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R. Soleri, H. Demey, S. A. Tria, A. Guiseppi-Elie, A. I. B. N. Had Hassine, et al.. Peptide conjugated chitosan foam as a novel approach for capture-purification and rapid detection of haptens - Example of ochratoxin A. *Biosensors & bioelectronics*, 2015, 67 (SI), pp.634-641. 10.1016/j.bios.2014.09.084 . hal-02914249

HAL Id: hal-02914249

<https://hal.science/hal-02914249>

Submitted on 4 Dec 2023

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Peptide conjugated chitosan foam as a novel approach for capture-purification and rapid detection of hapten – Example of ochratoxin A

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ABSTRACT

A novel bioassay for the detection and monitoring of Ochratoxin A (OTA), a natural carcinogenic mycotoxin produced by *Aspergillus* and *Penicillium* fungi, has been developed and applied for the screening of red wine. Here we report the immobilization and orientation of NOF4, a synthetic peptide, onto 3-D porous chitosan supports using a N-terminal histidine tag to allow binding to M^{++} ions that were previously adsorbed onto the high surface area biopolymer. Three divalent cations ($M^{++} = Zn^{++}, Co^{++}, Ni^{++}$) were evaluated and were found to adsorb via a Langmuir model and to have binding capacities in the order $Zn^{++} > Co^{++} > Ni^{++}$. Following Zn^{++} saturation and washing, C-terminus vs. the N-terminus His-tagged NOF4 was evaluated. At $1000 \mu\text{g L}^{-1}$ OTA the N-terminus immobilization was more efficient (2.5 times) in the capture of OTA. HRP labeled OTA was added to the antigen solutions (standards or samples) and together competitively incubated on biospecific chitosan foam. The chemiluminescence substrate luminol was then added and after 5 min of enzymatic reaction, light emission signals ($\lambda_{\text{max}} = 425 \text{ nm}$) were analyzed. Calibration curves of $\%B/B_0$ vs. OTA concentration in PBS showed that half-inhibition occurred at $1.17 \mu\text{g L}^{-1}$, allowing a range of discrimination of 0.25 and $25 \mu\text{g L}^{-1}$. In red wine, the minimum concentration of OTA that the system can detect was $0.5 \mu\text{g L}^{-1}$ and could detect up to $5 \mu\text{g L}^{-1}$. Assay validation was performed against immunoaffinity column (IAC) tandem reversed-phase high pressure liquid chromatography with fluorescence detection (HPLC-FLD) and provided quite good agreement. The association of chitosan foam and specific peptide represents a new approach with potential for both purification-concentration and detection of small molecules. In the future this assay will be implemented in a solid-state bioelectronic format.

Keywords:

Ochratoxin A
Immunoassay
Chitosan
Peptides
NOF4
Wine

1. Introduction

Haptens are low molecular weight chemicals that comprise a major percentage of the universe of pesticides, herbicides, toxins, metals or allergens. Haptens then are small molecules that can elicit an immune response only when attached to a large carrier such as a protein; the carrier may be one that, by itself, also does not elicit an immune response. Therefore, it is very difficult to obtain affine antibodies to such molecules. Moreover, there has been increasing demands for ultrasensitive detection for these small target analytes that can potentially induce disease. This mycotoxin, Ochratoxin A, (a secondary fungal metabolite produced mainly by several *Aspergillus ochraceus* and *Penicillium verrucosum*) is a powerful nephrotoxic, teratogenic, immunosuppressive agent that has been implicated as an endocrine disruptor as well as a

contributor to increased cancer risk. The International Agency for Research on Cancer (IARC) has classified OTA in Group 2B (possibly carcinogenic agent). OTA is mainly found in improperly stored foods such as cereals, dried fruit, nuts, and beverages such as beers and wine (Blesa et al., 2004a; Varga and Kozakiewicz, 2006; Zimmerli and Dick, 1995). Several authors have already reviewed wine contamination by OTA (Blesa et al., 2004b; Varga and Kozakiewicz, 2006). Wine is a major source of daily OTA intake for the population as it is widely consumed (Jørgensen, 2005). A level of $2 \mu\text{g kg}^{-1}$ of OTA in wines has been established by the Regulatory Commission of the European Community (European Commission Commission Regulation, 2005; European Commission Regulation, 2010).

There is a standardized method for the determination of this mycotoxin in food matrices (Lerda, 2011); however, food and beverage producers are constantly looking for simple, less expensive and faster bioanalytical solutions. Indeed, validated standard methods for the detection of OTA are based on chromatographic

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techniques with fluorescence detection due to the fact that OTA possesses natural fluorescence (Sofie et al., 2010; Tessini et al., 2010; Aresta et al., 2006; Visconti et al., 1999). However, recent studies have proposed new lower cost assays with higher rapidity and sensitivity compared to the methods already on the market (Nasir and Pumera, 2014). These assays belong to three broad classes of analytical techniques: enzyme linked immunosorbent assays (ELISAs), test strips and biosensors.

First, OTA detection has been widely done by competitive ELISA in the past few years. Morgan et al. (1986), reported an assay in barley. Later, the sensitivity of this assay in barley samples was ca. $5 \mu\text{g kg}^{-1}$ (Ramakrishna et al., 1990). Second, immunochromatographic strip (ICS) or the test strip, also called lateral flow device based on immobilized antibodies on a membrane, has also been used for the detection of OTA. These are semi-quantitative and give faster results (2–15 min) than ELISA assays (ca. 30–40 min). Test strips display different visual limits of detection (LOD) as a function of the nature of the sample (Krska and Molinelli, 2009; Shim et al., 2009). The LOD was initially set at ca. $500 \mu\text{g L}^{-1}$ of OTA (Cho et al., 2005; Rusanova et al., 2009), but, nowadays, the Food and Drugs Administration has allowed a maximum of $1 \mu\text{g L}^{-1}$, so the cutoff level was dropped down this the lower limit. Finally, immuno-biosensors are the last technique used to detect OTA in various samples, but their efficiency depends of the nature of the bioreceptor and biotransducer. A variety of immuno-biosensors were developed (e.g. electrochemical, impedimetric or conductimetric immunosensors) against mycotoxins like OTA (Alarcón et al., 2006; Liu et al., 2009; Prieto-Simón et al., 2008; Radi et al., 2009a, 2009b). Indeed, antibodies show high selectivity and affinity towards mycotoxins and so are configured into immuno-biosensors.

The use of antibodies in a detection system has some advantages (high affinity and selectivity) but also several major disadvantages depending the different sample matrix or experimental conditions of the assay. Among the disadvantages are denaturation and loss of structure-based activity in organic solvents, elevated temperatures or increased ionic strength. To overcome these drawbacks, diverse strategies have emerged. Alternatives to the use of OTA antibodies are being developed, including molecularly imprinted polymers (MIP) (Ali et al., 2010; Yu and Lai, 2010), peptides from phage display libraries (Giraudi et al., 2007) and DNA aptamers (Cruz-Aguado and Penner, 2008a, 2008b). DNA aptamers and synthetic receptor(s) (MIP) have some advantages compared to antibodies for the recognition of target molecules (He et al., 2013, 2012; Ma et al., 2013). We previously introduced a novel approach based on a peptide-based enzyme-linked immunosorbent assay (peptide-based ELISA) (Bazin et al., 2013). We have shown that the NOF4 peptide allowed the detection of OTA in red wine in a sensitive manner. The use of peptides for the development of biosensors offers a number of attractive benefits. Peptides represent the simplest biological recognition elements for binding of some small molecules. There are examples of highly selective metal-binding peptide motifs available from the protein literature (Chow et al., 2005), for the recognition of OTA (Giraudi et al., 2007) and very recently for the binding of BPA (Yang et al., 2014). Chitosan is the second most abundant biopolymer on Earth and its ability in the sorption of divalent metal ions from aqueous solutions has been widely demonstrated; different authors have reported that chitosan is an effective low-cost sorbent due to its easy availability (Demey et al., 2014).

In the present study, we report a new bioanalytical format for the peptide-based ELISA assay. This new format allows the rapid capture, concentration and detection of hapten molecules such as OTA using NOF4. (Fig. SM1, Supplemental materials). The histidine tagged labeled peptide was immobilized and oriented on chitosan foam through adsorbed divalent zinc ions. Following washing step,

OTA-HRP conjugate was added to antigen containing buffer solutions or wine samples and chemiluminescence was measured. As this approach is based on a competitive ELISA format, the concentration of antigen is inversely proportional to the chemiluminescence light intensity measured.

2. Material and methods

2.1. Materials and chemicals

Solutions of metal ions were prepared from $\text{ZnSO}_4 \cdot 6\text{H}_2\text{O}$; $\text{CoCl}_2 \cdot 6\text{H}_2\text{O}$ and $\text{Ni}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$ reagents provided by Panreac (France). Chitosan was supplied by Aber Technologies (France) and its molecular weight ($125,000 \text{ g mol}^{-1}$) determined using size exclusion chromatography (SEC) coupled with light scattering and refractometry was previously reported (Ruiz et al., 2001). The degree of deacetylation, determined by Fourier Transform infrared (FTIR) spectroscopy, was found to be 87% (Guibal et al., 1999). OTA was obtained from Sigma-Aldrich (France) from which a solution was prepared (1 mg ml^{-1}) in methanol at RT. Polyethylene glycol (PEG8000) and polyvinylpyrrolidone (PVPP) were obtained from Promega (France). Luminol was obtained from Pierce (France) and the peptide, NOF4, was synthesized by Smartox (France).

2.2. Preparation of chitosan adsorbent and chitosan foam

Chitosan foam, which served as a support for the immobilized NOF4 peptide, was prepared by dissolving chitosan to a final concentration of 2% (w/w) in 2% aqueous acetic acid solution under continuous agitation. The solution was poured into cylindrical molds (6 mm diameter/ height varies from 1 mm to 10 mm) and frozen for 3 h at 193 K. Then, the frozen solution was freeze-dried during 24 h (using a freeze-dryer Fisher Bioblock Scientific, France) at 223 K and 0.01 mbar. The resulting foam was put in contact with 1 M NaOH solution for 4 h and then was rinsed sequentially with 98% (w/w) and 50% (w/w) ethanol/water solution until pH 7. The resulting chitosan foam was used as sorbent of divalent metal ions (Zn^{+2} , Ni^{+2} , Co^{+2}).

2.3. Equilibrium sorption

In this work, the effectiveness of the chitosan foam to serve as a support for the immobilization of NOF4 via chelation with divalent metal ions was evaluated. In order to provide a material that was easy to handle, the metal ions Zn^{+2} , Co^{+2} and Ni^{+2} were separately introduced to the polymeric matrix of chitosan using a batch sorption system. The ability of chitosan to strongly interact with divalent metal ions through primary amine groups is well documented (Wan et al., 2010). Mono-component isotherms were obtained by mixing 0.2 g of sorbent (chitosan foam) at room temperature (20 °C) with a constant volume (0.2 L) of aqueous metal ion solution (Zn^{+2} , Co^{+2} and Ni^{+2}) at different concentrations (ranging from 50 to 6000 mg L^{-1}). The pH of the solutions was adjusted to 5.0 with a buffer solution (consisting of sodium acetate). After 72 h of agitation, the residual metals concentration was analyzed with an Inductively Coupled Plasma Atomic Emission Spectrometer ICP-AES (HORIBA JOBIN YVON, France) at the wavelength 221.6 nm for Ni^{+2} , 238.8 nm for Co^{+2} , and 213.8 nm for Zn^{+2} .

The Langmuir and Freundlich models were used to describe the experimental adsorption isotherm data. These models are represented by the following equations, respectively (Freundlich, 1906; Langmuir, 1918):

$$q = \frac{q_{\max} b C_e}{1 + b C_e} \quad (1)$$

$$q = K_F C_e^{1/n} \quad (2)$$

where q is the amount of metal adsorbed per gram of sorbent at equilibrium (mg g^{-1}), q_{\max} is the maximum adsorption capacity of the adsorbent (mg g^{-1}), and C_e is the equilibrium concentration of the solution (mg L^{-1}). In the Langmuir model (Eq. (1)), b is related to the energy of adsorption (L mg^{-1}), whereas K_F and n are the Freundlich adsorption constants, indicative of the relative capacity and the adsorption intensity, respectively.

2.4. Influence of contact time

The uptake kinetics experiment was performed by adding (under continuous stirring) a known amount of adsorbent (i.e., 0.2 g) to 200 mL of aqueous metal ion solution (200 mg L^{-1} , 600 mg L^{-1} and 900 mg L^{-1}) at pH 5. Aliquots of adsorbate (aqueous metal ion solution) were withdrawn at different times and filtered after 120 h of contact. The residual concentration was determined by ICP-AES. The kinetic profiles were compared for sorption of Ni^{+2} and Zn^{+2} ions. The intraparticle diffusion equation (Namasivayam and Yamuna, 1995) and the pseudo-first and pseudo-second order model were applied to fit the experimental data. These models are frequently used to describe the batch sorption system:

Pseudo-first order rate equation (PFORE) (Lagergreen, 1898):

$$\frac{dq_t}{dt} = K_1(q_1 - q_t) \quad (3)$$

Integrating for the boundary conditions $t=0$ to $t=t$ and $q_t = 0$ to $q_t = q_t$:

$$\log(q_{\text{eq}} - q_t) = \log(q_{\text{eq}}) - \frac{K_1}{2.303} t \quad (4)$$

Pseudo-second order rate equation (PSORE) (Ho and McKay, 1998):

$$\frac{dq_t}{(q_{\text{eq}} - q_t)^2} = K_2 dt \quad (5)$$

Integrating for the boundary conditions $t=0$ to $t=t$ and $q_t = 0$ to $q_t = q_t$:

$$\frac{1}{q_t} = \frac{1}{K_2 q_{\text{eq}}^2} + \frac{1}{q_{\text{eq}}} t \quad (6)$$

where q_{eq} is the equilibrium sorption capacity (mg g^{-1}), q_t is the sorption capacity (mg g^{-1}) at any time t (h) and k_2 is the pseudo-second order rate constant ($\text{g mg}^{-1} \text{ h}^{-1}$). The parameters q_{eq} and k_2 are pseudo-constants depending on the experimental conditions.

The intraparticle diffusion equation is (Namasivayam and Yamuna, 1995)

$$q_t = K_p t^{1/2} + C \quad (7)$$

where C is the intercept, and K_p is the intraparticle diffusion rate constant.

2.5. Peptide-based competitive enzyme-linked immunosorbent assay (peptide-based competitive ELISA) on chitosan foam

After washing with PBS, foam supports were placed in zinc solution overnight at 20°C . Foam were then coated with the synthetic peptide NFO4 in azide containing carbonate buffered ($15 \text{ mM Na}_2\text{CO}_3$, 35 mM NaHCO_3 , $0.2 \text{ g L}^{-1} \text{ NaN}_3$, pH 9.6) and were incubated in 96-well plates at 37°C for 3 h. Non-specific binding

sites of the peptide-coated foam were blocked with casein solution at room temperature (RT) for 3 h before performing the immobilization. OTA-HRP (horseradish peroxidase) conjugate was added to each well in combination with phosphate buffer saline (control) or red wine sample supplemented with unlabeled OTA. The reaction was left for 30 min at 4°C . After washing unbound OTA, $40 \mu\text{L}$ of luminol-hydrogen peroxide (Pierce, France) substrate was added to each well. After 5 min of enzymatic reaction, light emission signals ($\lambda_{\max}=425 \text{ nm}$) were analyzed using an automated microplate luminescence reader (Berthold, France). Light intensity was expressed in Relative Luminescent Unit (RLU). The results obtained were inversely proportional to the concentration of unlabeled OTA. During each test, nonspecific binding (negative control) was determined by using an incubation mixture (OTA-HRP) in which the peptide NFO4 was replaced by $100 \mu\text{L}$ of PBS buffer. Total analysis time per sample was ca. 40 min. All the samples were tested in triplicate and the mean of the peak light emission was taken as the final light signal value. Each point is the average \pm standard deviation of three independent assays each with 4 measurements.

2.6. Calculation methods

In order to evaluate the peptide-based competitive assay, a calibration curve was established by using solutions containing well-defined concentrations of OTA. In direct competitive peptide-based ELISA, results are expressed in B/B_0 dose logarithmic function. B and B_0 represent the enzyme-bound activity measured in the presence or absence of competitor, respectively. The standard curve was traced by plotting standard concentrations on x -axis (logarithmic scale) and percentage of maximal binding (express in % of B/B_0) on y -axis ($B/B_0 = f(\log [\text{OTA}])$). The binding values were obtained by dividing the light intensity of each testing well B (the luminescence measured when OTA-HRP and unlabeled OTA are in competition with NFO4 peptide) by the light intensity of the positive control well, B_0 (maximum luminescence obtained with OTA-HRP). This method allows the comparison of results between assays performed on different plates or on different days. While the absolute light emission may differ from plate to plate or day to day, the percentage of B/B_0 values are expected to be consistent from one plate to the next. All measurements were made in triplicate. A decreasing exponential function ($y = y_0 + Ae^{-R_0 x}$) was performed on the standard curve $B/B_0 = f(\log [\text{OTA}])$ by using Origin Lab software. The limit of detection (LOD) was obtain from the equation for $y=A$, the maximum with $y=y_0$ and IC_{50} with $y=50$.

2.7. Preparation of matrix samples for peptide ELISA: wine pretreatment

In order to study matrix-associated effects, a study with red wine was carried out. A sample of 10 ml of wine supplemented (or not) with OTA (1.25 to $15 \mu\text{g L}^{-1}$) (standard addition technique), was diluted with 10 mL of PEG8000 1%- NaHCO_3 5% solution. This mixture was incubated for 30 min at RT on a rocker. Afterwards, it was centrifuged at 8000 rpm for 15 min. The whole sample was filtered before analysis with the peptide-based enzyme-linked immunosorbent assay.

3. Results and discussion

3.1. Equilibrium studies for metal ion adsorption

Adsorption isotherms describe the distribution of the metal ions between the liquid and the solid phases at equilibrium. Fig. 1 compares the sorption isotherms for the three candidate ions at

pH=5. The curves are characterised by the appearance of a saturation plateau at high metal ion concentration. The initial slopes are very steep, indicating that the affinity of the sorbent for metal ions is very strong. Langmuir and Freundlich models were tested. The Langmuir equation provided a better fit of the experimental data ($0.852 < R^2 < 0.959$) than did the Freundlich equation ($0.835 < R^2 < 0.952$) (Table SM1); nevertheless both models were found to adequately fit the experimental results. The removal uptake follows this order: $Zn^{+2} > Co^{+2} > Ni^{+2}$ and the maximum sorption capacity reached 230.3 mg g^{-1} for Zn^{+2} , 87.3 mg g^{-1} for Co^{+2} and 62.0 mg g^{-1} for Ni^{+2} ; the molar ratio between metals and chitosan was determined as the ratio between the maximum amount of adsorbed metal (mol) and the mass of chitosan (mol) used to plot the isotherms. The corresponding value for Zn^{+2} , Co^{+2} and Ni^{+2} was found to be $440 \text{ mol}_{Zn(II)}(\text{mol}_{\text{chitosan}})^{-1}$, $185 \text{ mol}_{Co(II)}(\text{mol}_{\text{chitosan}})^{-1}$ and $132 \text{ mol}_{Ni(II)}(\text{mol}_{\text{chitosan}})^{-1}$ respectively. These results are consistent with previously reported results (Juang and Shao, 2002; Monier et al., 2010) and the sorption capacities are of the same order of magnitude.

Adsorption of heavy metals by raw and chemically modified chitosan materials has been widely studied (Guibal Milot and Tobin, 1998; Huang et al., 1996; Juang and Shao, 2002). Different processes such as adsorption, ion-exchange and chelation have been reported as the mechanisms responsible for complex formation between chitosan and metal ions; nevertheless, the type of interaction depends on the metal and on the pH of the solution (Vold et al., 2003). Ghaee et al. (2012) have reported the sorption mechanism of nickel ions on porous chitosan membrane as the combination of chelation and electrostatic adsorption; amino ($-NH_2$) and/or hydroxy groups serve as coordination sites (Wan et al., 2010). Juang and Shao (Juang and Shao, 2002) also pointed that the uptake of transition metals is performed via coordination with $-NH_2$ groups on chitosan. The possible reaction between amino groups and metal ions in this study are:



As shown in Fig. SM2, the sorption capacity for Zn^{+2} increased even at high metal concentrations; Juang and Shao (2002) attributed this increase to the possibility of a micro-precipitation of metals at the vicinity of adsorbent particles, as a result of very small change of the pH. Parameter R_L (Eq. 11), defined as a dimensionless separation factor, was used by Demey et al. (2014) to determine if an isotherm is favorable or unfavorable:

$$R_L = \frac{1}{1 + bC_0} \quad (11)$$

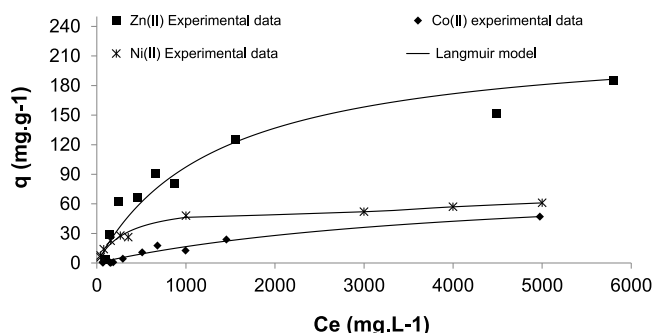


Fig. 1. Sorption of divalent metal ions; sorption mono-component isotherms for Zn (II), Co(II) and Ni(II).

where b is the Langmuir constant ($L \text{ mg}^{-1}$). According to Öztürk and Kavak [(Öztürk and Kavak, 2005)], the value of R_L characterises the shape of the isotherm: $R_L=1$ Linear; $R_L > 1$ Unfavorable; $0 < R_L < 1$ Favorable; $R_L=0$ Irreversible. The value of R_L calculated using Eq. (11) indicated that metal ion adsorption using chitosan foam is favorable (at 20°C) for a metal ion concentration of 100 mg L^{-1} (Table SM1).

3.2. Influence of contact time

Fig. SM2 shows the kinetic profile for the adsorption of Zn^{+2} and Ni^{+2} using chitosan foam as adsorbent at different initial metal concentrations; all of the plots have similar trend. Two steps can be observed; an initial fast sorption followed by a slow-rate step when approaching the equilibrium. As expected, the metal ion concentration influences the adsorption capacity at equilibrium and eventually the kinetic profile. The initial section of the kinetic profile usually governed by the resistance to ion diffusion (Demey et al., 2014) changes significantly in the case of both metals (Zn^{+2} and Ni^{+2}); increasing the concentration, the slope of this section becomes steeper. The final section usually governed by the resistance to film diffusion (Demey et al., 2014) is also affected; sorption capacity tends to be lower with decreasing metal concentration (Table SM2). As proposed by Demey et al. (2014), this can be due to the decrease of the concentration gradient between the solution and the surface of the sorbent, and between the surface of the sorbent and the core of the sorbent. As a result, the driving force decreased as well as the sorption rate.

The experimental results can be fitted by PFORE (pseudo-first order) and PSORE (pseudo-second order) models (Table SM2); the correlation coefficients for both models are similar. Fig. SM3 shows the linear plot obtained from Eq. (7); as it can see, it does not pass through the origin, verifying that intraparticle diffusion is not the unique step that controls the metal uptake kinetics. Increasing the initial concentration of metals increases the intraparticle diffusion rate constant.

3.3. Specific assembly with 6His-tagged protein

Despite advances, peptide/protein assembly onto surfaces remains challenging. Here, we report a method to assemble His-tagged peptide to chitosan membrane using the divalent metal ion, Zn^{+2} . Specific assembly with 6His-tagged protein or peptide was performed using two proteins: 6His-tagged GFP and non-His-tagged GFP. The ability to bind histidine tagged proteins was tested with various metal ions (Fig. 2). On one hand, for all divalent metal ions tested, we can see that in the presence of GFP without 6-histidine tag there is no adsorption and hence no fluorescence of the chitosan foam was observed. Interestingly, this confirms that there is little to no non-specific adsorption of proteins, such as GFP, to chitosan foam. The fluorescence level was similar to that of the negative control (chitosan saturated with divalent metals and without GFP). However, we observe a high level of fluorescence in the presence of the GFP containing a 6-histidine tag. This result is observed regardless of the metal used. But, the highest level of fluorescence was observed when the chitosan was saturated with zinc metal ions, consistent with the results obtained from isotherm calculations and loading capacity calculations. These results had been confirmed by chemiluminescence detection (on the same chitosan sorbent) by using a primary GFP antibody (rabbit) and a secondary anti-rabbit antibody HRP labeled (data not show). These data demonstrate that there exists specific binding of a 6-histidine tagged protein on chitosan foam saturated with divalent metal. The maximum sorption capacity was best for zinc metal ions and so

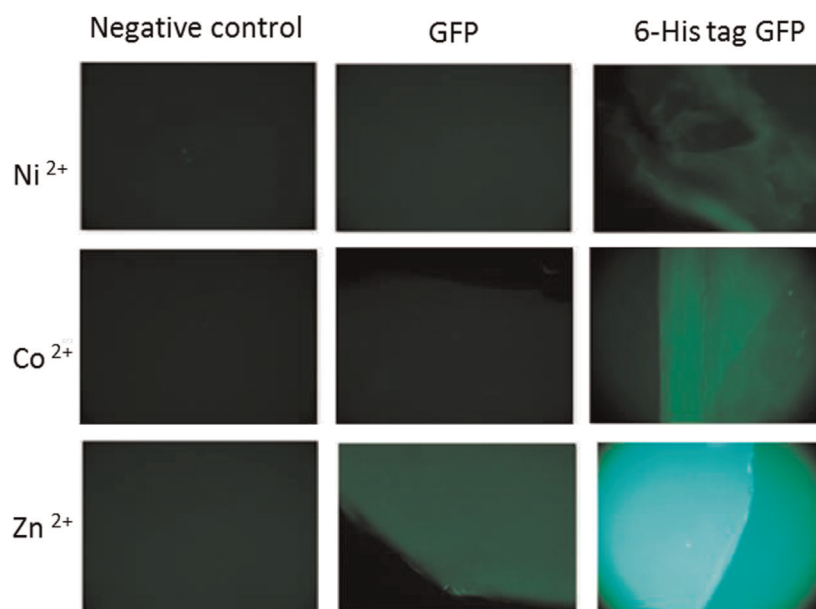


Fig. 2. Fluorescent microscopy images of chitosan foam.

the binding of the 6-histidine tagged protein was likewise better with this metal ion.

3.4. Optimization of ochratoxin A detection

To develop a reliable tool for OTA detection based on peptide competitive ELISA, different parameters should be optimized, including the immobilized peptide orientation and concentration, the volume of chitosan foam and the dilution factor of the OTA-HRP label.

3.4.1. Influence of the orientation of the peptide NFO4 on OTA-HRP detection

For this new approach of OTA detection, we use a peptide (NFO4), modified with and immobilized via 6-histidine tag onto Zn^{2+} loaded chitosan foam. The immobilization of this peptide can be achieved at the N-terminal or C-terminal extremity, leading to a binding to the OTA by the opposite extremity. To optimize the recognition of the toxin, we first tested the orientation of the peptide on the chitosan foam. The peptide was histidine tagged at the N-terminal or C-terminal extremity and immobilized through divalent zinc ion adsorbed on chitosan foam (Fig. 3a). The construct was evaluated using varying concentrations of OTA-HRP conjugate. For a concentration of $166.6 \mu\text{g L}^{-1}$ we could not discriminate the control (3600 ± 530 RLU) from the C-terminus ($11,820 \pm 6650$ RLU) and N-terminus ($25,440 \pm 11,600$ RLU) immobilized NFO4. For 250 and $500 \mu\text{g L}^{-1}$, we can clearly see a difference between the control (5220 ± 1410 RLU and $11,920 \pm 3840$ RLU) and the presence of peptide, but no difference was observed between the two peptide orientations; C-terminus ($112,540 \pm 40,460$ RLU and $97,540 \pm 43,800$ RLU) or N-terminus ($88,020 \pm 31,190$ RLU and $69,410 \pm 19,570$ RLU). While, in the case of $1000 \mu\text{g L}^{-1}$ OTA-HRP conjugate, the recognition by the N terminus is close to 2.5 times that of the C-terminus (respectively $611,850 \pm 21,028$ RLU and $251,160 \pm 78,380$ RLU). For all of the subsequent optimization steps, the NFO4 peptide oriented with N-terminus his-tag modification was used as the recognition element.

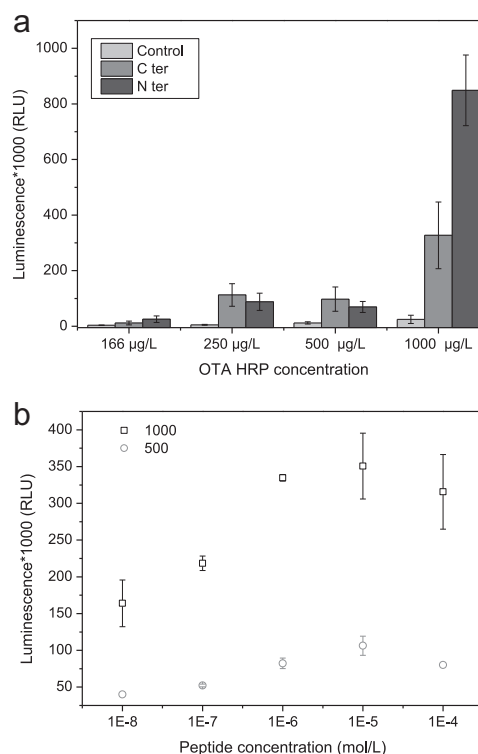


Fig. 3. Optimization of peptide ELISA based on chitosan foam parameters: (a) Influence of the orientation of the peptide NFO4. Peptide-based competitive ELISA assays for the detection of OTA in PBS on chitosan foam. The negative control is the luminescence emitted with OTA-HRP without NFO4 peptide. Each point are the average \pm standard deviation of four assays, each of triplicate measurement ($n=12$). (b) Optimization of peptide NFO4 concentrations and OTA-HRP concentration. ELISA type assays carried out on chitosan foam for different peptide NFO4 concentration and an OTA-HRP concentration at $1000 \mu\text{g L}^{-1}$ (rectangle) or $500 \mu\text{g L}^{-1}$ (circle). Each point is the average \pm standard deviation of three independent essays each with 4 measurement ($n=12$).

3.4.2. Optimization of peptide NFO4 and OTA-HRP labeled concentration.

The optimal concentration of NFO4 peptide and OTA-HRP were then determined by ELISA assay. Different concentrations of peptide were prepared in carbonate buffer and ELISA assays were carried out with a concentration of OTA HRP at $500 \mu\text{g L}^{-1}$ or $1000 \mu\text{g L}^{-1}$. When OTA-HRP was used at a concentration of $1000 \mu\text{g L}^{-1}$, responses were always higher compared to the OTA-HRP concentration at $500 \mu\text{g L}^{-1}$ and the responses obtained at different NFO4 concentrations can be clearly discriminated (Fig. 3b). However, when $500 \mu\text{g L}^{-1}$ OTA HRP was used the resulting luminescence results were in the same range. Therefore, the OTA-HRP concentration at $1000 \mu\text{g L}^{-1}$ was chosen for all subsequent experiments. Concerning the peptide concentration, we can see a response increase with the increase of peptide concentration up to $10^{-6} \text{ mol L}^{-1}$, followed by a decrease of the signal known as hook effect (Agarwal et al., 2010). In order to obtain a maximum response while avoiding the hook effect, a concentration of $10^{-6} \text{ mol L}^{-1}$ of peptide was chosen for subsequent experiments.

3.4.3. Optimization of chitosan foam volume

To develop this new detection system, we produced porous chitosan foam to serve as the immune-support. Depending on the volume used, various chitosan foams (Fig. 4a) were fabricated. With small volumes were created thick slices of chitosan foam and with larger volumes, large disks or tubes. Analysis of foams by SEM showed the developed materials to be highly porous and to present a large exchange surface. As the aim of this project was to develop reliable tools for the detection of haptens, this requires a format that can be produced on a large scale and also allow multiple measurements. For these reasons the slice format was chosen. We then investigated the effect of chitosan foam slice volume on the luminescence obtained with a peptide concentration of $10^{-6} \mu\text{g} \cdot \text{L}^{-1}$ and OTA-HRP concentration of $1000 \mu\text{g L}^{-1}$. As shown on Fig. 4c, the use of foam ranging from 10 to $70 \mu\text{L}$ gave the same luminescence intensity while a clear increase of the signal was obtained with higher volumes ranging from $80-100 \mu\text{L}$. To achieve a better sensitivity, foam of $100 \mu\text{L}$ are chosen for the detection of OTA in the subsequent experiments.

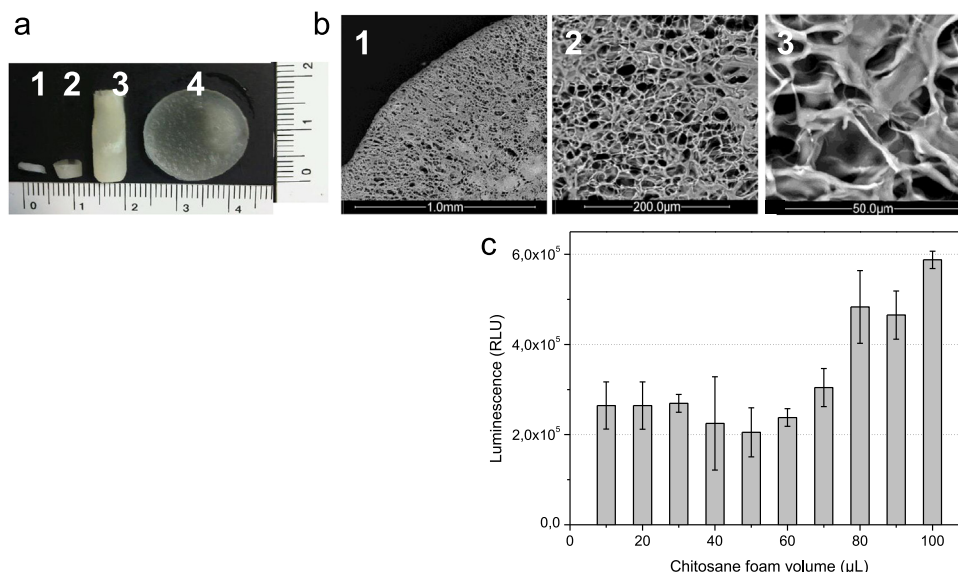


Fig. 4. Optimization of chitosan foam volume. a. Various production of chitosan foam. 1. foam of $30 \mu\text{L}$; 2. foam of $100 \mu\text{L}$; 3 and 4 foam of 1 mL ; b. SEM images of chitosan foam at different magnification 1. $\times 50$, 2. $\times 200$ and 3. $\times 1000$. c. Luminescence in function of chitosan foam volume with 10^{-6} M of peptide NFO4.

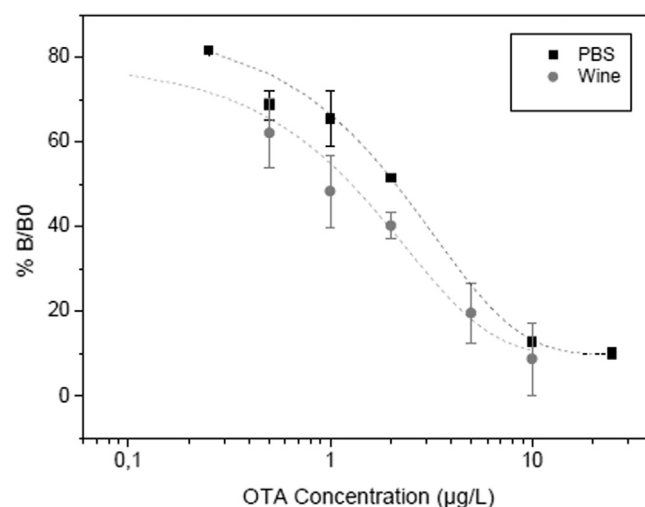


Fig. 5. OTA calibration curves in PBS and red wine on chitosan foam. a. Competitive ELISA for the detection of OTA in PBS were performed with a concentration of peptide NFO4 of 10^{-6} M for a concentration of OTA-HRP labeled at $1000 \mu\text{g L}^{-1}$. B and B_0 represent the bound enzyme activity measured in the presence or absence of competitor respectively. Each point is the average \pm standard deviation of three independent assays each with 4 measurement ($n=12$). b. Calibration curve in red wine for OTA spiked samples: Competitive ELISA for the detection of OTA in wine were performed with a concentration of peptide NFO4 of 10^{-6} M for a concentration of OTA-HRP labeled at $1000 \mu\text{g L}^{-1}$. B and B_0 represent the bound enzyme activity measured in the presence or absence of competitor respectively. Each point is the average \pm standard deviation of three independent assays each with 4 measurement ($n=12$).

3.5. Direct detection of OTA in PBS

Competitive ELISAs were performed with a concentration of peptide NFO4 at 10^{-6} M and for a concentration of HRP-labeled OTA (OTA-HRP conjugate) at $1000 \mu\text{g L}^{-1}$ using foam support slices that were formed from $100 \mu\text{L}$ of chitosan solution. The concentration of OTA was varied from well to well ($0 \mu\text{g L}^{-1}$, $0.25 \mu\text{g L}^{-1}$, $0.5 \mu\text{g L}^{-1}$, $1 \mu\text{g L}^{-1}$, $2 \mu\text{g L}^{-1}$, $5 \mu\text{g L}^{-1}$, $10 \mu\text{g L}^{-1}$ and $25 \mu\text{g L}^{-1}$). The standard curves obtained for peptide-based competitive ELISA on chitosan foam in PBS are shown in Fig. 5 (squares). The competitive binding process was represented by the exponential curve fit for the standard OTA in PBS. Inhibition was observed to start at $0.25 \mu\text{g L}^{-1}$. The maximum inhibition was

Table 1

Comparison test of wine sample from Inter Rhone laboratory and the peptide ELISA based on chitosan foam.

Wine sample #	%B/B ₀	OTA concentration in sample (ppb)	OTA concentration measured (ppb)
161	41.55	1.3	1.84
164	54.57	2.9	1.02
170	28.16	3.0	3.14
173	24.48	4.0	3.67
176	27.96	3.9	3.16
179	13.84	5.7	6.77
191	17.14	5.4	5.32

obtained at $10 \mu\text{g L}^{-1}$ and half inhibition occur at $2.11 \mu\text{g L}^{-1}$. Inhibition was complete, which was expected since the tracer is also OTA-based. From the calibration curve parameters, and with the SD values, the range of detection of OTA in PBS was established to be between 0.25 and $10 \mu\text{g L}^{-1}$.

3.6. Direct detection of OTA in wine

The measurement of OTA in real-world samples and the direct comparison of these results with standard laboratory analysis procedures served to establish the efficacy of this new method. Natural red wine samples were spiked with various concentrations of OTA. These results were used for a repeat of the calibration curve (Fig. 5 (circles)) in the wine matrix. Wine containing OTA could readily be measured by the system, with a reduction in efficacy which can easily be explained by the complexity of the wine matrix and the enhanced number of non-specific compounds co-present in wine samples. The minimum concentration of OTA that the system can detect was $0.5 \mu\text{g L}^{-1}$ and it can detect more than $5 \mu\text{g L}^{-1}$. The current assay method was validated in a study using real wine samples from the "Domaine de Pech Rouge-11430 Gruissan, France", which are documented to naturally contain OTA and have been previously analyzed (Fabiani et al., 2010). The results of the current assay method were compared with those obtained using a reference method (Fabiani et al., 2010; Visconti et al., 1999). This method of reference has been made by Inter Rhône laboratory and used immunoaffinity column (IAC) recovery followed by reversed-phase high pressure liquid chromatography using fluorescence detection (HPLC-FLD). The results obtained (Table 1) are in generally good agreement confirming the applicability of the current assay for the successful screening of wines for OTA.

4. Conclusion

A novel method has been described for the immobilization of the biorecognition peptide NFO4 onto three-dimensional porous chitosan foam that was pre-adsorbed with divalent Zn^{+2} ions. The porous chitosan foam was shown to adsorb divalent cations with binding capacities in the order $\text{Zn}^{+2} > \text{Co}^{+2} > \text{Ni}^{+2}$; maximum sorption capacities reached 230.3 mg g^{-1} for Zn^{+2} , 87.3 mg g^{-1} for Co^{+2} and 62.0 mg g^{-1} for Ni^{+2} . Peptides were immobilized via a histidine tag. Comparison of the efficacy of histidine tag modification and hence immobilization using the C-terminus vs. the N-terminus has revealed that at $1000 \mu\text{g L}^{-1}$ OTA the N-terminus immobilization was more efficient (2.5 times) in the capture of OTA. Sequential optimization of the key process variables has established that the immobilized peptide NFO4 was best at 10^{-6} M for which, in competitive format, an OTA-HRP concentration of $1000 \mu\text{g L}^{-1}$ should be used on a chitosan foam volume of $100 \mu\text{L}$. Calibration of OTA detection in PBS and in wine matrix

revealed some small differences reflective of the molecular complexity of wine. Validation of assay results against the reference method has provided quite good agreement consistent with the use of this peptide-based competitive bioassay technique for the successful screening of wines for OTA. In the future this assay will be implemented in a solid-state bioelectronic format.

Acknowledgements

AG-E acknowledges EMA for a Visiting Distinguished Professorship and ABTECH Scientific, Inc. for financial support. Special thanks go to the French National Research Agency for supporting the COMBITOX Project (ANR-11-ECOT-009-04), which has contributed to this work. Special thanks go to D. Caboulet (Institut Français de la Vigne & du Vin Pôle Rhône-Méditerranée, France) for real wine samples.

Appendix A. Supplementary information

Supplementary data associated with this article can be found in the online version at <http://dx.doi.org/10.1016/j.bios.2014.09.084>.

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