

Impact of Physician Expertise on Probe Trajectory During Obstetric Ultrasound A Quantitative Approach for Skill Assessment

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1	Impact of physician expertise on probe trajectory during obstetric ultrasound: a
2	quantitative approach for skill assessment.
3 4	-Obstetrical Ultrasound Trajectory Metrics-
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22 Abstract

Introduction The objective of the study was to identify objective metrics to evaluate the significance of a sonographer's expertise on trajectories of ultrasound probe during obstetric ultrasound training procedures.

26 Methods This Prospective observational study was conducted at Rennes University 27 Hospital, department of obstetrics and gynecology. We evaluated a panel of sonographers 28 (expert, intermediate and novice) in performing three tasks (Brain, Heart and Spine) with 29 an obstetric ultrasound simulator (Scantrainer, MedaphorTM, Cardiff, UK). The 30 trajectories of the probe were logged and recorded by a custom data acquisition software. 31 We computed metrics on the trajectories (duration, path length, average velocity, average 32 acceleration, jerk, working volume) to compare the three groups and identify 33 discriminating metrics.

Results A total of 33 participants were enrolled: 5 experts, 12 intermediates, and 16 novices. Discriminatory metrics were observed among the three levels of expertise for duration, velocity, acceleration and jerk for Brain and Spine tasks. Working volume was discriminatory for the Brain and the Heart task. Path length was discriminatory for the Brain task.

39 **Conclusions** Our results suggest a relationship between the sonographer's level of 40 expertise and probe trajectory metrics. Such measurements could be used as an indicator 41 of sonographer proficiency and contribute to automatic analysis of probe trajectory to 42 evaluate the quality of sonography and the sonographer.

43

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45 Keywords Ultrasound; Obstetrics; Simulation training; Education; Standard setting.

46 Introduction

Education in the field of obstetric ultrasound has shifted from an exclusively observation-based training to simulation-based training over the past decade¹. Multiple factors may have contributed to the more widespread use of simulation: concerns for diagnostic errors, patient volunteers' or teachers' availability, and technological advances based on virtual reality (VR)²³. Obstetric ultrasound simulators (OUS) may revolution ize the Obstetric and Gynecologic (OB/GYN) residents' curriculum for both training and evaluation⁴.

The utility of OUS for ultrasound training is now well supported by evidence ^{5,6,7,8}. In a series of eight Danish studies, Toslgaard et al. successively explored the learning curves for novices, examined how to improve the efficiency of training with the use of dyad practice, and explored if improvements were sustained over time⁹. They also demonstrated skill transfer to subsequent clinical training¹⁰. Finally, they demonstrated an improvement for the patients after simulation training, such as a decrease in discomfort and improvements in their perception of safety and their confidence¹⁰.

Evaluation of competency in obstetric ultrasound is a time-consuming process and requires pregnant volunteers who are willing to be used for training. One study has shown the potential of OUS as a substitute for evaluating trainees¹¹. In this study, dexterity and quality of images obtained during evaluation were assessed by two independent examiners. However, dexterity was subjectively scored between 0 and 10 based on observation.

67 A fundamental issue for evaluation with OUS is the need for metrics. VR based 68 simulators allow automatic recording of probe trajectories during training and 69 evaluation. OUS could be a suitable tool to extract data from these probe trajectories

for objective evaluation, and to identify metrics that may discriminate the level of expertise of participants during their training. The aim of our study was to assess the potential of OUS to identify objective metrics to measure expertise in ultrasonography.

75 Methods

76

77 **Participants**

The experimental set-up was conducted at the Department of Gynecology and Obstetrics at the University Hospital of Rennes. All training and assessments were carried out in an undisturbed environment. The participants were recruited in June 2018 and the study was conducted from July to September 2018. Approval was obtained from our local institutional review board.

83 The participants were divided into three groups based on their levels of 84 experience: medical students (novice), OB/GYN residents (intermediate), and OB/GYN 85 consultants (experts). All participants were recruited locally at the department of 86 Gynecology and Obstetrics, and provided oral and written informed consent. The experts 87 were professional who had every day practice on genuine patients (about 25 morphologic 88 scans a week). The intermediates were interns who are familiar with routine examination 89 scans (fetal movements, amniotic fluid, estimation of fetal weight, about 5 scans a week) 90 but not with morphologic examination. The novices had absolutely no ultrasound 91 experience. The participants in the 3 groups never practiced on the simulator before the study, as the simulator was bought right before study beginning. 92

The medical program at the University of Rennes is a 6-year traditional curriculum, and the gynecology rotations are completed during the 2 final years. The Novices were recruited during their gynecology rotations. During their prior medical training, the students had completed courses in pelvic anatomy, and ultrasound theory, but had no hands-on training. The Intermediates included OB/GYN residents who had not graduated in ultrasound but who were familiar with ultrasound equipment. The Experts were OB/GYN consultants who used ultrasound on a daily basis.

100

101 Virtual reality simulator

102 Training and assessments were performed using a high-fidelity VR based 103 simulator (Scantrainer, MedaphorTM, Cardiff, UK) designed for obstetric ultrasound 104 training. It is composed of a monitor, an abdominal probe similar to a real one, docked 105 into a Sigma haptic device, two screens and a computer (Figure 1). The haptic device 106 provides realistic force feedback, when operator applies pressure on the abdominal probe. 107 One monitor displays B-Mode 2D ultrasound pictures provided by the system and 108 obtained from real patients. The second monitor displays an animated illustration of the 109 probe position in a virtual patient.

110

111 Tasks performed

112 Step 1: Identification of tasks

113 Most fetal malformations are detected during the second trimester scan. This 114 scan examines the fetus in 11 planes as requested by the National Committee for 115 Prenatal Ultrasound¹².

116 Tasks reflecting the standardized second trimester examination of the fetus were 117 selected to obtain a large sample of fetal anatomy screening, in particular tasks which 118 involved switching from transverse to coronal or sagittal planes. We selected the tasks 119 which would potentially reflect differences in ultrasound competences and provided the 120 most realistic view of the fetus in three consecutive standardized planes. For Task 1 121 (Brain at 24 weeks of gestation), participants were asked to successively obtain the 122 standardized view of the fetal head circumference, then the standardized plane of the 123 cerebellum, and finally a coronal view of the brain through the cavum of septum 124 pellucidum. For Task 2 (Heart at 22 weeks of gestation), participants were asked to 125 successively obtain the standardized view of the four chambers, the view of the left 126 ventricle and the aorta, and the view of the right ventricle and the pulmonary artery. For 127 Task 3 (Spine at 22 weeks of gestation), participants were asked to obtain successively the standardized frontal view of the kidneys, a sagittal view of the spine, and the 128 129 parasagittal view of the left diaphragm. Figure 2 shows a pictorial representation of the 130 three tasks. The participant judged himself that the view was exact and he froze the image to finish exercise. 131

All participants were asked to provide their age, gender, and years of clinical 132 133 experience, and were assigned an identifier to anonymize the data. They then received a 134 short introduction to the simulated setting, including how to operate the simulator and its 135 functions. They also received a course about the recommended fetal planes. All trainees 136 practiced 10 minutes in a "probe manipulation exercise" to familiarize themselves with 137 the device, and to check the expertise difference between the groups. The score of this 138 exercise was calculated by adding the scores of six multiple choice questions (pass: 1; 139 fail: 0) designed to test recognition of six different 3-dimensional geometric solids (cone, 140 pyramid, spiral spheres, other complex geometric solids) by scanning them with the 2-D 141 probe. Technical assistance was provided during the simulator test, but no instructions, 142 feedback or time limit were provided. Each participant had to perform the three tasks 143 three times.

144

145 Metric evaluation

146	The data were logged and recorded by a custom data acquisition software
147	developed with Scantrainer, Medaphor TM , Cardiff, UK. The probe position frequency
148	sampling was 20 Hz. Computation of all metrics and trajectory analysis were run on a
149	dedicated computer (Xeon E5-1650V4 @3.60GHz with 32Go RAM) using
150	Matlab_R2017b. The analysis was done following a previously published technique ¹³ . A
151	total of 6 selected metrics was analyzed:
152	1. Duration (D) corresponds to the execution time between the first time the
153	hand moves the probe, until it has been released at the end of the task. It is
154	measured in seconds (s).
155	2. Path Length (PL) represents the total distance travelled by the probe during
156	the execution of the task. It is measured in millimeters (mm).
157	3. Average Velocity (AV) corresponds to the average linear speed of the probe
158	during the task. It is measured in $mm.s^{-1}$.
159	4. Average Acceleration (AA) corresponds to the average instantaneous
160	acceleration of the probe during the task. It is measured in mm.s ⁻² .
161	5. Average Jerk (AJ) corresponds to the average jerk (derivative of the
162	acceleration) during the task, also known as "smoothness" measure. It is
163	measured in mm.s ⁻³ .
164	6. Working volume (WV) represents the volume of the convex hull for each
165	trajectory. The convex hull of a trajectory is the smallest convex volume
166	among those which contain it. It is measured in mm ³ .
167	One-way Anova-3 tests were conducted to detect differences between the three
168	groups of participants. The Bonferroni correction was applied to the results to

- 169 control alpha inflation (p<0.08). The participants were absolutely not told about
- 170 what the metrics measured were.
- 171

172 **Results**

173 **Demographics**

174 Participant demographics according to expertise level are presented in **Table 1**.

175 Manipulation probe exercise

For the manipulation probe exercise, out of a total of six points (six multiple choice questions, pass: 1; fail: 0), the Experts' mean score was 5.6 ± 0.5 , the Intermediates' mean score was 4.7 ± 1.2 , and the Novices' mean score was 3.4 ± 1.2 points (p=0.002). **Table 1**.

180 Trajectory Metrics

181 Analysis of the probe trajectory metrics revealed significant differences for Tasks
182 1, 2 and 3 between the Expert, Intermediate and Novice groups (Table 2).

183 *Duration of the exercise(s)*

The mean Duration(s) of the exercise differed between Novices, Intermediates, and Experts for Task 1 (respectively $157.5s \pm 176.2$ versus $111.2s \pm 110.3$ versus $35.6s \pm 16.3$, p<0.001), Task 3 (112.8s ± 64.7 vs. $82.3s \pm 50.6$ vs. $35.5s \pm 11.4$ p<0.001). For Task 2 (109.9s ± 69.7 vs. $103.7s \pm 61.1$ vs. $51.7s \pm 47.4$ p=0.009) it was not significant.

188 Path length (mm)

The Path Length (mm) was shorter with increasing level of expertise for Task 1 (Novices: 1442.3 ± 1134.4 vs. Intermediates: 1795.4 ± 1071.9 vs. Experts: 1005.7 ± 409.7 , p<0.001) and for Task 3 (respectively, 1515.3 ± 569.4 vs. 1590.8 ± 589.0 vs. 1071.2 ± 638.3 , p=0.013).

For Task 2 (the "Heart" exercise), the Path Length was not statistically different between the three groups (1 428.7 \pm 508.2 vs. 1 266.5 \pm 517.5 vs. 1 027.0 \pm 1 138.3, NS).

195 Average velocity (mm/s)

The average velocity (mm/s) was significantly higher with increasing level of expertise for Task 1 and 3. For Task 1, average velocity was 19.2mm/s ± 5.7 for Novices vs. 19.5mm/s ± 13.8 for Intermediate and 29.5 mm/s ± 8.7 for Experts (p<0.001), and for Task 3 it was respectively 15.6mm/s ± 5.2 vs. 22.2 ± 7.5 vs. 29.1 ± 8.6 (p<0.001). For Task 2, it was respectively 15.7 mm/s ± 6.4 vs. 14.5 ± 7.0 vs. 20.1 ± 6.4 (p=0.024, NS).

201 Average Acceleration (mm.s⁻²)

The average acceleration was statistically different between the three groups for Task 1 (137.0 $mm.s^{-2} \pm 48.2$ vs. 138.6 \pm 105.1 vs. 228.9 \pm 59.8, p<0.001), and for Task 3 (109.5 \pm 37.0 vs. 157.3 \pm 54.6 vs. 225.7 \pm 80.6, p<0.001), but not for Task 2 (115.8 \pm 62.8 vs. 101.7 \pm 40.1 vs. 149.6 \pm 37.5, NS)

206 Average Jerk (mm.s⁻³)

207Jerk was statistically different between the three groups for Task 1 (2 755.7±1208 $357.0 \text{ vs. } 2728.5 \pm 2283.5 \text{ vs. } 4528.0\pm 1358.4, p<0.001$) and for Task 3 (2 154.7 ± 845.5209vs. 3 099.7 ± 1 300.4 vs. 4 378.1 ± 1 605.7, p<0.001) increasing with level of expertise.</td>210For Task 2, there was no significant difference (2 426.8±1 886.4 vs. 2 012.1±716.7 vs. 2211929.7±761.1, NS).

212 *Working Volume (mm³)*

The total Working Volume covered was statistically different between the three groups for Task 1 (1 118 661.6 mm³ \pm 622487.1 vs. 1 438 677.7 \pm 716 948.1vs. 761 105.7 \pm 603 917.3 p=0.002).

216For Task 2 (1 755 $821.8 \pm 1 318 436.4 \text{ vs.} 1 275 117.0 \pm 674 373.0 \text{ vs.} 825 782.0$ 217 $\pm 962 957.2$, NS) and Task 3, the difference was not significant (1 618 668.3 \pm 624 129.9218vs. 1 759 287.7 $\pm 1 250 355.0 \text{ vs.} 867 504.4 \pm 717 940.5$, NS).

219 **Discussion**

220 Main Findings

This paper presents for the first time the use of metrics computed on probe trajectory during simulated fetal ultrasound with OUS to objectively assess the expertise of the user and his/her dexterity. The main result was that objective metrics (duration, acceleration, velocity and jerk) differed statistically according to the level of expertise in two of the three tasks.

The time for each task (Duration) decreased as the level of expertise increased ranging from 35s to 52s for Experts and from 109s to 157s for Novices. The Path Length, although significantly shorter for Experts in the "Brain" and "Spine" exercise, was not significantly different for the "Heart" exercise. This might be explained by the fact that the planes in the heart exercise are much more tightly bunched in a very small volume.

There must have been a task effect. The "heart" exercise must have been less discriminant using trajectory metrics, because it implied tiny probe movements. The same could have been argued for the "Brain" exercise because there isn't a lot a movement between the head circumference and the transcerebellar view, but a lot a movement is necessary to obtain the coronal view. It is to notice that some amount of initial movement among experts, must be tied to translating positioning and movements with the model to recall of positioning and movements with genuine patients.

Velocity and Acceleration were significantly higher with the increase in level of expertise suggesting that experienced sonographers move from one plane to another with a faster movement. Jerk, which is a derivative of Acceleration, may be interpreted as the variation of acceleration, or how sudden the variations are. We could have assumed that jerk would have been smaller and the gesture smoother for the experts, as it has been

shown for surgical procedures¹⁴. However, during ultrasound examination, jerk was 243 244 higher for experts because they most often combined a quick translation followed by a 245 quick 90° rotation of the probe to switch, for example, from a transverse view of the 246 kidney to a sagittal view of the spine. For the "Heart" exercise, average Jerk did not differ between the 3 groups, with may be explained again with the small quantity of movements 247 248 between the different views. The Working Volume was smaller for the Experts than for 249 the Intermediates and Novices, implying that the Experts remained within the area of 250 interest. These results are similar to those observed by Zago et al about FAST (Focused 251 Assessment with Sonography in Trauma) examination. In this study, they also used hand 252 motion analysis to discriminate expertise, and found similar results : longer hand path and 253 higher working volume for the novices¹⁵. In our study, intermediates performed more like 254 novices than experts on many measures because they may not feel comfortable with 255 morphologic examination.

256 These data are all the more important in France where, for the first time next year, 257 the practical exam for students will be by OUS rather than on volunteers. Other developed 258 countries are following the same trend, i.e., relying more on assessment by OUS. 259 Objective metrics are thus required to respond to this move towards automatic and 260 objective evaluation. Recording the trajectories of the probe, and comparing them to 261 trajectories obtained with experts is an interesting way of evaluating students' level. In a 262 clinical diagnostic perspective, trajectory metrics, taken separately, may not be relevant 263 to measure performance. However, these metrics are a first step. We tested some metrics, 264 and not all of them will have clinical meaning, but they do have a kinematic meaning. Some are obvious (duration) and some are not but may be discriminant (jerk, volume). It 265

is part of the method to go from the identification of differences to explanation of thedifferences observed.

268 Madsen et al. also analyzed simulator-generated metrics on a high fidelity 269 ultrasound transvaginal simulator⁶. They evaluated a group of 16 ultrasound novices 270 along with a group of 12 OB/GYN consultants. The score was calculated by adding the 271 scores of the seven modules (0, fail; 1, pass) for each participant. Of the 153 metrics, 48 272 reliably discriminated between levels of competence and demonstrated evidence of 273 construct validity. However, in that study, simulator-generated metrics were dichotomic, 274 marked either pass or fail, which is different from the present study with a continuous 275 variable.

276 Few other studies have analyzed simulator-generated metrics, and none have 277 analyzed trajectories. Furthermore, most publications on simulator-generated metrics focus on laparoscopy training¹⁶¹⁷. Jones D et al. conducted a study extracting data form a 278 279 laparoscopic simulator. They suggested a relationship between the training level of the 280 surgeon and the forces imparted on the tissue during a laparoscopic simulation¹⁸. In 281 another study about laparoscopic training, Rivard et al. selected 36 individual metrics on 282 four tasks, including speed, motion path length, respect for tissue, accuracy, task-specific 283 errors, and successful task completion. Time and motion path length were significantly 284 different for all four tasks, and the other metrics for some of the tasks. They then used the validated metrics to create summary equations for each task, which successfully 285 distinguished between the different experience levels¹⁶. Lastly, another study about 286 287 laparoscopic procedures explored the correlation between path length or smoothness and 288 outcome measures such as accuracy error, knot slippage, leakage, tissue damage, and 289 operating time¹⁹. In that study, no correlation was found between the metrics and surgery

290 outcomes, except for operative time. Finally, in another study by Sánchez-Margallo, the 291 suturing performance was successfully assessed by the motion analysis method. They 292 demonstrated construct validity for the execution time and path length²⁰.

293 To integrate a simulator in a training and assessment program, it is necessary to demonstrate face, content and construct validity of that simulator. The construct validity 294 295 means the ability to discriminate between different levels of expertise. By opposition, 296 face and content validity means how convincing or realistic the simulator is according to 297 experts, in a more subjective way²¹. It is interesting to notice how objective measures are 298 used to inform construct validity. A study by Van Dongen et al. which aimed to 299 demonstrate construct validity for a laparoscopic virtual reality simulator, used the 300 clinical experience as a definition of expertise. Indeed, simulator metrics were tested in 301 16 novices, 16 residents and 16 experts to construct content validity of a laparoscopic 302 simulator²². It appeared that performance of the various tasks on the simulator 303 corresponded to the respective level of laparoscopic clinical experience.

304 In a study by Ramos et al., participants completed three virtual reality (VR) 305 exercises using the Da Vinci Skills Simulator, as well as corresponding dry lab versions 306 of each exercise. Simulator performance was assessed by metrics measured on the 307 simulator. Dry lab performance was blindly video-evaluated by expert review using the 308 six-metric GEARS tool. This study is interesting because their definition of expertise was based on an exercise and not just the years of clinical experience. Additionally, 309 participants were ask to complete a questionnaire to evaluate face and content validity.²³ 310 311 In another study by Kenney et al, construct validity of a robotic surgery virtual-reality trainer was assessed²⁴. The performance was recorded using a built-in scoring algorithm 312 313 including total task time, total instrument motion, and number of instrument collisions.

Experienced robotic surgeons outperformed novices in nearly all variables. Again, each subject completed a questionnaire after finishing the modules to assess face and content validity. All experienced surgeons ranked the simulator as useful for training and agreed

- 317 with incorporating the simulator into a residency curriculum.
- 318

319 Strengths and Limitations

320 One limitation of our study is linked with the definition of expertise. The three 321 expertise levels were defined by the clinical experience, not the quality of the scans or 322 images that the participants actually produced. However, clinical experience levels were 323 clearly defined (experts who had everyday practice of fetal ultrasound, residents who 324 were much less experienced, and novices who were medical students with no experience 325 at all). Moreover, to address the potential bias on how to define an expert, every 326 participant achieved a probe manipulation exercise, which confirmed levels in the three 327 groups. Another limitation is that we did not assess face and content validity, because we

328 focused on objective metrics.

329 Implications-Interpretation

One challenge when teaching ultrasound is to explain how to obtain the view of the fetus and how to switch from one plane to another, especially to sagittal views. Future explorations are required to approach the optimal trajectory of the probe. This could help to better teach the technique, optimize scan duration, and assess the dynamic quality of the exploration. Future works should also assess skill transfer to clinical practice and trajectories on actual patients.

336

338 Conclusion

This study shows that objective trajectory metrics differ according to level of expertise in two OUS tasks. The connected OUS interface between the operator's hand and the patient, provides numerical data that can help better understand and assess skill acquisition. It is the responsibility of the clinicians to let the developers know what data they are interested in that would make the simulators suited for training.

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351	
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353	MLL carried out the study, analyzed the literature, and wrote up the paper.
354	FD conducted the analyze of the metrics.
355	MK and EF had a role in participants enrollment, helped with experiments and data
356	collection, read and corrected the paper.
357	VL read and added correction to the draft and had a role in the conception and
358	correction of the paper.
359	PJ had a role in the conception, planning, and correction of the paper.
360	
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 432 1288–1292.
- 433

- 434 Legends
- 435 Figure 1. The virtual reality ultrasound simulator (Scantrainer, MedaphorTM, Cardiff,
 436 UK).
- 437 **Figure 2.** Pictorial representation of the three tasks.