce (38–39), fragment (40), and coalesce into two bubbles perpendicular to their mother bubbles (41). This process repeats itself, until insonification ends (66). The two remaining free gas bubbles still pulsate, and collide while doing so. These collisions may possibly be attributed to secondary radiation forces. In frame 82, the bubbles coalesce. This coalescence is induced by the pressure field exerted by the bubbles themselves. The remaining bubble has a maximum of $3.8 \mu\text{m}$. It pulsates at 1.7 MHz. Hence, the pulsations may be attributed to reflections.

Note that the radii of the bubble fragments after a fission event are all: $R_i < 1 \mu\text{m}$. From equations (4)–(6), using the empirical relation [8]:

$$R_f \approx \frac{2}{3} R_i, \quad (11)$$

it follows that the drainage times, and with it the fragment coalescence times are:

$$\tau_d < 0.1 \mu\text{s}, \quad (12)$$

consistent with the observed fast coalescence of fragments in the space of an inter-frame distance ($0.1 \mu\text{s}$).

The bouncing bubbles in Fig. 3 might be considered as an $n = 2$ spherical harmonic mode system. This is supported by the alternating perpendicular orientations observed. The estimated number of fragments ($N \approx 2^3 = 8$) cannot be verified by these observations, because right after fragmentation, the fragments are too small to be observed.

V. CONCLUSIONS

Expanding gas bubble coalescence has been observed with released gas. Bubble surface flattening is observed to be consistent with the Weber number criterium for colliding bubbles.

Calculated drainage times from an inertial drainage model assuming clean, stress-free interfaces are consistent with the observations: For large (fully expanded) bubbles the drainage times are too large (larger than a bubble oscillation cycle) to allow for film drainage and coalescence. Smaller microbubble fragments, however, easily coalesce on very short timescales.

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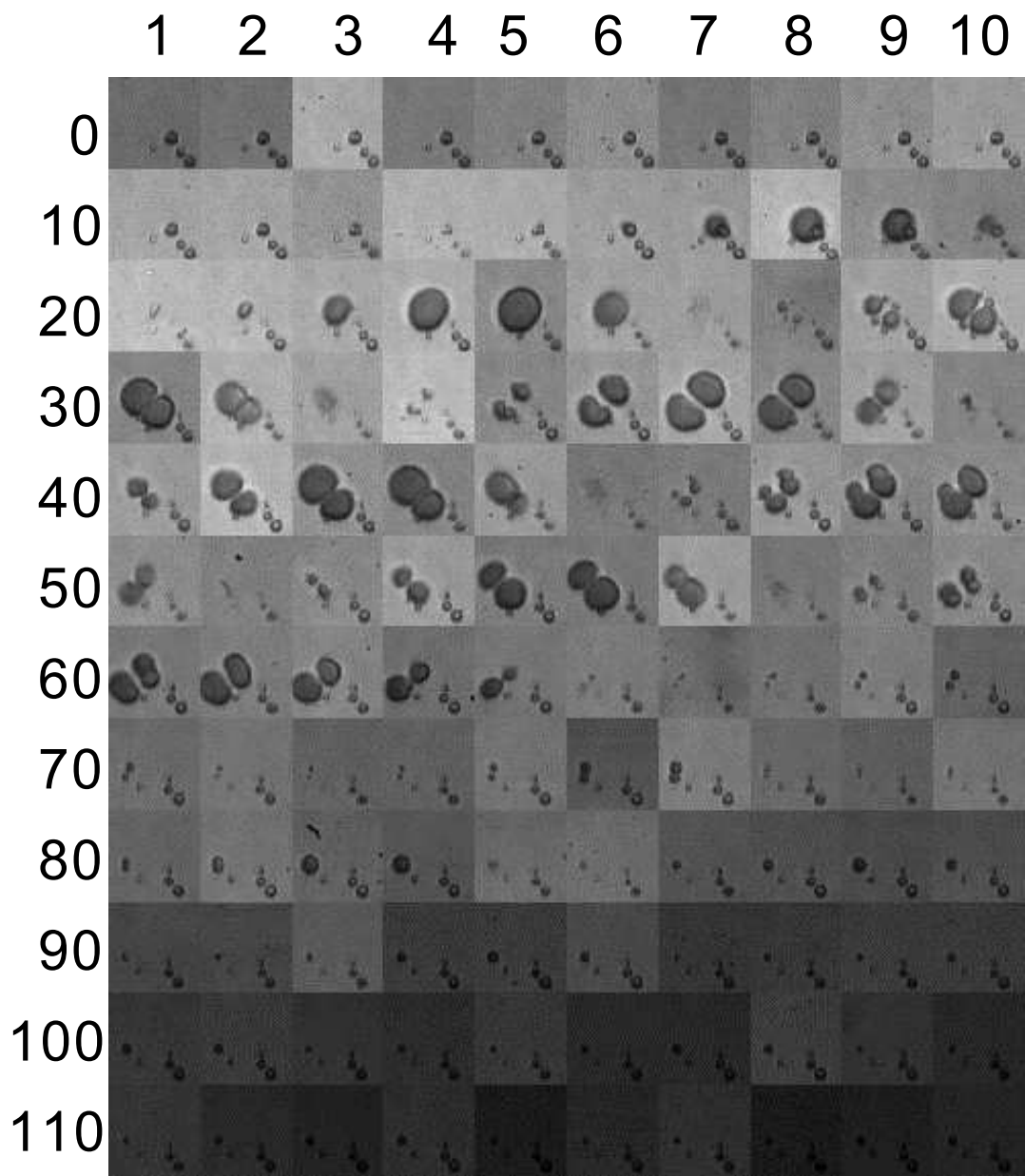


Fig. 3. Gas release at 1.7 MHz from PB127 microbubbles, captured at 10 Mfps. Each frame corresponds to a $23 \times 23 \mu\text{m}^2$ area. Spontaneous coalescence of free gas microbubbles takes place in frames 81–83.