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Multi-Parametric Maps From Multi-contrast Steady-State Sequences on Multiple Manufacturers and Fields

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Purpose/Introduction

- Fast steady-state sequences provide a variety of contrasts sensitive to various MR parameters (TR, RF amplitudes and phases, spoiling gradient) [1] from which multiple parametric mapping approaches can be derived [1-5].
- Here, multi-contrast raw images and reconstructed parametric maps from the same volunteer are compared on multiple manufacturers and fields.

Subjects and Methods

- Imaging was performed on a healthy volunteer at 1.5 T (Philips Achieva, Siemens Avanto) and 3 T (Siemens Verio).
- Whole-brain slice-selective 3D RF and gradient spoiled gradient-echo sequence allowing sequential acquisition with different RF amplitude, phase increment, spoiling gradient direction and area was used.
- Thirteen volumes were acquired sequentially with different flip angles, phase increments, and effective dephasing distance between each TR (noted *a*) leading a total scan time of 6.5 min. Choice of the optimized parameter set was described in [6].
- A gradient-echo phase map estimated as the complex sum of volumes with 0° and 180° RF phase increments was removed from all volumes providing **SSFP phase-induced maps** independent of TE.
- Parametric M0, R1 and R2 maps were calculated on a voxel-by-voxel basis by least-squares fitting complex signals to the Bloch-Torrey equation assuming uniform flip angles and a diffusion coefficient of 2.10⁻⁹m²s⁻¹[7].

Results

- Mixed contrasts dependent on flip angle amplitude, phase cycling and spoiling gradient area both on magnitude and SSFP phase-cycling-induced contrasts were observed (Fig.1).
- Good agreement was obtained at 1.5T between Philips and Siemens, and noticeable differences were observed at 3T as expected due to different relaxation parameters. SSFP-phase maps can be easily used to rapidly assess similarities between 1.5T implementations.
- The parametric reconstruction displayed in Fig.2 accounts for gradient hardware limitation and provides similar R1 and R2 maps at 1.5T on both systems. At 3T, the general trend for a smaller R1 and a larger R2 was observed as expected.

References and acknowledgements

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Figure 1: Sample axial slice on the same healthy volunteer on Philips 1.5T and Siemens 1.5 and 3 T. Magnitude images are shown in the first row, phase-cycling SSFP induced phase-contrast is shown in the second row. Spoiling gradient, flip angle and RF cycling phase increment are provided below each set. Corresponding slices were registered manually.

Figure 2: Reconstructed proton density M0 map (with remaining coil sensitivity profile weighting, first row), corrected from receiver coil profile inhomogeneity for Philips 1.5 T, non-corrected for Siemens 1.5 T and 3 T, R₁ and R₂ maps displayed with their respective same window levels (in s⁻¹).

Discussion/Conclusion

- Precise control of **RF** and gradient spoiling is crucial to obtain the same contrasts in SSFP sequences, as shown *in vivo* here.
- SSFP-phase contrast images, unexploited up-to-now, linked to relaxation, insensitive to the receive coil profile inhomogeneity, could be used for diagnosis.
- Parametric maps processed identically accounting for gradient hardware differences tend to further reduce variability at 1.5 T.
- Emphasizes the need for sequence and reconstruction standardization and validation to enhance the reproducibility among sites and manufacturers which is critically needed for more robust multi-centric studies.

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