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Studying polymer diffusiophoresis with Non-Equilibrium Molecular Dynamics

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We report a numerical study of the diffusiophoresis of short polymers using non-equilibrium molecular dynamics simulations. More precisely, we consider polymer chains in a fluid containing a solute which has a concentration gradient, and examine the variation of the induced diffusiophoretic velocity of the polymer chains as the interaction between the monomer and the solute is varied. We find that there is a non-monotonic relation between the diffusiophoretic mobility and the strength of the monomer-solute interaction. In addition we find a weak dependence of the mobility on the length of the polymer chain, which shows clear difference from the diffusiophoresis of a solid particle. Interestingly, the hydrodynamic flow through the polymer is much less screened than for pressure driven flows.

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I. INTRODUCTION

In a bulk fluid, concentration gradients cannot cause fluid flow. However, a gradient in the chemical potential of the various components in a fluid mixture, can cause a net hydrodynamic flow in the presence of an interface that interacts differently with the different components of the mixture. Such flow induced by chemical potential gradients is usually referred as diffusio-osmosis (see e.g.¹). The same mechanism that causes diffusio-osmosis can also drive the motion of a colloid, or other mesoscopic moiety, under the influence of chemical potential gradients in embedding fluid. Clearly, if the mesoscopic particle (say a colloid) is very large compared to the characteristic length scale on which adsorption or depletion occurs, it is reasonable to use the Derjaguin approximation^{2,3}, i.e. to describe the colloid-fluid interface as locally flat, and thus estimate the speed of diffusiophoresis. However, the Derjaguin approach is likely to fail if the particles that are subject to phoresis are no longer large compared to the range of adsorption/depletion. There is yet another situation where the Derjaguin approach is obviously questionable, namely in the case of particles that do not have a well-defined surface. One particularly important example is the case of diffusiophoresis of polymers: molecules that have a fluctuating shape and an intrinsically fuzzy surface. One manifestation of this fuzziness is the fact that the magnitude of the Kirkwood approximation for the hydrodynamic radius R_h of a long self-avoiding polymer is about 63% of the radius of gyration R_g ⁴: for a smooth sphere, this ratio would be $\approx 107\%$ (the Kirkwood expression for R_h is only an approximation: the point is that the averages are different and that hydrodynamic radius is smaller than for a corresponding solid object). This difference implies that the density inhomogeneity of a self-avoiding polymer results in penetration of hydrodynamic flow fields into its outer “fuzzy” layer. In addition, solutes can diffuse through the polymer. This fuzziness clearly makes it difficult to describe a polymer as a solid sphere surrounded with pure liquid, and hence a Derjaguin approach is questionable. The lack of predictive power of the colloidal approximation was pointed out previously by experiments with λ -DNA by Palacci et al^{5,6}.

There is another factor that makes diffusiophoresis of polymers unusual: since the driving force for diffusiophoresis comes from an excess (or deficit) of solute in the fluid surrounding the polymer, the stronger a solute is attracted to a polymer, the larger this excess will be. However, a strongly binding solute may result in the collapse of the polymer to a compact globule (scaling exponent 1/3). Hence, unlike in the case of colloids, one cannot assume that the size of polymers subject to diffusiophoresis is independent of the polymer-solute interaction. Furthermore, a so-

lute excess/deficit may not be sufficient for the occurrence of diffusiophoresis: if the solutes are strongly adsorbed onto the polymer, they become effectively immobile relative to the polymer, in which case the excess/deficit do not contribute to diffusiophoresis.

In this paper, we report systematic molecular dynamic simulations of diffusiophoretic transport of short polymers. Specifically, we apply non-equilibrium molecular dynamic simulations using a microscopic force acting on each species, and examine the effect of interaction parameters between the monomer and the solute on the induced diffusiophoretic velocity of the polymer. Our simulations indeed reveal a non-monotonic dependence of the phoretic mobility Γ_{ps} on ϵ_{ms} , the interaction strength between the polymer and solute. We have investigated the influence of the size of the polymer on its diffusiophoretic mobility. We find a weak polymer-size dependence of the mobility. We compare these findings with the corresponding theoretical predictions for a colloidal particle.

II. THERMODYNAMICS FORCES AND THEIR MICROSCOPIC REPRESENTATION

Conceptually the most straightforward way of simulating diffusiophoresis would be to carry out a Non-Equilibrium Molecular Dynamics (NEMD) with an imposed concentration gradient, following a procedure similar to Heffelfinger and Van Swol⁷ and Thompson and Heffelfinger⁸. Nonetheless, there are several drawbacks associated with this approach for modeling diffusiophoresis, the most significant being that periodic boundary conditions are incompatible with the existence of constant concentration gradients as advection deforms the concentration profiles (see Supplementary Material). However, in analogy with simulations of systems in homogeneous electrical fields, we can replace the gradient of a chemical potential by an equivalent force per particle that can be kept constant, and therefore compatible with periodic boundary conditions^{9,10}. This field-driven non-equilibrium approach has been often applied in other contexts¹¹. The idea is to impose a mechanical constraint (i.e an external field) that mimics the effect of the force¹². To see how this approach works in the systems that we study, we first consider diffusio-osmosis in a binary mixture of solvent (f) and solute (s) particles, which are subjected to a gradient of chemical potential of one of the species (e.g. s), and a gradient in the pressure (in bulk fluids in the absence of external body forces, the pressure gradient will typically vanish). We assume that the system is at constant temperature. Ajdari and Bocquet¹³ derived an expression for the transport

matrix Γ that relates the fluxes, *viz.* the total volume flow \mathbf{Q} and the excess solute flux $\mathbf{J}_s - c_s^B \mathbf{Q}$, with the gradient of pressure $-\nabla P$ and the gradient of the chemical potential of one of the species; where c_s^B is the solute concentration in the bulk. There are only two independent thermodynamic driving forces as, at constant temperature, only two of the three quantities ∇P , the solute $\nabla \mu_s$ and the solvent $\nabla \mu_f$ are independent. In fact, it is convenient to define a slightly modified chemical potential gradient $\nabla \mu'_s$ by $\nabla \mu'_s \equiv [1 + c_s^B/c_f^B] \nabla \mu_s$, in which c_s^B/c_f^B is the ratio between the solute (s) and solvent (f) concentrations in the bulk. With this definition, the linear transport equations can be written as

$$\begin{bmatrix} \mathbf{Q} \\ \mathbf{J}_s - c_s^B \mathbf{Q} \end{bmatrix} = \begin{bmatrix} \Gamma_{qq} & \Gamma_{qs} \\ \Gamma_{sq} & \Gamma_{ss} \end{bmatrix} \begin{bmatrix} -\nabla P/T \\ -\nabla \mu'_s/T \end{bmatrix}, \quad (1)$$

where Γ_{ij} 's are the Onsager transport coefficients connecting the different fluxes with the thermodynamic driving forces. In what follows, it is convenient to replace $\nabla \mu_i$ the gradient of the chemical potential on species i by an equivalent external force \mathbf{F}_i^μ , such that $\mathbf{F}_i^\mu = -\nabla \mu_i$. This approach to replace the chemical potential gradient by an equal (and opposite) ‘‘color’’ force was previously used in the context of diffusion and transport in microporous materials by Maginn *et al.*^{14,15}. In the context of diffusio-osmosis, Liu *et al.*¹⁰ showed that simulations using color forces yield the same results as those obtained with explicit gradients of concentration. Furthermore, Yoshida *et al.*⁹ used the Green-Kubo formalism¹⁶ to show that Onsager’s reciprocity is also fulfilled. Ganti *et al.* have applied and validated a similar approach in the context thermo-osmosis^{17,18}.

Having considered the case of a binary solvent-solute mixture, we now add a third component, namely the polymer, to the system. Again, not all chemical potential gradients are independent, as it follows from the Gibbs-Duhem equation:

$$VdP = SdT + \sum_i N_i d\mu_i. \quad (2)$$

In what follows, we assume there are no global pressure and thermal gradients in the system. As a consequence, we can write:

$$\mathbf{F}_p^\mu = -(\mathbf{F}_s^\mu N_s + \mathbf{F}_f^\mu N_f), \quad (3)$$

where $\mathbf{F}_p^\mu, \mathbf{F}_s^\mu, \mathbf{F}_f^\mu$ denote the equivalent forces on the polymer, solute and solvents mimicking the corresponding chemical potential gradients. N_s, N_f refer to the total number of solutes and solvents in the system as a whole. This equation simply expresses the fact that there can be no net external

force on the fluid: if there were, the system would accelerate without bound, as there are no walls or other momentum sinks in the system. In simulations, it is convenient to work with a force per monomer, rather than a force on the center-of-mass of the polymer: $\mathbf{F}_m = \mathbf{F}_p^{\mu}/N_m$, where N_m denotes the number of beads in the polymer. Equation (3) establishes a connection between all chemical potential gradients (or the corresponding microscopic forces), which must be balanced throughout the system as phoretic flow cannot cause bulk flow.

We will now compute the rate of polymer diffusiophoresis using Eq. (3) as our starting point.

III. MOLECULAR DYNAMICS (MD) SIMULATIONS

We performed non-equilibrium Molecular Dynamics (NEMD) simulations using LAMMPS¹⁹. In most simulations, particles interact via a 12-6 Lennard-Jones potential (LJ) $V_{LJ}(r) = 4\varepsilon_{ij}^{LJ}[(\sigma_{ij}^{LJ}/r)^{12} - (\sigma_{ij}^{LJ}/r)^6]$ shifted and truncated at $r = r_c$, such that

$$V_{TS}(r) = \begin{cases} V_{LJ}(r) - V_{LJ}(r_c), & \text{if } r \leq r_c \\ 0, & \text{otherwise.} \end{cases} \quad (4)$$

The indices i and j denote the particle types in our simulations: solutes (s), solvents (f) and monomers (m). To keep the model as simple as possible, we assume that in the bulk the solute and solvent behave as an ideal mixture. We therefore choose the same Lennard-Jones interaction for the particle pairs ss , sf , ff with $\varepsilon_{ij}^{LJ} = \varepsilon_0$ and $\sigma_{ij}^{LJ} = \sigma_0$. We use these same parameters also for the monomer-solvent interaction ms . However, the monomer-solute interaction strength ε_{ms}^{LJ} was varied to control the degree of solute adsorption or depletion around the polymer. Yet, we kept σ_{ms}^{LJ} equal to σ_0 . For the monomer-monomer interaction, we use a purely repulsive Weeks-Chandler-Andersen potential²⁰, i.e. a Lennard-Jones potential truncated and shifted at the minimum of the LJ potential, $r_c = 2^{1/6}\sigma_0$. For all other interactions, $r_c = 2.5\sigma_0$. Finally, neighboring monomers are connected by a finite extensible, nonlinear elastic (FENE) anharmonic potential $U_{FENE}(r)$,^{21,22}

$$U_{FENE}(r) = -\frac{kR_0^2}{2} \ln \left[1 - \left(\frac{r}{R_0} \right)^2 \right], \quad (5)$$

with $k = 7\varepsilon_0/\sigma_0^2$ and $R_0 = 2\sigma_0$. In what follows, we use the mass m_0 of all the particles (s, f and m) as our unit of mass and we set our unit of energy equal to ε_0 , whilst our unit of length is equal to σ_0 , all other units are subsequently expressed in term of these basic units. As a result, forces are expressed in units ε_0/σ_0 , and our unit of time is $\tau \equiv \sigma_0\sqrt{m_0/\varepsilon_0}$.

A. Equilibration

We studied the diffusiophoresis of a single polymer chain composed of 30 monomers, $N_m = 30$, suspended in an equimolar ideal mixture of solute and solvent molecules. The initial simulation box dimensions were $L_x = 20\sigma_0$, $L_y = 20\sigma_0$, $L_z = 30\sigma_0$ and the number of fluid particles was 8748. After equilibration, chemical potential gradients were applied along the x -axis. We distinguished two types of domains in the simulation box: one periodically repeated domain with width $20\sigma_0$ in the z -direction centered around the polymer’s center of mass in the z -coordinate. The remainder of the system (a domain with width $10\sigma_0$), contains only bulk fluid (see Fig 1 – note that because this figure is centered around the polymer, one half of the bulk domain is shown above and one half below the polymer domain). We verified that the composition of the mixture in this bulk domain is not influenced by the presence of the polymer in the other domain (See Supplementary material). The system is periodically repeated on each direction.

Our aim was to carry out simulations under conditions where the composition of the bulk fluid was kept fixed, even as we varied the monomer-solute interaction. Moreover, we prepared all systems at the same hydrostatic pressure. Therefore, we performed NPT simulations using a Nosé-Hoover thermostat/barostat²³. The equations of motion were integrated using a velocity-Verlet algorithm with time step $t = 0.005\tau$. After the relaxation of the initial configuration, the box was allowed to fluctuate in the y direction, fixing $k_B T / \epsilon_0 = 1.0$ and $P\sigma_0^3 / \epsilon_0 = 1.0$ for 2×10^4 steps.

During the NPT equilibration, fixing the bulk concentration of the liquid requires a careful protocol, in particular in cases where the solute binds strongly to the polymer. In our simulations, we accelerated the equilibration of the solute adsorption on the polymer by attempting to swap solvent and solute molecules 10^4 times for every MD step throughout the simulation box. Simultaneously, we swapped solutes and solvents in the bulk, to ensure that adsorption on the polymer does not deplete the solute concentration in the bulk. To this end, we swapped solutes and solvents in the bulk every 200 steps such that the bulk solute concentration remained fixed at $c_s^B \approx 0.376$. Note that these swaps were only carried out during equilibration.

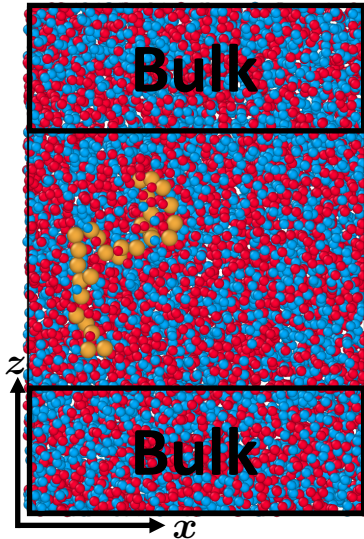


FIG. 1: Simulation box showing solutes (red), solvents (blue) and monomers (orange). The bulk regions are shown inside black boxes. In the bulk, the solute and solvent concentrations are assumed to be unperturbed by the presence of the polymer.

B. Field-driven simulation

Having prepared a system of polymer in a fluid mixture with a pre-determined pressure and bulk composition, we now consider the effect of chemical potential gradients on the phoretic motion of the polymer in NVT simulations. As discussed above, we represent the chemical potential gradients by equivalent external forces that are compatible with the periodic boundary conditions. Importantly, the forces are chosen such that a) there is no net force on the system as a whole and b) there is no net force on the bulk solution away from the polymer. These two conditions imply that there is only one independent force that can be defined in the system. In the present case, we chose to fix the force on the solutes F_s^μ , which was varied between 0 and $0.1 \epsilon_0/\sigma_0$ for different runs. During all the field-driven simulations, we employed a dynamical definition of the bulk and polymer domains such that the z -coordinate of the center of mass of the polymer is always in the middle of the polymer domain. This procedure ensures that the “bulk” region remains unperturbed by the polymer. Having specified the force on the solute, the force on the solvent particles follows from mechanical equilibrium in the bulk in Eq. (3) (see Fig. 1):

$$\mathbf{F}_s^\mu N_s^B + \mathbf{F}_f^\mu N_f^B = 0, \tag{6}$$

where N_s^B , N_f^B denote the number of solutes and solvent in the bulk region. Once the forces in the bulk have been specified, the phoretic force on the polymer \mathbf{F}_p^μ is obtained by imposing force balance on the system as a whole (Eq. (3)).

Due to the finite size of the bulk domain there are inevitably fluctuations in the composition of this domain. These fluctuations would lead to unphysical velocity fluctuations in the bulk (unphysical because in the thermodynamic limit this effect goes away). These velocity fluctuations would contribute to the noise in the observed phoretic flow velocity. To suppress this effect, we could either adjust the composition in the bulk domain at every time step, or adjust the forces on solute and solvent (\mathbf{F}_p^μ and \mathbf{F}_f^μ) such that the external force on the bulk domain is always rigorously equal to zero. We opted for the latter approach, because particle swaps would affect the stability of the MD simulations.

IV. RESULTS AND DISCUSSION

A. Phoretic velocity

In Fig 2 the polymer velocities in the direction of the gradient v_p^x are plotted for three different pair of LJ parameters. When there is adsorption of solutes around the polymer ($\epsilon_{ms}^{LJ} = 1.5$), the polymer follows the gradient, migrating towards regions where the solute concentration is higher. Conversely, when there is depletion ($\epsilon_{ms}^{LJ} = 0.5$) the polymer will move in the opposite direction. As a null check, we also performed simulations for the case where the $\epsilon_{ms}^{LJ} = \epsilon_{mf}^{LJ}$. In that case, there should be no phoresis, as is indeed found in the data shown in Fig. 2. The inversion of the velocity depending on the sign of the monomer-solute interaction is expected on the basis of irreversible thermodynamics¹ and has previously been observed in simulations of for nano-dimers, using hybrid molecular dynamics-multiparticle collision (MD-MPC) dynamics^{24,25}.

The figure also shows that our simulations appear to be in the linear regime, as the magnitude of the phoretic velocity increases linearly with the strength of the applied field.

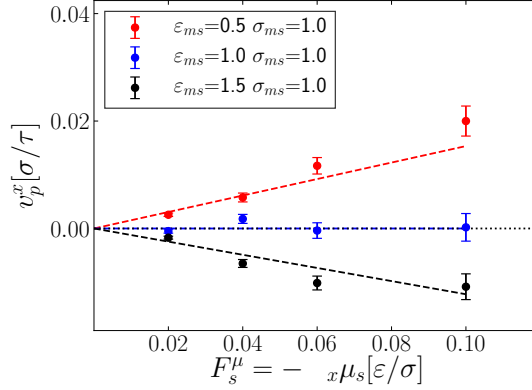


FIG. 2: Polymer velocities in the direction of the gradient for different LJ interactions ($\epsilon_{ms}^{LJ}, \sigma_{ms}^{LJ}$) vs the force applied on the solute particles.

B. Mobility dependence on the interaction

The mobility Γ_{ps} of a polymer moving under the influence of a gradient in the solute chemical potential is defined through:

$$\mathbf{v}_p^x = \Gamma_{ps} \nabla_x \mu_s. \quad (7)$$

We can compute Γ_{ps} as a function of the polymer-solute interaction strength from the slope of the v_p^x vs. $\nabla_x \mu_s$ plots, such as the ones shown in Fig 2. This procedure allows us to obtain Γ_{ps} as a function of the monomer-solute interaction strength ϵ_{ms}^{LJ} . We stress that, whilst we determine Γ_{ps} by varying $\nabla_x \mu_s$, we keep the bulk composition of the mixture fixed (as well as the temperature and the pressure). The resulting relation between ϵ_{ms}^{LJ} and Γ_{ps} is shown in Fig 3. As expected, Γ_{ps} is linear in ϵ_{ms}^{LJ} when $\epsilon_{ms}^{LJ}/\epsilon_{mf}^{LJ}$ is close to one. However, as the monomer-solute interaction gets stronger, Γ_{ps} saturates, and subsequently decays with increasing ϵ_{ms}^{LJ} .

The observed decrease of Γ_{ps} for large values of ϵ_{ms}^{LJ} suggests that when solute particles bind strongly to the polymer, they become effectively immobilised and hence cannot contribute to the diffusio-osmotic flow through and around the polymer. This argument would suggest that the diffusiophoretic velocity should vanish as ϵ_{ms}^{LJ} becomes much larger than the thermal energy. However, that does not seem to be the case: rather Γ_{ps} seems to level off at a small but finite value. This suggests that not all fluid particles involved in the phoretic transport are tightly bound to the polymer. One obvious explanation could be that the LJ potential that we use is sufficiently long-ranged to interact with solute particles that are in the second-neighbour shell around the monomeric units of

the polymer. To test whether this is the case, we repeated the simulations with a shorter-ranged short-ranged Lennard-Jones-like potential (SRLJ)²⁶ that has a smaller cut-off distance ($r_c = 1.6$) where the potential and its first derivative vanish continuously. In the insert of Fig. 3 this narrower potential is shown compared with the standard truncated and shifted LJ potential with $r_c = 2.5$, $\epsilon^{LJ} = 1$ and $\sigma^{LJ} = 1$. In our simulations we only used the SRLJ potential for the monomer-solute interactions. For all other interactions we still use the standard LJ potential.

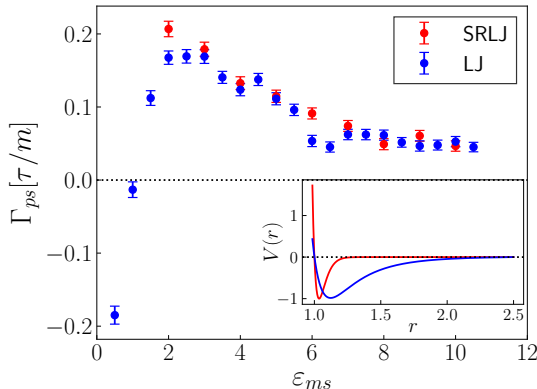


FIG. 3: Mobilities for different LJ interaction energies (ϵ_{ms}). All the simulations were performed keeping the thermodynamic conditions in the bulk constant (T, P, c_s^B). The insert shows a LJ potential for $r_c = 2.5$, $\epsilon^{LJ} = 1$ and $\sigma^{LJ} = 1$ and a SRLJ potential, showing the narrow range of the monomer-solvent interaction.

Figure 3 shows a comparison of the results obtained with the LJ and the SRLJ potentials. Interestingly, even with the short-ranged monomer-solute interaction for which next-nearest neighbour interactions are excluded, Γ_{ps} still does not decay to zero at large ϵ_{ms}^{LJ} . This suggests that the phoretic force is not just probing the excess of solute particles that are directly interacting with the polymer, but also the density modulation of solutes (and solvent) that is due to the longer-ranged structuring of the mixture around the polymer coil. In Fig. 4, we show an extreme case ($\epsilon_{ms}^{LJ} = 8.0$) where the polymer has collapsed and particles within a hydrodynamic radius R_h from the center of mass do not contribute to phoresis as they are tightly bound. In contrast, particles in the structured liquid layer further away from the center of the polymer ($r > R_H$) are mobile and can therefore contribute to the diffusio-osmotic flow.

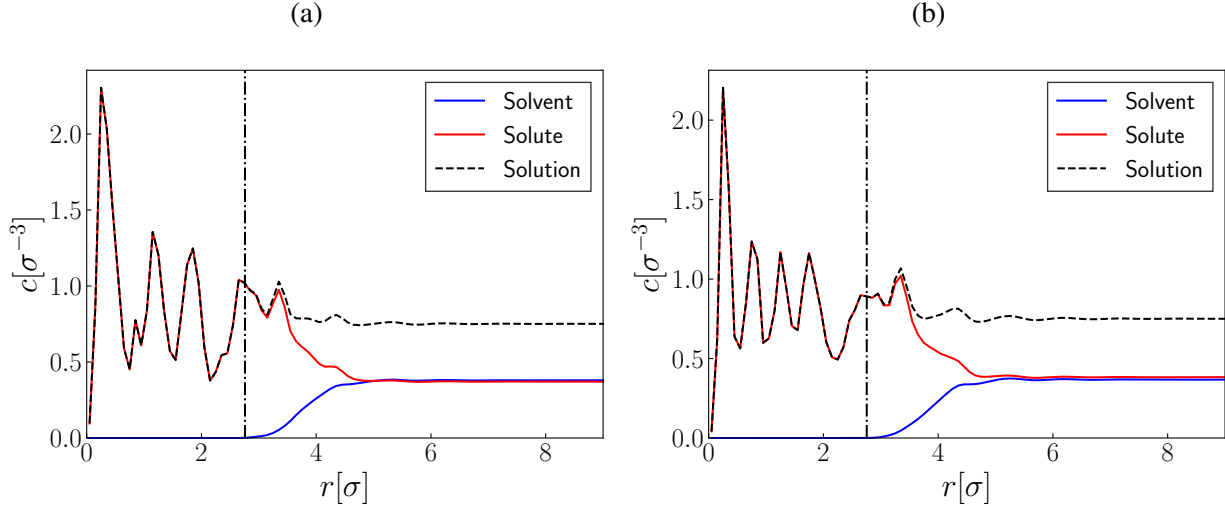


FIG. 4: Distribution of solutes, solvents and the total solution measured from the center of mass of the polymer for (a) LJ, (b) SRLJ. The vertical line represents the hydrodynamic radius R_h of the polymer, in both cases $\epsilon_{ms}^{LJ} = 8.0$. Mobile particles in the heterogeneous region outside the collapsed polymer coil contribute to the diffusio-osmotic flow in a similar way for both ranges of interaction.

C. Scaling of the phoretic mobility with the length of the polymer

For colloidal particles with a radius much larger than the range of the colloid solute interaction, the diffusiophoretic mobility is independent of the colloidal radius²⁷. As the diffusion of a polymer in a fluid is often described as that of a colloid with an equivalent “hydrodynamic radius” R_h , one might be inclined to assume that the diffusiophoretic mobility of a sufficiently large polymer might also be size independent. To our knowledge, this size dependence has not been tested in simulations. However, experiments by Rauch and Köhler²⁸ showed that thermophoretic mobility of polymers varies with the molecular weight M_w for short polymers (fewer than 10 monomers), but very little for longer polymers (10-100 monomers).

For colloids, Anderson²⁷ derived an expression for the diffusiophoretic mobility of colloids in the case where the interfacial layer thickness L is smaller, but not much smaller than the radius a of the colloid. Introducing the small parameter $\lambda \equiv L/a$, Anderson derived the following asymptotic expression for the diffusiophoretic velocity v of a colloidal particle:

$$v = v_0 \left[1 - \frac{(K+H)}{L} \lambda + \mathcal{O}(\lambda^2) \right]. \quad (8)$$

In this approximation, the first term corresponds to the Derjaguin limit $L \ll a$:

$$v_0 = \frac{\alpha}{\beta \eta} L^* K, \quad (9)$$

where α is the magnitude of the concentration gradient, $\beta = 1/(k_B T)$, η is the shear viscosity and ϕ is the potential of mean force experienced by solutes at a distance $y = r - a$ from the surface of the colloid. K , L^* , H are proportional to moments of the excess solute distribution $c_s(y) = c_s^B \exp[-\beta \phi(y)]$,

$$K = \int_0^\infty [\exp[-\beta \phi(y)] - 1] dy, \quad (10)$$

$$L^* = \frac{\int_0^\infty y [\exp[-\beta \phi(y)] - 1] dy}{K}, \quad (11)$$

$$H = \frac{\int_0^\infty \frac{1}{2} y^2 [\exp[-\beta \phi(y)] - 1] dy}{\int_0^\infty y [\exp[-\beta \phi(y)] - 1] dy}. \quad (12)$$

The corrections terms in Eq. (8) account for the effect of the curvature of the particle. All the above equations apply to the case where there is no hydrodynamic slip on the surface of the colloid. However, if solute particles are strongly adsorbed to the colloid, they become immobile and the result is simply that the surface of no slip, and hence the effective colloidal radius, increases. Eq. (8) was derived assuming no-slip boundary conditions to solve the Navier-Stokes equation. However, Ajdari and Bocquet¹³ showed that a correction due to the hydrodynamic slip captures the transport enhancement at interfaces. Including the amplification factor due the surface slip, for moderate adsorption or depletion of solutes, the corrected diffusiophoretic velocity v' reduces to:

$$v' = v \left(1 + \frac{b}{L} \right). \quad (13)$$

where b is the hydrodynamic slip length.

To study the dependence of the phoretic motion of a polymer on the number of monomers of the chain N_m , simulations were performed for a range of N_m from 5 to 60. As our polymers are fully flexible (but self-avoiding) a chain of 60 beads corresponds to a medium-sized polymer. The simulation box was scaled accordingly with the Flory exponent for a polymer in a good solvent $\nu \approx 0.6$ thus ensuring that the chain could not overlap with its periodic images. All the NEMD simulations were carried out for 10^8 time steps.

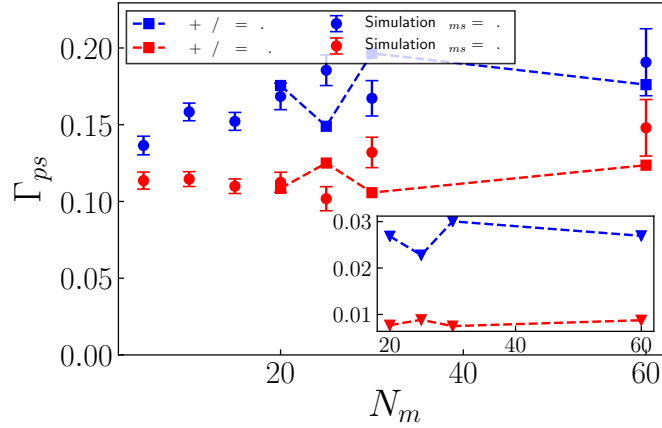


FIG. 5: Diffusiophoretic mobility Γ_{ps} of a polymer vs the number of monomers in the polymer N_m . The results $\epsilon_{ms}^{LJ} = 1.5$ are shown in red and in blue for $\epsilon_{ms}^{LJ} = 0.5$. The simulation results are represented as dots and the theoretical predictions (Eq. (8), including the amplification due to the hydrodynamic slip), are shown as squares. The insert shows the theoretical predictions without the slip correction. In the theoretical calculations $a = R_h$, where R_h is the hydrodynamic radius estimated, for the specific interaction ϵ_{ms} and thermodynamic conditions, using Stokes-Einstein relation (Eq. (14))

In Fig. 5, the simulation results are shown together with theoretical predictions replacing the polymer by an equivalent hard sphere with a radius $a = R_h$, with the hydrodynamic radius R_h given by Stokes-Einstein relation (Comparison with the Kirkwood approximation for R_h ²⁹ are shown in SI),

$$R_h \equiv \frac{k_b T}{6\pi\eta D}, \quad (14)$$

where η denotes the viscosity of the solution in the bulk, which was computed independently, using the Green-Kubo expression relating η to the stress auto-correlation function, in an equilibrium simulation of the bulk fluid (see, e.g.¹⁶). The diffusion coefficient D was also computed from equilibrium simulations³⁰ taking into account the different interactions ϵ_{ms} . Fig. 5 shows that the diffusiophoretic mobility of the polymer increases with N_m . The large quantitative differences between the simulations and the theoretical approximations for a colloid with the same hydrodynamic radius are to be expected: First of all, the assumption that the polymer coil behaves as a hard sphere with $a = R_h$ is rather drastic. To be more precise, this approximation (that was also used by Kirkwood²⁹) assumes that the liquid molecules within the coil region move together, such that the whole assembly moves as a rigid sphere (see e.g.³¹). This might be a good approximation

for the diffusion of long polymer coils, but in the case of phoresis, it is unrealistic to assume that no solute/solvent can be transported through the polymer at distances less than R_h . The second (but related) questionable approximation is that R_h defines the surface of the equivalent colloid in the integrals in Eqs. (10)-(12). As a consequence, the contribution of any excess solute at a distance less than R_h from the polymer center is ignored. As is clear from Fig. 4 this assumption is incorrect and is likely to underestimate the real diffusiophoretic flow, in view of the fact that Fig. 6b shows that there can be considerable solute advection for $r < R_h$.

Our simulations suggest that better theoretical models for polymer diffusiophoresis are needed. In Fig. 6 we show the velocity field for a polymer with $N_m = 30$ for two cases: when it is subjected to a body force i.e pressure gradient 6a and under the influence of diffusiophoresis 6b. As is obvious from the figure, in both cases there is fluid motion within the polymer at distances less than R_h from its center of mass. However, there is an important difference between the flows inside the polymer for the pressure-driven and phoretically driven flows: strong hydrodynamic screening is found in the case of a pressure gradient while for diffusiophoresis, screening seems to be effectively absent. Notice that the density profile is somewhat asymmetric due to the advection produced by the pressure-driven flow.

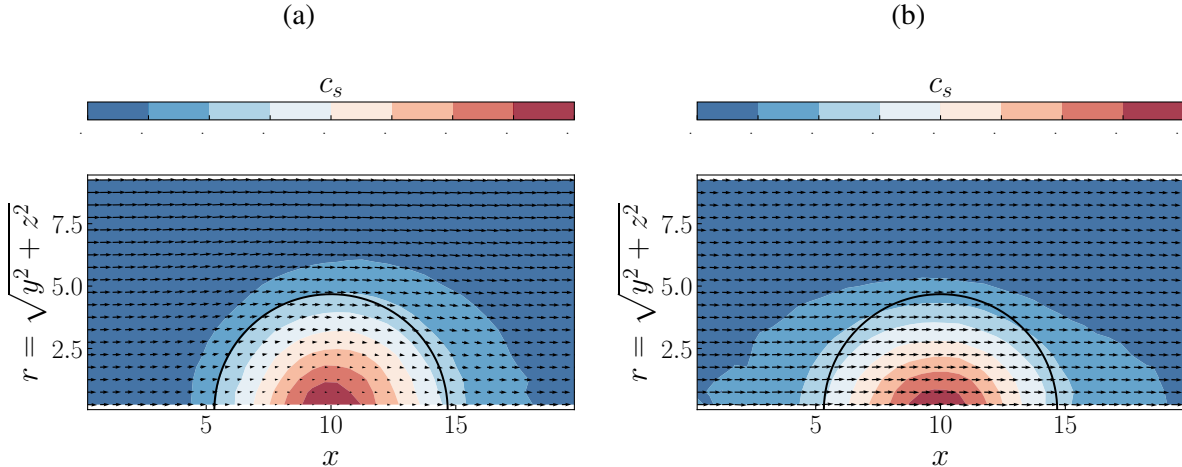


FIG. 6: Flow around a polymer coil. (a) when a body force is applied and (b) for the diffusiophoretic case. The velocity field is measured in a coordinate system moving with the center of mass of the polymer. The black semicircle shows the equivalent colloid and the contours show the solute concentration, for both cases $\epsilon_{ms} = 1.5$. The measurements were taken inside a cylinder with axis along the direction of the applied force passing through the center of mass of the polymer. The contours show the solute concentration c_s .

Shin *et al.* reported evidence for a similar absence of hydrodynamic screening in a dense plug of colloidal particles moving under the influence of diffusiophoresis³². Shin *et al.* argued that the difference in screening in the case of phoretic flow, as opposed to flow due to body forces or pressure gradients, could be attributed to the difference in the range of the hydrodynamic flow fields in these two cases ($\sim 1/r$) for body-forces and pressure driven flow, ($\sim 1/r^3$) of phoretically induced flows³³.

V. CONCLUSIONS

We have performed molecular dynamics simulation on the diffusiophoresis of polymers in a fluid mixture under the influence of a concentration gradient of solutes. In our non-equilibrium molecular dynamics simulation, we mimicked the effect of an explicit concentration gradient in the system by imposing equivalent microscopic forces on the solute, solvent and monomers. This approach allows us to use periodic boundary conditions and facilitates a systematic investigation

of diffusiophoresis. Our results reveal a non-monotonic relation between the diffusiophoretic mobility and the interaction strength between the polymer and the solute. The findings imply that, in the strong interaction regime, the phoretic mobility decreases with increasing monomer-solute interaction strength. This result can be understood by noting that solutes that are strongly bound to the polymer cannot contribute to diffusiophoresis. Furthermore, we have demonstrated that the diffusiophoretic mobility of a (short) polymer cannot be explained in terms of a model that assumes that polymers behave like colloids with the same hydrodynamic radius. Finally, we found effectively no screening of hydrodynamic flow inside a polymer moving due to diffusiophoresis, as opposed to what is observed in the case of a polymer that is moved through a fluid by an external force.

VI. SUPPLEMENTARY MATERIAL

In the supplementary material we show the concentration distribution of solvent, solute, and solution as a function of radial coordinate from the center of mass of the polymer for $\epsilon_{ms} = 1.5$. We discuss simulations of a single, fixed colloid in a concentration gradient, and finally we show the diffusiophoretic mobilities of the polymer Γ_{ps} vs the number of monomers in the polymer N_m and compare with theoretical predictions based on the Kirkwood approximation for the hydrodynamic radius.

VII. ACKNOWLEDGEMENTS

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VIII. DATA AVAILABILITY

The data that support the findings of this study are available from the corresponding author upon reasonable request.

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(Supplementary Material) Studying polymer diffusiophoresis with Non-Equilibrium Molecular Dynamics

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I. CONCENTRATION DISTRIBUTIONS

In Fig. 1 we show the concentration distribution measured from the center of mass of the polymer in the radial direction for $\epsilon_{ms} = 1.5$. The figure shows that for $r > 7\sigma_0$ the solution is unperturbed by the presence of the polymer. This also holds for all the ϵ_{ms} in the present study.

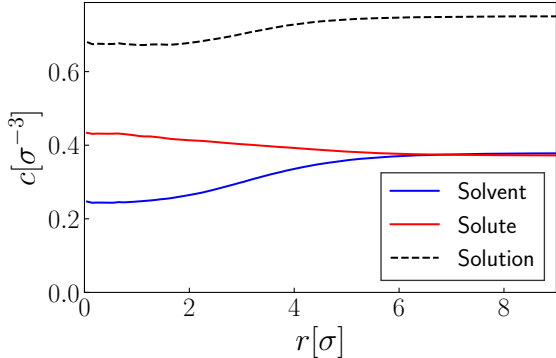


FIG. 1: Concentration of solvent, solute, and solution as a function of radial coordinate from the center of mass of the polymer for $\epsilon_{ms} = 1.5$.

II. COLLOIDAL SYSTEM SIMULATIONS

We performed simulations for a colloidal particle under the influence of both an explicit concentration gradient and the implicit method applying color forces. For the explicit system, the box size is (51.30 x 20.52 x 30.78) (in units of σ_0). A colloid was fixed in the center of the simulation box by placing a single Lennard-Jones particle with $\sigma_{cs} = \sigma_{cf} = 3.23 \sigma_0$, where the subscript c denotes the colloid. The solution has the same properties as those described in the main text. The concentration gradient was imposed by using two-particle reservoirs, with the concentration of solutes fixed at $0.6 \sigma^{-3}$ in the high concentration reservoir and $0.15 \sigma^{-3}$ in the low concentration one (see Fig. 2). The imposed concentration gradient is equivalent to $\nabla\mu_s \sim 0.06$ and is linear when there is no preferential interaction between the colloid and the solutes $\epsilon_{cs} = 1.0$. As soon as phoresis starts, the concentration gradient becomes non-linear (in fact, exponential) due to advection. As a result, the local concentration gradient at the location of the colloid is decreased (see also¹). The Péclet numbers for the solution in the bulk are shown in Fig 3

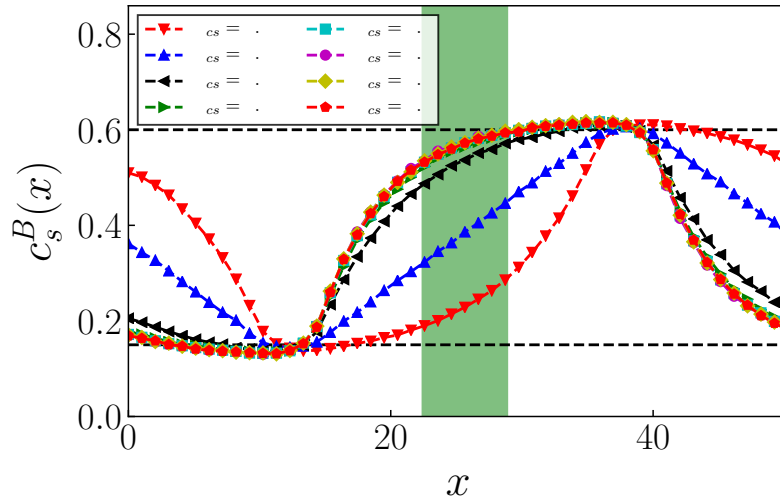


FIG. 2: Solute concentration profile in the case of a constant imposed concentration difference. The figure shows the results for difference phoretic flow velocities, corresponding to different values of ϵ_{cs} . We measure the concentration profiles at a lateral distance of at least 10σ from the colloid, where the colloid does not directly perturb the concentration profile. The shaded region represents the x position of the colloid and it is shown to emphasize the asymmetry in the concentration distribution created by advection.

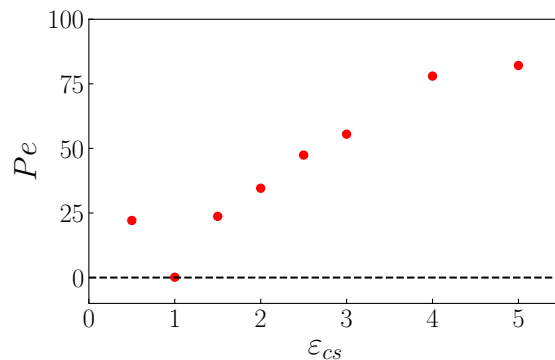


FIG. 3: Péclet number Pe for the diffusiophoretic flow with several colloid-solute interaction strengths ϵ_{cs} using explicit gradients. Note that, even for the smallest non-zero phoretic flow velocities $Pe > 20$.

For the implicit method, we used a simulation box ($20.52 \times 20.52 \times 30.78$) (in units of σ_0) with a colloid located in the center of the box. A snapshot of both systems is shown in Fig. 4

Note that the deformation of the concentration profile in figure (b) (colour forces) is barely visible. This observation illustrates the advantage of using colour forces rather than explicit gradients. In contrast, in Figure (a) (explicit gradient), the colloid is not in the center of the concentration profile (if it were, it would be at the red-blue boundary).

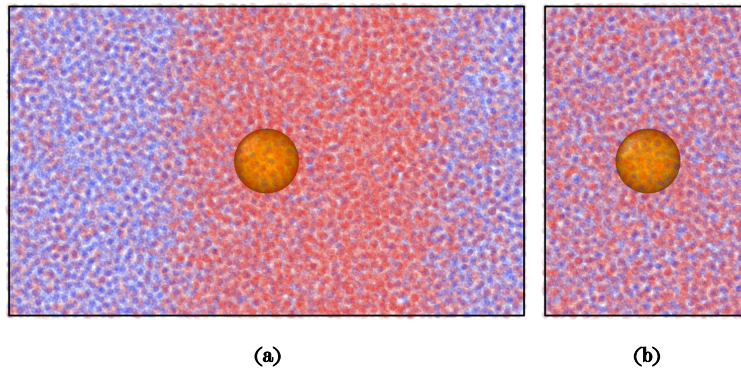


FIG. 4: Simulation boxes for (a) the explicit and (b) the implicit gradient systems

In Fig.5 we show the results obtained using the explicit and implicit gradients, together with the theoretical predictions using Anderson's theory including curvature corrections². The results show that the explicit method is only suitable for small phoretic effects (small gradients or small ϵ_{CS} as it is difficult to impose a linear gradient without using methods as described by Sharifi et al³ which artificially forces the concentration profile to be linear but at the expense of introducing (unphysical) sources/sinks of solute particles throughout the simulation box.

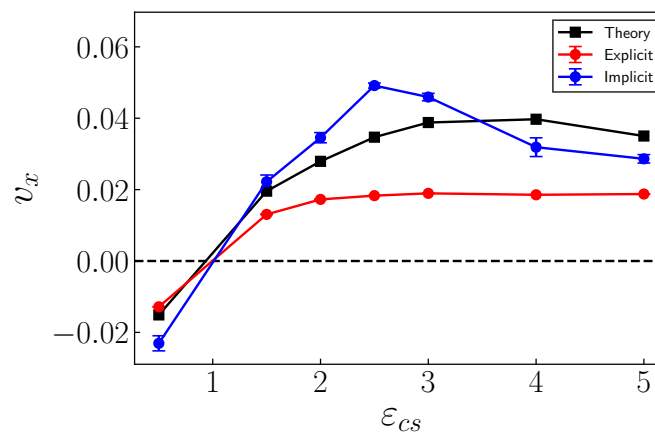


FIG. 5: Phoretic velocity v_x with several colloid-solute interaction strengths ϵ_{CS} obtained with explicit, implicit gradients and theoretical predictions.

To conclude, the advantages that the implicit gradient offers over the explicit gradient implementation are listed below:

- Allows simulating moving objects (polymers, colloids, etc) inside the concentration gradient. This would not be possible under periodic boundary conditions
- Only one parameter is required to change the chemical potential gradient, while in the explicit gradient method a new equilibrated system is required
- There is no overhead due to exchange movements
- The system size is considerably smaller
- The explicit gradient method is only efficient for small Péclet number, otherwise the concentration gradient is disturbed by flow advection

III. DIFFUSIOPHORETIC MOBILITIES USING THE KIRKWOOD APPROXIMATION FOR R_h

In Fig. 6, the simulation results are shown together with theoretical predictions replacing the polymer by an equivalent hard sphere with a radius $a = R_h$, with the hydrodynamic radius R_h given Kirkwood's approximation of R_h ⁴.

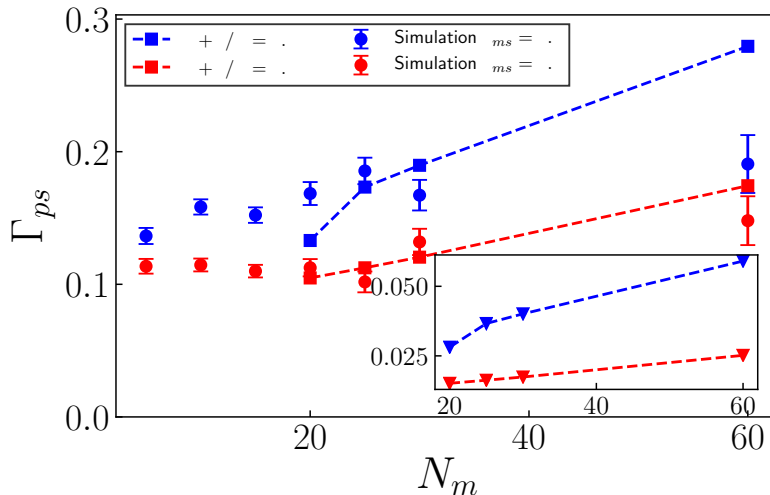


FIG. 6: Diffusiophoretic mobility Γ_{ps} of a polymer vs the number of monomers in the polymer N_m . The results are shown in red for $\epsilon_{ms}^{LJ} = 1.5$ and blue for $\epsilon_{ms}^{LJ} = 0.5$. The simulation results are presented as dots and the theoretical predictions using Anderson's prediction², including the correction due to the hydrodynamic slip, are shown as squares. The insert shows the theoretical predictions without the correction for hydrodynamic slip.

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