

A 2D FEM for shear wave modeling applied to soft tissues

M Bilasse, S Chatelin, Guillaume Altmeyer, J Vappou, I Charpentier

► To cite this version:

M Bilasse, S Chatelin, Guillaume Altmeyer, J Vappou, I Charpentier. A 2D FEM for shear wave modeling applied to soft tissues. EMI International Conference, Oct 2016, Metz, France. hal-03040357

HAL Id: hal-03040357 https://hal.science/hal-03040357

Submitted on 4 Dec 2020

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers. L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

A 2D FEM for shear wave modeling applied to soft tissues

M. Bilasse^{*1,2}, S. Chatelin^{1,3}, G. Altmeyer^{1,2}, J. Vappou¹ and I. Charpentier¹

April 2016

Over the past two decades, dynamic elasticity imaging has emerged as a virtual palpation tool allowing for a qualitative investigation of the in vivo mechanical response of biological soft tissues.

From an experimental point of view, the three main steps [1] are (i) the generation of shear waves in the organ under sutdy, (ii) the measurement of the displacement field using medical imaging, then (iii) the identification of mechanical properties. Clearly, coupling wave physics and biomechanics in an appropriate mechanical model is key issue for such an identification.

Although most of shear wave inverse approaches for Magnetic Resonance Elastography (MRE) make the assumption of isotropic viscoelasticity, computer models should better describe the complexity of the computational domain to be of general use. In particular, boundary conditions, heterogeneity and anisotropy that strongly impact the wave propagation have to be accounted in a fair manner, whether set to estimated values in the modeling or identified during the course of the inverse problem solution.

MRE experiments have been developed since 5 years in the Icube laboratory [2]. Computational mechanics aspects are now considered in their full complexity to go further and to foresee, at a medium term, a clinical validation of the proposed methods. To that end, our modeling builds on a 2D FEM based on composite plate elements that moreover account for a vertical transverse displacement. Such a choice is motivated by a lower computational cost compared to a 3D modeling and the straightforward comparison with classical 2D MRI images. The nonlinear wave propagation is solved following [3].



Figure 1: Left: Reference hydrogel phantom. Right: Hydrogel phantom with stiff and soft inclusions

The modeling will be evaluated with respect to MRE experiments realized on hydrogel phantoms with stiff and soft inclusions.

References

- Vappou J (2012) Magnetic resonance and ultrasound imaging-based elasticity imaging methods: a review, Biomedical Engineering 40:121–134.
- [2] Corbin N, Vappou J, Breton E, Boehler Q, Barbé L, Renaud P and de Mathelin M (2016) Interventional MR elastography for MRI-guided percutaneous procedures, Magnetic Resonance in Medicine 75:1110-8.
- [3] Bilasse M, Charpentier I, Daya EM, Cherkaoui M (2009) A generic approach for the solution of nonlinear residual equations. Part II: Homotopy and complex nonlinear eigenvalue method, Computer Methods in Applied Mechanics and Engineering 198:3999–4004.

^{*}Corresponding Author bilasse@unistra.fr; ¹Icube, CNRS & University of Strasbourg; ²ECAM, Strasbourg; ³IHU Strasbourg.