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# Investigation of the electrical limit conditions effects in piezoelectric transducer arrays utilized in medical imaging

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## Abstract

Crosstalk is considered as an undesirable phenomenon disturbing the electromechanical behavior of the ultrasonic transducer arrays used in medical imaging applications. Indeed, when one element of a transducer array is excited, it generates parasitic voltages and/or displacement fields on the adjacent passive elements. Consequently, these interactions between elements decrease the array's electroacoustic performance, which affects the obtained image quality. To overcome the crosstalk's problem, several research works propose active cancellation techniques. In this case, the correction voltages are determined by considering the array's elements grounded, contrary to the conventional crosstalk's definition which considers the array elements in Open-Circuit. The novelty of this paper is in one hand the study of the electrical limit conditions' effects on the physical behavior of a piezoelectric transducer array radiating in a fluid medium (water). On the other hand, a displacement method is proposed to evaluate the crosstalk level when the array elements are grounded. The limitations of the proposed method are also discussed. For this purpose, a piezoelectric transducer array is firstly modeled using a Two-dimensional Finite Elements Method (FEM), when the array elements are not grounded (open-circuit). Then, the results are compared to those obtained when the neighboring elements are grounded (as in the case of the crosstalk's active cancellation techniques).

34 Finally, measurements are realized on a fabricated transducer array vibrating in air medium and are  
35 successfully compared to the results predicted using FEM.

36 **Keywords**—*Piezoelectric transducer arrays, displacement measurement, electrical limit conditions.*

37

## 38 **1. Introduction**

39 Ultrasonic transducers and transducer arrays are usually utilized in medical diagnostics  
40 and therapeutic applications [1-5]. The major objective of ongoing and future research in this  
41 area is to optimize the electroacoustic performance of these transducers, to obtain a high image  
42 resolution for more reliable and safe diagnostics. For this purpose, several works investigate  
43 the crosstalk phenomenon, which decreases the performance of the ultrasonic transducer arrays  
44 [6-14]. Indeed, when one element of a transducer array is driven, it generates parasitic voltages  
45 and/or displacement fields on the passive neighboring elements, which affects the performance  
46 of these devices. It is mainly responsible for anomalous behavior in the directivity of the  
47 ultrasonic transducer arrays, i.e. in presence of crosstalk, the main lobe is not obtained in the  
48 axial direction of the transducer array and several undesirable side lobes can be observed [15-  
49 16]. The crosstalk level in the ultrasonic transducer arrays is generally evaluated as the ratio  
50 between the parasitic voltages obtained on the passive neighboring elements and the  
51 excitation's amplitude applied to the active element [11, 14]. In this definition, one element of  
52 the studied transducer array is electrically driven, while its neighboring elements are  
53 considered electrically in Open-Circuit (not grounded).

54 In literature research works devoted to the minimization of crosstalk can be divided into  
55 three approaches. The first one investigates the contribution of the passive elements, i.e.  
56 filling material, matching layers, and backing, to the mechanical crosstalk [17-21]. The  
57 second approach consists of developing a systematic method for the active cancellation of  
58 crosstalk. The last method concerns specific treatments realized on the excitation and  
59 reception signals to reduce crosstalk [22-23]. The active cancellation of crosstalk is based on  
60 the application of adequate voltages to the elements adjacent to the excited one, to minimize  
61 the parasitic signals (crosstalk). The required voltages can be determined using different  
62 methods. Cugnet et al. [24] proposed a numerical technique to calculate them from the  
63 average normal displacement computed at the surface of the array elements. In the same  
64 manner, Bybi et al. [16] determined the correction voltages from punctual displacement  
65 measurements realized using a Laser Vibrometer. Zhou et al. [25-26] developed another

66 method using the transfer function matrix relating input voltages  $V_i$  to output pressures  $P_i$ . In  
67 this case, the measurement of the elements transfer function is realized using a hydrophone.  
68 Finally, Bybi et al. [7, 27] proposed another simple electrical method to cancel crosstalk in  
69 acoustical arrays, using the analogy between the motional current and normal displacement.  
70 In this situation, the determination of the correction voltages requires average measurements,  
71 i.e. impedance and current measurements, instead of punctual displacement measurements.

72 In all active crosstalk cancellation techniques, the determination of the correction  
73 voltages considers the neighboring elements electrically in Short-Circuit, i.e. the passive  
74 neighboring elements are connected to the ground, contrary to the conventional definition  
75 (neighboring elements are not grounded). The main objective of this paper is to study the  
76 effects of the electrical limit conditions (neighboring elements grounded or not grounded) on  
77 the electromechanical behavior of the piezoelectric transducer arrays utilized in medical  
78 imaging. An alternative solution to the conventional crosstalk's evaluation method, i.e. based  
79 on the ratio between the parasitic voltages measured on each passive element and the  
80 excitation voltage, is also proposed and tested when the array elements are grounded. It is  
81 expected that this study will be helpful in terms of crosstalk definition and accurate evaluation  
82 and suppression.

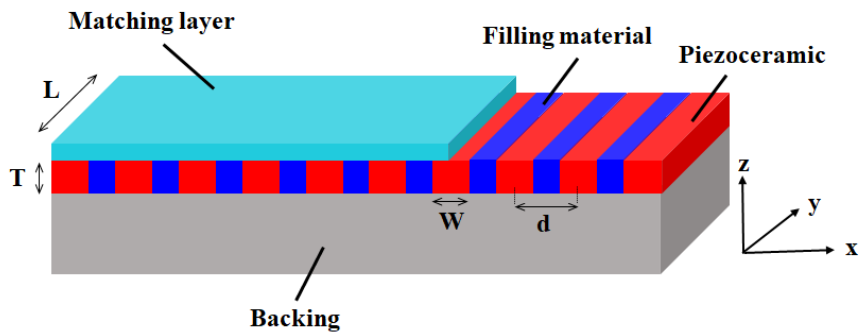
83 The first part of this paper is devoted to the description of a conventional piezoelectric  
84 transducer array and the presentation of the experimental setup utilized to evaluate the  
85 crosstalk level. In the second part, a transducer array composed of seven piezoelectric elements  
86 made of PZ 27 ceramic is modeled using a two-dimensional finite element method. In the last  
87 section, a prototype is fabricated and the experimental results, i.e. electrical impedance and  
88 displacement curves are compared to the numerical ones (FEM). Finally, the crosstalk level is  
89 evaluated experimentally considering both electrical limit conditions: neighboring elements  
90 ground and not grounded.

## 91 **2. Piezoelectric transducer arrays for medical imaging applications**

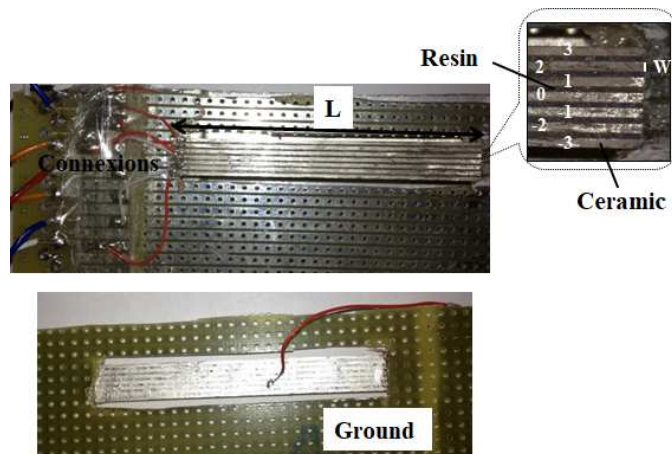
### 92 **2.1 Structure description**

93 Transducer arrays utilized in medical imaging and NDT applications are generally  
94 composed of an even number of piezoelectric elements having a thickness  $T$ , a width  $W$ , and a  
95 length  $L$ , spaced by a distance  $d$  and aligned as illustrated in Fig. 1. The elements are  
96 polarized in the thickness direction ( $z$ -direction) and are bonded to each other by a non-  
97 conductive resin. The transducer array elements' are also equipped with front and back

98 matching layers, to minimize the mismatching problem, which creates a prolonged ringing  
 99 after pulse excitation. Generally, the acoustic impedance of a conventional transducer is  
 100 matched to that of the propagation medium (tissues in medical applications) by one or two  
 101 matching layers on its front face and a thick backing layer on its back face. In our study, the  
 102 manufactured array is only composed of piezoelectric elements bonded to each other by a  
 103 non-conductive acrylic resin, PLEXCIL (ESCIL). The matching layers are not taken into  
 104 account to facilitate the fabrication of the prototype. This kind of transducer arrays is utilized  
 105 to understand the crosstalk phenomenon and to study the effects of the electrical limit  
 106 conditions on the array's electromechanical behavior. This also allowed as testing our  
 107 crosstalk correction methods easily [16, 27].



108  
 109 **Figure 1:** Schematic description of a conventional piezoelectric transducer array.



110  
 111 **Figure 2:** Seven-element transducer array.

112 To get a full symmetry of the transducer array and to simplify calculations and analysis,  
 113 an odd number of transducers is assumed. As shown in Fig. 2, the fabricated prototype is  
 114 composed of seven piezoelectric elements made of PZ27 Ferroperm ceramic, having the  
 115 following dimensions:  $T = 3.3$  mm,  $W = 0.7$  mm,  $L = 37$  mm and  $d = 1.2$  mm. The  
 116 piezoelectric material (PZ27) properties are listed in Table I.

$S_{11}^E$ pPa <sup>-1</sup>	$S_{12}^E$ pPa <sup>-1</sup>	$S_{13}^E$ pPa <sup>-1</sup>	$S_{33}^E$ pPa <sup>-1</sup>	$S_{44}^E$ pPa <sup>-1</sup>	$S_{66}^E$ pPa <sup>-1</sup>	$d_{15}$ pC/N	$d_{31}$ pC/N	$d_{33}$ pC/N	$\frac{\epsilon_{33}^S}{\epsilon_0}$	$\frac{\epsilon_{11}^S}{\epsilon_0}$	$\rho$ kg/m <sup>3</sup>
17	-6.71	-8.53	23	43.47	47.42	500	-170	425	1130	914	7700

117  
118

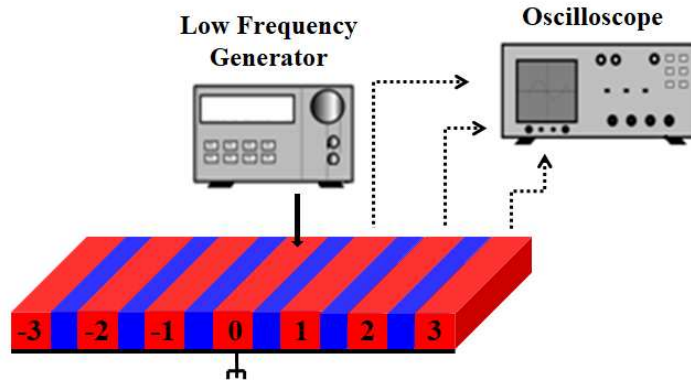
**Table I:** Physical properties of PZ27 ceramic.

119 **2.2 Crosstalk measurements**

120 Crosstalk measurements are performed on the studied transducer array using two  
121 methods as shown in Fig 3 and Fig. 4. In the first technique (Fig. 3), the central element "0" is  
122 excited using Agilent 33250A Low Frequency Generator delivering an electrical sine signal  $V_0$ .  
123 The neighboring elements "1", "-1", "2", "-2", "3" and "-3" are connected individually to a  
124 digital oscilloscope, displaying the parasitic voltage generated on each element ( $V_i$ ,  $i = 1, -1, 2,$   
125  $2, 3,$  and  $-3$ ). In the literature [11, 14] the crosstalk level  $C$  (dB) is evaluated from the  
126 measurements using the relation (1):

127 
$$C(\text{dB}) = 20 \text{Log}\left(\frac{V_i}{V_0}\right), \quad (1)$$

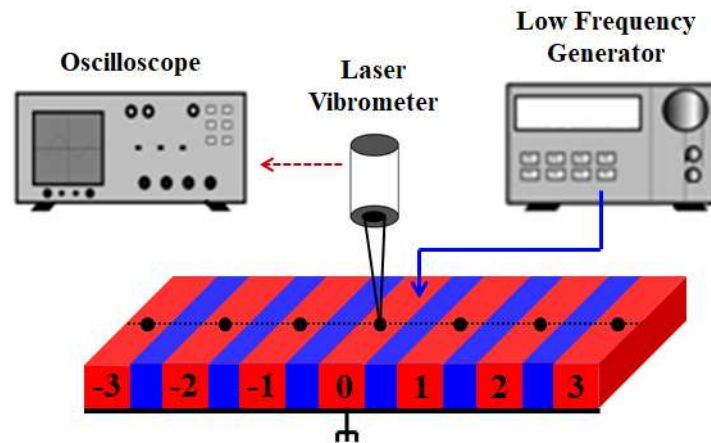
128 This definition considers one element of the studied transducer array as electrically driven,  
129 while its neighboring elements are electrically in Open-Circuit (not grounded). In this paper, a  
130 second method is proposed to evaluate the crosstalk level when the neighboring elements are  
131 connected to the ground, as in the case of the crosstalk's active cancellation methods [16, 24,  
132 25, 26, 27]. In this situation, voltage measurement cannot be utilized because the elements are  
133 not in Open-Circuit as suggested by the definition (Fig.3).



134  
135

**Figure 3:** Crosstalk's evaluation using voltage measurements.

136 Another solution is to utilize the displacement measurements instead of the voltage ones  
 137 as shown in Fig. 4. One of the objectives of this research work is to test the validity of this  
 138 method and to evaluate its limitations. For this purpose, displacement measurements are  
 139 carried out in the middle of the fabricated array elements using a Polytech psv400 laser  
 140 vibrometer (Fig. 4). The results obtained using both methods (Fig. 3 and 4) are compared  
 141 numerically and experimentally in the frequency domain.



142

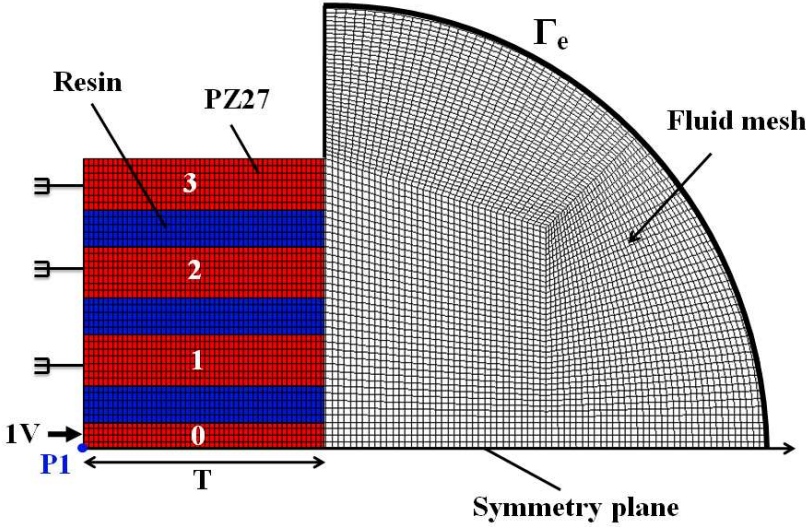
143

**Figure 4:** Crosstalk's evaluation using displacement measurements.

### 144 3. Numerical study

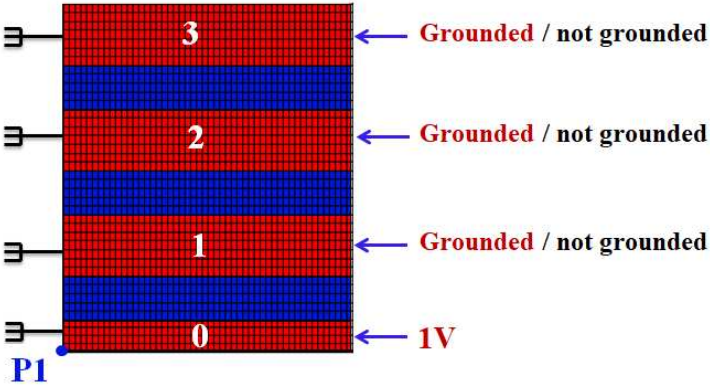
145 The piezoelectric transducer array is first modeled numerically using the ATILA code  
 146 (FEM code for elastic and piezoelectric structures radiating in fluid) [28] to determine its  
 147 Transmitting Voltage Response (TVR) and to predict the normal displacement at the radiating  
 148 surface of each array element. The numerical model is also utilized to compute the array's  
 149 electrical impedance and to evaluate the crosstalk level. As shown in Fig. 5(a), the studied  
 150 array is composed of seven piezoelectric elements made of PZ27 ceramic bounded to each  
 151 other by Acrylic PLEXCIL resin (filling material). Both the piezoelectric array elements and  
 152 the filling material (resin) are meshed using isoparametric quadratic elements respecting the  
 153  $\lambda/4$  criterion, i.e. the piezoelectric array elements are divided into seven elements along their  
 154 width  $W$  and fifty elements along their thickness  $T$ , whereas the resin elements are divided into  
 155 five elements along their width and fifty elements along their thickness. The spacing between  
 156 the array elements ( $d$ ) is chosen equal to 1.2 mm to respect the Nyquist criterion and to avoid  
 157 grating lobes. Each element of the studied array has a thickness  $T = 3.3$  mm, a width  $W = 0.7$   
 158 mm and its length is chosen to be 37 mm long, with a Length-to-Thickness Ratio ( $L/T$ ) of  
 159 about 11.21, thus this length can be considered as infinite and a plane strain approximation

160 assumed. In the literature, it is demonstrated that a dominant thickness mode is obtained when  
 161 the width-to-thickness ratio  $W / T$  is less than or equal to 0.5 [29-30]. This aspect ratio is  
 162 chosen about 0.21 to enable the separation of the thickness mode about the undesirable lateral  
 163 modes (width and length modes). Furthermore, in our previous work (ref. 8), it was also  
 164 demonstrated numerically and experimentally that the influence and the contribution of these  
 165 undesirable modes (width and length modes) is negligible. The transducer array radiates in a  
 166 fluid medium (water in medical imaging applications) meshed with isoparametric quadratic  
 167 elements respecting the  $\lambda/4$  criterion. This medium is limited by a non-reflecting surface  $\Gamma_e$   
 168 made up of dipolar elements that absorb the outgoing acoustic wave almost completely [15].  
 169 Furthermore, only half the domain is meshed due to symmetry.



170  
 171

(a) Structure's mesh.



172  
 173

(b) Electrical limit conditions.

174 **Figure 5:** Schematic description of a seven-element transducer array radiating in water.

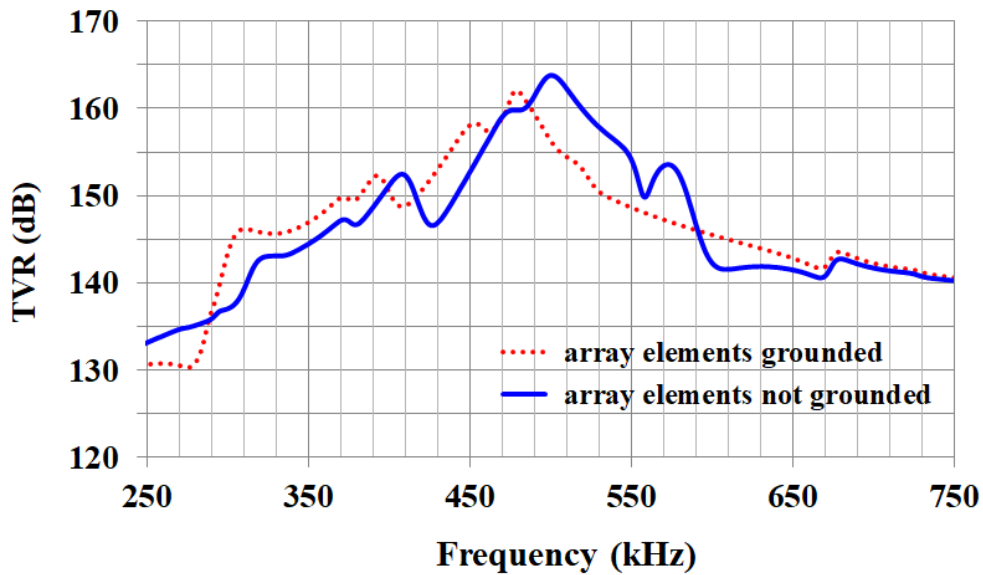


175 To study the effects of the electrical limit conditions on the array’s electromechanical  
176 behavior, two limit conditions are considered (Fig. 5(b)):

- 177 i) The array’s central element “0” is driven, while its neighboring elements “1”, “2” and “3”  
178 are grounded.
- 179 ii) The central element “0” is driven and its neighboring elements “1”, “2” and “3” are not  
180 grounded (open-circuit).

### 181 3.1 Transmitting Voltage Response (TVR)

182 Firstly, the Transmitting Voltage Response (TVR) of the seven-element transducer  
183 array is computed between 250 kHz and 750 kHz, for a relative reference pressure  $1 \mu\text{Pa} / \text{V}$   
184 at 1 m. Fig. 6 compares the TVR obtained considering the electrical limit conditions (i) and  
185 (ii). After analysis, it is observed that the two curves follow relatively the same variation, i.e.  
186 the same maximums and minimums. Nevertheless, a frequency shift about 20 kHz is obtained  
187 between the curves. Furthermore, a parasitic mode (maximum of TVR) is observed around the  
188 frequency of 570 kHz, in the curve corresponding to the limit condition (ii). Finally, the  
189 maximum of TVR obtained for the limit condition (i) is somewhat less than that computed for  
190 the condition (ii) (about 2 dB).

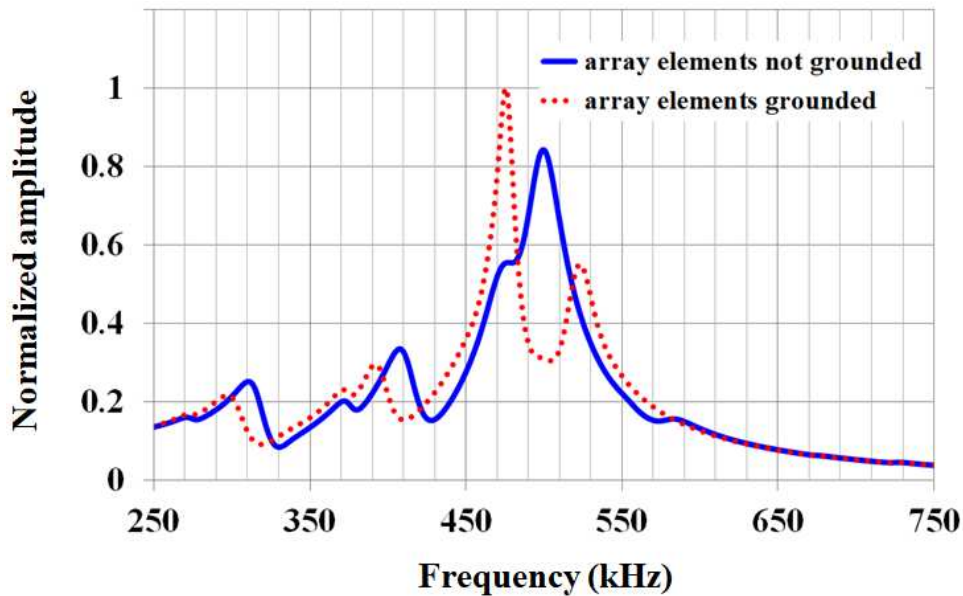


191  
192 **Figure 6:** Transmitting Voltage Response (TVR) of the seven-element transducer array.

### 193 3.2 Displacement

194 The normal displacement is also computed in the middle of the radiating surface of the  
195 central element “0”, i.e. at the position P1 (Fig. 5b) between 250 kHz and 750 kHz. Fig. 7

196 compares the normalized displacement curves (all values are divided by the maximum value  
 197 reached by one of the compared curves) obtained considering the electrical limit conditions (i)  
 198 and (ii). It is observed from this figure that the results are different, particularly between 450  
 199 kHz and 550 kHz. In this frequency domain, a maximum of displacement is obtained around  
 200 500 kHz (mechanical resonant frequency), for the limit condition (ii). Whereas, in the case of  
 201 the limit condition (i), two resonance frequencies 475 kHz and 520 kHz are obtained. Finally,  
 202 the comparison of the two curves indicates a frequency shift (about 25 kHz) between the two  
 203 displacement peaks observed in the frequency band 450 kHz – 550 kHz.

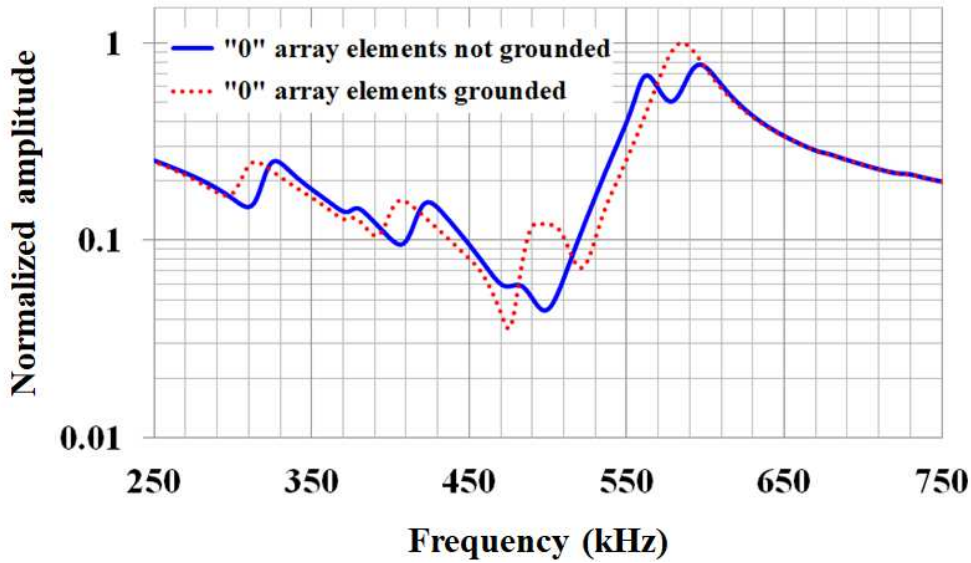


204  
 205 **Figure 7:** Normal displacement computed at the radiating surface of the element “0”.

206 **3.3 Electrical impedance**

207 To observe the effect of the limit conditions (i) and (ii) on the electrical behavior of the  
 208 transducer array, the electrical impedances computed using the numerical model are  
 209 compared in the frequency domain 250 kHz – 750 kHz, as shown in Fig. 8. After analysis, it  
 210 is observed that the two curves follow the same behavior in the frequency domains 250 kHz –  
 211 470 kHz and 590 kHz – 750 kHz. Nevertheless, a frequency shift (about 20 kHz) is obtained  
 212 between the two curves in the first frequency band. The major differences are observed  
 213 around the thickness mode, i.e. in the frequency band 470 kHz – 590 kHz. In this domain, two  
 214 resonance frequencies (475 kHz and 520 kHz) and a one anti-resonance frequency (581 kHz)  
 215 are obtained for the limit condition (i), whereas in the case of the condition (ii), one resonant  
 216 frequency is obtained at about 500 kHz and two anti-resonance frequencies are observed at  
 217 571 kHz and 595 kHz. As seen previously in Fig. 7, the resonance frequencies (minimum of

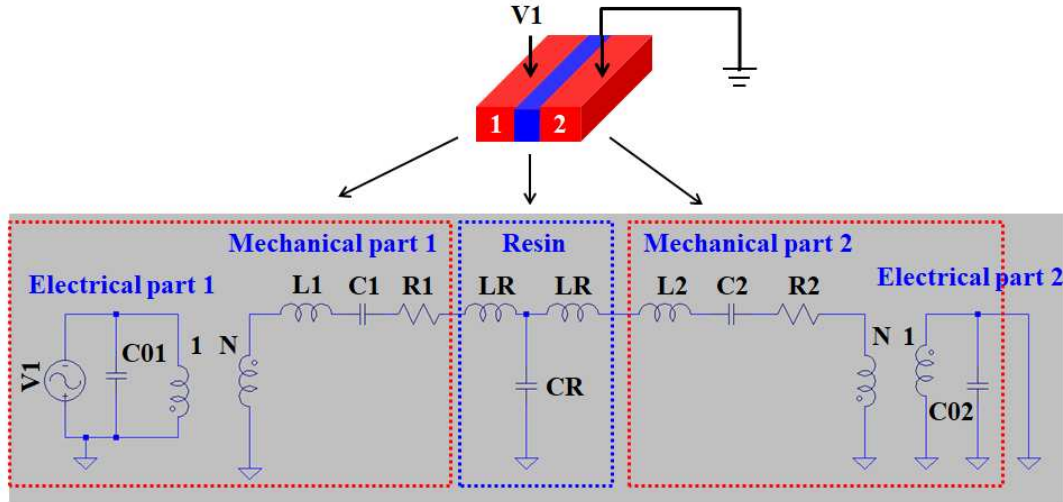
218 impedance) correspond also to the mechanical resonance frequencies (maximum of  
 219 displacement).



220  
 221 **Figure 8:** Numerical electrical impedance of the central element “0”.

222  
 223 The differences between the results obtained under the limit conditions (i) and (ii), i.e.  
 224 TVR, displacement and impedance curves, can be explained by the simplified equivalent  
 225 circuit represented in Fig. 9. In this case, only two piezoelectric elements bonded to each  
 226 other by a non-conductive resin are considered, i.e. an active piezoelectric element (part 1)  
 227 and its neighbouring element grounded or in open-circuit (part 2). The piezoelectric elements  
 228 are represented by their equivalent electromechanical circuit composed of an electrical part  
 229 ( $R_{01,2}$ ,  $C_{01,2}$ ) and a mechanical part ( $R_{1,2}$ ,  $L_{1,2}$  and  $C_{1,2}$ ). The elements  $R_{1,2}$ ,  $L_{1,2}$  and  $C_{1,2}$   
 230 correspond to a mass - spring system, for which  $R_{1,2}$  represents the mechanical dissipations,  
 231  $L_{1,2}$  the mass and  $C_{1,2}$  the compliance (flexibility) of the material.  $R_{01,2}$  and  $C_{01,2}$  represent the  
 232 dielectric losses and the static capacitance of the piezoelectric material. The two parts are  
 233 connected by a transformer converting the electrical energy to mechanical energy and vice-  
 234 versa and having a transformation ratio  $N$ . Because of their very large value (several  $M\Omega$ ), the  
 235 resistors  $R_{01,2}$  are neglected. In the same manner, the non-conductive resin is represented by its  
 236 equivalent circuit ( $L_R$ ,  $C_R$ ). In our previous work [7], it was demonstrated that this  
 237 representation is more accurate in the vicinity of the considered resonant frequency (thickness  
 238 resonance). According to the equivalent circuit, it is clear that when the element 2 is  
 239 grounded, its static capacitance  $C_{02}$  is short-circuited, i.e. the contribution of the electrical  
 240 branch ( $C_{02}$ ) is suppressed. Consequently, only the mechanical branch ( $R_2$ ,  $L_2$  and  $C_2$ )  
 241 contributes to the total electrical impedance of the structure composed of the elements 1 and

242 2. Finally, in the case of the transducer array composed of seven piezoelectric elements, the  
 243 limit condition (i) is responsible in the elimination of the individual static capacitances and it  
 244 results in non-negligible differences between the curves obtained under the limit conditions (i)  
 245 and (ii), e.g. the observed frequency shifts.



246  
 247 **Figure 9:** Equivalent circuit of two piezoelectric elements bonded to each other by resin.

248 **3.4 Crosstalk**

249 The crosstalk level is firstly evaluated at the two characteristic frequencies (maximum  
 250 of displacement) 475 kHz and 520 kHz using both methods. The estimation of the crosstalk  
 251 level  $C$  utilizes the conventional method (relation (1)) when the neighboring elements are not  
 252 grounded (limit condition (ii)). In the case of the limit condition (i) (neighboring elements  
 253 grounded) the proposed method is to evaluate the crosstalk from the displacement values in  
 254 the middle of the array elements) using the relation (2):

255 
$$C(\text{dB}) = 20 \text{Log}\left(\frac{u_i}{u_0}\right), \quad (2)$$

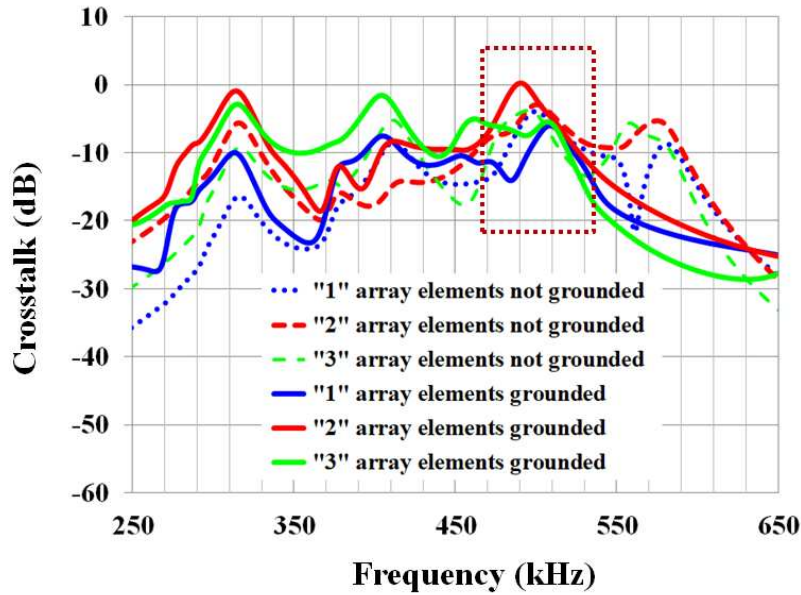
256 where  $u_0$  represents the normal displacement computed in the middle of the central  
 257 element "0" and  $u_i$  ( $i = 1, 2, 3$ ) the displacement in the middle of the neighboring elements  
 258 "1", "2" and "3". The results obtained using the two methods are summarized in Table II. The  
 259 comparison shows that the two methods, i.e. evaluation of crosstalk level by the relation (1)  
 260 and using parasitic displacements instead of voltages  $C_u$  (relation 2), give relatively similar  
 261 crosstalk values at the resonance frequencies. The difference (about 1 dB) is probably because  
 262 the definition of the crosstalk is based on the voltage, which is an average value, whereas, the  
 263 displacement's method is punctual (obtained in the middle of the elements).

Element	"1"	"2"	"3"
Crosstalk $C_u$ (dB)	-11.8	-5.2	-6.1
	-8.8	-7.9	-10
Crosstalk $C$ (dB)	-12.7	-7.4	-7.7
	-8.1	-6.7	-11.1

264

265 **Table II:** Crosstalk evaluated at the resonance frequencies 475 kHz and 520 kHz (bold values).

266 The comparison is then extended to a large frequency band between 250 kHz and 650  
 267 kHz, as shown in Fig. 10. After analysis, it is observed that the crosstalk evaluated using both  
 268 methods are similar around the two characteristic frequencies (see dashed rectangular). The  
 269 difference between the two curves increases beyond the resonance frequencies. In other  
 270 words, the crosstalk evaluated using the displacement in the middle of the array elements is a  
 271 good approximation in the vicinity of the considered mode (thickness mode in this work).



272

273 **Figure 10:** Crosstalk computed using relation 1 (array elements not grounded) compared to  
 274 that obtained from the relation 2 (array elements grounded).

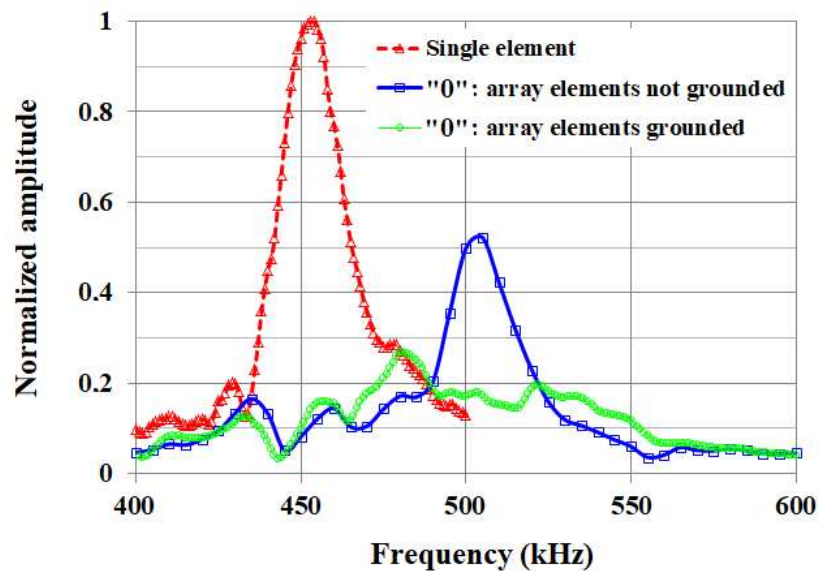
#### 275 4. Experimental Characterization

276 The manufactured transducer array (Fig. 2), is characterized experimentally by electrical  
 277 impedance and displacement measurements, in both conditions (i) and (ii). The crosstalk level

278 is also evaluated using the previous methods, i.e. from the parasitic voltages (relation (1)) and  
 279 using the proposed displacements method (relation (2)). For the sake of simplification,  
 280 measurements are realized in air. The results are then compared to those obtained numerically  
 281 in the air medium instead of water. It is important to notice that the FEM calculations are first  
 282 done in the water medium (section 3) to see the effects of the limit conditions on the  
 283 transducer arrays utilized in medical imaging, and then done in the air medium to compare the  
 284 numerical results with the experimental ones.

#### 285 4.1 Displacement

286 To avoid the edge effects, displacement measurements are realized in the middle of the  
 287 central element “0” using a Polytech OFV353 Laser Vibrometer. The curves obtained in both  
 288 conditions (i) and (ii) are compared with that measured in the middle of a single element (Fig.  
 289 11).

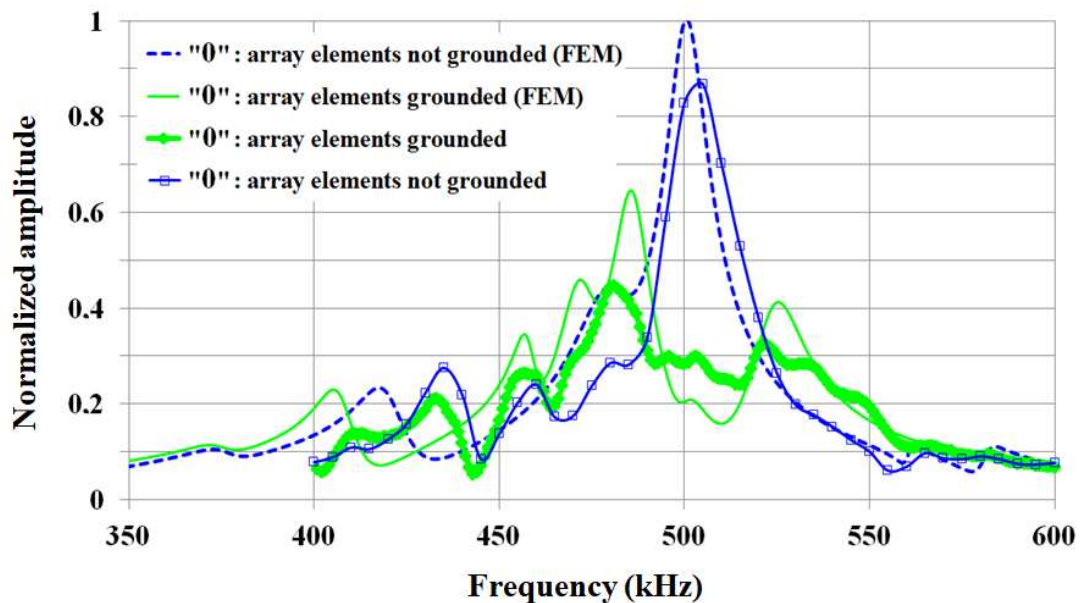


290  
 291 **Figure 11:** Normalized displacement amplitude measured in the middle of the central element  
 292 “0” compared to that obtained in the middle of a single piezoelectric element.  
 293

294 As expected, the curves measured on the element “0” (conditions (i) and (ii)) are  
 295 different, particularly in the frequency band 450 kHz - 550 kHz. In this domain, the  
 296 maximum displacement is obtained at about 500 kHz for the condition (ii). Whereas, in the  
 297 case of the condition (i), two mechanical resonance frequencies 481 kHz and 520 kHz are  
 298 obtained. Furthermore, the displacement amplitudes at both frequencies are lower than those  
 299 observed at 500 kHz. Finally, a frequency shift is obtained between the single element’s  
 300 resonance frequency (452 kHz) and the array’s resonance frequencies. This result is due to the

301 presence of the neighboring elements, which shifts the resonance frequencies towards the high  
302 frequencies and reduces the amplitude of the displacement, e.g. the maximum displacement  
303 for the condition (ii) is about half that obtained in the case of the single element.

304 Fig. 12 compares the displacements measured in the middle of the element “1”, in both  
305 conditions (i) and (ii) to the numerical results (FEM). It is seen from this figure that the results  
306 obtained are similar. Nevertheless, a small frequency shift is observed between the curves  
307 (about 4 kHz), due to the materials’ incertitude. Furthermore, the displacement’s amplitude  
308 obtained numerically is relatively high compared to the measured one, because the resin’s real  
309 losses are not taken into account (about 5%) and the piezoelectric material losses are not  
310 considered.

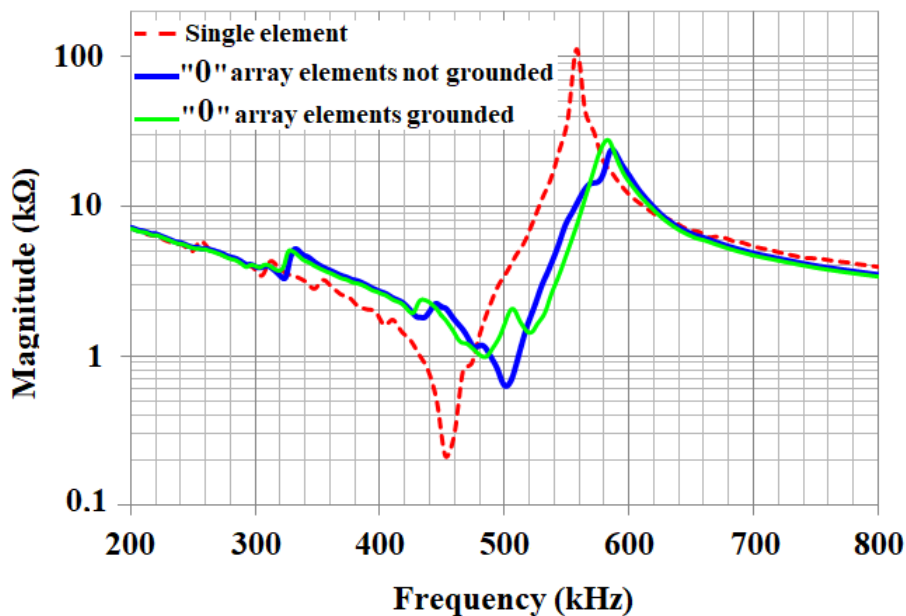


311  
312 **Figure 12:** Normalized displacements amplitude measured in the middle of the central  
313 element “0” compared to the numerical results (FEM).  
314

## 315 4.2 Electrical impedance

316 The electrical impedance of the transducer array is also measured in the frequency band  
317 200 kHz – 800 kHz. Fig. 13 compares the curves obtained considering the limit conditions (i)  
318 and (ii). To show the effects of the interactions between the array elements (crosstalk), the  
319 transducer array’s curves are also compared to that of a single piezoelectric element. After  
320 analysis, different conclusions can be made. Firstly, concerning the single element, a  
321 minimum and a maximum of impedance are observed at 452 kHz and 558 kHz respectively.  
322 Secondly, a frequency shift can be observed between the transducer array curves and the

323 electrical impedance of the single element (about 30 kHz). This result is due to the presence  
 324 of the neighboring piezoelectric elements, which shifts the resonance and anti-resonance  
 325 frequencies towards the high frequencies. Furthermore, due to the crosstalk phenomenon,  
 326 parasitic vibrations are obtained around the array's resonance (condition (i)) and anti-  
 327 resonance frequencies (condition (ii)), contrary to the single piezoelectric element. Finally, in  
 328 the same manner as the numerical results, differences are observed between the electrical  
 329 impedance curves obtained in the case of the conditions (i) and (ii). Indeed, two resonance  
 330 frequencies (481 kHz and 520 kHz) and a one anti-resonance frequency (580 kHz) are  
 331 obtained in the case of the condition (i), whereas in the case of the condition (ii), a one  
 332 resonance frequency is obtained at 500 kHz and two anti-resonance frequencies are observed  
 333 at 565 kHz and 583 kHz. As seen in Fig. 11, the resonance frequencies (minimum of  
 334 impedance) correspond also to the mechanical resonance frequencies (maximum of  
 335 displacement).

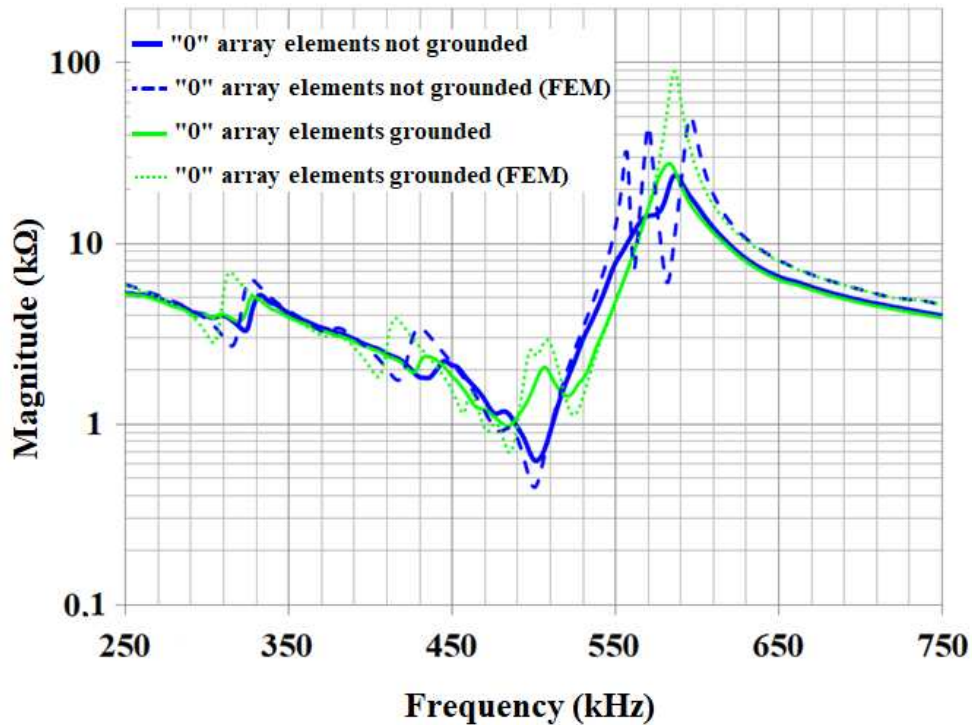


336  
 337 **Figure 13:** Experimental electrical impedance of the element “0” compared to that of a single  
 338 piezoelectric element (dashed line).  
 339

340 Fig. 14 compares the experimental and numerical (FEM) electrical impedances in both  
 341 conditions (i) and (ii): array elements grounded and not grounded. It is seen from this figure  
 342 that the results obtained are similar. Nevertheless, a small frequency shift is observed between  
 343 the curves in the frequency band 250 kHz – 450 kHz, due to the materials' incertitude.  
 344 Furthermore, in the case of the condition (ii), i.e. when the central element “1” is excited and  
 345 its neighboring elements are grounded, only two anti-resonance frequencies are observed in



346 the measured curve, instead of three frequencies as obtained numerically. This result is mainly  
 347 due to the resin losses chosen in the numerical model (about 5 %) and the piezoelectric  
 348 material losses, which are not taken into account.



349  
 350 **Figure 14:** Electrical impedance measured on the element “0” compared to the numerical one.

351 **4.3 Crosstalk**

352 The experimental setup presented previously in Fig. 3 is first utilized to measure the  
 353 parasitic voltages generated on the neighboring elements “1”, “-1”, “2”, “-2”, “3”, and “-3”,  
 354 when the central element “0” is excited by a harmonic signal having 10 V amplitude. In this  
 355 case, measurements are realized at the first resonant frequency of 481 kHz. The crosstalk  
 356 level  $C$  (dB) is then evaluated using the relation (1). The obtained results are given in Table  
 357 III.

358

Element	“-3”	“-2”	“-1”	“0”	“1”	“2”	“3”
Voltage (V)	5.04	1.64	3.23	10	2.73	1.62	4.47
Crosstalk $C$ (dB)	-5.95	-15.7	-9.81	0	-11.28	-15.81	-7

359

360

**Table III:** Crosstalk evaluated using parasitic voltages.

361 The measurements show that when the central element “0” is excited, it vibrates mainly  
362 in its thickness mode, but it generates significant undesirable voltages on its passive  
363 neighboring elements “1”, “-1”, “2”, “-2”, “3” and “-3”. These results demonstrate the  
364 presence of crosstalk in the fabricated transducer array, i.e. the measured average values about  
365 -10.54 dB, -15.75 dB, and -6.47 dB on the first, second and third neighboring elements  
366 respectively. Furthermore, a high level of crosstalk is noticed in the case of the third  
367 neighboring elements “3” and “-3” due to edge effects. As explained previously, in the case of  
368 active cancellation of crosstalk, the determination of the correction voltages considers the  
369 neighboring elements electrically in Short-Circuit (condition (i)). In this situation, the  
370 crosstalk cannot be estimated using the conventional definition (relation (1)). The proposed  
371 solution to evaluate the crosstalk level is to measure the parasitic displacements generated on  
372 the neighboring elements using the experimental setup given in Fig. 4 and then deduce the  
373 crosstalk  $C_u$  (dB) from the relation (2). In this case, the results obtained when the central  
374 element “0” is excited (at the frequency 481 kHz) and its neighboring elements are connected  
375 to the ground (Fig. 4) are summarized in Table IV. In the same manner as the previous results  
376 (Table III), significant parasitic displacements are observed on the passive neighboring  
377 elements. Consequently, strong crosstalk is noticed on the first (“1”, “-1”) and third (“3”, “-  
378 3”) neighboring elements particularly.

Element	“-3”	“-2”	“-1”	“0”	“1”	“2”	“3”
<b>Displacement (nm)</b>	6.21	2.73	5.48	11.8	3.62	1.8	5.59
<b>Crosstalk <math>C_u</math>(dB)</b>	-5.58	-12.71	-6.66	0	-10.26	-16.33	-6.49

379

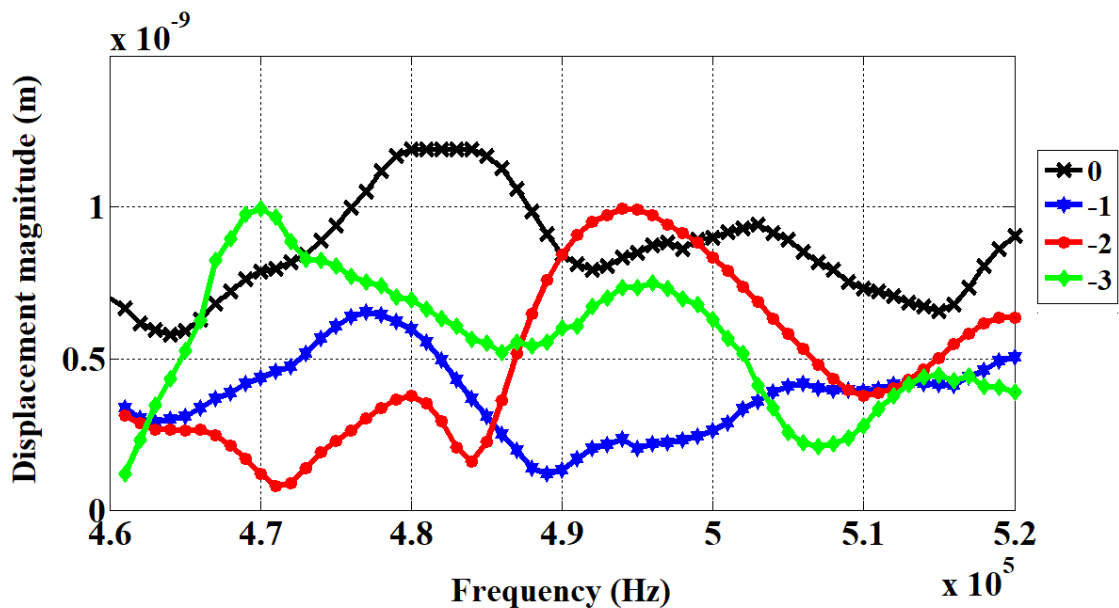
380

**Table IV:** Crosstalk evaluated using parasitic displacements.

381 The comparison of the results given in Tables III and IV shows that the two methods,  
382 i.e. estimation of the crosstalk level by the relation (1) and using parasitic displacements  
383 instead of voltages, give relatively similar crosstalk values at the resonant frequency. The  
384 difference is because the definition of the crosstalk is based on the voltage, which is an  
385 average value, whereas, the displacement’s method is punctual, i.e. measurements are realized  
386 only in the middle of the transducer array elements (Fig. 4), to avoid edge effects. In other  
387 words, this method supposes the displacement uniform at the surface of the individual  
388 elements, which is not true. For more precision, it would be better to measure the  
389 displacement at the whole surface of the array elements, to take into account the contribution

390 of the parasitic length mode [8, 16]. The latter makes the displacement not uniform.  
 391 Measurements can be achieved with a Scanning Laser Vibrometer, e.g. Polytech psv400. In  
 392 this situation, average displacement values can be obtained and the precision of crosstalk  
 393 evaluation can be improved.

394 To estimate the crosstalk level in a relatively large frequency band (460 kHz – 520 kHz)  
 395 using the relation (2), displacement measurements are first done in the middle of the array  
 396 elements. The results obtained on the elements “0”, “-1”, “-2”, and “-3”, when the central  
 397 element “0” is excited by a harmonic signal having 1V amplitude and its neighboring  
 398 elements are grounded (limit condition (i)) are shown in Fig. 15. After analysis, it is observed  
 399 that significant parasitic displacements are obtained on the passive neighboring elements due  
 400 to the crosstalk phenomenon. At the resonant frequency 481 kHz, a maximum of  
 401 displacement is measured on the central element “0” ( $u_0 = 1.19$  nm). The parasitic  
 402 displacements measured on the element “-1”, “-2” and “-3” are about 46 %, 25 % and 56 %  
 403 the amplitude of the excited element “0” respectively.



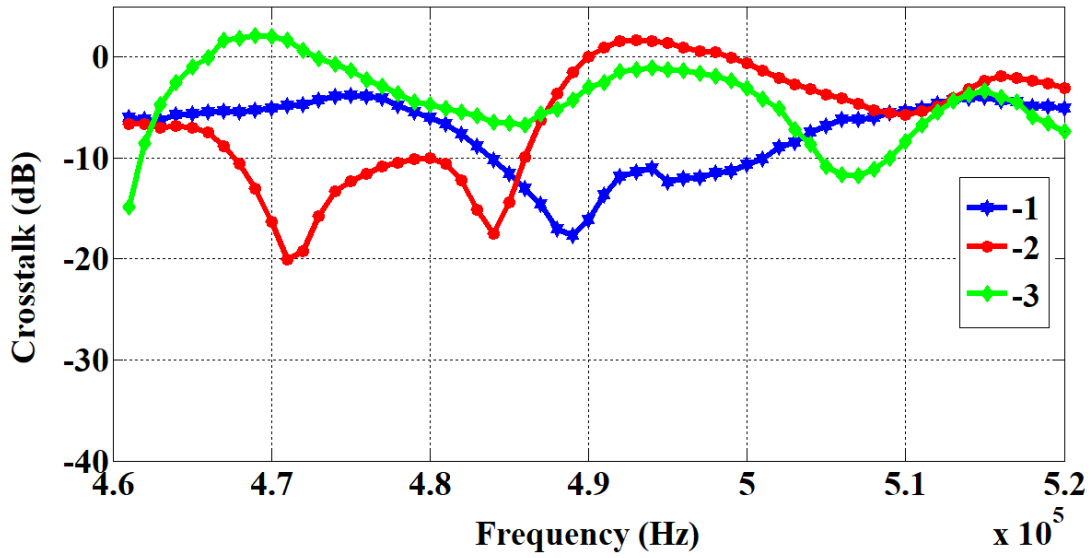
404

405 **Figure 15:** Displacement measured in the middle of the array elements “0”, “-1”, “-2” and “-  
 406 3”, when the central element “0” is excited by a harmonic signal having 1V  
 407 amplitude and its neighboring elements grounded.

408

409 The relation (2) is then utilized to evaluate the crosstalk level in terms of displacement  
 410 as shown in Fig. 16. According to the latter, it is clear that in the frequency band 460 kHz –  
 411 520 kHz, the transducer array presents a strong crosstalk level (greater than -20 dB). Around  
 412 the central element’s resonant frequency 481 kHz, i.e. between 475 kHz – 487 kHz, the

413 highest crosstalk level is obtained for the third element “-3”, located on the array’s edge. In  
 414 the same frequency band, a relatively similar crosstalk level is measured on the first “-1”.  
 415 Finally, the crosstalk level observed of the second neighbor “-2” is also not negligible (higher  
 416 than -20 dB). Because of these high crosstalk levels, active crosstalk cancellation methods are  
 417 successfully proposed and utilized to reduce the interactions between the array elements  
 418 (crosstalk) and to improve its performance [16, 27].



419  
 420 **Figure 16:** Crosstalk estimated on the array elements “-1”, “-2” and “-3” by using the relation  
 421 2 (array elements grounded).  
 422

## 423 5. Conclusion

424 In this paper, the effects of the electrical limit conditions on the electromechanical  
 425 behavior of a piezoelectric transducer array are investigated numerically and experimentally.  
 426 A seven-element transducer array radiating in water is first modeled using the 2D Finite  
 427 Element Method. Globally, the computed results (TVR, electrical impedance and  
 428 displacement) indicated that the influence of the limit conditions (central element’s  
 429 neighboring elements grounded or not) is mainly observed around the thickness mode’s  
 430 resonance and anti-resonance frequencies. Furthermore, a frequency shift is obtained between  
 431 the curves computed considering the two limit conditions (about 20 kHz). However,  
 432 concerning the crosstalk, it is shown that the values calculated under the two electrical limit  
 433 conditions are relatively similar (about 1 dB of difference) at the mechanical resonance  
 434 frequencies (maximum of displacement) 475 kHz and 520 kHz. The difference between the  
 435 computed curves increases beyond the resonance frequencies. The numerical results

436 (electrical impedance and displacements) computed in the air medium are successfully  
437 compared to those measured using an impedance analyzer and a Laser Vibrometer  
438 respectively. In both cases, it is shown that the influence of the limit conditions is mainly  
439 observed around the thickness mode's resonance and anti-resonance frequencies.  
440 Furthermore, the crosstalk level is evaluated experimentally at the mechanical resonance  
441 frequency 481 kHz using two methods, i.e. voltage and displacement measurements. The  
442 results obtained are relatively similar. Nevertheless, for more precision, a Scanning Laser  
443 Vibrometer should be utilized to achieve average displacement values instead of punctual  
444 ones. Finally, the crosstalk level is estimated in the frequency band 460 kHz – 520 kHz using  
445 the proposed method, i.e. deduced from punctual displacement measurement. According to  
446 the results, the manufactured seven-element transducer array presents a strong crosstalk level  
447 (greater than -20 dB), which should be reduced to improve the array's electromechanical  
448 behavior. For this purpose, active crosstalk cancellation methods can be utilized, i.e. the  
449 application of adequate correction voltages to the array elements can be a solution to reduce  
450 the crosstalk level. Dicing the inter-element filling material can also contribute to reduction of  
451 this undesirable phenomenon (crosstalk).

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