

Hypofractionated stereotactic radiotherapy for large brain metastases: Optimizing the dosimetric parameters

L. Brun, G. Dupic, V. Chassin, E. Chautard, J. Moreau, V. Dedieu, T. Khalil, P. Verrelle, M. Lapeyre, J. Biau

▶ To cite this version:

L. Brun, G. Dupic, V. Chassin, E. Chautard, J. Moreau, et al.. Hypofractionated stereotactic radiotherapy for large brain metastases: Optimizing the dosimetric parameters. Cancer/Radiothérapie, 2020, 10.1016/j.canrad.2020.04.011. hal-03052669

HAL Id: hal-03052669

https://hal.science/hal-03052669

Submitted on 13 Feb 2023

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.



Hypofractionated stereotactic radiotherapy for large brain metastases: optimizing the dosimetric parameters

Radiothérapie stéréotaxique hypofractionnée des métastases cérébrales volumineuses : optimisation de la dosimétrie

Lucie Brun^a, Guillaume Dupic^{a*}, Vincent Chassin^b, Emmanuel Chautard^{c,d}, Juliette Moreau^a, Véronique Dedieu^b, Toufic Khalil^e, Pierre Verrelle^a, Michel Lapeyre^a, Julian Biau^{a,c}

- ^a Department of Radiation Oncology, Jean Perrin Center, Clermont-Ferrand, France
- ^b Department of Medical Physics, Jean Perrin Center, Clermont-Ferrand, France
- ^c Clermont Auvergne University, INSERM, U1240 IMoST, 63000 Clermont-Ferrand, France
- ^d Department of Pathology, Clermont Auvergne University, Jean Perrin Center, 63011 Clermont-Ferrand, France
- ^e Department of Neurosurgery, Clermont-Ferrand Hospital, Clermont-Ferrand, 63003, France

*Corresponding author:

Guillaume Dupic

Department of Radiation Oncology, Jean Perrin Center, 63011 Clermont-Ferrand, France

Tel: +334 73 27 81 42 Fax: +334 73 27 81 25

guillaume.dupic@clermont.unicancer.fr

Running title: Brain stereotactic radiotherapy

SUMMARY

Purpose: Stereotactic radiotherapy plays a major role in the treatment of brain metastases

(BM). We aimed to compare the dosimetric results of four plans for hypofractionated

stereotactic radiotherapy (HFSRT) for large brain metastases.

Material and Methods: Ten patients treated with upfront NovalisTx® non-coplanar multiple

dynamic conformal arcs (DCA) HFSRT for ≥ 25 mm diameter single BM were included.

Three other volumetric modulated arc therapy (VMAT) treatment plans were evaluated: with

coplanar arcs (Eclipse®, Varian, VMATc_{Eclipse®}), with coplanar and non-coplanar arcs

(VMATnc_{Eclipse®}), and with non-coplanar arcs (Elements Cranial SRS®, Brainlab,

VMATnc_{Elements®}). The marginal dose prescribed for the PTV was 23.1 Gy (isodose 70%) in

three fractions. The mean GTV was 27 mm³.

Results: Better conformity indices were found with all VMAT techniques compared to DCA

(1.05 vs 1.28, p<0.05). Better gradient indices were found with VMATnc_{Elements®} and DCA

(2.43 vs 3.02, p<0.001). High-dose delivery in healthy brain was lower with all VMAT

techniques compared to DCA (5.6 to 6.3 cc vs 9.4 cc, p<0.001). Low-dose delivery (V5Gy)

was lower with VMATnc_{Eclipse®} or VMATnc_{Elements®} than with DCA (81 or 94 cc vs 110 cc,

p=0.02).

Conclusions: NovalisTx® VMAT HFSRT for ≥ 25 mm diameter brain metastases provides

the best dosimetric compromise in terms of target coverage, sparing of healthy brain tissue

and low-dose delivery compared to DCA.

Keywords: brain metastasis, stereotactic radiotherapy, dosimetry, VMAT, NovalisTx®

SUMMARY IN FRENCH

Objectif de l'étude : La radiothérapie stéréotaxique joue un rôle majeur dans le traitement des métastases cérébrales. L'objectif était de comparer les résultats dosimétriques de quatre planifications de radiothérapie stéréotaxique hypofractionnée pour des métastases cérébrales volumineuses.

Matériel et Méthodes : Ont été inclus dix patients traités sur NovalisTx® par irradiation stéréotaxique hypofractionnée en arcthérapie dynamique conformationnelle non coplanaire (ADC) pour une métastase cérébrale ≥ 25 mm. Trois autres plans avec modulation d'intensité volumétrique (RCMI) ont été comparés: avec des arcs coplanaires (Eclipse®, Varian, RCMIcEclipse®), des non coplanaires (Elements Cranial SRS®, Brainlab, arcs RCMInc_{Elements®}), et des arcs coplanaires et non coplanaires (RCMInc_{Eclipse®}). La dose d'enveloppe était 23,1 Gy (isodose 70%) en trois fractions. Le volume moyen du volume tumoral macroscopique (GTV) était 27 mm³.

Résultats : Les indices de conformité étaient meilleurs pour les RCMI (1,05 contre 1,28, p < 0,05). Les indices de gradient étaient meilleurs avec la RCMInc_{Elements®} par rapport à l'ADC (2,43 contre 3,02, p < 0,001). Moins de fortes doses délivrées dans le parenchyme cérébral sain ont été observées avec les RCMI (5,6 à 6,3 cc contre 9,4 cc, p < 0,001). Moins de faibles doses délivrées (V5Gy, volume recevant 5 Gy) ont été observées avec les RCMI non coplanaires par rapport à l'ADC (81 ou 94 cc contre 110 cc, p = 0,02).

Conclusion: Les meilleurs résultats dosimétriques de sradiothérapie téréotaxique hypofractionnée en termes de couverture du volume cible et d'épargne du parenchyme cérébral sain à faibles et fortes doses sont obtenus avec les RCMI utilisant des arcs non coplanaires.

Keywords: métastases cérébrales, radiothérapie stéréotaxique, dosimétrie, RCMI,

NovalisTx®

Background

Brain metastases are the most common intracranial tumors in adults. Twenty to 40% of cancer

patients will develop brain metastases [1–3]. There are different therapeutic possibilities and

stereotactic radiotherapy occupies an increasingly important place [4–6]. Local control is

similar to that following surgery [7]. Stereotactic radiotherapy aims to deliver a high dose on

the target, and it is found that the higher the dose delivered, the lower the risk of recurrence

[8]. Conversely, the lower the dose, the lesser the risk of radionecrosis, especially for large

brain metastases [9]. In order to limit the appearance of radionecrosis, irradiation of healthy

brain parenchyma should be reduced as far as possible. To enable this while maintaining

treatment efficiency, hypo-fractionated stereotactic radiotherapy (HFSRT; currently 3 to 5

fractions) is often a solution for large-diameter metastases [10-12]. For LINAC-based

HFSRT, non-coplanar multiple dynamic conformal arcs (DCA) have often been used to

achieve high conformity while sparing healthy tissues [13]. More recently, volumetric

modulated arc therapy (VMAT) has been widely developed [14–16].

The purpose of our study was to compare the dosimetric impact of four different HFSRT

techniques for the treatment of large brain metastases (over 25mm in diameter): DCA

(Iplan®, Brainlab), VMAT with coplanar arcs (Eclipse®, Varian; VMATc_{Eclipse®}), VMAT

with coplanar and non-coplanar arcs (Eclipse®, Varian; VMATnc_{Eclipse®}), and VMAT with

non-coplanar arcs (Elements®, Brainlab; VMATnc_{Elements®}). The dosimetric impact was

studied in terms of target coverage and the sparing of organs at risk (OAR), especially low

and high doses delivered to healthy brain tissues.

Methods

Patients

Ten consecutive patients, treated in our institution with upfront HFSRT between November 2014 and March 2016 for a single brain metastasis with a greatest diameter -of 25 mm or more, were included in this study. Patient and brain metastasis characteristics are detailed in Table 1. The mean brain metastasis largest diameter was 26.6 mm (25-30 mm).

All patients were treated with NovalisTx® equipped with a high definition MultiLeaf Collimator (HD MLC 120) (Varian Medical Systems, Palo Alto, CA, USA and Brainlab, Munich, Germany) using a noninvasive thermoplastic mask plus a localizer box (Brainlab). Positioning of the patients was performed using an ExacTrac® stereoscopic X-ray system (Brainlab) and a robotic couch with six degrees of freedom. Treatments were permitted when the setup error was < 0.7 mm in translation and 0.7° in rotation.

Treatment planning

A planning CT of 1.25-mm thickness was acquired and was matched with the dosimetric MRI sequences of interest using Iplan®, version 4.1 (Brainlab). Three MRI sequences were used: a FLAIR 3D MRI sequence with a 1mm*1mm*1mm voxel size, a T1 3D MPRAGE MRI sequence with contrast agent and a voxel size of 0.8mm*0.8mm*1mm and T1 EG with a 0.6mm*0.6mm*4mm voxel size. The gross tumor volume (GTV) was defined using post Gadolinium contrast-enhanced T1 weighted MRI sequences. The GTV was then extended symmetrically by 2 mm in all dimensions to create the planning target volume (PTV). Mean GTV and PTV were 8.7 cc (5.7-13.6 cc) and 14.5 cc (10.5-21.4 cc) respectively.

The following OARs were contoured: brainstem, eyeballs, lenses, optic nerves, chiasm, cochlea, cranial cavity, and healthy brain (entire cranial cavity – GTV). No margins were around the OARs to create planning OAR volumes (PRVs).

Treatment plans

Non-coplanar dynamic conformal arcs (Iplan®, Brainlab; DCA)

All DCA plans were created with arcs of 6-MV photons. The prescribed dose was 33 Gy at the isocenter and 23.1 Gy (70%) at the PTV envelope in three fractions. Five non-coplanar arcs were used for all patients (Figure 1). The final calculations were performed using Iplan® TPS, version 4.1 (Brainlab), using a pencil-beam algorithm with a spatial resolution of 2.5 mm. This formed a conformational treatment where the leaf positions were adjusted every 10° using Beam Eye View. The collimator was set at zero for all plans.

VMAT (Eclipse®, Varian)

All VMAT plans were created with arcs for 6-MV photons. The prescribed dose was 33 Gy for the GTV and 23.1 Gy (70%) for the PTV. Final calculations were performed using the AAA algorithm on Eclipse® TPS version 13.5 (Varian Medical Systems) [24]. The arc optimization algorithm, the Progressive Resolution Optimizer used in Rapidarc®, optimized leaf position, dose rate, and gantry speed. Optimization parameters with *Normal Tissue Objectives* (NTO) were used to spare healthy tissues and were defined as following: 1) distance from the PTV border (Xstart) = 1 mm, 2) start dose (f0) = target coverage isodose (e.g. 70%), 3) end dose (f ∞) = 5% and 4) the fall-off coefficient (k) = 0.3 mm⁻¹. The maximum dose rate was set at 600 MU/min. Couch parameters were also added to the plan to account for attenuation of the mega-voltage beams. VMAT plans followed the

recommendations of the International Commission on Radiation Units and Measurement Report 83.

Coplanar VMAT (VMATc_{Eclipse})

The plans were created with two full coplanar arcs (Figure 1). The first arc was planned in a clockwise direction and the second in a counter-clockwise direction. For all the plans, the collimator was rotated to 30° for the first arc and to 330° for the second arc to reduce the tongue-and-groove effect.

Coplanar and Non-coplanar VMAT (VMATnc_{Eclipse})

The plans were created with one full coplanar arc and 3 partial non-coplanar arcs spaced by 45° (Figure 1). The maximum arc rotation amplitude was 160°. The rotation of the collimator was 10°, 350°, 350°, 350° and 10° for the first, second, third and fourth arcs respectively.

➤ VMAT (Elements Cranial SRS®, Brainlab; VMATnc_{Elements})

The prescribed dose was 33 Gy at the isocenter and 23.1 Gy (70%) at the PTV envelope in three fractions. Plans were generated using the 4Pi optimization algorithm on Elements Cranial SRS® (Brainlab). Optimal placement of non-coplanar arcs (Figure 1), gantry starting and stopping, optimized leaf position, dose rate, and gantry speed were automatically generated. The maximum dose rate was set at 600 MU/min. Couch parameters were also added to the plan to account for attenuation of the mega-voltage beams.

Statistical analysis

The plan analyses were based on dose-volume histogram (DVH) data. For target volume coverage, V70% (23.1Gy), mean dose (Dmean) to the GTV and PTV were noted. For healthy brain high and low-dose delivery, V23.1Gy, V20Gy, V18Gy were used and low doses with

V10Gy and V5Gy. We also calculated two indexes for the PTV: the inverse Paddick conformity index (CI) and the gradient index (GI).

The inverse Paddick CI is defined as follows:

$$CI = \frac{(\textit{Total volume receiving} \ge \textit{Dcoverage})}{(\textit{PTV volume receiving} \ge \textit{Dcoverage})} * \frac{(\textit{PTV volume})}{(\textit{PTV volume receiving} \ge \textit{Dcoverage})}$$

A value of 1 is the ideal case. The larger the value, the less conformal is the treatment.

The GI is defined as follows:

$$GI = \frac{(Total\ volume\ receiving \ge 50\%\ Dcoverage)}{(Total\ volume\ receiving \ge 100\%\ Dcoverage)}$$

The GI describes the steepness of the dose fall-off from the 23.1 Gy isodose (Dcoverage in our case) to the 11.55 isodose (50% of Dcoverage). The larger the value, the shallower is the gradient.

Statistical analyses were performed using R v2.15.1 (http://www.cran.r-project.org). To explore changes across the four sets of data obtained (DCA, VMATc_{Eclipse}, VMATnc_{Eclipse} and VMATnc_{Elements}), Kruskal-Wallis tests were performed, followed by Dunn tests for pairwise comparisons. If the associated p-value was under the significance level (α =0.05), it was assumed that there was a statistically significant difference between the data sets compared.

Results

All dosimetric results are presented in Table 2.

> Target volume coverage

For all four plans, the mean PTV coverage with the 23.1Gy (V70%) isodose was over 99%. Mean CIs were significantly lower with all VMAT techniques vs DCA (1.28, 1.04, 1.05 and 1.07 for DCA, VMATc_{Eclipse}, VMATnc_{Eclipse} VMATnc_{Elements} respectively; p<0.05). Mean GIs were significantly lower with VMATnc_{Elements} and DCA vs VMATc_{Eclipse} and VMATnc_{Eclipse} (p<0.001). There were no significant differences between Dmeans to the GTV or PTV between the different techniques.

➤ Heathly brain

Table 2 shows all HDV results for the healthy brain (entire cranial cavity – GTV). Mean V23.1Gy were significantly lower for all VMAT techniques vs DCA (9.35cc, 5.9 cc, 5.6 cc and 6.3cc for DCA, VMATc_{Eclipse}, VMATnc_{Eclipse}, VMATnc_{Elements} respectively; p<0.001). Mean V18Gy were significantly lower for all VMAT techniques vs DCA (15.5cc, 12.2 cc, 10.9 cc and 11.3cc for DCA, VMATc_{Eclipse}, VMATnc_{Eclipse}, VMATnc_{Eclipse}, VMATnc_{Elements} respectively; p=0.04).

➤ Low-dose delivery

For DCA, VMATc_{Eclipse}, VMATnc_{Eclipse} and VMATnc_{Elements}, mean V5Gy were 109.7 cc, 146.4 cc, 82 cc and 94 cc respectively (p<0.05 VMATnc vs VMATc_{Eclipse} and DCA); mean V10Gy were 40.1 cc, 45.3 cc, 30.0 cc and 32.6 cc respectively (ns).

Discussion

The aim of our study was to optimize the dosimetric parameters of HFSRT for treatment of large brain metastases (>25 mm diameter), especially concerning predictive factors of radionecrosis. Several authors have demonstrated the link between the volume of brain receiving a specific isodose and the risk of radionecrosis [17], particularly with the volume of high-dose irradiated healthy brain [18–20]. In the context of single fraction radiosurgery, Minniti et al. found that V12Gy > 10.9 cc corresponded to a 47% risk of developing radionecrosis [21]. Other authors found similar outcomes with V12Gy [18]. As far as HFSRT is concerned, little data is available. Minniti et al. found that for brain metastasis treated with three-fraction HFSRT, the 1-year risk of radionecrosis was up to 24% for V18Gy >30.2 cc, and up to 14 % for V21Gy >20.9 cc [22,23]. Inoue et al. found that for brain metastasis treated with three-fraction HFSRT, a V23Gy over 7cc was a significant predictive factor of radionecrosis [24]. Interestingly, in our study, the mean V23.1Gy was 9.4 cc for DCA and was reduced to 5.6-6.3 cc (i.e. about 36% reduction) with VMAT techniques, and mean V18Gy was reduced from 15.5 cc to 10.9-12.2 cc (i.e. about 25% reduction). According to literature, these reductions may be clinically important. The benefits of VMAT on dose distribution have already been demonstrated in several intracranial stereotactic studies for the treatment of vestibular schwanomas [25] or meningiomas of the skull base [26].

In this study, we paid particular attention to dosimetric parameters relating to predictive factors of radionecrosis described in the literature. Radionecrosis incidence ranges from 2 to 22% for radiological radionecrosis and 1 to 14% for symptomatic radionecrosis (15–17). Radionecrosis appears within 3 years in 80% of cases [29] traditionally 6-12 months after stereotactic radiotherapy. Differentiation between progressive recovery and radionecrosis is difficult. The definition of radionecrosis is histological and corresponds to the appearance of cerebral vascular lesions secondary to irradiation resulting in ischemic injury, possible

hemorrhage and in severe cases white matter demyelination. [30]. Appart from high-dose healthy brain irradiation discussed above, other predictive factors for radionecrosis have been identified: CI [31], total dose [32,33], fractionation [33], number of isocenters [34], previous radiotherapy [35], infratentorial location of the BM [36] and concomitant chemotherapy [33]. Concerning CI, we found that all VMAT plans gave excellent results between 1.04 and 1.07, vs 1.27 for DCA (p<0.001).

Concerning the different VMAT techniques that we studied, although they all yielded acceptable dosimetric results, some differences can be noted. We found that VMAT including non-coplanar arcs provided the best dosimetric compromise in terms of target coverage, sparing of healthy brain tissue and low-dose delivery. Even if treatment time is longer, in our institution we favor the use of multiple non-coplanar arcs because they enable the reduction of low-dose delivery over coplanar arcs only. This could be of elinical interest, especially in case of regional brain recurrence requiring new stereotactic irradiation, which is often the case with upfront HFSRT. Indeed, in case of repeated treatments, this may lower the cumulative dose to the healthy brain, even if, up-to-date it has not been proven that it might have a clinical impact. In our study, VMATnc_{Eclipse} and VMATnc_{Elements} provided similar dosimetric results except for GI which was significantly better for VMATnc_{Elements}. For this reason, we now favor the use of VMATnc_{Elements}, especially since, in daily routine practice, the computing time to generate the dosimetry is almost instantaneous for VMATnc_{Elements} and can take several dozen minutes for VMATnc_{Eclipse} (using the AAA algorithm on Eclipse® TPS version 13.5).

Conclusions

The use of VMAT with non-coplanar arcs for HFSRT in the treatment of large brain metastases provides excellent dosimetric results in terms of target coverage, sparing of

healthy brain and low-dose delivery. We found that V23.1Gy and V18Gy were reduced by

36% and 25% respectively, which may be clinically important concerning the risk of

radionecrosis. We found that Eclipse® and Elements Cranial SRS® provided similar

dosimetric results, with a better GI for Elements Cranial SRS®.

List of abbreviations

CI: Conformity Index

DCA: Dynamic Conformal Arcs

Dmean: Mean Dose

DVH: Dose-Volume Histogram

GI: Gradient Index

GTV: Gross Tumor Volume

HFSRT: Hypo-Fractionated Stereotactic Radiotherapy

NTO: Normal Tissue Objectives

OAR: Organ At Risk

PRV: Planning OAR Volume

PTV: Planning Target Volume

VMAT: Volumetric Modulated Arc Therapy

VMATc_{Eclipse}: VMAT with coplanar arcs (Eclipse®, Varian)

VMATnc_{Eclipse}: VMAT with coplanar and non-coplanar arcs (Eclipse®, Varian)

VMATnc_{Elements}: VMAT with non-coplanar arcs (Elements Cranial SRS®, Brainlab)

Declarations

Ethics approval and consent to participate

This work did not require any written patient consent. The local ethics committee of Centre Jean Perrin approved this work.

Consent for publication

Not applicable

Availability of data and material

The datasets supporting the conclusions of this article are included in the article.

Competing interests

JB had speaker honoraria from Brainlab. The remaining authors declare that they have no competing interests.

Funding

Not applicable

Authors' contributions

LB designed the study, collected the data and wrote the manuscript. VC and VD participated in the study design and interpretation and performed treatment plan analyses. EC performed the statistical analyses and participated in interpretation. JM, PV, TK and ML participated in the study design and interpretation. JB designed the study, participated in interpretation of the data and wrote the manuscript. GD was also in charge of data analysis, manuscript writing and editing. All authors read and approved the final manuscript.

Acknowledgements

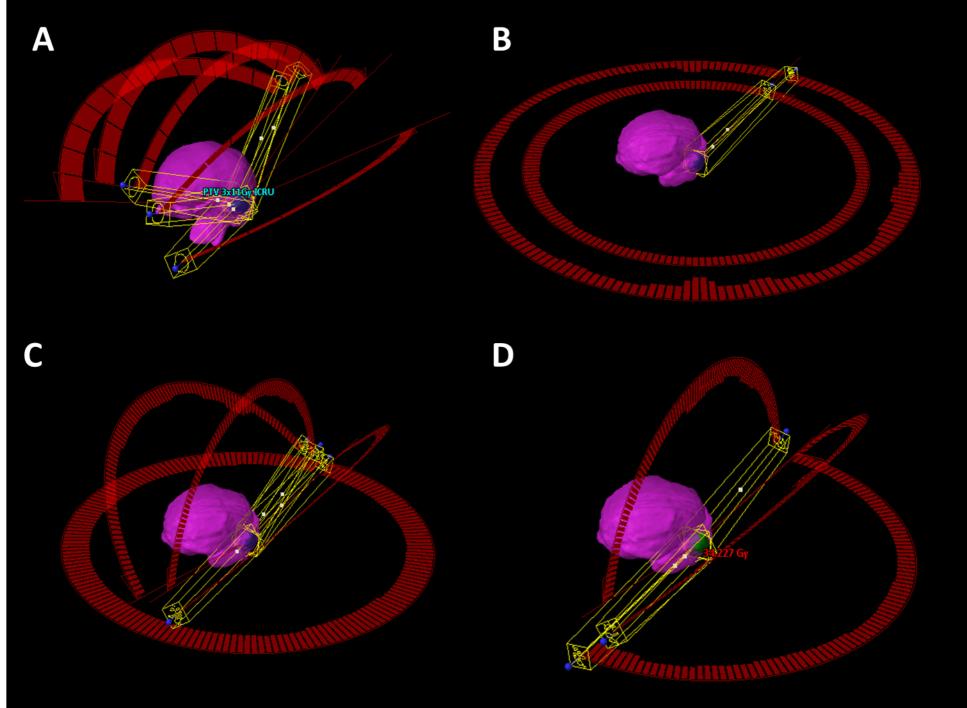
Not applicable

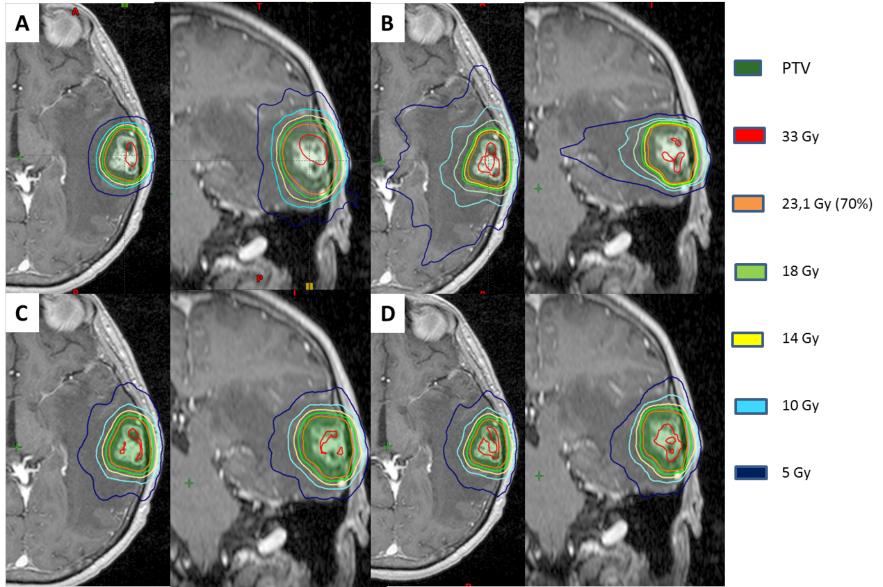
References

- [1] Johnson JD, Young B. Demographics of brain metastasis. Neurosurg Clin N Am 1996;7:337–44.
- [2] Lin X, DeAngelis LM. Treatment of Brain Metastases. J Clin Oncol Off J Am Soc Clin Oncol 2015;33:3475–84. https://doi.org/10.1200/JCO.2015.60.9503.
- [3] Linskey ME, Andrews DW, Asher AL, Burri SH, Kondziolka D, Robinson PD, et al. The role of stereotactic radiosurgery in the management of patients with newly diagnosed brain metastases: a systematic review and evidence-based clinical practice guideline. J Neurooncol 2010;96:45–68. https://doi.org/10.1007/s11060-009-0073-4.
- [4] Patchell RA. The management of brain metastases. Cancer Treat Rev 2003;29:533–40.
- [5] Antoni D, Noël G. [Radiotherapy of brain metastases according to the GPA score (Graded Prognostic Assessment)]. Cancer Radiother J Soc Française Radiother Oncol 2013;17:424–7. https://doi.org/10.1016/j.canrad.2013.06.030.
- [6] Kocher M, Soffietti R, Abacioglu U, Villà S, Fauchon F, Baumert BG, et al. Adjuvant whole-brain radiotherapy versus observation after radiosurgery or surgical resection of one to three cerebral metastases: results of the EORTC 22952-26001 study. J Clin Oncol Off J Am Soc Clin Oncol 2011;29:134–41. https://doi.org/10.1200/JCO.2010.30.1655.
- [7] Chen JC, Petrovich Z, O'Day S, Morton D, Essner R, Giannotta SL, et al. Stereotactic radiosurgery in the treatment of metastatic disease to the brain. Neurosurgery 2000;47:268-279-281.
- [8] Vogelbaum MA, Angelov L, Lee S-Y, Li L, Barnett GH, Suh JH. Local control of brain metastases by stereotactic radiosurgery in relation to dose to the tumor margin. J Neurosurg 2006;104:907–12. https://doi.org/10.3171/jns.2006.104.6.907.
- [9] Minniti G, Clarke E, Lanzetta G, Osti MF, Trasimeni G, Bozzao A, et al. Stereotactic radiosurgery for brain metastases: analysis of outcome and risk of brain radionecrosis. Radiat Oncol Lond Engl 2011;6:48. https://doi.org/10.1186/1748-717X-6-48.
- [10] Manning MA, Cardinale RM, Benedict SH, Kavanagh BD, Zwicker RD, Amir C, et al. Hypofractionated stereotactic radiotherapy as an alternative to radiosurgery for the treatment of patients with brain metastases. Int J Radiat Oncol Biol Phys 2000;47:603– 8.
- [11] Narayana A, Chang J, Yenice K, Chan K, Lymberis S, Brennan C, et al. Hypofractionated stereotactic radiotherapy using intensity-modulated radiotherapy in patients with one or two brain metastases. Stereotact Funct Neurosurg 2007;85:82–7. https://doi.org/10.1159/000097923.
- [12] Kwon AK, Dibiase SJ, Wang B, Hughes SL, Milcarek B, Zhu Y. Hypofractionated stereotactic radiotherapy for the treatment of brain metastases. Cancer 2009;115:890–8. https://doi.org/10.1002/cncr.24082.
- [13] Wurm RE, Erbel S, Schwenkert I, Gum F, Agaoglu D, Schild R, et al. Novalis frameless image-guided noninvasive radiosurgery: initial experience. Neurosurgery 2008;62:A11-17-18. https://doi.org/10.1227/01.neu.0000325932.34154.82.
- [14] Ma Y, Li M, Yin Y, Kong L, Sun X, Lin X, et al. Hypofractionated stereotactic radiotherapy for brain metastases: a dosimetric and treatment efficiency comparison between volumetric modulated arc therapy and intensity modulated radiotherapy. Technol Cancer Res Treat 2010;9:499–507. https://doi.org/10.1177/153303461000900508.

- [15] Mayo CS, Ding L, Addesa A, Kadish S, Fitzgerald TJ, Moser R. Initial experience with volumetric IMRT (RapidArc) for intracranial stereotactic radiosurgery. Int J Radiat Oncol Biol Phys 2010;78:1457–66. https://doi.org/10.1016/j.ijrobp.2009.10.005.
- [16] Andrevska A, Knight KA, Sale CA. The feasibility and benefits of using volumetric arc therapy in patients with brain metastases: a systematic review. J Med Radiat Sci 2014;61:267–76. https://doi.org/10.1002/jmrs.69.
- [17] Le Rhun E, Dhermain F, Vogin G, Reyns N, Metellus P. Radionecrosis after stereotactic radiotherapy for brain metastases. Expert Rev Neurother 2016;16:903–14. https://doi.org/10.1080/14737175.2016.1184572.
- [18] Blonigen BJ, Steinmetz RD, Levin L, Lamba MA, Warnick RE, Breneman JC. Irradiated volume as a predictor of brain radionecrosis after linear accelerator stereotactic radiosurgery. Int J Radiat Oncol Biol Phys 2010;77:996–1001. https://doi.org/10.1016/j.ijrobp.2009.06.006.
- [19] Voges J, Treuer H, Sturm V, Büchner C, Lehrke R, Kocher M, et al. Risk analysis of linear accelerator radiosurgery. Int J Radiat Oncol Biol Phys 1996;36:1055–63.
- [20] Doré M, Martin S, Delpon G, Clément K, Campion L, Thillays F. Stereotactic radiotherapy following surgery for brain metastasis: Predictive factors for local control and radionecrosis. Cancer Radiother J Soc Francaise Radiother Oncol 2017;21:4–9. https://doi.org/10.1016/j.canrad.2016.06.010.
- [21] Minniti G, Clarke E, Lanzetta G, Osti MF, Trasimeni G, Bozzao A, et al. Stereotactic radiosurgery for brain metastases: analysis of outcome and risk of brain radionecrosis. Radiat Oncol Lond Engl 2011;6:48. https://doi.org/10.1186/1748-717X-6-48.
- [22] Minniti G, Scaringi C, Paolini S, Lanzetta G, Romano A, Cicone F, et al. Single-Fraction Versus Multifraction (3 × 9 Gy) Stereotactic Radiosurgery for Large (>2 cm) Brain Metastases: A Comparative Analysis of Local Control and Risk of Radiation-Induced Brain Necrosis. Int J Radiat Oncol Biol Phys 2016;95:1142–8. https://doi.org/10.1016/j.ijrobp.2016.03.013.
- [23] Minniti G, D'Angelillo RM, Scaringi C, Trodella LE, Clarke E, Matteucci P, et al. Fractionated stereotactic radiosurgery for patients with brain metastases. J Neurooncol 2014;117:295–301. https://doi.org/10.1007/s11060-014-1388-3.
- [24] Inoue HK, Seto K, Nozaki A, Torikai K, Suzuki Y, Saitoh J, et al. Three-fraction CyberKnife radiotherapy for brain metastases in critical areas: referring to the risk evaluating radiation necrosis and the surrounding brain volumes circumscribed with a single dose equivalence of 14 Gy (V14). J Radiat Res (Tokyo) 2013;54:727–35. https://doi.org/10.1093/jrr/rrt006.
- [25] Lagerwaard FJ, Meijer OWM, van der Hoorn EAP, Verbakel WFAR, Slotman BJ, Senan S. Volumetric modulated arc radiotherapy for vestibular schwannomas. Int J Radiat Oncol Biol Phys 2009;74:610–5. https://doi.org/10.1016/j.ijrobp.2008.12.076.
- [26] Baumert BG, Norton IA, Davis JB. Intensity-modulated stereotactic radiotherapy vs. stereotactic conformal radiotherapy for the treatment of meningioma located predominantly in the skull base. Int J Radiat Oncol Biol Phys 2003;57:580–92.
- [27] Telera S, Fabi A, Pace A, Vidiri A, Anelli V, Carapella CM, et al. Radionecrosis induced by stereotactic radiosurgery of brain metastases: results of surgery and outcome of disease. J Neurooncol 2013;113:313–25. https://doi.org/10.1007/s11060-013-1120-8.
- [28] Stockham AL, Ahluwalia M, Reddy CA, Suh JH, Kumar A, Vogelbaum MA, et al. Results of a questionnaire regarding practice patterns for the diagnosis and treatment of

- intracranial radiation necrosis after SRS. J Neurooncol 2013;115:469–75. https://doi.org/10.1007/s11060-013-1248-6.
- [29] Walker AJ, Ruzevick J, Malayeri AA, Rigamonti D, Lim M, Redmond KJ, et al. Postradiation imaging changes in the CNS: how can we differentiate between treatment effect and disease progression? Future Oncol Lond Engl 2014;10:1277–97. https://doi.org/10.2217/fon.13.271.
- [30] Na A, Haghigi N, Drummond KJ. Cerebral radiation necrosis. Asia Pac J Clin Oncol 2014;10:11–21. https://doi.org/10.1111/ajco.12124.
- [31] Valéry CA, Cornu P, Noël G, Duyme M, Boisserie G, Sakka LJ, et al. Predictive Factors of Radiation Necrosis after Radiosurgery for Cerebral Metastases. Stereotact Funct Neurosurg 2003;81:115–9. https://doi.org/10.1159/000075114.
- [32] Shaw E, Scott C, Souhami L, Dinapoli R, Kline R, Loeffler J, et al. Single dose radiosurgical treatment of recurrent previously irradiated primary brain tumors and brain metastases: final report of RTOG protocol 90-05. Int J Radiat Oncol Biol Phys 2000;47:291–8.
- [33] Ruben JD, Dally M, Bailey M, Smith R, McLean CA, Fedele P. Cerebral radiation necrosis: incidence, outcomes, and risk factors with emphasis on radiation parameters and chemotherapy. Int J Radiat Oncol Biol Phys 2006;65:499–508. https://doi.org/10.1016/j.ijrobp.2005.12.002.
- [34] Flickinger JC, Lunsford LD, Kondziolka D, Maitz AH, Epstein AH, Simons SR, et al. Radiosurgery and brain tolerance: An analysis of neurodiagnostic imaging changes after gamma knife radiosurgery for arteriovenous malformations. Int J Radiat Oncol 1992;23:19–26. https://doi.org/10.1016/0360-3016(92)90539-T.
- [35] Korytko T, Radivoyevitch T, Colussi V, Wessels BW, Pillai K, Maciunas RJ, et al. 12 Gy gamma knife radiosurgical volume is a predictor for radiation necrosis in non-AVM intracranial tumors. Int J Radiat Oncol Biol Phys 2006;64:419–24. https://doi.org/10.1016/j.ijrobp.2005.07.980.
- [36] Keller A, Doré M, Cebula H, Thillays F, Proust F, Darié I, et al. Hypofractionated Stereotactic Radiation Therapy to the Resection Bed for Intracranial Metastases. Int J Radiat Oncol Biol Phys 2017;99:1179–89. https://doi.org/10.1016/j.ijrobp.2017.08.014.





Patient	Age	Site of the primitive	GTV largest	GTV volume	PTV volume	Brain metastasis
		tumour	diameter	(cc)	(cc)	localization
			(mm)			
1	71	Lung	26	11.6	19.0	Cerebellum
2	56	Anal canal	26	7.3	12.4	Parietal
3	81	Kidney	28	6.8	12.2	Temporal
4	74	Melanoma	25	5.7	10.5	Parietal
5	65	Kidney	26	6.3	11.1	Temporal
6	68	Lung	25	7.3	12.5	Cerebellum
7	65	Lung	25	11.3	17.8	Frontal
8	81	Rectal	25	13.6	21.4	Cerebellum
9	77	Lung	30	7.9	13.3	Frontal
10	32	Breast	30	8.9	14.5	Insula

Table 1 : Patient characteristics

Table 2 : Results of the dosimetric parameters for the 10 patients according to the four treatment plans

	DCA	VMATCEclipse	VMATnc _{Eclipse}	VMATnc _{Elements}	Kruskal- Wallis Test p-value	Dunn Test p-value	
Target Volume							
V70%	99.64 ± 0.12 (98.70 - 100.00)	99.26 ± 0.16 (98.90 - 100.00)	99.16 ± 0.13 (98.80 - 100.00)	99.00 ± 0.00 (99.00 - 99.00)	ns		
CI	1.28 ± 0.01 (1.23 - 1.31)	1.04 ± 0.01 (1 - 1.10)	1.05 ± 0.01 (1.01 - 1.10)	1.07 ± 0.01 (1.03 - 1.10)	< 0.001	DCA vs all VMAT Between all VMAT	< 0.01
Gl	2.41 ± 0.05 (2.10 - 2.60)	3.02 ± 0.13 (2.50 - 3.50)	3.02 ± 0.13 (2.50 - 3.50)	2.45 ± 0.04 (2.20 - 2.70)	< 0.001	DCA vs VMATnc _{Eclipse} VMATnc _{Eclipase} vs VMATnc _{Elements}	< 0.001 < 0.001
Healthy Brain						- 2.0	
V23.1Gy (cc)	9.35 ± 0.58 (7.10 - 12.30)	5.89 ± 0.56 (3.90 - 8.70)	5.58 ± 0.49 (3.60 - 8.30)	6.26 ± 0.36 (5.00 - 8.30)	< 0.001	DCA <i>vs</i> all VMAT Between all VMAT	< 0.01 ns
V20Gy (cc)	12.81 ± 0.84 (9.40 - 17.40)	9.68 ± 0.93 (6.30 - 14.40)	8.62 ± 0.77 (5.60 - 13.10)	9.06 ± 0.58 6.90 - 12.30)	< 0.01	DCA vs all VMAT Between all VMAT	< 0.05 ns
V18 (cc)	15.52 ± 1.06 (11.10 - 21.60)	12.23 ± 1.18 (8.10 - 19.70)	10.94 ± 1.01 (7.10 - 16.90)	11.30 ± 0.75 (8.50 - 15.50)	< 0.05	DCA vs all VMAT Between all VMAT	< 0.05
Low-dose delivery							
V10Gy (cc)	40.14 ± 3.30 (26.20 - 58.30)	45.31 ± 5.49 (25.80 - 74.70)	30.09 ± 3.09 (19.30 - 50.00)	32.56 ± 2.61 (23.00 - 48.50)	ns		
V5Gy (cc)	109.71 ± 10.35 (69 - 155.40)	146.36 ± 19.43 (91.80 - 273.30)	82.01 ± 8.98 (47.90 - 133.00)	94.02 ± 8.18 (58.00 - 135)	< 0.05	VMATnc _{Eclipse} VS VMATc _{Eclipse} VMATnc _{Elements} VS VMATc _{Eclipse}	<0.01 <0.05

Data are presented as the mean doses of all patients ± standard deviation (min – max). Vx% (Gy) = minimum x% (Gy) of prescribed dose received by the volume. CI = Conformity index (Inverse Paddick). GI = Gradient index. VMAT = volumetric modulated arc therapy. DCA = dynamic conformal arcs (Iplan®). VMATc_{Eclipse} = VMAT technique with coplanar arcs only (Eclipse®). VMATnc_{Eclipse} = VMAT technique with coplanar arcs (Elements Cranial SRS®). ns = non-significant. Techniques in bold means that the technique is superior for this organ in particular.