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# Sintering and biocompatibility of copper-doped hydroxyapatite bioceramics

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**Abstract:** Addition of copper in biomaterials is currently investigated because it is expected to enhance the biological properties of bone graft substitutes. Copper-doped hydroxyapatite (CuHA) ceramics were prepared by high temperature solid-state reaction sintering between HA and CuO powder mixtures. The reaction occurred from 950 °C and copper-doped apatites were obtained up to 5.3 wt% of copper. For higher copper content, the presence of secondary phases of CuO and Cu<sub>2</sub>O remained in the material. Structural analyses (XRD, FTIR) showed the substitution of hydrogen by copper into the hydroxyapatite hexagonal channels in agreement with the following chemical composition  $\text{Ca}_{10}(\text{PO}_4)_6\text{Cu}^{\text{II}}_z\text{Cu}^{\text{I}}_y\text{O}_2\text{H}_{2-2z-y}$  with  $x = y + z$  and  $0 \leq x \leq 0.7$ . Dense single phased apatitic HA ceramics containing up to 5.3 wt% of copper could be produced after natural sintering in air at 1100 °C. But, copper-substituted HA was found to be metastable leading to apatitic grains and Cu-rich grain boundaries during cooling to room temperature, which resulted in the formation of CuO grains at the material surface after annealing at 500 °C. Quenching from the sintering temperature was carried out to prevent this phenomenon and obtain ceramics made of single Cu-HA phase with a homogeneous fine grain microstructure. In vitro biological assays using MC3T3-E1 cells indicated that the sintered CuHA ceramics were biocompatible, neither cell adhesion nor proliferation being affected by copper addition. A negative effect on cell differentiation appears only from 5 wt% of copper in HA.

**Keywords:** Sintering ; Microstructure-final ; Apatite ; Biomedical applications

## 1. Introduction

Calcium phosphates, mainly hydroxyapatite (HA), are of great interest for biomedical applications due to their chemical composition close to the bone. HA, with general formula  $\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$ , is a biocompatible, osteoconductive and bioactive material [1,2]. It has been widely used as drug delivery system, implant coating and bone substitute [[3], [4], [5]]. The bioactivity of HA allows new bone formation through biochemical bonding at the bone implant interface. In addition, the manufacturing of scaffolds with interconnected macropores (typically in the size range 300–500 μm [6] improves the implant osteointegration through its colonization by cells involved in the bone formation, vascular invasion and circulation of the nutrients. Ceramic scaffolds with large dimension may be used to replace damaged bone tissues but the cellular and vascular ingrowth hardly exceeds 1 cm in depth from the native bone apposition [7,8]. Therefore, complete osseointegration is limited. A lack of vascularization within the scaffold seems to originate the low bone ingrowth [9]. As osteogenesis is not possible without angiogenesis, the improvement of vascularization is the key point for a better osseointegration and for the development of large size HA scaffolds.

Biological apatite is similar to a carbonate hydroxyapatite enriched with traces of various ionic species ( $\text{Na}^+$ ,  $\text{Mg}^{2+}$ ,  $\text{Sr}^{2+}$ ,  $\text{F}^-$ ,  $\text{SiO}_4^-$  ...) [10]. Some of these elements play a significant role in bone mineralization process: for instance, zinc, strontium or manganese favour osteogenesis while magnesium, copper and cobalt improve angiogenesis [11]. Hydroxyapatite is known for its capacity to accept ion substitution in its lattice. Many studies have demonstrated that the addition of trace elements to stoichiometric HA tends to enhance its bioresorbability, its mechanical performances and/or its biological properties [[12], [13], [14]]. Regarding the improvement of angiogenesis, Mg-doped HAs have been the most studied compounds in the literature. Pure apatitic phases were obtained only for low magnesium concentrations (up to 0.6 wt% [15]). For higher content, Mg-doped HAs are unstable above 800 °C and their decomposition occurs at lower temperatures with the increase of magnesium amount [16,17]. Cobalt-substituted HA has only been studied at low temperature (below 600 °C) [18,19] while Zykin et al. succeeded to embed dioxocobaltate anions in the HA lattice by solid-state reaction [20]. Using the same synthesis process, several authors obtained pure and thermally stable copper-doped HA (CuHA) crystals [[21], [22], [23], [24]]. In addition to the expected potential to stimulate angiogenic properties, copper is well known for its antibacterial effect [25,26], so the development of copper-doped HA ceramics for bone reconstruction appears of a twofold interest.

Synthesis of CuHA powders can be performed by aqueous coprecipitation route. It leads to the substitution of calcium by copper and to a theoretical product  $\text{Ca}_{10-x}\text{Cu}_x(\text{PO}_4)_6(\text{OH})_2$ . In the literature, pure light blue compounds were obtained at low temperature (below 600 °C). XRD analyses showing lower cell parameters for CuHA than HA, the substitution of calcium by copper was confirmed [[27], [28], [29], [30], [31]]. However, none of the as-prepared copper-doped hydroxyapatites was thermally stable above 800 °C [[29], [30], [31]]. By solid state reaction, thermally stable CuHAs were synthesized but secondary phases of copper oxides and tricalcium phosphates (TCP) can also be observed [[32], [33], [34]]. The increase of the unit cell parameters with copper content and the detection of copper at the 2b Wyckoff position (0,0,0) by Rietveld analysis showed the copper insertion into the hexagonal channels leading to a theoretical  $\text{Ca}_{10}(\text{PO}_4)_6\text{Cu}_x\text{O}_y\text{H}_z$  composition [[21], [22], [23],33,34]. Copper oxidation state is still not clearly established: mixed valences  $\text{Cu}^+/\text{Cu}^{2+}$  [21,23,24,33], as well as  $\text{Cu}^+/\text{Cu}^{3+}$  pairs are stated [22,34]. Literature mainly highlighted the crystallographic structure of CuHA powders but there is no available data regarding the sintering and microstructure of pure copper-substituted HA ceramics. Additionally, copper is known for its potential toxicity towards cells [35,36]. However, only few studies performed biocompatibility tests on copper-doped HA. Depending on the synthesis method and the *in vitro* culture protocol, the results diverge. For the same Cu/Ca = 0.01 M ratio, CuHA pellets obtained from an ion exchange method, by Li et al., were cytotoxic after one day of incubation [37] whereas the biphasic pellets (1.4 wt% of TCP) calcined at 1200 °C by Gomes et al. were found to be biocompatible after one week of culture [33]. A cytotoxic concentration of copper ion released in the culture medium was found to be as low as 0.082 ppm in the first study [37], while about 10 ppm in the second one was not found toxic [33]. This last study also shows the major influence of the HA/TCP ratio on copper ion release and cell viability. Therefore, the chemical structure, the secondary phases as well as the microstructure of the tested compound may greatly influence the biocompatibility (e.g. by governing copper ion release from the material to the surrounding biological fluid). Consequently, it appears of prime importance to investigate both the sintering and the microstructure of pure apatitic phase CuHA ceramics.

This paper focuses on the processing of copper-doped hydroxyapatite ceramics by solid-state reaction sintering and on their microstructural characterization. Preliminary *in vitro* biological tests using MC3T3-E1 cell line was also performed to evaluate their biocompatibility. To this end, CuHAs ceramics with different copper concentrations from 0.8 to 10.7 wt% ( $x = 0.1\text{--}1.5$  mol in regard of the general formula  $\text{Ca}_{10}(\text{PO}_4)_6\text{Cu}_x\text{O}_y\text{H}_z$ ) were prepared.

## 2. Material and methods

### 2.1. Samples preparation

### 2.1.1. Starting powders

Pure calcium phosphate HA was first synthesized by a conventional aqueous precipitation method detailed in a previous work [38]. Briefly, a solution of diammonium hydrogenphosphate  $(\text{NH}_4)_2\text{HPO}_4$  (1.55 M, 1.2 L; Fisher Scientific) was dropwise added to a calcium nitrate solution  $\text{Ca}(\text{NO}_3)_2 \cdot 4\text{H}_2\text{O}$  (1.31 M, 2 L; Sigma-Aldrich). The pH of the liquid medium was maintained at 8.5 by addition of ammonium hydroxide  $\text{NH}_4\text{OH}$  (Fisher Scientific) and the temperature was fixed at 85 °C. The solution was continuously stirred and refluxed under argon atmosphere in order to prevent the carbonation of HA. After total addition of the phosphate solution, the suspension was ripened for 5 h. The precipitate was extracted by centrifugation, washed two times with distilled water, dried over night at 100 °C and grinded in a mortar. The as-prepared powder (around 200g per synthesis) was annealed at 600 °C for 1 h to eliminate the by-products. It will be referred as HA600. After precipitation and annealing at 600 °C, a pure HA phase was obtained. All the diffraction peaks indexed according to ICDD-PDF card n°9–0432, corresponded to the HA crystal lattice (Fig. A1(a) - see appendix). Phase purity of the powder was checked and a Ca/P molar ratio of 1.667 was determined after calcination at 1000 °C for 15 h according to the standard specifications of ISO 13779–3:2018 [39].

A commercially available copper oxide powder was purchased (Alfa Aesar). The X-ray diffraction pattern of the raw CuO powder is given in Figure A1(b).

### 2.1.2. Cu-doped HA powder blend and pellet preparation

HA600 and copper oxide CuO powders were intimately mixed and milled by attrition (NETZSCH device). The following copper oxide weight contents were added to HA600: 0.8, 2.3, 3.8, 5.3 and 10.7 wt% leading respectively to a copper content  $x$  of 0.1, 0.3, 0.5, 0.7 and 1.5 mol in accordance with a general formula  $\text{Ca}_{10}(\text{PO}_4)_6\text{Cu}_x\text{O}_y\text{H}_z$ . Milling was carried out in water, with 1 wt% of dispersant Darvan CN (Vanderbilt Minerals) towards the total amount of powders. Attrition milling was carried out at 800 rpm, during 3 h in a Teflon container using yttrium-stabilized zirconia balls of 1 mm diameter. The volumetric particle size distributions of the initial raw powders HA600 and CuO oxides and of the 3 h-milled suspension ns-CuHA0.5 are reported in Figure A2. The particle size distributions were determined using a laser particle size analyzer (Partica LA-950V2, Horiba). While the raw powders get particle size distribution with average size larger than 5  $\mu\text{m}$ , the average particle size of the CuO-HA mixture after attrition was around 1.5  $\mu\text{m}$ . Attrition milling was performed because the particle size reduction improves the solid-state reaction between the two powders to form copper-substituted CuHAX. The milled blends of HA and CuO powders will be referred as ns-CuHAX. Finally, they were dried over night at 100 °C and sieved at 80  $\mu\text{m}$ .

Green pellets of ns-CuHAX blends were shaped by uniaxial pressing at 100 MPa and sintered under air atmosphere from 900 °C to 1200 °C with a dwell time of 30 min and a heating rate of 10 °C/min. The CuHA bulk density was measured by helium pycnometry (AccuPyc II 1340, Micromeritics) after a grinding of the sintered pellets. Ten measurements were done. The apparent relative density of the pellets was measured by Archimede method from pellet immersion into water. The ratio of the apparent relative density on the bulk density gives access to the densification rate.

## 2.2. Characterization techniques

### 2.2.1. Chemical analyses

Copper content in Cu-doped HA was measured by ICP-OES (PerkinElmer Optima 8300). The apparatus was calibrated using standard solutions of copper and an average of 3 measures by sample was done. Samples were prepared by dissolving 15 mg of powder in 6 mL  $\text{HNO}_3$ -HCl (3:2) heated by microwave radiations. Then, the solution was diluted in distilled water to reach a total volume of 100 mL. To focus on the chemical composition,

infrared spectra of the samples were obtained on a Spectrum One FTIR spectrometer from PerkinElmer. 32 scans were recorded between 4000 and 400  $\text{cm}^{-1}$  with a 4  $\text{cm}^{-1}$  resolution using the KBr pellet method.

### 2.2.2. X-ray diffraction

(i) - Temperature reaction between HA and copper oxide was investigated by means of temperature programmed XRD using a furnace (HTK1200 N, Anton PAAR) mounted into a Brüker D8 Advance Da Vinci diffractometer with a Bragg-Brentano geometry. A pellet of the ns-CuHA0.5 powder was shaped. XRD patterns were collected from 23 to 43° ( $2\theta$ ) with a step size of 0.02° and a step time of 1.5s. A Cu  $K\alpha$  radiation was used at 40 kV and 40 mA. In situ XRD acquisitions were performed every 50 °C from 900 to 1150 °C as follows: ramp of 10 °C/min, dwell time of 15 min at the desired temperature to stabilize the system before the pattern acquisition of 30 min duration.

(ii) - Phase purity of CuHax samples was confirmed by XRD patterns collected at room temperature with a Brüker D8 Advance Serie II diffractometer equipped with a Cu  $K\alpha$ 1 radiation X-ray tube and a rear monochromator. Acquisitions were operated at 40 kV and 40 mA from 10 to 60° ( $2\theta$ ) using a step size of 0.02° and a step time of 1.4s. Samples were rotated at 10 rpm during the measurements to avoid particle orientation effects. The crystal structure of the apatite phases was refined in space group  $P6_3/m$  using the FullProf program.

### 2.2.3. Thermal analyses

(i) - The thermal behaviour of pure HA and CuHax was investigated by thermogravimetry coupled with differential thermal analysis (TG/DTA, STA 449 F3 Jupiter, NETZSCH). The HA600 powder and a mixture containing 80 wt% of HA600 and 20 wt% ( $x = 3.2$ ) of copper oxide were analysed (CuHA3.2). This high amount of CuO was chosen voluntary to allow the easiest identification of the thermal effects occurring between HA and CuO by making them as intense as possible. Indeed, it corresponds to an excess of CuO which cannot react completely with HA. Measurements were performed up to 1500 °C with a heating rate of 20 °C/min under air flow.

(ii) - The sintering behaviour of the ceramics was followed by dilatometry using a thermomechanical analyzer SETSYS evolution (SETARAM instrumentation). A contact force of 5 g was applied on the green ns-CuHax pellets. Pellets were heated up to 1250 °C during 30 min with a heating rate of 10 °C/min under air flow.

### 2.2.4. Electron microscopy (SEM)

(i) - The surface of the sintered pellets was imaged by SEM with a Zeiss microscope LEO 1530 VP. The working distance was fixed at 5 mm, the EHT at 1 kV and a secondary electron detector was used. The average grain size of the pellets was determined via the ImageJ software. Different areas were analysed collecting grain size distribution on a set of 300 grains or more.

(ii) - Elemental cartography was imaged on a field emission electron microscope JEM 2100F (JEOL, 200 kV field emission) coupled with an energy dispersive X-ray spectrometer. A lamella of a few hundred nanometers was cut in the bulk of a sintered pellet using a FIB-SEM (Zeiss Crossbeam 550). A copper holder was used to fix the sample, which did not allow making a quantitative analysis of copper.

## 2.3. In vitro biological assays

### 2.3.1. Ceramic substrates preparation

Before the biological assays, pellets of pure HA and CuHax were sintered respectively at 1200 °C and 1100 °C for 1 h. The substrates were polished using a series of silicon carbide grits (P600 to P4000) and sterilised at 200 °C for 2 h at least under air atmosphere. Finally, they were equilibrated during 1 h into a culture plate (Thermo Fisher Scientific) in complete alpha modified Eagle's medium MEM- $\alpha$  (Gibco) without ascorbic acid and supplemented with 10% fetal calf serum (Invitrogen), 50  $\text{UI}\cdot\text{mL}^{-1}$  penicillin and 50  $\mu\text{g mL}^{-1}$  streptomycin

(Gibco) in an incubator heated at 37 °C under 5% CO<sub>2</sub> wet atmosphere. This culture medium is hereafter called growth medium – GM.

### 2.3.2. Cell culture and seeding

Pre-osteoblastic cells MC3T3-E1 subclone 14 (ATCC, then referred as MC3T3-E1) were routinely cultured in GM in an incubator heated at 37 °C under 5% CO<sub>2</sub> wet atmosphere. The medium was replaced every 2–3 days and cells were split when the cell confluence reached 70–80% of the culture area. After counting cells on a Malassez haemocytometer, an amount of 10,000 cells/cm<sup>2</sup> was seeded dropwise onto the HA and CuHax pellets in GM. Cells were cultured at 37 °C under 5% CO<sub>2</sub> wet atmosphere for 1, 3 and 5 days for the viability assays and 7 days for the differentiation tests. These time points were chosen because the MC3T3 Subclone 14 cells exhibit a high level of differentiation after growth in ascorbic acid and 3–4 mM inorganic phosphate. They form a well mineralized extracellular matrix (ECM) after 10 days (ATCC technical datasheet). Thus, this cell line allowed us to check abnormalities of the differentiation process in the early times of cell culture. The classical time points for the study of differentiation are 3, 7, 14 and 21 days, the two later are usually for characterizing the mineralization step which is conditioned by the completion of the initial phases of cell differentiation.

### 2.3.3. Cell viability

The viability of MC3T3-E1 cells was tested by using the AlamarBlue<sup>®</sup> reagent (Thermo Fisher Scientific, USA). An amount equal to 10% of the well volume was added at the beginning of the cell culture. The AlamarBlue<sup>®</sup> reduction, resulting in a colour change from blue to pink over incubation time, reflects the metabolic activity of the growing cells. The fluorescence of AlamarBlue<sup>®</sup> was measured before the end of the incubation time at 585 nm with a FLUOstar OPTIMA spectrophotometer (BMG Labtech, Germany). The results were normalized on the HA sample after 2 h incubation. Viable cells were stained immediately after with 10 µM calcein red-orange AM (ThermoFisher), incubated during 15 min at 37 °C and rinsed in GM. All the nuclei were then stained by incubating the cells with 20 µM Hoescht 33342 for 5 min. Pellets were observed by fluorescence microscopy (AxioImager, Carl Zeiss). The ratio of calcein positive cells to the total cells (number of nuclei) was used to calculate the viability rate. For each experiment, the analysis was performed on a minimum of five fields and more than 1000 cells were counted.

### 2.3.4. Cell differentiation

MC3T3-E1 cells were seeded at a density of 15,000 cells/cm<sup>2</sup> in 12-well plates containing ceramic pellets in a differentiation medium (DM) consisting in GM with the addition of 100 nM dexamethasone (AppliChem), 10 mM beta-glycerophosphate (AppliChem) and 50 µM l-ascorbic acid (Sigma Aldrich). Two controls were done without ceramic material: cells in GM and in DM were respectively used as negative and positive controls. After 3 days of culture, the medium was changed to fresh medium. Cells were lysed and RNA extracted using a commercial kit according the instruction of the manufacturer (RNeasy<sup>®</sup> Plus Micro kit, Qiagen) with a modification as previously described [12]. Eluates from RNA isolation on the column were kept at –20 °C for protein precipitation and extraction according to the protocol set up by Morse et al. [40]. The concentration of the precipitated proteins was measured for each sample by spectrophotometry at 280 nm (Nanodrop, ThermoFisher). For each condition, 15 µg of heat-denaturated proteins were loaded on 10% polyacrylamide gels and separated by electrophoresis. Then, the proteins were transferred on 0.45 µm polyvinylidene fluoride membranes (Biorad). After the saturation of the specific antigenic sites, the membranes were first hybridized with primary antibodies overnight at 4 °C and then with the appropriate secondary antibody (goat anti-rabbit; goat anti-mouse or mouse anti-goat) coupled to the Horse Raddish Peroxydase (all from Dako) for 1 h at RT. The proteins of interest were detected by chemiluminescence using a luminol-based reagent (Millipore) using a G-Box system (Syngene). The primary antibodies used in this study were: mouse anti RUNX2 (Abcam), goat anti-osteopontin (R&D), and mouse anti GAPDH (Santa-Cruz Biotechnology). Analysis of the western blots was done using the ImageJ software and the densities of the signals of interest were normalized to those of GAPDH.

### 2.3.5. Statistics

The calcein viability tests and the differentiation tests were conducted with three independent *in vitro* experiments for each ceramic group. For the AlamarBlue® reduction, one and two independent experiments were considered respectively for 1 and 3 days while three independent experiments have been performed for 4 and 5 days. Data were assayed for normality using the Shapiro-Wilk test using PAST [41]. According to the data set and normality test results, the Kruskal-Wallis test was followed by a Dunn's post hoc test, or one-way analysis of variance (ANOVA) was performed followed by a Tukey's multiple comparison test using GraphPad Prism 6. Differences were considered significant for  $p < 0.05$ .

## 3. Results and discussion

### 3.1. Solid-state reaction between HA and CuO

In a first step, temperature programmed XRD was performed on ns-CuHA0.5 powder. The HA and CuO phases of the powder blend are detected up to 950 °C (Fig. 1a). The reaction occurs at a temperature around 1000 °C. A pure apatite phase is detected above this temperature; no secondary crystalline phase is identified in the compound. This indicates that copper is fully incorporated in the apatite lattice to produce a copper substituted HA (CuHAx).

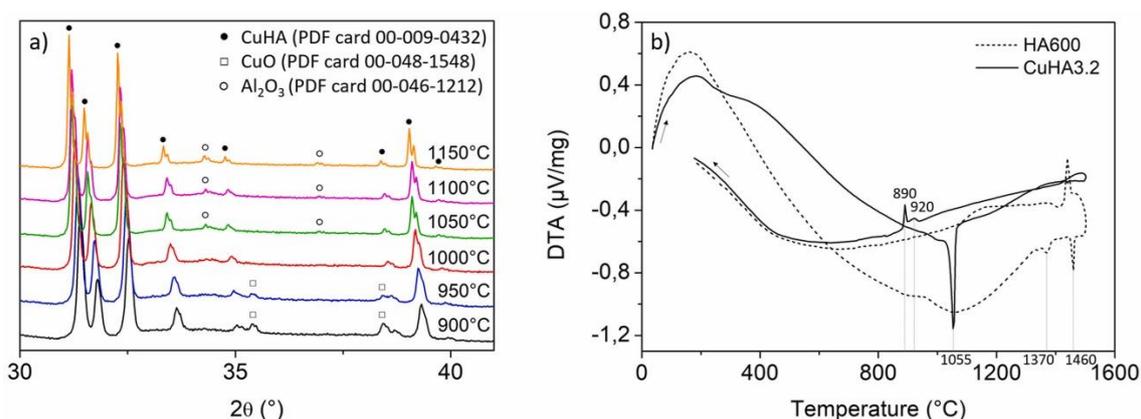
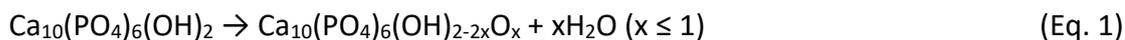


Fig. 1. Temperature programmed XRD of ns-CuHA0.5 samples, peaks associated with corundum are due to the alumina sample holder (a) and DTA measurement on CuHA3.2 sample, powder blend containing 80 wt% of HA600 and 20 wt% -  $x = 3.2$  mol-of CuO (b).

On the DTA curve of pure HA (Fig. 1b), the wide endothermic effect from 950 °C and the small endothermic peak at 1370 °C are due to its dehydroxylation (Eq. (1)). Then, the formed oxyapatite decomposes into  $\alpha$ -tricalcium phosphate and tetracalcium phosphate monoxide at 1460 °C (Eq. (2)). These endothermic reactions are reversible in air atmosphere: exothermic effects at similar temperatures can be seen during cooling to room temperature. These two well-documented reactions are typical of HA samples [38,42].



In presence of copper, a sharp and intense endothermic phenomenon is observed during heating with a maximum at 1055 °C. The temperature at which this effect begins is difficult to assess because of the presence of a secondary endothermic shoulder. This main peak is associated with the reaction between HA and CuO to form copper substituted HA. Indeed, the temperature is in agreement with the reaction temperature detected from in situ XRD analyses. Surprisingly, the formed CuHA phase does not dehydrate or decompose up to 1500 °C, so the presence of copper ions seems to stabilize the apatite structure at higher temperature.

According to the Ellingham diagram relative to copper element, the reduction of CuO into Cu<sub>2</sub>O occurs at 960 °C in atmospheric air conditions ( $P_{O_2} = 0.2$  bar, see fig. A.5). The endothermic shoulder registered during heating around this temperature in the foot of main endothermic peak of copper-HA reaction can be associated to the reduction of copper oxide that has not yet reacted with HA. During cooling, two exothermic peaks are observed with maxima at 920 °C and 890 °C. Therefore, these two peaks may be due to the reoxidation of the remaining Cu<sub>2</sub>O phase that has not reacted with HA. Indeed, in this experiment a very high amount of copper oxide was used (i.e. 20 wt% –  $x = 3.15$ ), which is over the maximum amount leading to pure CuHA compounds after reaction, as exposed in the following paragraph (see Fig. 3b for  $x = 1.5$ ). These results show that a copper-doped hydroxyapatite phase stable up to 1500 °C can be obtained by solid-state reaction from 950 °C. Furthermore, the introduction of copper ions into the apatite structure occurs while there is a partial reduction of the copper oxidation state.

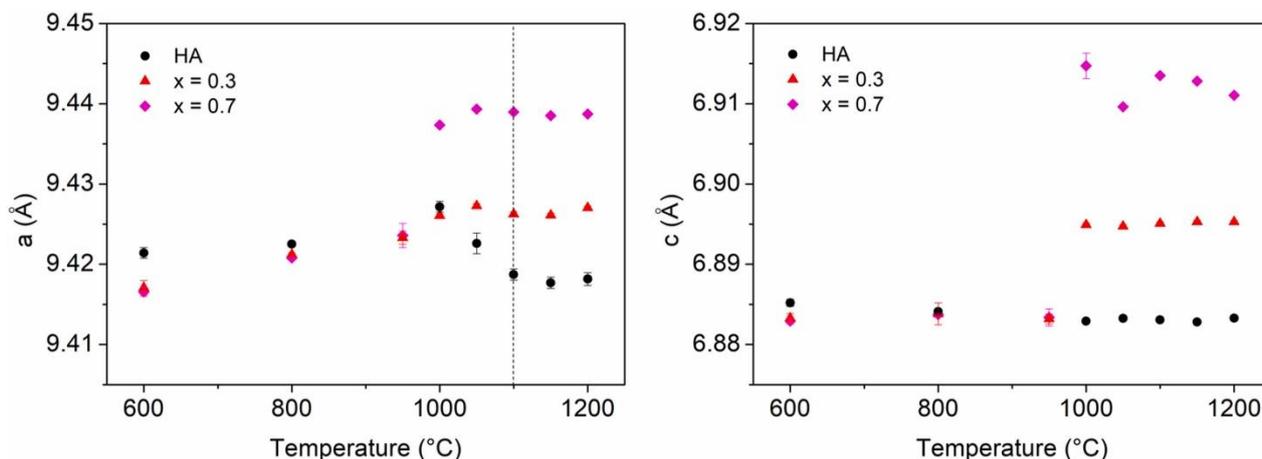


Fig. 2. Evolution of the lattice parameters  $a$  and  $c$  of the apatite phase in pure HA, CuHA0.3 and CuHA0.7 powders vs the calcination temperature (dwell time 1 h).

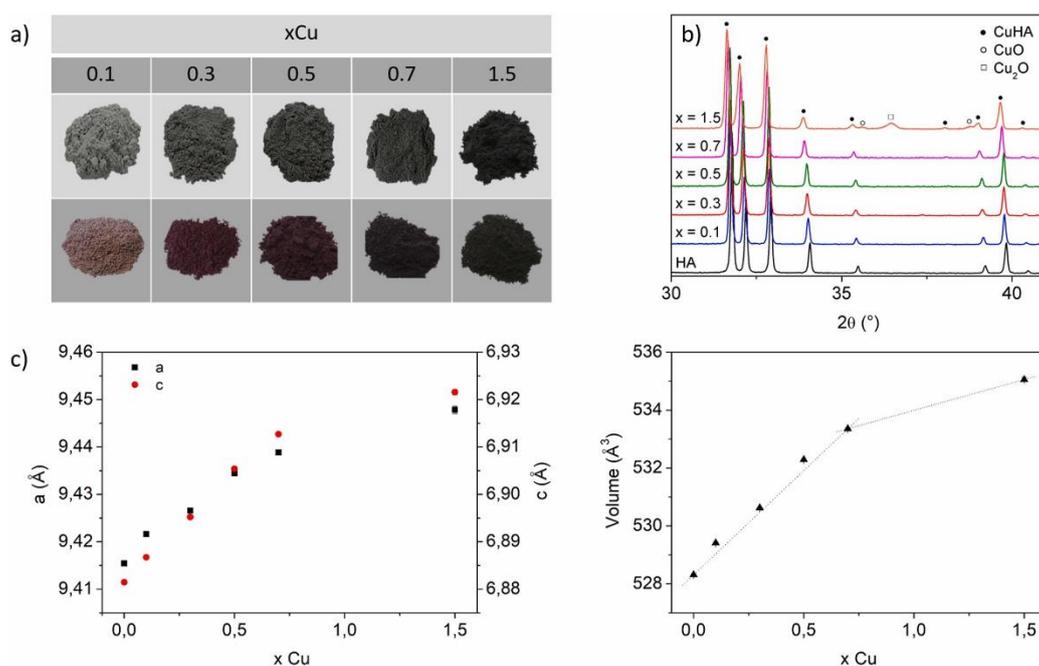


Fig. 3. CuHA $x$  powders characterisation. Initial blends of HA and CuO powders ns-CUHAx (top) and CuHA $x$  powders (bottom) obtained after grinding pellets sintered at 1100 °C for 1 h (a) with the XRD patterns (b) and the lattice parameters and volume of the sintered powdery samples, the error bars do not exceed the symbol size (c).

Pellets of pure HA600, ns-CuHA0.3 and ns-CuHA0.7 mixtures were heated at different temperatures from 600 °C to 1200 °C for 1 h and the lattice parameters of the formed apatite were refined from XRD patterns to evaluate the influence of the temperature and copper amount on the kinetics of copper incorporation (Fig. 2). The lattice parameters  $a$  and  $c$  of the apatite phase remains the same below 800 °C, an abrupt deviation occurs between 800 and 1050 °C leading to an increase of the unit-cell parameters with the copper concentration. Then, from 1050 °C both  $a$  and  $c$  lattice parameters are constant whatever the copper content. The decrease of the  $a$  parameter for pure HA from 1000 °C is due to its dehydroxylation that occurs from this temperature. This phenomenon is quite not observed on CuHA $x$  compounds. Thus, the incorporation of copper appears completed from 1050 °C. The influence of the dwell was studied at 1100 °C. The lattice parameters remain constant for dwell durations between 0.5 and 4 h (data not shown).

Finally, ns-CuHA $x$  blends of raw HA and CuO powders were die pressed into pellets and sintered at 1100 °C for 1 h to investigate the influence of the copper amount, as these sintering conditions allow to complete the reaction of copper oxide with HA. After thermal treatment, pellets were crushed into powder before analysis. A colour change of the pellets, from grey to purple is observed (Fig. 3a). On the XRD patterns (Fig. 3b), a pure apatite phase is obtained up to  $x = 0.7$ . For the pure phases, experimental copper contents measured by ICP-OES are similar to those introduced in the powder blend. The presence, besides the main apatite phase, of both cupric CuO and cuprous Cu<sub>2</sub>O oxides for  $x = 1.5$  confirms the partial reduction of Cu<sup>II</sup> in Cu<sup>I</sup> stated from DTA. The mixed valence of copper in the copper-substituted apatite explains the purple colour of the ceramic pellets, pure Cu<sup>II</sup>-doped HA being reported as blue-coloured [[27], [28], [29], [30], [31]]. The shift of the XRD peaks towards small angles is associated to a linear increase of the lattice volume and parameters of the apatite phase with copper amount (Fig. 3c). The plot of the unit-cell volume versus copper content shows a slope decrease between  $x = 0.7$  and  $x = 1.5$  compositions which is in agreement with a limit of copper insertion in the HA lattice and the presence of secondary phases of copper oxides in the CuHA1.5 compound.

FTIR spectra show that all the heated samples exhibit the bands characteristic of apatite structure (Figure A3) [38,43]. Two regions are of particular interest: the first one from 400 to 1200 cm<sup>-1</sup>, mainly characteristic of the phosphate groups (Fig. 4a) and the second one from 3000 to 4000 cm<sup>-1</sup> corresponds to the hydroxyl group vibrations (Fig. 4b). In the range 950–1100 cm<sup>-1</sup>, the bands are assigned to the P–O stretching vibration of the phosphate groups while the bands from 430 to 605 cm<sup>-1</sup> correspond to the phosphate bending vibration. The stretching vibration of the single hydroxyl groups gives bands around 3570 and 630 cm<sup>-1</sup>. With the increase of copper content, the two latter bands decrease in intensity, which suggests that copper substitutes the hydrogens of the hydroxyl groups into the hexagonal channels. Three new bands also appear at 3425, 3340 and 3230 cm<sup>-1</sup>, which must correspond with hydroxyl group vibrations in modified environments due to the close neighbouring of copper. This was already observed in the literature [21,23]. The OH groups can be affected either by their direct bonding with copper atom or indirectly by hydrogen bonding Cu–O–H–O in copper neighbouring [21,[44], [45], [46], [47]]. Insertion of copper in the hexagonal channels of hydroxyl location is also supported by the increase of the lattice parameters. Indeed, the smaller ionic radius of copper would have led to a decrease of the lattice parameters in case of a copper for calcium substitution in the apatite. Unit-cell volume expansion relates to the insertion of copper in the apatite structure along the OH channels. Similar results were previously reported in the literature [22,33,34]. New IR bands also appear in the range 675–900 cm<sup>-1</sup>: two weak bands are observed at 675 and 760 cm<sup>-1</sup> and three others around 810, 840 and 865 cm<sup>-1</sup>. This region can be associated with Cu–O vibrations. The Cu–O–H bonds give bending absorptions at different frequencies depending on the strength of the hydrogen bonding [21,44,45]. The results, especially the hydroxyl group IR band splitting, confirm the insertion of copper into the HA hexagonal channels.

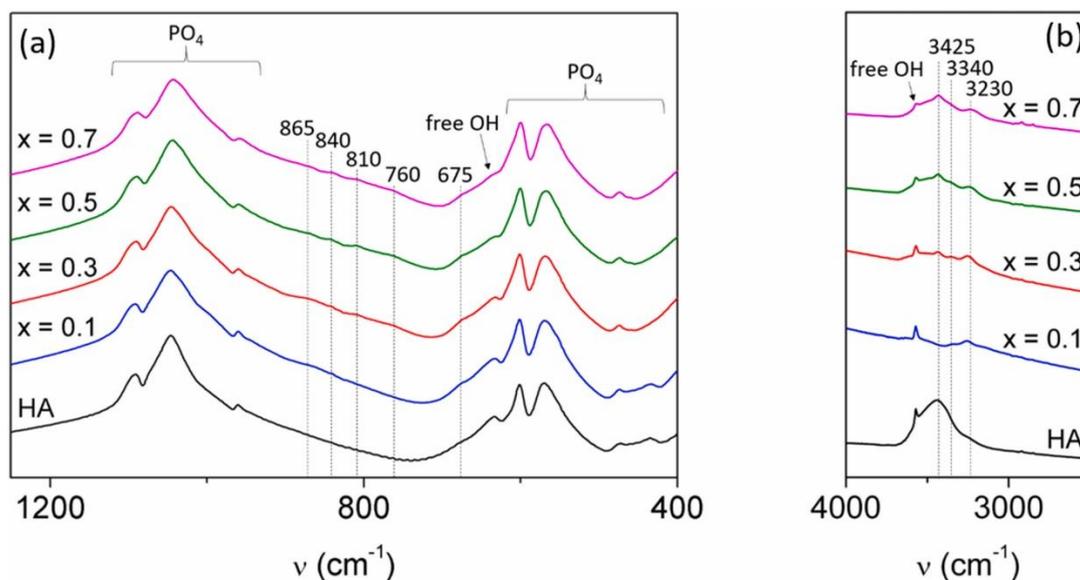


Fig. 4. FTIR spectra of HA600 and CuHAx powdery samples prepared by grinding pellets sintered at 1100 °C for 1 h, zoom on the phosphate group region (a) and the hydroxyl group region (b).

Finally, the overall results show that pure copper-substituted HA containing up to 0.7 mol of copper can be obtained by solid state reaction from 1050 °C. Copper of mixed valence I and II is inserted in the apatite lattice along with the OH channel. The disappearance of some hydrogens for charge balance conducts to propose the following formula for the apatite phase of CuHAx after thermal treatment:  $\text{Ca}_{10}(\text{PO}_4)_6\text{Cu}^{\text{II}}_z\text{Cu}^{\text{I}}_x\text{O}_2\text{H}_{2-2x}$  with  $x = y + z$ . An advanced structural analysis to determine the exact positions and oxidation degrees of copper in the apatite lattice, including in particular  $^1\text{H}$  and  $^{31}\text{P}$  nuclear magnetic resonance (NMR), extended X-ray absorption fine structure (EXAFS), electron paramagnetic resonance (EPR), diffuse reflectance (DR) spectroscopies and XRD refinements was carried out [48]. The results will be published elsewhere.

### 3.2. Sintering

Only mixtures leading to apatite monophasic compounds were investigated in this part (i.e. CuHAx with x up to 0.7 mol). The dilatometric shrinkage curves show that the temperatures of sintering onset (beginning of the pellet shrinkage) and maximum sintering rate (inflexion point of the shrinkage curve or minimum on derivative curve) are similar for the pure HA and the CuHAx pellets (Fig. 5a). The sintering begins around 700 °C and the maximum rate for HA is around 1010 °C with a light shift that does not exceed 20 °C towards high temperatures for CuHAx. Therefore, copper does not influence the sinterability of HA. As the temperature reaction between HA and CuO is close to the sintering temperature, a direct “reaction-sintering” can be used to produce ceramic parts. To investigate this possibility, the influence of the sintering temperature, for a dwell time of 30 min, on the final densification of CuHAx ceramics was studied. Dense monophasic ceramics made of pure apatite crystalline phase are obtained from ns-CuHAx biphasic mixtures with a densification rate higher than 96% from 1100 °C for 30 min (Fig. 5b), which confirms the possibility to achieve reaction sintering. The densification rates of pure HA and CuHA0.1 slightly increase from 1050 to 1200 °C temperatures while there is no evolution or even a light decrease for higher copper contents. This phenomenon is visible at 1200 °C for which the ceramics with the lowest copper rate (CuHA0.1) have a densification rate close to 99% while it is only of 96% for the other CuHAx ceramics. It may be due to the classical Ostwald ripening due to grain coarsening in some ceramic materials at high temperature.

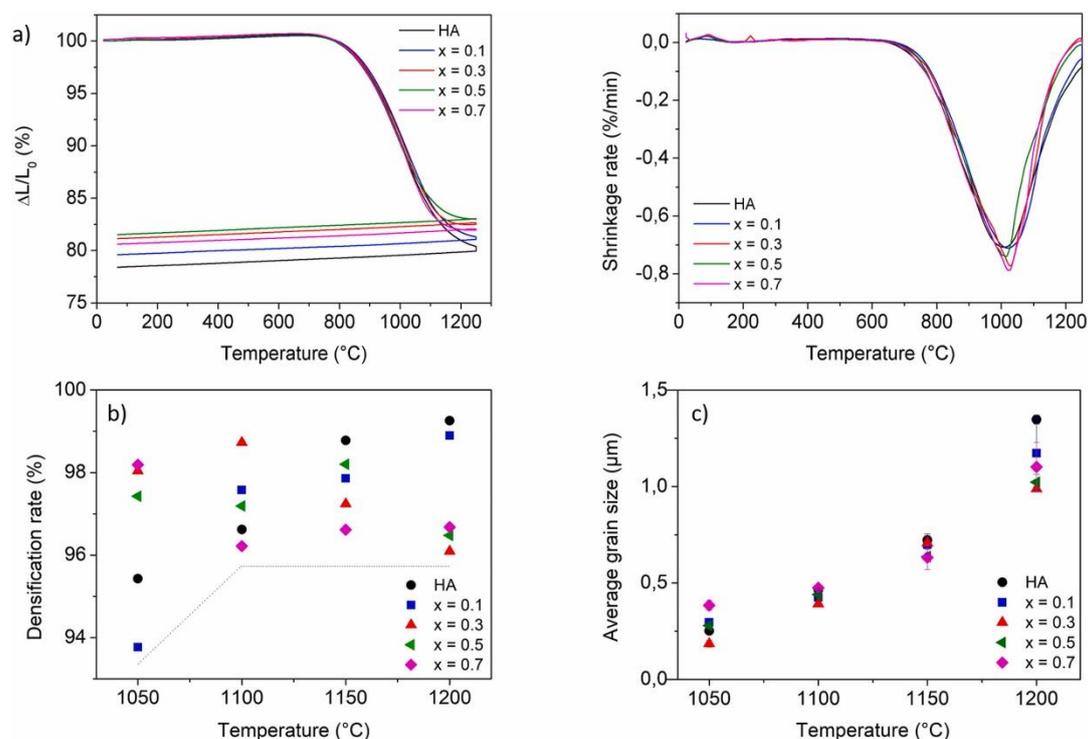
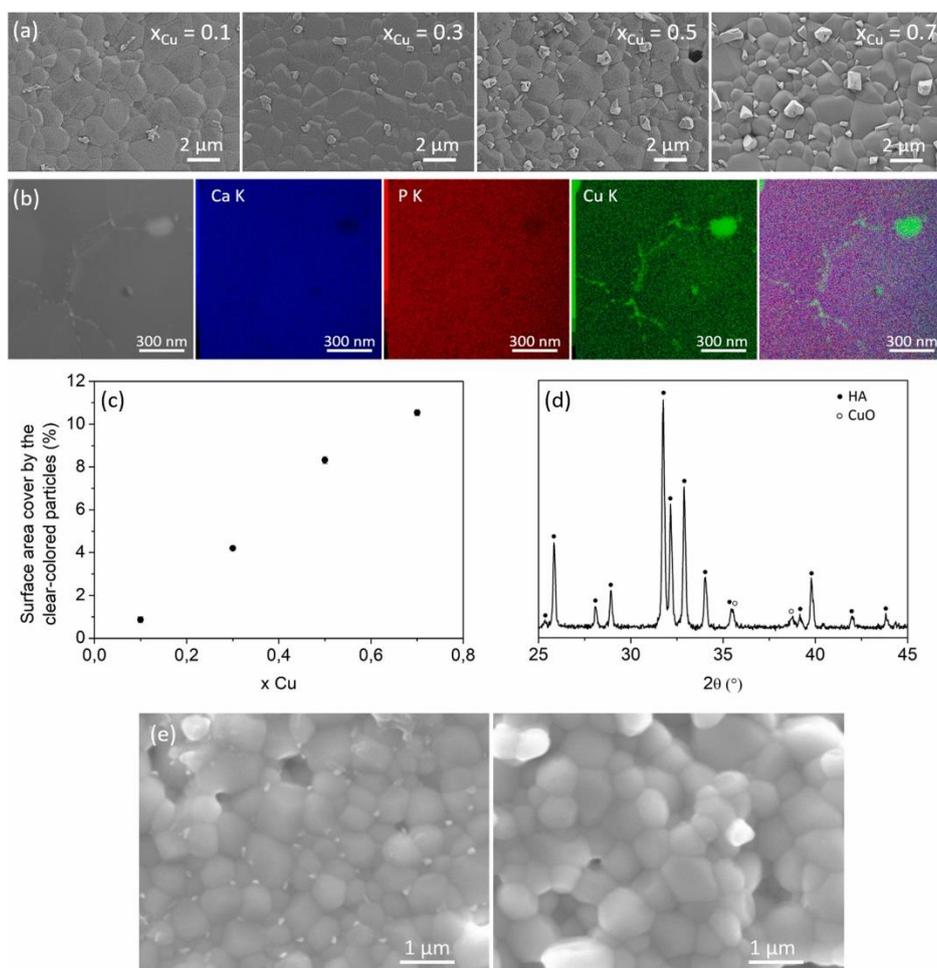


Fig. 5. Dilatometric shrinkage curves of HA600 and CuHA<sub>x</sub> pellets and derivative plot of densification vs the temperature (a), densification rate of ceramic parts after sintering for 1 h at different temperatures (b) and the associated grain size (c).

Regarding the microstructures of the ceramics, the average grain size, determined from SEM images of pellets surface (examples can be found in Figure A4), increases according to an exponential law with the temperature in the range 1050–1200 °C (Fig. 5c). Average grain size remains submicrometric up to 1150 °C, so temperatures between 1100 and 1150 °C seems to be optimal to manufacture pure dense copper-substituted hydroxyapatite ceramics having fine microstructures. Two types of grains are observed on SEM images at the pellet surface (Fig. 6a). The amount of the “light” grains increases proportionally to the copper rate (Fig. 6c) but remains stable for each composition whatever the sintering temperature may be from 1050 °C to 1200 °C (see figure A4 in the case of CuHA<sub>0.5</sub> for example). STEM-EDX cartographies of phosphorus, calcium and copper on a bulk lamella exhibit the presence of copper-rich compositions at the grain boundaries (Fig. 6b).

Two hypotheses can be put forward to explain these results. On the one hand, copper segregation at the grain boundaries has already been observed in copper-rich phase due to oxido-reduction mechanisms [49,50]. As mentioned above, during heating, Cu<sup>II</sup>O reduces into Cu<sub>2</sub>O above 960 °C and copper, mainly in Cu<sup>I</sup> form, is incorporated into the apatite structure. However, Cu<sup>I</sup> is only stable at high temperatures, so during cooling to room temperature, some Cu<sup>+</sup> ions (located near the material surface) could have been oxidized into Cu<sup>2+</sup>. This oxidation would be accompanied with the migration of part of this species to leave the apatite structure in order to maintain the crystal charge balance, forming thus copper-rich grain boundaries. On the other hand, Zykin et al. [34] showed that the solubility of copper (at the equilibrium) in the HA lattice grows with the temperature and indicates a reversible incorporation-deposition of copper in HA on the thermal treatment.



*Fig. 6. SEM micrographs of CuHA<sub>x</sub> ceramics surface after sintering at 1200 °C for 30 min (a); Calcium, phosphorus and copper STEM-EDX cartographies of CuHA0.7 sample sintered at 1200°C-30 min (b); Percentage of surface area covered by the “light” particles, the error bars do not exceed the symbols (c); XRD pattern of CuHA0.5 ceramic surface after sintering at 1100°C-30 min and annealed at 500 °C for 1 h (d); SEM micrographs of CuHA0.7 sintered at 1200°C-30 min and quenched from the sintering to the room temperature in air (left) or in water (right) (e).*

This hypothesis appears highly consistent with regard to our result. Indeed, some of the copper incorporated at high temperature in the HA crystals could have migrated to the grains surface (i.e. at the grain boundary) during cooling to room temperature due to the temperature dependent solubility. Annealing the samples at 500 °C for 1 h after sintering confirmed the reversibility of Cu incorporation in the HA. A change of colour of the pellets from purple to grey was observed and the DRX patterns of the ceramics surface showed the presence of copper oxide (Fig. 6d). Conversely, the purple colour remained after quenching in air or in water from the sintering temperature to room temperature and the concentration of “light” grains decreased in air to disappear totally in water. Thus, demixion occurs while, during the cooling down, new CuO is formed from Cu<sup>+</sup> previously incorporated in the HA. In agreement with Ellingham diagram of copper (figure A5), the demixion seems to proceed due to the oxidation of Cu<sup>+</sup> into Cu<sup>2+</sup>, showing thus the difficulty for the HA network to incorporate Cu<sup>2+</sup> cations (hence, it tends to confirm the majority of +I oxidation state of copper in the HA lattice). The temperature of oxidation under air atmosphere is about 900 °C, which also explains that a quenching from 1100 °C (from Cu<sup>+</sup> stability domain in Ellingham diagram) to room temperature allows to keep a large amount of copper +I inside the HA structure in comparison with a slow cooling down.

On the overall, these results agree with a thermodynamical metastability of the CuHA<sub>x</sub> phase at room temperature. They also show the importance of an accurate characterisation of the sintered ceramics, requiring complementary techniques to ensure that phase pure apatitic materials are produced.

Finally, dense monophasic ceramics made of copper-substituted HA  $\text{Ca}_{10}(\text{PO}_4)_6\text{Cu}^{\text{II}}_z\text{Cu}^{\text{I}}_y\text{O}_{2\text{H}_2-2z-y}$  ( $y \gg z$ ) with a fine microstructure can be produced by reaction-sintering between mixtures of HA and CuO powders providing adjusted thermal treatments are performed.

### 3.3. Preliminary *in vitro* biological behaviour

For the cell culture experiments, pellets of pure HA and CuHAX ( $x \leq 0.7$ ) were sintered respectively at 1200 °C and 1100 °C for 1 h to ensure a high densification rate. Taking HA pellets as reference, no change in the cell viability is observed after 1 and 3 days of culture on CuHAX samples. The observation of the viable cell morphology after 3 days of culture (Fig. 7c, upper panel) does not highlight any effect of the presence of copper in the ceramic. The cells are well spread with a comparable morphology and they seem to be healthy. After 5 days, the cell viability is significantly decreased for CuHA0.7 that contains the highest amount of copper (Fig. 7a). For the two highest copper amounts, a few cells, positive to calcein, present a reduced surface area and a particular morphology of their nuclei indicating that they have likely entered a process of apoptotic cell death (Fig. 7c, see arrows on lower panel). Nevertheless, even at 5 days, the viability rates remain close to 100% in all of the cases (Fig. 7a). Therefore, copper seems to have only a light negative influence on the cell physiology at this time. For all the time points, no necrotic cells are observed, regardless of the ceramic chemical composition. The CuHAX ceramics do not cause sudden cell death.

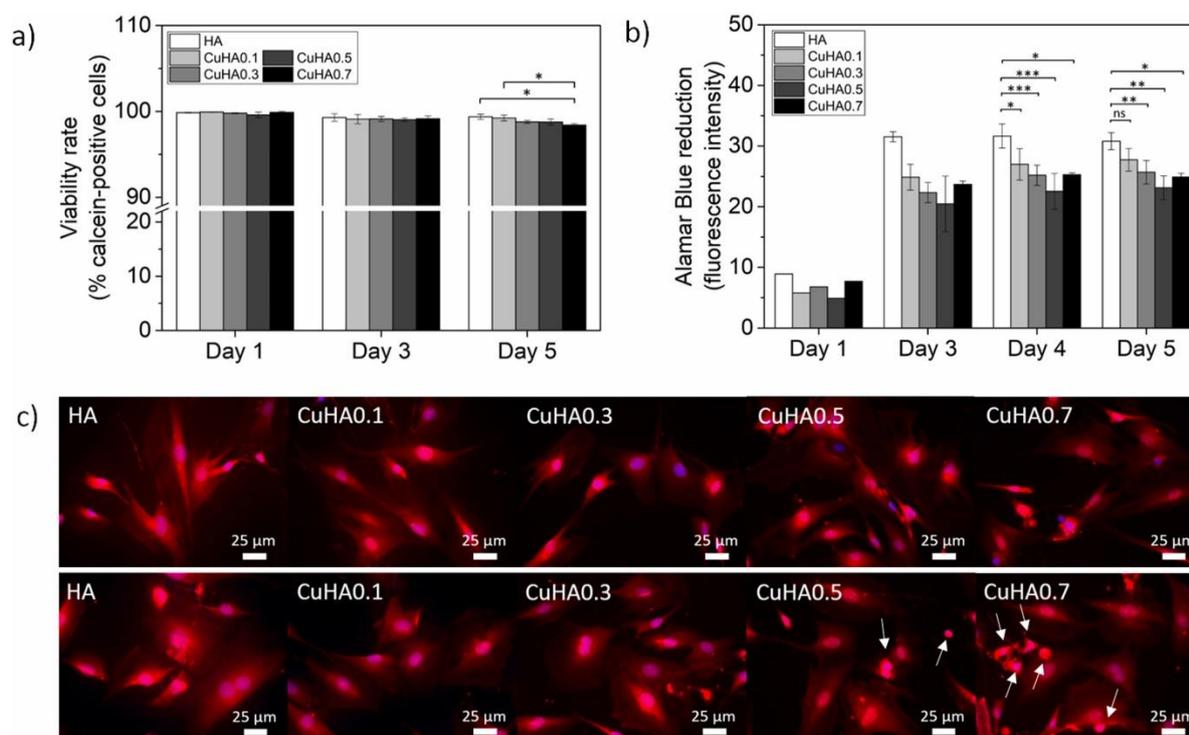


Fig. 7. The viability rate at the ceramic material surface (a) and the metabolic activity of the cell population over time (b). Statistical analysis: ANOVA-One way followed by Tukey post-hoc test: ns: non significant; \*:  $p < 0.05$ ; \*\*:  $p \leq 0.01$ ; \*\*\*:  $p \leq 0.0001$ . Morphology of the viable cells observed in fluorescence microscopy after staining with calcein red-orange (in red); the nuclei were stained with Hoescht 33342 (in blue) after 3 days (upper panel) and 5 days (lower panel) of culture, arrows indicate cells presenting apoptotic morphology (c). (For interpretation of the references to colour in this figure legend, the reader is referred to the Web version of this article.)

The metabolic activity of the cells increases before becoming constant after 3 days (Fig. 7b). However, a significantly lower cell growth is observed on CuHAX ceramics in comparison with HA. On the fluorescence microscopy images (Fig. 7c), the confluence was not reached, which cannot explain this lower cell growth. The same behaviour is observed for all CuHAX ceramics up to 5 days whatever the copper amount may be. As the cell density remains similar on the HA and CuHAX samples (Figure A6), it can be stated that copper does not affect cell proliferation but cell activity. The alteration of cell functionality in presence of copper could be linked

to the generation of reactive oxygen species [51]. Nevertheless, the cell activity on CuHAx is always more than 75% that of pure HA (used as a biocompatible material of reference), which is above the cytotoxicity threshold fixed at 70% by the ISO standard 10993-5 [52]. In light of these results, the copper-substituted HA ceramics are non-cytotoxic after 5 days of culture.

To deepen this biological evaluation, the ability of the pre-osteoblastic cells to differentiate on the surface of the ceramics was evaluated through the detection of protein markers associated with osteogenesis by western-blot (Fig. 8). The evaluated proteins were the master transcription factor RUNX2 (Runt-related transcription factor 2), expressed early in the differentiation process, and osteopontin (OPN), a bone extracellular matrix protein associated to the mineralization process, expressed later. The expression of RUNX2 (Fig. 8b) is significantly lower when cells grew up on the ceramic materials than on the plastic in DM. In addition, RUNX2 expression tends to be reduced with the increasing amount of copper. But, it becomes significantly lower when compared to cells grown on HA only for CuHA0.7.

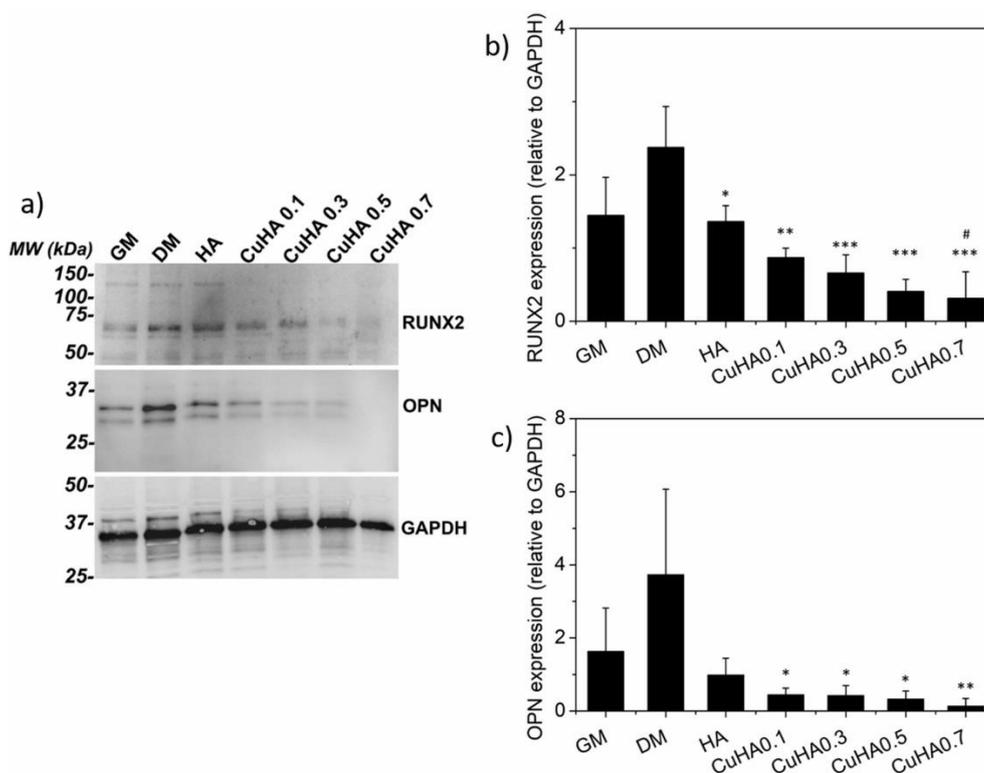


Fig. 8. Western-blot evaluation of the expression of RUNX2 and OPN in MC3T3-E1 cells (a). Semi-quantitative evaluation of the expression of RUNX-2 (b) and OPN (c) by densitometry analysis of the western-blot results. The values were normalized on GAPDH signal. Statistical analysis: ANOVA one way followed by a Tukey post hoc test. \*: vs. DM,  $p \leq 0.05$ ; \*\*: vs. DM,  $p \leq 0.01$ ; \*\*\*: vs. DM,  $p \leq 0.001$ ; #: vs. HA,  $p \leq 0.05$ .

In light of the expression profile of RUNX2 during osteogenesis, two hypotheses can be formulated. The osteogenic process is inhibited by the presence of copper in HA, or, conversely, differentiation is accelerated. Indeed, the cells used in this study are the subclone 14 derived from MC3T3-E1 pre-osteoblasts and selected for their capacity to differentiate easily. At the chosen time point, it is possible that the peak of expression associated with the initiation of osteogenesis may have already passed for the cells on the samples with higher copper content and still in progress for the cells on the plastic in DM. The reduction of RUNX2 for cells cultured on ceramics compared to cells on plastic in osteogenic culture medium was previously observed [12] and attributed to the second hypothesis.

The analysis of osteopontin expression levels (Fig. 8c) show no significant change when cells grown on plastic are compared according to the culture medium: GM or DM or on pure HA ceramics in DM. When cells were cultured on CuHA ceramics, the expression of OPN is significantly lower than that of cells on plastic in DM

(positive control of differentiation) and is decreased comparatively to pure HA for the condition CuHA0.7. The visual observation of the cells during the experiment did not show any sign of a mineralization process. Therefore, the second hypothesis formulated above should likely be rejected. All together the osteoblastic differentiation-associated protein expression results suggest a negative effect of copper on pre-osteoblast differentiation *in vitro* when the copper amount in ceramics reaches 0.7 mol (5.3 wt%). At this step, an extensive biological study of cell behaviour including both osteoblastic and endothelial cells is needed for a wider understanding of the influence of copper substitution in HA. To make it possible, the precise control of the ceramic composition and purity is a prerequisite. As shown in this study, this can be achieved using an adjusted processing route to prevent copper segregation and the formation of secondary crystalline phase.

## 4. Conclusion

Calcium phosphate hydroxyapatite and copper oxide react at temperature close to 1000 °C to form copper-substituted HA. This temperature is in the same range as that necessary to sinter the material. Thus, pure and dense copper-substituted HA ceramics containing up to 5.3 wt% of copper can be produced by solid-state reaction sintering at 1100 °C. Using these conditions, fine microstructures with submicronic CuHA<sub>x</sub> grains are obtained. Due to copper reduction during heating, copper with a mixed valence (and predominantly Cu<sup>I</sup>) substitutes for hydrogen into the hexagonal channels of the apatite lattice leading to a solid solution Ca<sub>10</sub>(PO<sub>4</sub>)<sub>6</sub>Cu<sup>II</sup><sub>x</sub>Cu<sup>I</sup><sub>y</sub>O<sub>2</sub>H<sub>2-2x-y</sub>. The temperature dependant solubility of copper in the HA lattice can induce CuHA phase demixion and formation of CuO during cooling to room temperature. A quenching of the material can be performed to prevent this formation. The biocompatibility of the CuHA<sub>x</sub> ceramics towards the MC3T3-E1 cell line was assessed after 5 days of culture for ceramics containing up to 3.8 wt% of copper (CuHA0.5), the cell viability decreasing lightly above this amount. Nevertheless, a detrimental effect on cell growth was observed in the presence of copper at any amount in the HA. From these results, the biological behaviour of these bioceramics will be thoroughly investigated using more advanced biological models including primary osteogenic progenitors and endothelial cells.

## Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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## Appendix A. Supplementary data

The following is the Supplementary data to this article: [Download : Download Word document \(813KB\)](#)  
Multimedia component 1.

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