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DATA IMPUTATION AND COMPRESSION FOR PARKINSON'S DISEASE CLINICAL QUESTIONNAIRES

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ABSTRACT

Medical questionnaires are a valuable source of information but are often difficult to analyse due to both their size and the high possibility of having missing values. This is a problematic issue in biomedical data science as it may complicate how individual questionnaire data is represented for statistical or machine learning analysis. In this paper, we propose a deeply-learned residual autoencoder to simultaneously perform non-linear data imputation and dimensionality reduction. We present an extensive analysis of the dynamics of the performances of this autoencoder regarding the compression rate and the proportion of missing values. This method is evaluated on motor and non-motor clinical questionnaires of the Parkinson's Progression Markers Initiative (PPMI) database and consistently outperforms linear coupled imputation and reduction approaches.

Keywords Autoencoders · Medical questionnaires · Data imputation · Parkinson's disease · PPMI

1 Introduction

Data representation is a critical problem in biomedical data science, in which the data available concerning an individual patient can be simultaneously large, uncertain, heterogeneous, and incomplete. It is common knowledge in the machine learning community that accurately curating data and providing a uniform representation are often critical to the success of later approaches. Medical questionnaires are one of the major ways of assessing the clinical state of a patient, providing crucial information necessary to diagnose and monitor patients. Extracting this information is crucial to ensuring patient care in the era of computerised, personalised medicine. Unfortunately, medical questionnaires databases often suffer from missing values for various reasons: some tests cannot be performed by some patients or aren't performed at each visit, problems can occur when data is computerised, or paper records can be lost. This issue is well known to the research community and addressing it remains an active field of research [1] [2].

Data imputation is an element that addresses this type of heterogeneity by estimating the value of missing values in an incomplete data vector based on the non-missing values and the population distribution [3]. Data imputation methods are often employed in research to estimate the value of missing data allowing for downstream analysis or statistical processing to be performed. It has been shown that ignoring data points with missing values not only substantially limits the performance of downstream analysis [4], but also that more accurately imputed data yield improves performance in downstream analysis [5] [6].

A related problem is dimensionality reduction in which a large data vector is reduced into a smaller one that can be more readily analysed to monitor and assess the patient’s situation. Keeping a high dimensional input data vector leads to a problem known in the artificial intelligence community as the ‘curse of dimensionality’ [2]. It has been shown, specifically on electronic health records data, that projecting data into a smaller latent space yield better results than using the original space [7]. The current clinical paradigm is to aggregate related values, summing them into a single score and normalising to account for any missing values. Although simple to implement, this method has been difficult to design [8] with the exact partitioning and summation schemes leading to model misfit and misrepresentation in questionnaires used in Parkinson’s disease [9].

Separately, both data imputation and dimensionality reduction are well-known issues in health informatics recently tackled by machine learning [2], and have both been proven to be beneficial for downstream analysis. Abedia [10] showed that projecting incomplete data to a compressed latent space can be beneficial for data imputation, motivating us to tackle and evaluate these problems altogether. Although compressive autoencoders and deep learning have already been used for data imputation [11], there is, to the best of our knowledge, no paper investigating the dynamics of imputation and reconstruction performance varying the compression amount and the proportion of missing values.

Autoencoders are a family of artificial neural networks trained to reproduce its input with a lower dimensional immediate stage or bottleneck [12], which have long been used for data imputation [13]. These networks often consist of a series of encoding layers leading up to a central bottleneck which is then followed by a symmetric series of decoding layers. The central bottleneck creates an “internal representation” of the input data with a lower dimensionality. Autoencoder-based approaches to analysing medical data have been shown to provide useful patient representations for screening broad disease classes [14].

In this paper, we bundle both prospective data imputation and dimensionality reduction into a single method, allowing us to effectively summarise the Parkinson Disease patient’s questionnaire data in a way that can be more readily used for further machine learning methods and population research. We also investigate the impact of differing levels of compression and differing levels of data corruption on imputation performance.

2 Theory and Related Work

2.1 Data Imputation

Imputation can be conceptually split into methods that are applied *prospectively*, where a possibly complete or incomplete training database is used to estimate missing values for an incomplete and previously unseen data vector, and methods that are applied *retrospectively*, where information from an incomplete database is extracted in order to estimate its own missing values. In a clinical context, prospective imputation is of greater utility, allowing new patient records to be processed, although retrospective is more commonly used in research contexts in which an entire database is often analysed at the same time.

The most common way of performing retrospective imputation is case deletion, in which every sample with at least one missing value is removed from the database. This method has the benefit of being easy to use, but suffers from two main drawbacks, in addition to not being capable of prospective use. First, if missing values are distributed amongst a large number of samples, it can substantially reduce the size of the database, limiting the power of any statistical or machine learning method. Secondly, if the probability of which values are missing is not independent or changes based on the value the variable would have otherwise taken, removing incomplete lines can introduce bias into the study [15].

A common but more nuanced method for data imputation is fitting a linear model to the data. Principal Component Analysis (PCA) in particular can be naturally extended to perform prospective imputation by removing the PCA eigenvector components corresponding to the missing values when calculating the PCA scores but using the full eigenvector when transforming the scores back into the data space. Assuming the training database also contains missing values, the PCA decomposition can be determined through several methods [16]. *Pairwise correlation PCA* (PPCA), for example, computes the mean vector and correlation matrix from all the data vectors available with the corresponding values [16]. *Iterative PCA* (IPCA) is an expectation-maximisation algorithm that iterates a process of PCA decomposition and imputation until the PCA decomposition converges [17, 18]. These methods are designed to preserve the mean and covariance of the observed data through the process of imputation. The fact that PCA is also a common dimensionality reduction method makes it even more suitable for patient normalisation, although their linear nature may be problematic as aspects of the question may be coupled in a fundamentally non-linear manner.

2.2 Autoencoders

To perform non-linear dimensionality reduction, autoencoders (AE's) have shown promising results. They have the benefit of capturing more complex or non-linear relations between the inputs. Stacked denoising AE's [19] are particularly useful as they have highly robust denoising capabilities resulting from having noise (theoretically of the same distribution as would be observed in the testing phase) injected into their input during training.

AE's can also be designed with large-scale data imputation explicitly in mind. For example, *correlation neural networks* [20] attempt to find correlated, modality independent internal representations from missing modality problems, where large portions of the data vector are missing simultaneously. Unfortunately, the regularisation term which encourages this correlation requires a low number of modalities and complete data vectors for training which limits their applicability to medical questionnaires where this may not be the case.

Nevertheless, neural networks can be difficult to design and to train for various reasons. Primarily, the shape of the neural network highly affects its performance. For example, even assuming low parameterisation and risk of overfitting, a shallow neural network may not be able to capture the non-linearities of the inputs, while a too deep neural network could suffer from training issues such as inability to propagate gradients effectively.

In this paper, we propose a method relying on an autoencoder architecture with a densely-connected encoder and decoder consisting of fully-connected layers, which we call a Fully Connected Autoencoder (FCAE), to address both data imputation and dimensionality reduction.

3 Materials and Methods

The input data is first rescaled in the range [0,1], with min-max scaling based on the highest and lowest values possible for each question. Although this does not necessarily reflect the semantic meaning behind different levels in the ordinal variables, it does ensure that the number of levels in each does not excessively bias the training of the network and is commonly used even for ordinal data [21]. Denoising autoencoders are then constructed with masking noise applied to the input layer in order to simulate missing values. Unlike truly missing values, their reconstruction quality can still appear in the loss function. This is implemented through a custom masking layer which randomly removes an entire modality (collection of inputs taken from the same test and thus tend to be missing or be present *en bloc*).

The input to the encoder consists of both the data and a mask which indicates the presence of missing data. The encoder consists of the bias layer, which chooses particular initial values to assign to missing variables as a form of initial naive imputation, followed by a series of dense layers, the output of which is concatenated to the input for the successive layers, as shown in Figure 1(a). This alternation between dense and concatenation layers is motivated in a similar way as residual networks [22] in that they allow for short-cuts, minimising issues with propagating gradients while allowing for higher depths to be used to capture non-linearities, and has already been used successfully for data imputation [23]. The final layer of the encoder is a dense layer used to estimate the internal representation. The decoder is constructed similarly to the encoder, with a series of computational blocks each receiving the internal representation and the output of all previous decoder layers as input. Each dense layer is composed of 10 neurons and both the encoder and decoder have a depth of 7 layers, leading to an overall depth of 15. Dropout (5%) was applied to the input of each layer except the final one. Rectified Linear Units (ReLU) were used as the activation functions for each dense layer. The proposed structure (shown in Figure 1) is similar to that of *multimodal autoencoders* [24] with the exception of our concatenation structure and that the noise operator is performed within the network as a layer rather than used to augment the dataset prior to training.

In order to improve the convergence of the autoencoder during training and to minimize the effects of random weight initialisation, each FCAE began with an initialisation step. The bias layer was initialised to replace missing values with the mean value of the respective variable. Each encoder layer was then greedily initialised to the PCA transform that preserved the largest amount of information from its input. Each decoder layer was initialised with linear regression to create the optimal reconstruction given the input to that particular output layer. This initialization guarantees that the training set performance of the FCAE is at worst equivalent to that of the pairwise PCA variant. This step was performed using the entirety of the training dataset simultaneously, but did not involve data augmentation.

The hyperparameters for the network were determined in a two-step process. First, we defined the topology of the network using a grid search, in order to optimize the number of neurons per dense layer and the depth of the network while keeping the other parameters at a constant value. Second, we optimized training-related parameters (keeping the network structure fixed), such as learning rate, batch size and dropout rate, in a Bayesian manner using a Gaussian processes as a surrogate model and expected improvement as the criterion.

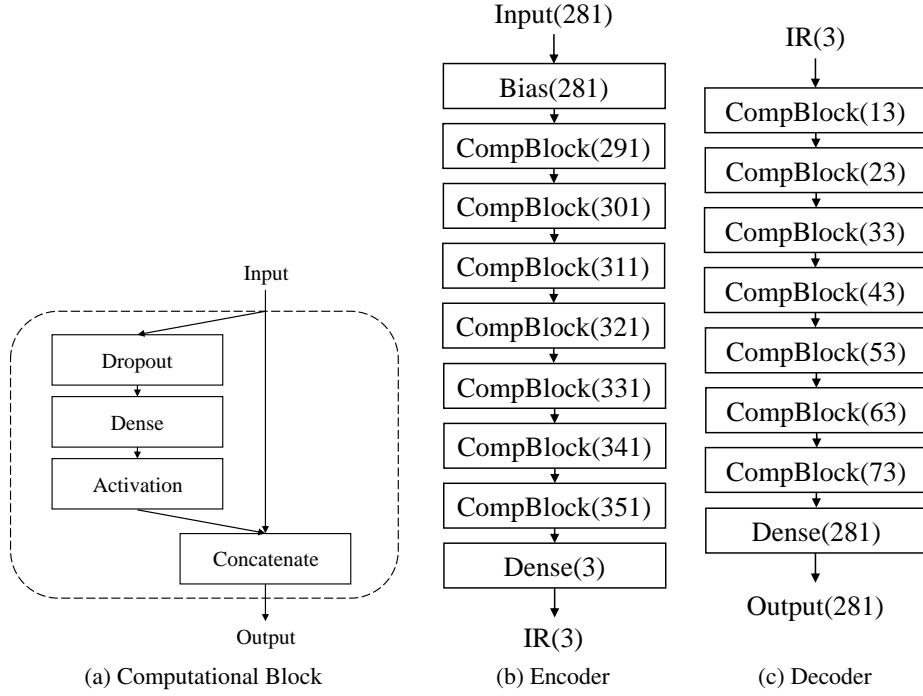


Figure 1: Structure of the FCAE, relying on the chaining of a residual substructure called "Computational Block", presented in (a). The input is passed through the encoder, which produces the internal representation, as shown in (b). The decoder tries to reconstruct/impute the input from this internal representation, as shown in (b). The size of the output of each block is shown in parenthesis. In the given example, the internal representation (IR) size is equal to 3.

The networks were implemented in Keras using a TensorFlow back-end with NAdam as the optimizer. We have made available the code to build and compile our proposed autoencoder, at <https://github.com/m-pr1/PatInAE>.

3.1 Accuracy, Loss and Regularisation Metrics

For the purpose of evaluating each compressing data imputation approach, two measures of accuracy based on the input, x , and reconstruction values, \hat{x} , were used:

$$A_1 = \frac{1}{K} \sum_{i=1}^N \sum_{j=1}^M (\hat{x}_j^{(i)} - x_j^{(i)})^2 * M_j^{(i)} \quad (1)$$

$$A_2 = \frac{1}{U} \sum_{i=1}^N \sum_{j=1}^M (\hat{x}_j^{(i)} - x_j^{(i)})^2 * (1 - M_j^{(i)}) \quad (2)$$

where K is the number of known values and U the number of unknown values in the dataset being evaluated, and $M_j^{(i)}$ is a mask identifying the known values. For A_2 , additional unknown values must be inserted into the dataset in order for their ground-truth value ($x_j^{(i)}$) to be known for evaluation purposes.

For training, the loss metric, analog to the one used by Sanchez [5], used a weighted mean squared reconstruction error using both a binary mask to identify missing data (M_{miss}) and a second binary mask to identify data that has been dropped in the process of data augmentation (M_{drop}):

$$L = \frac{1}{K+U} \sum_{i=1}^N \left(\sum_{j=1}^M (\hat{x}_j^{(i)} - x_j^{(i)})^2 * (1 - M_{miss,j}^{(i)}) + 4 * \sum_{j=1}^M (\hat{x}_j^{(i)} - x_j^{(i)})^2 * M_{drop,j}^{(i)} \right) \quad (3)$$

The weighting factor of is equivalent to put a higher importance into reconstructing the dropped data and thus preferentially improves the network's A_2 accuracy. A weighting factor of 4 showed the most interesting results.

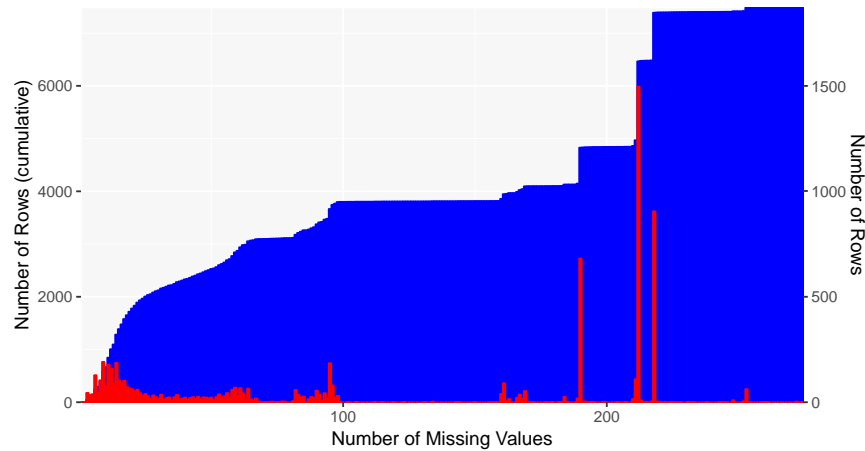


Figure 2: Histogram of PPMI questionnaire data by number of missing values. The cumulative histogram is shown in blue (left axis) and the frequency in red (right axis).

3.1 SPEECH

Instructions to examiner: Listen to the patient’s free-flowing speech and engage in conversation if necessary. Suggested topics: ask about the patient’s work, hobbies, exercise, or how he got to the doctor’s office. Evaluate volume, modulation (prosody) and clarity, including slurring, palilalia (repetition of syllables) and tachyphemia (rapid speech, running syllables together).

- 0: Normal: No speech problems.
- 1: Slight: Loss of modulation, diction or volume, but still all words easy to understand.
- 2: Mild: Loss of modulation, diction, or volume, with a few words unclear, but the overall sentences easy to follow.
- 3: Moderate: Speech is difficult to understand to the point that some, but not most, sentences are poorly understood.
- 4: Severe: Most speech is difficult to understand or unintelligible.

SCORE

Figure 3: First question of Part 3 (motor examination) of the MDS-UPDRS test (version as of May 2, 2019).

3.2 PPMI Questionnaire Database

The Parkinson’s Progression Markers Initiative (PPMI) [25] is a program sponsored by the Michael J. Fox Foundation for Parkinson’s Research. It is an observational clinical study which tracks cohorts of subjects with different forms of Parkinson’s disease for up to 8 years with the goal of identifying biomarkers of disease progression using MR imaging, biologic sampling as well as clinical and behavioural assessments.

This work is focused on the clinical and behavioural assessments which were designed to provide a satisfactory amount of information regarding the patient’s motor, cognitive, neuro-behavioural and neuro-psychological state. The database was built collecting and merging data from most of the motor and non-motor tests. The tests presented on the database are: MDS-UPDRS (all parts), Physical Activity Scale for the Elderly - Household Activity, Modified Schwab & England ADL, SCOPA-AUT, Clinical Cognitive Categorisation, Geriatric Depression Scale (Short), Questionnaire for Impulsive-Compulsive Disorders (QUIP), State-Trait Anxiety Inventory, Benton Judgement of Line Orientation, Hopkins Verbal Learning Test, Letter-Number Sequencing (PD), Montreal Cognitive Assessment (MoCA), Semantic Fluency, Symbol Digit Modalities Text, Epworth Sleepiness Scale, Features of REM Behaviour Disorder. Some parts were discarded because they were performed too sparsely (on too few patients or just at one visit). We built our database by pooling the tests of each cohorts at each visit, on April 2018. The constructed PPMI database has 281 columns and 7490 rows across 1011 patients. 42.9% of the data is missing in a highly heterogeneous manner. The questions used in these tests mostly permit ordinal answers. These tests do not include questions that permit

Questionnaire	% comp.	% incomp.	% mod. miss.	miss. rate
UPDRS I	98.84	0.03	1.13	16.67
UPDRS I PQ	98.80	0.04	1.16	23.81
UPDRS II	96.52	2.43	1.05	10.99
UPDRS III	2	94.73	3.27	6.51
UPDRS IV	55.91	0.04	44.05	61.11
S&E	98.79	0	1.21	N/A
PASE	13.72	15.41	70.87	22.12
SCOPA AUT	0	50.89	49.11	9.37
MCI	38.65	0	61.35	N/A
Ger. Dep.	50.68	0.17	49.15	9.23
QUIP	32.03	18.85	49.12	15.04
STA Inv.	50.43	0.41	49.16	9.27
Benton JLO	40.60	0	59.40	N/A
Hopkins VLT	40.76	0.81	58.42	39.47
L-N Seq. PD	4.15	37.25	58.60	30.60
MoCA	46.33	0.12	53.55	13.10
Sem. Flu.	41.54	0	58.46	N/A
Symb. Dig. Mod.	41.44	0.07	58.49	50.00
Epworth sleep.	50.80	0.04	49.16	12.50
REM SD Quest.	54.07	0.65	45.27	6.32
Average	47.80	11.10	41.10	21.01

Table 1: Statistics of PPMI questionnaires regarding missing values. The second, third and fourth columns show the percentage of rows being complete, with missing values, and with the entire modality missing, respectively. The last row shows the mean percentage of missing values for the incomplete rows.

categorical answers, but there are a few that permit continuous-valued ones. Figure 3 shows the first item of part 3 of the MDS-UPDRS test, which is a question with an ordinal answer. Table 1 gives statistics regarding missing values and modalities for each questionnaire used in this study. The names of the questionnaires have been shortened for clarity purpose, and are in the same order than presented in this section. This table shows a great heterogeneity in the way that values are missing. Nonetheless, the major cause of missing values is when the whole modality is missing *en bloc*. Note that the large majority of missing values are due to the protocol design, as not all tests are performed, nor are intended to be performed, at each visit for each cohort. This is well described in the PPMI database’s protocol information.

An extensive study on the MDS-UPDRS questionnaire (present in the PPMI database) as been performed by Goetz et. al. [26], showing that the loss of information is consequential even with only a few missing values. In their analysis, removing 0-27% of answers completely at random drastically reduces the coherence of the remaining answers. This scenario is obviously worsened by the removal of entire modalities, rather than individual questions, a not uncommon occurrence as shown in Table 1. This shows the quasi-independent nature of the questions of medical questionnaires, even between different items of a same test.

3.3 Comparative Approaches

We compared our results with three comparative approaches. The most simple is *mean imputation*, in which each missing value is replaced with the mean of the corresponding variable. This is the most accurate solution when no internal representation (i.e. no information about the available data) is allowed to be used in the reconstruction process. Pairwise correlation principle component analysis (PPCA) [16] and iterative principle component analysis (IPCA) [17] are the two others comparative approaches. As stated in Section 2.1, they are common PCA-based approaches to dimensionality reduction simultaneous with data imputation.

4 Experiments

We have three hypotheses to experimentally verify:

- H1: there is an optimal internal representation (IR) size to minimise error. That is, there is a degree of flexibility in terms of the networks’ performance that diminishes the network’s A_2 performance. This is expected for PCA in which, after a certain point, additional variables allows the IR to “remember” missing values as the mean of their corresponding variable rather than impute them.

- H2: the network reconstructs data vectors more accurately when they are more complete, decreasing in performance as data becomes missing.
- H3: there is a benefit from learning from incomplete data points. Although complete data vectors are unarguably better, using case deletion to restrict the training dataset to only those data points reduces performance.

All p-values shown are post Bonferroni correction to account for multiple tests. All tests performed are paired t-tests. Prior to the experiments, all the data is normalized to the $[0, 1]$ range using each variable’s theoretical maximum and minimum values. This equally weights variables regardless of discrepancies in their range.

H1: Optimal IR Size

This experiment consists of training and testing autoencoders (and comparative PCA approaches) with IR sizes ranging from 1 to 10. In order to handle the low number of data-points, 20-fold cross-validation was performed to estimate the error. After splitting the dataset into 20 folds, one fold was iteratively selected as the testing dataset. The testing dataset was randomly corrupted with 10% chance of a modality being removed. This corruption process was repeated 40 times in order to have 40 differently corrupted versions of each testing dataset and total number of 800 datapoints for comparison. The datasets were saved to ensure that the same ones were used for evaluating each method, allowing for paired tests.

The remaining 19 folds were again split at each iteration with 80% as training data and 20% as validation data. The FCAE were re-initialised and retrained 8 times per iteration, and the one receiving the lowest validation A_2 error was selected to be evaluated on the testing dataset.

Dataset splitting was performed patient-wise, assigning all of the data from a patient into the same fold, implying that clinical records for one patient at two different times could not appear in both training and testing simultaneously. The validation dataset is corrupted in the same manner as the testing dataset to ensure that the validation loss represents both A_1 and A_2 testing error.

The A_1 and A_2 errors are shown in Figure 4. As expected, the A_1 error decreased monotonically with IR size for all methods ($p < 0.01$). As hypothesised, A_2 did show an optimal IR size for the PCA approaches with both methods monotonically decreasing until $IR = 4$ ($p < 0.01$) and monotonically increasing afterwards ($p < 0.01$ with the exception of PPCA between $IR = 7$ & 8). For FCAE, however, this consistent monotonic increase did not appear indicating that the learning process encouraged the AE to more actively impute that data. Our FCAE also performed better ($p < 0.01$) than both PCA-based methods for both A_1 and A_2 at all IR sizes indicating that there is some non-linearity in the underlying structure of the data.

H2: Predicting with Missing Data

This experiment was performed by training each method on all the available data and verifying that the testing error increases with an increasing corruption ratio. The methods were assigned an IR size of 4, corresponding to the optimal size determined in Section 4. The FCAE was trained with a corruption ratio of 10%, matching the lowest level of corruption performed. The results of this experiment are shown in Figure 5. As expected, the performance of all methods degraded as the corruption ratio increased ($p < 0.01$ between each consecutive corruption ratio, for every method), reflecting the decreasing amount of information available to the network to use in reconstruction.

The FCAE method outperformed both PCA approaches for both metrics at every corruption level ($p < 0.01$). FCAE’s seem to be more sensitive to the amount of data missing compared to PCA, which may be the result of the discrepancy between the corruption ratio used during training and the one used in evaluation, significantly changing the training and testing distributions.

H3: Learning from Incomplete Data

This experiment consisted in training and testing FCAE and comparative PCA approaches, with IR size of 4, by discarding training and validation data samples that presents more than a fixed percentage of variables missing (which we will call the *discard threshold*). No testing data was removed. This was done in a cross-validation style similar to Section 4. The A_1 and A_2 results are shown in Figure 6.

Generally speaking, each method performed slightly better as more (although more incomplete) training data was provided. For all approaches, the improvement was very modest between consecutive discard thresholds with the exception of 10% and 20%. As shown in Figure 7, this is likely due to the larger number of added rows between those discard thresholds, compared to later thresholds. There was another swift increase between 60% and 80%, which can be

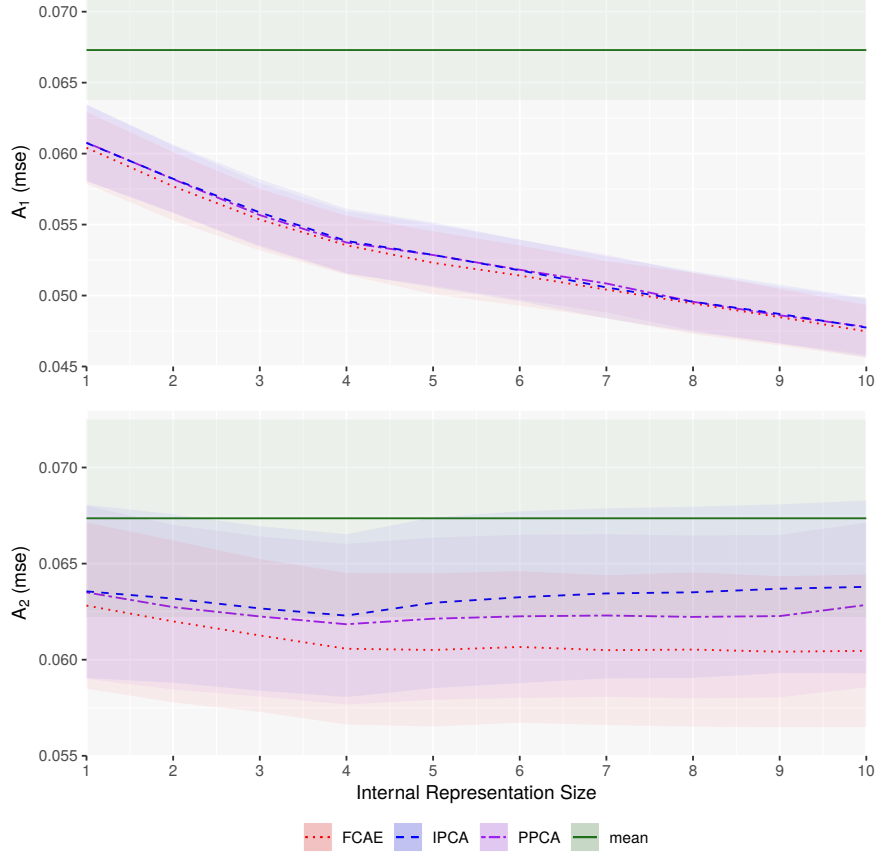


Figure 4: A_1 (top) and A_2 (bottom) error for data reconstruction using FCAE (red) and comparative IPCA (yellow) and PPCA (blue) under varying IR size. The solid green line is the performance of mean data imputation with the dotted green lines representing the standard deviation thereof.

seen in the improvements in the FCAE’s A_1 and A_2 errors. This provides some evidence that training with incomplete data is beneficial, even if a sizeable portion of the dataset is largely incomplete.

It is interesting to note that the FCAE initially performed statistically significantly worse for A_1 than the comparative PCA approaches at the lowest discard thresholds (10% and 20%, $p < 0.01$), but significantly better at higher ones (70% to 90%, $p < 0.01$). This is likely because of the greater flexibility of the model, having more degrees-of-freedom and thus requiring more data to successfully fit.

4.1 Computation time

In order to quantify the computation time required for our method and the baselines, we ran a 20-fold cross-validation and measured the time required to compress and to uncompress the testing set. The results, in microsecond per sample, are displayed in Table 2, using an Intel Xeon E5-1620 v4 CPU at 3.50GHz.

Although our proposed autoencoder requires about 30 times more time to compress and uncompress a data sample, this would not be significant in a clinical setting as each method can be easily considered real-time.

Method	Comp. time (μs)	Uncomp time (μs)
PPCA	1.14	1.16
IPCA	1.05	1.27
FCAE	33.9	26.1

Table 2: Average per sample compression and decompression time for our proposed autoencoder and the two baselines, with an Intel Xeon E5-1620 v4 CPU at 3.50GHz. All values are expressed in microseconds.

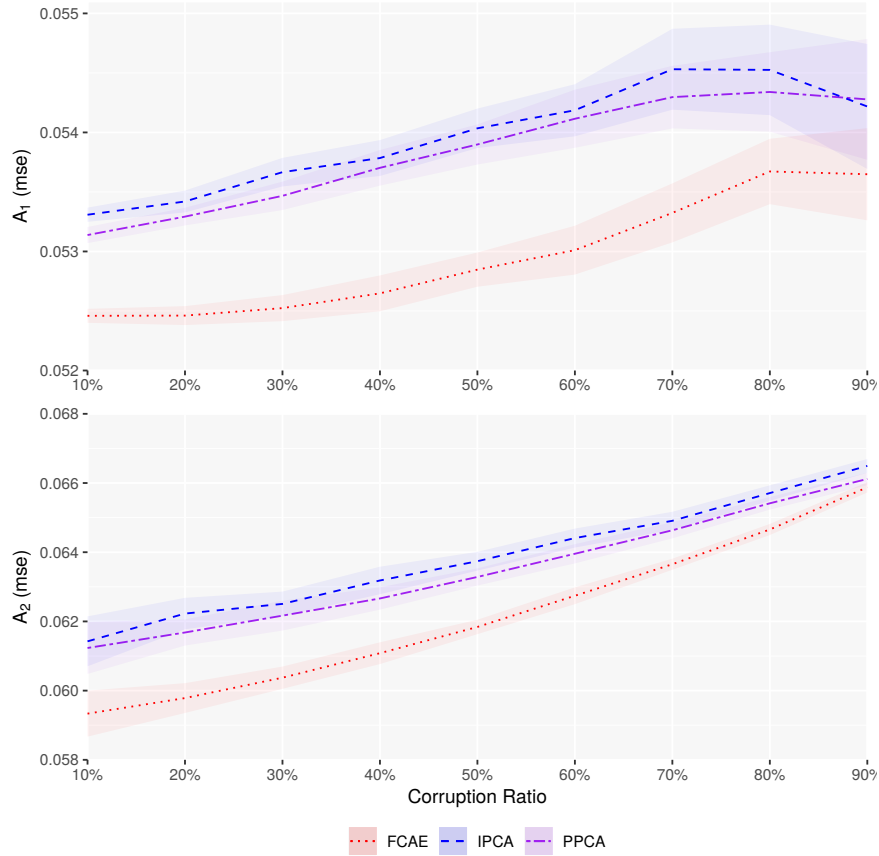


Figure 5: A_1 (top) and A_2 (bottom) error for data reconstruction using FCAE (red) and comparative IPCA (yellow) and PPCA (blue) under varying levels of corruption.

5 Discussion and Future Work

The first point of discussion is the relatively good performance of the two variants of PCA, indicating that a large amount of the variation can be addressed by a linear model equipped with simple missing-value handling. The difference between the two approaches to constructing linear models (PPCA and IPCA) was smaller than initially expected, with the more complex IPCA underperforming PPCA, illustrating that the linear approximation of the dataset’s underlying structure is only that: an approximation.

The issue with using these linear models for reconstruction was expected: a sufficiently large internal representation allows PCA to “remember” the missing variables as their mean value rather than impute them. The deterioration of A_2 after a certain point in PCA is visible even at the relatively low IR sizes shown in Figure 4 (bottom). This trade-off is much less pronounced in the FCAE likely due to the application of modality masking noise which implies that the loss metric encodes both A_1 and A_2 . This combination of losses means that the FCAE must take a more complex imputation strategy even at higher IR sizes.

We observed the distribution of the output prediction of each item, as seen in Figure 8. In this figure, we compare the output distribution of the first question of the part 3 (motor examination) of the MDS-UPDRS questionnaire as reconstructed using FCAE and PPCA on a test set against the true distribution as recorded in the database. 40 iterations have been performed, with a corruption ratio of 10% and IR size of 4. We can notice that there is an important loss of variance in the distributions, especially with PPCA reconstruction. We can explain that by the reconstruction algorithms being designed to minimize a variant of the mean squared error, thus biasing predictions values towards the mean of the distribution and penalising extrema. This behaviour is seen in both reconstruction methods although less distinctly in FCAE indicating that it has a higher capability of reconstructing these extreme values.

In future, we would like to extend our analysis of medical questionnaire imputation and compression for a particular downstream analysis goal, such as the classification of different Parkinsonian patient groups or the stratification of the

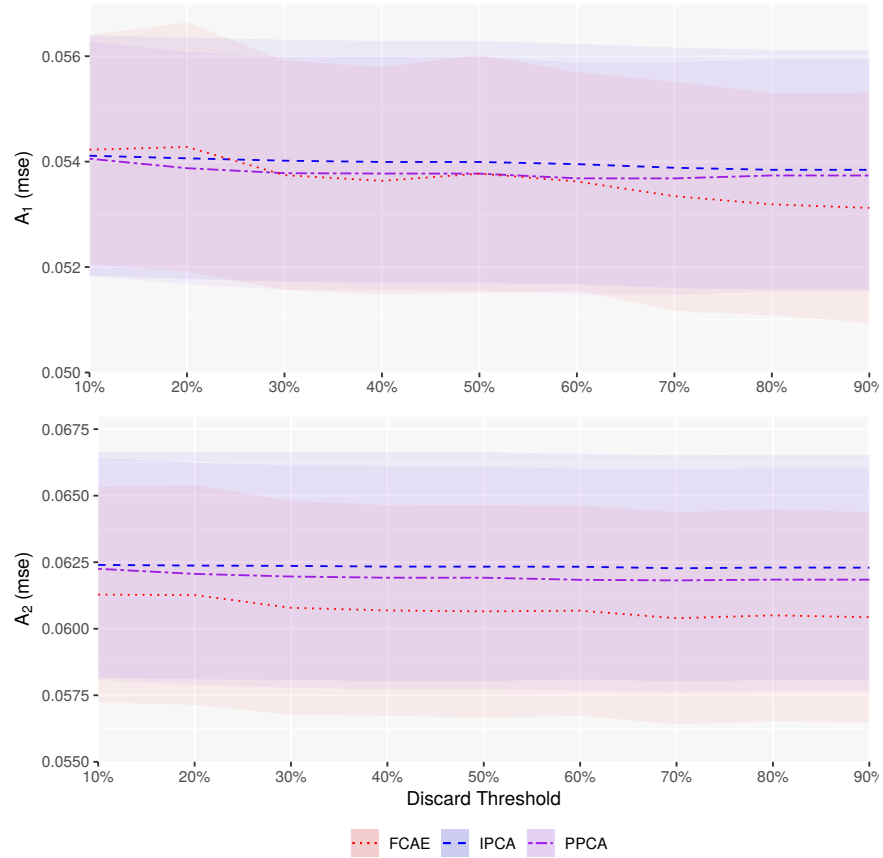


Figure 6: A_1 (top) and A_2 (bottom) error for FCAE (red) and comparative IPCA (yellow) and PPCA (blue) methods with varying toss ratios.

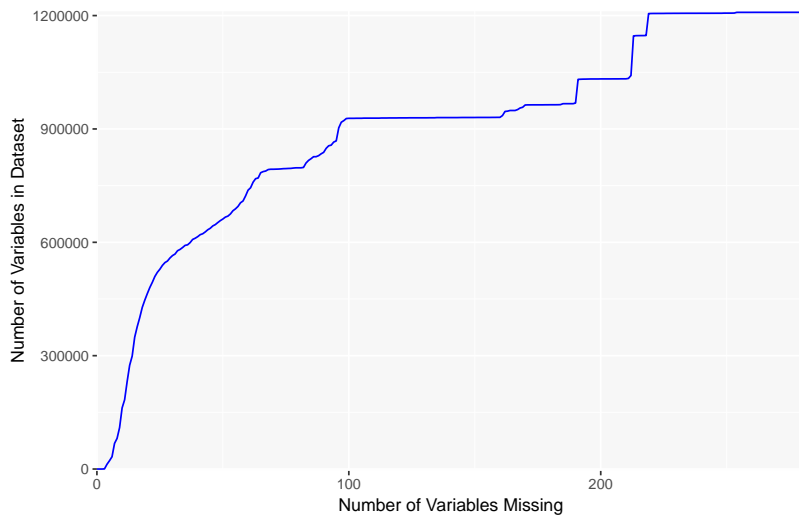


Figure 7: Number of variables available when all rows with more than a certain number of missing variables (x-axis) are removed.

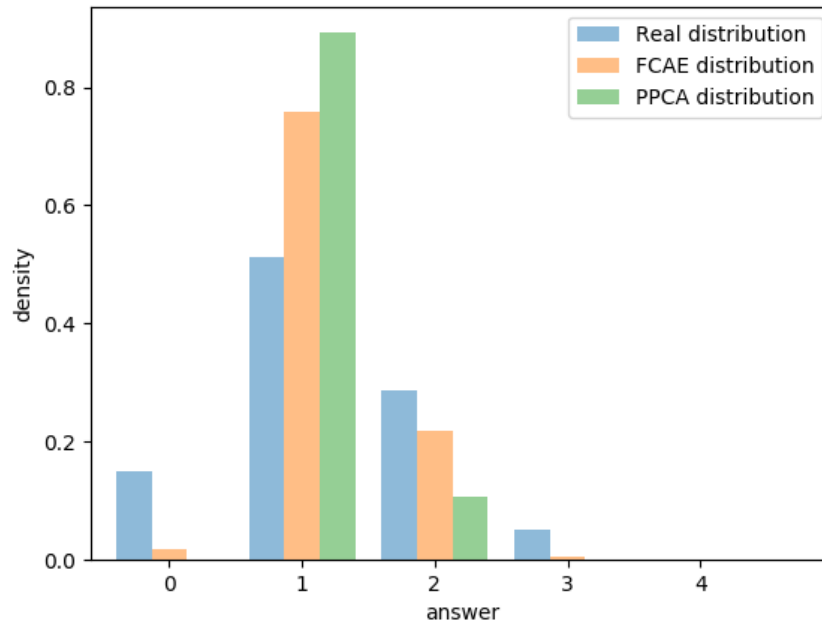


Figure 8: True distribution of the first question of MDS-UPDRS part 3 (motor examination), compared with output distribution of FCAE and PPCA.

disorder. At the moment, diagnosis and stratification are done by a neurologist using some of the data provided by the medical questionnaire, indicating the utility of making the analysis thereof more objective and robust to heterogeneous, incomplete data.

One fact that complicates this study is the relatively low number of data points, especially complete data points, given the relatively high dimensionality and lack of simplifying structure in each point. These issues are further complicated by the majority of tests in the PPMI database used having a middling number of ordinal values (most variables took on values in $\{0..5\}$) rather than simpler categorical or continuous values which thus limit their utility as input.

Ordinal and categorical data handling

It is important to note that, with this database, all the variables were numerical or ordinal. Thus, we did not test the framework with categorical variables, which can be present in other medical questionnaires. We would suggest the use of one-hot encoding for this type of variable in addition to a custom output layer capable of handling different loss functions for the different variable types.

Imputing ordinal variables is problematic. Although ordered, the leap between two successive categories is not consistent, nor quantified. Thus, an error in imputation for an ordinal variable can be more or less significant in certain parts of the answers range. In medical questionnaires, some questions suffer greatly from this problem, as a '0' could mean complete absence of a symptom, and '1' to '4' could quantify its severity. To this extent, the difference between '0' and '1' has more impact on clinical interpretation than the difference between '1' and '2'. Neither our method, nor the baselines, straightforwardly address the specificities of ordinal variables, but instead treat them as continuous, a common approach in the literature [21]. One way of tackling this problem with our framework would be to use a loss function tailored for ordinal variables, such as the weighted kappa loss proposed by De la Torre [27]. Ideally, the weights of each consecutive error of each ordinal variable should be defined by clinicians according to its impact on clinical interpretation, thus leading to a greater practical applicability.

An alternative approach would be to use an adversarial loss that could, in theory, learn what continuous values correspond with possible levels for each ordinary variable and well as what combination of values are realistic [6]. Such an approach would require a significant database consisting of full rows, i.e. data that can be used as true fully sampled data for training the discriminator. However, this is not representative of the PPMI database as described in Section 3.2.

6 Conclusions

This paper presents an autoencoder specifically designed for data imputation and compression of medical questionnaires, in which entire modalities may be missing. This represents some of the initial steps into performing deep learning on specific medical tasks that are challenging due to the dataset size compared to the high number of features, the data types provided and the complexity of the learning problem. We have shown that significant and consistent improvements can be made over linear methods, especially when a lower number of features is missing. We have also shown that there is an interest in learning on incomplete data vector, and that the imputation performances of our framework is not negatively impacted by a high internal representation size, making the downstream choice of the compression rate easier.

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