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► **To cite this version:**

Zhengwei Zhou, Mei Cong, Mengyao Li, Aura Tintaru, Jia Li, et al.. Negative dendritic effect on enzymatic hydrolysis of dendrimer conjugates. *Chemical Communications*, 2018, 54 (47), pp.5956 - 5959. 10.1039/c8cc01221k . hal-02992951

HAL Id: hal-02992951

<https://hal.science/hal-02992951>

Submitted on 6 Nov 2020

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ChemComm

Chemical Communications

rsc.li/chemcomm



ISSN 1359-7345



ROYAL SOCIETY
OF CHEMISTRY

COMMUNICATION

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Cite this: *Chem. Commun.*, 2018, **54**, 5956

Received 11th February 2018,
Accepted 3rd April 2018

DOI: 10.1039/c8cc01221k

rsc.li/chemcomm

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Dendrimers possess intriguing “dendritic effects”, which are unique characteristics that stem from the dendrimer generation and size. Here we report a “negative dendritic effect” observed during enzymatic hydrolysis of dendrimer conjugates. Such negative dendritic effects, though rarely reported, may be explored for tailored and generation-dependent drug release.

Drug delivery systems (DDSs) aim to improve drug bioavailability and facilitate controlled delivery of the drug to the disease lesion in order to maximize drug potency while minimizing toxicity.^{1–3} Dendrimers are emerging as promising DDSs because of their unique dendritic structure and multivalent cooperativity, which stem from their highly branched yet perfectly controllable architecture.^{4,5} Both physical encapsulation and chemical conjugation have been implemented for developing dendrimer-based DDSs in biomedical applications such as drug delivery, gene transfection, tissue engineering and imaging agents *etc.*^{6–13} We have been actively engaged in developing functional dendrimers as nanovectors for nucleic acid delivery,^{14,15} and we have recently established self-assembling amphiphilic dendrimer nanosystems to physically encapsulate drugs and nucleic acid molecules as innovative delivery platforms.^{16–19} Here, we report covalently conjugated amphiphilic dendrimers as drug delivery systems, with the aim of combining the advantages of multivalent dendrimers with stable drug loading. It is notable that, in addition to their well-known multivalent cooperativity, dendrimers also

possess intriguing properties called “dendritic effects”, *i.e.* the unique characteristics of dendrimers which stem from and are associated with their different generation level and size.^{20,21} These dendritic effects are not only observed for the dendrimers themselves, but also for the functions grafted onto them, which lead to different properties.^{21,22} Remarkably, DDSs created from our amphiphilic dendrimer conjugates had “negative dendritic effects” on enzymatic hydrolysis for the release of bioactive entities. We expect that these negative dendritic effects, which are seldom reported, can be further exploited for constructing tailored and controllable DDSs.

For the dendrimer conjugates studied in this work, we chose the triazole nucleoside analog **1** as the bioactive drug candidate because of its potent anticancer activity and novel mode of action in inhibiting heat shock factor 1 (HSF1) and androgen receptor expression.^{23,24} In addition, nucleoside analogues are an important class of drug candidate and have been used in pharmacologically diverse applications, including as antiviral, anticancer, antimicrobial and immuno-modulatory agents.²⁵ In the 2000s, Jacobson’s group reported the use of dendrimer-nucleoside conjugates to improve the affinity and selectivity of adenosine derivatives as adenosine receptor agonists by harnessing the multivalent properties of dendrimers.^{26–28} Recently, Sk *et al.* exploited the steric crowdedness of dendrimer terminals to prevent rapid degradation of the nucleoside anticancer drug cytarabine (Ara-C) *via* covalent conjugation to PAMAM dendrimer terminals.²⁹ Nevertheless, there is no report describing the conjugation of nucleoside analogues to amphiphilic dendrimers for drug delivery. In this work, we appended the nucleoside analogue **1** to the dendrimer terminals *via* biodegradable ester bonds with the aim of achieving drug release *via* enzymatic hydrolysis. Scheme 1A shows the enzymatic hydrolysis of a dendrimer conjugated with the nucleoside analogue **1**, while Scheme 1B shows the two dendrimers **I** and **II** described in this work.

The synthesis of the dendrimer conjugates **I** and **II** was achieved successfully *via* click chemistry using the alkynyl-bearing nucleoside analogue **2** and the corresponding azido-containing

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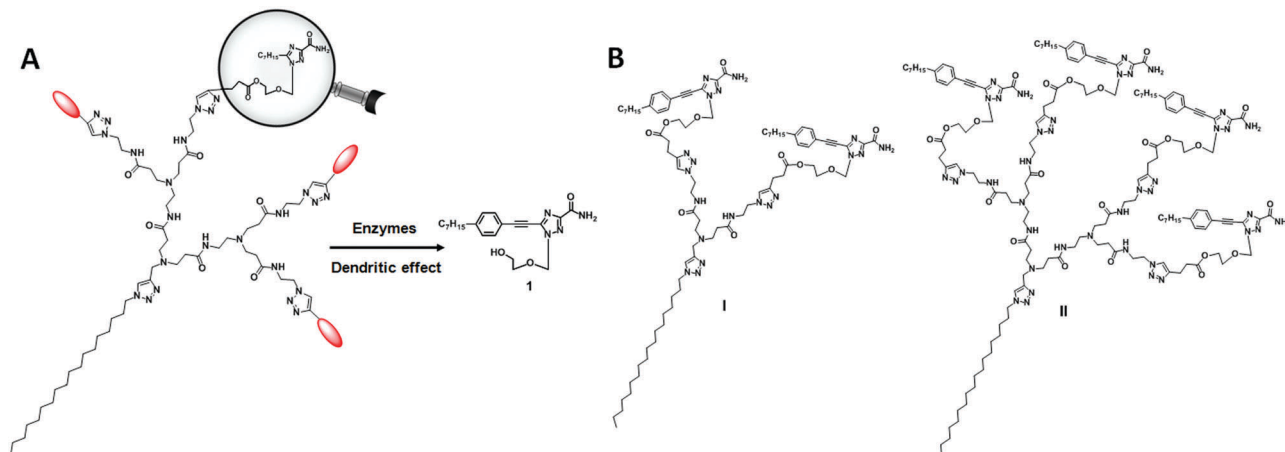
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† Electronic supplementary information (ESI) available. See DOI: 10.1039/c8cc01221k

‡ ZZ and MC contribute equally to this work.





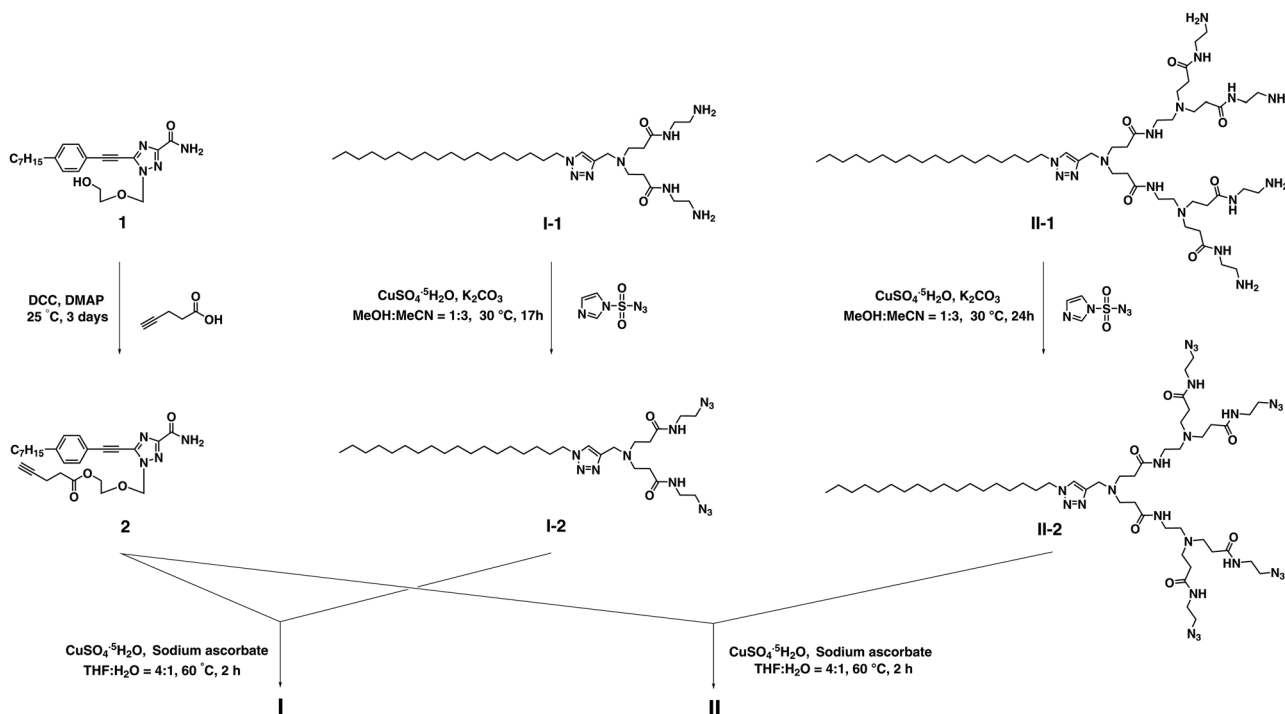
Scheme 1 (A) Cartoon illustration of the enzymatic release of the biologically active parent nucleoside analogue from the covalent dendrimer conjugate. (B) Structures of the nucleoside–dendrimer conjugates **I** and **II** studied in this work.

dendrimers **I-2** and **II-2** (Scheme 2 and Schemes S1, S2, ESI[†]). **2** was made through esterification of **1** with 4-pentynoic acid, whereas **I-2** and **II-2** were prepared starting with the respective amine-terminated dendrimers **I-1** and **II-1**³⁰ via diazo-transfer.³¹ For the synthesis of dendrimers **I** and **II**, it should be mentioned that a slight excess of **2** considerably suppressed the formation of unknown side-products during the Cu(I)-catalyzed Huisgen click reaction.

The chemical structure of both **I** and **II** was examined using ¹H- and ¹³C-NMR. Fig. 1A illustrates the ¹H-NMR spectra of **II** as an example. Compared to the precursor dendrimer **II-2**, the nucleoside–dendrimer conjugate **II** has new and characteristic ¹H-NMR signals (Fig. 1A), which can be ascribed to the

introduced 1,2,4-triazole nucleoside and the 1,2,3-triazole linkage. Likewise, the ¹³C-NMR spectrum of **II** (Fig. 1B) exhibits specific NMR signals belonging to the carbons in the triazole nucleoside component and the triazole connection, further supporting the chemical structures of **I** and **II**.

We also performed high-resolution mass spectrometry (MS) analysis of **I** and **II**. For **I**, the protonated species [**I+H**]⁺ was detected at *m/z* 1559.9 (Fig. 1C, top panel), while the ESI-MS spectrum of **II** (Fig. 1C, bottom panel) revealed the formation of double- and triple-protonated ions, observed at *m/z* 1499.9 and *m/z* 999.5, respectively. Further MS/MS analysis highlighted the characteristic structural features of the dendrimer conjugates (data not shown). Additionally, the elementary composition of



Scheme 2 Synthesis of the nucleoside–dendrimer conjugates **I** and **II** via click chemistry.



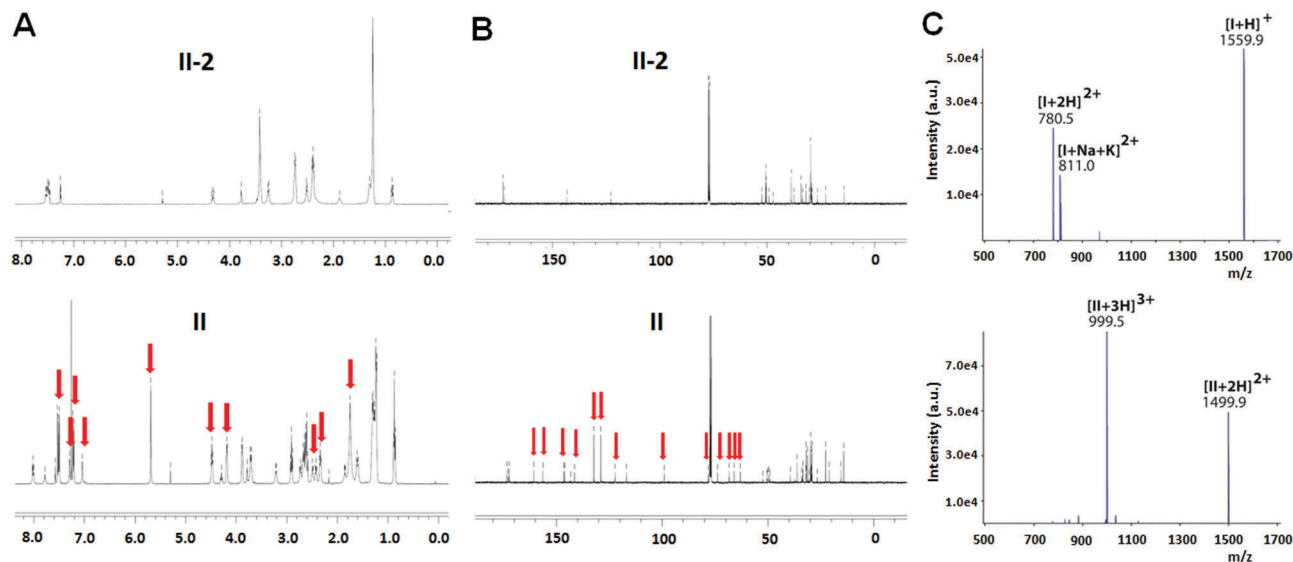


Fig. 1 (A) ^1H - and (B) ^{13}C -NMR characterization of the triazole nucleoside–dendrimer conjugate **II** in comparison with the azide-terminated dendrimer **II-2**. The red arrows indicate the NMR signals related to the triazole nucleoside and linker entities in **II**. (C) ESI-MS spectra of the dendrimer conjugates **I** (top) and **II** (bottom).

the dendrimer conjugates **I** and **II** was confirmed by detection of molecular ions at the expected values: $\text{C}_{83}\text{H}_{122}\text{N}_{20}\text{O}_{10}^{2+}$ for **I**, $((m/z)_{\text{th}} 780.4899, (m/z)_{\text{exp}} 780.4899, \text{error } +0.0 \text{ ppm})$ and $\text{C}_{155}\text{H}_{225}\text{N}_{40}\text{O}_{22}^{3+}$ for **II**, $((m/z)_{\text{th}} 999.5900, (m/z)_{\text{exp}} 999.5902, \text{error } +0.2 \text{ ppm})$, respectively.

Both **I** and **II** are not soluble in water, with CMC values being 26 and 15 μM respectively. Nevertheless, they are readily soluble in the co-solvent systems of water and organic solvents. They are also stable at both physiological pH 7.4 and acidic pH 5.0, and no release of the nucleoside analogue **1** was observed even after 2 days.

We then studied the release of **1** from **2**, **I** and **II** upon treatment with pig liver esterase (PLE) in fetal bovine serum (FBS) in the co-solvent system of DMSO/ H_2O (ESI $^+$). PLE is widely applied to hydrolyze a wide variety of esters including water-insoluble esters, and can be used in co-solvent systems of H_2O and organic solvents.³² Notably, the release of **1** from **2** was around 23% within 4 h, and this increased to 30% after 8 h (Fig. 2A). After 2 days, a total of 50% of **1** was released from **2**. This result illustrates the effective enzymatic hydrolysis of the ester linkage in **2** to deliver **1**. In contrast, the release of **1** from the dendrimer conjugate **I** was gradual and much slower than that from **2** (Fig. 2B). More remarkably, the release of **1** from the dendrimer conjugate **II** was dramatically reduced (Fig. 2C). Only around 10% of **1** was released after 2 days. The release rate of **1** from **II** is almost 2-fold slower than that from conjugate **I**, and around 5-fold slower than that from **2** at 4 h. This finding highlights that both **I** and **II** are much more resistant to enzymatic hydrolysis than **2** when releasing **1**. This can be ascribed to the steric crowding of the dendrimer–nucleoside terminals, which impeded the access of the enzyme and hence the cleavage of the ester linkage. Importantly, this generation-dependent dendritic effect is a negative dendritic effect, unlike the synergic and enhanced effects that are usually associated with dendrimers.²¹

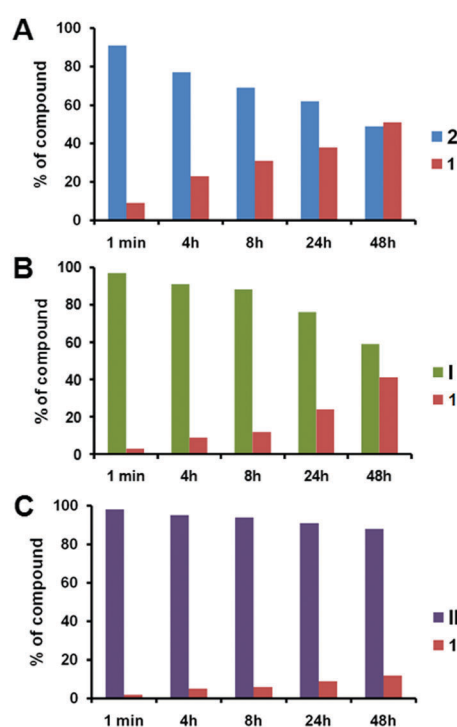


Fig. 2 Enzymatic release of triazole nucleoside **1** from (A) **2**, (B) **I** and (C) **II** in the presence of pig liver esterase in FBS.

As bond energy is one important descriptor of bond stability, we further estimated the bond energy for the ester linkages in **I**, **II** and **2**.^{33–35} The calculation results showed that the order of average bond energy of the ester linkage in **2**, **I** and **II** was $\Delta E_{\text{II}} > \Delta E_{\text{I}} > \Delta E_{\text{II}}$ (Table S2, ESI $^+$), indicating that the order of stability of the ester bond is $2 < \text{I} < \text{II}$. Taken together, these data provide a reasonable explanation for the slower release of **1** from **I** and **II** than from **2**, as well as the slower release from **II** than from **I**.



The negative dendritic effect is rarely reported in the literature and has been frequently ignored because it is often considered as uninteresting.²¹ Nevertheless, we think that it can be positively explored for drug delivery, because it can increase the stability of drug conjugates, hence allowing sustained drug release after accumulation of the conjugates in the disease lesion. For example, the covalent conjugation of the nucleoside anticancer drug cytarabine (Ara-C) to PAMAM dendrimer terminals prevented rapid metabolism and degradation of Ara-C.²⁹ This can also be considered as a negative dendritic effect. The increased stability resulting from the negative dendritic effect can be tailored to design generation-dependent dendrimer conjugates for controlled release.

In summary, we successfully prepared covalent dendrimer conjugates using click chemistry and studied the release of a bioactive entity from the conjugates during enzymatic hydrolysis of the ester linkage. Our results showed that the enzymatic hydrolysis of the dendrimer conjugates was greatly impacted by dendritic structure and dendrimer generation. Higher-generation dendrimers had considerably slower enzymatic hydrolysis. This negative yet interesting dendritic effect can be positively exploited to design and construct generation-dependent dendrimer conjugates with tailored stability for achieving controllable drug release. We believe that covalent chemical conjugation is a promising alternative strategy to enable controlled delivery of therapeutic agents, and we are working actively in this direction.

Financial support was from the National Natural Science Foundation of China (81502920, 21672251), the Chongqing Natural Science Foundation (cstc2015jcyjA10093), the Fundamental Research Funds for the Central Universities (106112017CDJQJ468823), the Instrumental Analysis Foundation of Chongqing University (201712150020), La Ligue Nationale Contre le Cancer (EL2016.LNCC/LPP) and the French National Research Agency under the frame of EuroNanoMed II (ANR-15-ENM2-0006-02, ANR-16-ENM2-0004-02). We thank Prof. Zhining Xia for HPLC assistance.

Conflicts of interest

There are no conflicts to declare.

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