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1 2 3	Comparison of biophysical models with experimental data for three cell lines in response to irradiation with monoenergetic ions					
4	Caterina Monini ^{a*} , Gersende Alphonse ^{a,b,c} , Claire Rodriguez-Lafrasse ^{a,b,c} , Étienne Testa ^a , Michaël Beuve ^a					
5 6	^a Univ. Lyon, Univ. Claude Bernard Lyon 1, CNRS/IN2P3, IP2I Lyon, F-69622, Villeurbanne, France					
7	^b Laboratoire de Radiobiologie Cellulaire et Moléculaire, Faculté de Médecine Lyon-Sud					
8	^c Hospices Civils de Lyon, Service de Biochimie, Centre Hospitalier Lyon-Sud, 69495 Pierre-Bénite France					
9						
10 11 12	Corresponding author: Caterina Monini, <u>monini@ipnl.in2p3.fr</u> Bâtiment Paul Dirac, Rue Enrico Fermi, 69622 Villeurbanne, France					
$\begin{array}{c} 13\\ 14\\ 15\\ 16\\ 17\\ 18\\ 9\\ 22\\ 23\\ 24\\ 25\\ 27\\ 28\\ 29\\ 31\\ 32\\ 33\\ 35\\ 36\\ 37\\ 38\\ 9\\ 41\\ 42\\ 44\\ 45\\ 46\\ 47\\ 48\end{array}$	 Highlights: The accuracy of biophysical modeling is crucial for particle therapy Comparison of LEM(I-IV), MKM and NanOx models with data for 3 cell lines χ² scoring for α(LET) curves NanOx yields the highest score more often than the other models Financial support: ITMO Cancer in the framework of Plan Cancer 2009-2013 and Plan Cancer 2016-2019 (Project Nos. PC201312 and PC201606) referred to as: "Domaine de la physique, des mathématiques ou des sciences de l'ingénieur appliqués au Cancer".					

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50 ABSTRACT

51 The relative biological effectiveness (RBE) in particle therapy is currently estimated using biophysical models. We 52 compared experimental measurements to the α (LET) curves computed by the Local Effect Model (LEM I-IV), the 53 Microdosimetric Kinetic Model (MKM) and the NanOx model for HSG, V79 and CHO-K1 cells in response to 54 monoenergetic irradiations. Although the LEM IV and the MKM predictions accurately reproduced the trend observed in 55 the data, NanOx yielded a better agreement than the other models for more irradiation configurations. Its χ^2 estimator 56 was indeed the lowest for 3 over 7 considered cases.

1. INTRODUCTION

59 Due to its increased efficiency in inducing biological damage, particle therapy offers advantages over the standard 60 radiotherapy modalities for the treatment of radioresistant, unresectable tumors close to organs at risk [1, 2]. Several 61 experimental studies have shown evidence that the relative biological effectiveness (RBE) of ions with respect to photons 62 depends on multiple parameters related to the incident beam, the irradiation conditions and the intrinsic properties of the 63 biological system [2]. Therefore, to optimize the 3-dimensional distribution of the dose to be received by the patient 64 during a session, the predictions of RBE are integrated into the treatment planning system (TPS). While the first 65 approach used in clinics was based on RBE values derived empirically from the *in-vitro* response of a well-known tumor 66 cell line to neutron beams [3], the progressive diffusion of active beam delivery favored the implementation of 67 biophysical models in the TPS. This triggered the development and the improvement of many frameworks, the most 68 acknowledged ones being the Local Effect Model (LEM) and the Microdosimetric Kinetic Model (MKM).

The LEM I [4, 5], II [6], III [7] ascribes the biological effectiveness of ions to the specific energy deposition pattern at "local" scale, which is estimated in terms of a radial dose (D(r)). Although enabling fast and efficient calculations, the use of the expected quantity D(r) to describe processes occurring at the nanoscale leads to some incongruities; for example, the shoulder in cell survival curves results from an artifact due to the superimposition of the radial doses associated to several impacting ions [14]. The issue was solved in the LEM IV [8], a substantially different version of the local effect model in which the cell nucleus is divided into critical regions corresponding to DNA giant loops. In these domains the microscopic spatial distribution of DNA double strand breaks is computed on the basis of the radial dose.

76 The MKM [9] combines a microdosimetric description of the energy deposition (accounting for the statistical 77 fluctuations) with a kinetic representation of the repair and injury processes. The probability of cell survival, however, is 78 not computed considering an average process over the irradiation configurations, but simply in terms of a Poisson 79 distribution of the mean number of lethal lesions. The distribution is corrected defining a geometry for the cell nucleus in 80 order to avoid the overestimation of the ions efficacy in the tumor [10].

81 More recently, NanOx [11, 12, 13] was developed by the authors to address the challenge of implementing the 82 stochasticity of the energy depositions at nanometric and microscopic scales when predicting radiation-induced effects. 83 This is fulfilled in the modeling of the number of radiation impacts associated to a given dose, of the dose-deposition 84 pattern along the track and of the inter-track processes. The cell inactivation is ascribed to two classes of biological 85 events occurring at different spatial and temporal scales, in a manner similar to that proposed by Katz *et al.* [15]. Local 86 lethal events are attributed to one track and are described in terms of nanodosimetry, while global events resulting from 87 the contribution of several tracks are represented by the accumulation of oxidative stress and sublethal damages.

88 We decided to benchmark the predictions issued from these models against experimental data to verify if the 89 implementation of a fully stochastic theory at nano and micro-scale had an impact on the precision of the predictions. In 90 this paper we considered as biological endpoint the slope of cell survival curves since this is the one reported most 91 extensively in the literature, both for measurements and theoretical calculations. 92

2. MATERIALS AND METHODS

95 2.1 Experimental data

93 94

96 Our study focused on the response of three cell lines to monoenergetic beams of several ion types (from hydrogen to neon) and energies (from 0.8 to 266 MeV/n).We chose normal lung fibroblast (V79) and ovary (CHO-K1) cells from a
98 Chinese hamster due to the large amount of data available in the literature, and human tumor cells from salivary glands
99 (HSG) since head and neck cancers match the therapeutic indications for particle therapy.

100 The experimental α values were gathered from the database made available by the PIDE project [17]. Although for most 101 of the measurements the error bars are not reported, the great data dispersion allows one to infer the important biological

- 102 variability and the effects of the use of different biological and irradiation protocols. In spite of this dispersion, however,
- 103 it is noticeable that α values rise for LET values up to 150-200 keV/ μ m (depending on the ion type), and drop for higher 104
- LET values. The initial trend is associated to the action of swift ions, which scarcely ionize the traversed biological 105
- tissues by depositing only small amounts of energy; progressively slower ions, on the contrary, produce a considerable 106 ionization density in the medium leading to the increase of the biological effectiveness. The decrease of the α curves is
- 107 due to the "overkill" effect, which may be explained in terms of two phenomena: firstly, for constant irradiation doses the
- 108 fluence of incident particles is inversely proportional to the LET, and secondly, the tracks of high LET ions are narrow;
- 109 110 the probability of hitting the cellular sensitive targets and inducing biological damages is, thus, fairly low.

111 2.2 Models predictions

112 The α values predicted by the LEM I, II, III, IV and the MKM for all the considered radiation types and cell lines were 113 extracted from [8, 16] and for each of these models, the calculations were reported only for the irradiation cases for 114 which published results could be found. The values of α predicted by NanOx, on the contrary, were computed by the 115 authors especially for this work. Precisely, theoretical cell survival curves were first calculated as explained in [11, 13], 116 and then a linear fit at low doses allowed extraction of the slope α .

117 As Table 1 shows, all the models were evaluated considering a unique set of parameters per cell line, *i.e.* avoiding tuning 118 and optimizations which would depend on the irradiation ion type. As explained in [8, 12, 16], the choice of the 119 parameters was made in order to optimize the conformity between the predicted α values and the experimental ones 120 121 available from the literature.

122 2.3 Benchmark estimator

123 In order to quantify the agreement between the predictions issued from each model and the data, we computed the χ^2 as:

124
$$\chi^2 = \frac{1}{M} \sum_{i=1}^{M} \left(\frac{\alpha_{exp}^i - \alpha_{pred}^i}{\alpha_{exp}^i} \right)^2$$
(1)

125 In Eq. 2, M represents the total number of experimental points pertaining to the PIDE dataset [17] for a given cell line and ion type, and α_{exp}^{i} (respectively α_{pred}^{i}) denotes the *i*th experimental (resp. predicted) α value. 126

3. RESULTS

127

128 129 130 Figure 1 shows the slope α as a function of LET for HSG, V79 and CHO-K1 cells in response to hydrogen, helium, 131 carbon, oxygen and neon ions. While the LEM I was inadequate to reproduce the experimental trend for almost all of the 132 considered cell lines and radiation types, some amelioration was visible for the LEM II and III, mostly in the high LET 133 range. An important disagreement between theoretical and observed α values, however, was apparent in the low LET 134 range: the curves predicted by the LEM II (except for CHO-K1 cells in response to carbon ions) and by the LEM III in 135 the case of irradiation by light ions, were overestimated, whilst the curves predicted by the LEM III for heavy ions 136 irradiation, on the contrary, were underestimated. On the other hand, the experimental increase of α for LET values up to 137 150-200 keV/ μ m and the subsequent decrease observed for higher LET were overall well reproduced by the MKM, the 138 LEM IV and the NanOx model. Figure 2 and Table 2 present the χ^2 estimator for each model, cell line and ion type. The 139 intercomparison highlighted that NanOx's predictions were the most precise over the seven configurations, yielding the 140 minimum χ^2 in three cases: for HSG cells in response to He ions, for V79 cells in response to C ions and for CHO-K1 141 cells in response to C ions. Our model was followed by the LEM IV and the MKM, which achieved the smallest χ^2 in two 142 cases each. 143

144 DISCUSSION

145 The optimization of treatment plans in particle therapy strongly relies on the link between the energy deposition pattern 146 and the expected biological response. Since such a link is currently provided by the biophysical model specifically 147 implemented, it is of utmost importance to review and compare the main existing frameworks.

148 Recently, Stewart et al. [18] pointed out the differences among the LEM IV, the MKM and the Repair-Misrepair-149 Fixation (RMF) model in the input parameters, the relevant biological targets and the computational strategies. The main 150 principles and the seemingly contradictory aspects of the models were discussed, but the article did not report an 151 extensive benchmark of the different predictions against radiobiological measurements. Stewart et al. concluded that

- 152 "future comparisons of model predictions with experimental data are needed to fully discriminate among competing
- 153 mechanisms and models of particles RBE". We hence decided to test the accuracy of well-known cell survival models

- 154 considering a common biological endpoint, the α (LET) curves of HSG, V79 and CHO-K1 cells in response to
- monoenergetic irradiations, and as well as to examine the predictive power of NanOx. In order to quantify the agreement of the predictions with the experimental measurements found in the literature, a χ^2 calculation was performed for each
- 157 of the predictions with the experimental measurements found in the inertatine, a χ calculation was performed for each cell line and irradiation type: NanOx yielded the lowest χ^2 for more configurations than the other models. This result
- should be considered in light of two facts: first, in some cases the difference in the χ^2 was small; and second, according to
- 159 the published references several calculations were missing for the seven irradiation configurations that we considered. In
- 160 particular, since the LEM IV predictions were available for only 3 cases, this model achieved the highest percentage of
- 161 lowest χ^2 values. More generally, our study highlighted that the predictions issued by the LEM IV, the MKM and the
- 162 NanOx model were appropriate considering the important dispersion of the experimental data, while the LEM I, II and III
- 163 did not satisfactorily reproduce the observed biological effect of ions.
- Even though the irradiation of *in-vitro* cells considered in our study are by far not representative of particle therapy treatments, a question may arise on the relevance of the current implementation of biophysical models in the clinical TPS.
- 167 The LEM I represents the standard in the European particle therapy facilities since it minimizes the risk of overestimating 168 the doses prescribed to patients, and complies with the need of radiotherapists to rely on stable protocols. However, its 169 description of the radiobiological response of V79, CHO-K1 and HSG cells was the least accurate among the models 170 considered in our study. A modified version of the MKM (mMKM [21, 22, 23]) developed by Kase et al. is instead 171 integrated in the Japanese clinical TPS. It predicts the decrease of RBE caused by the overkill effect owing to a revised 172 saturation correction, and is based on amorphous track structure models (i.e. on the controversial radial dose), allowing 173 fast calculations. We believe that in the context of clinical research it would be relevant to evaluate the predictive 174 qualities of other biophysical models and of the several modified and improved versions of the existing frameworks. This 175 could be achieved, for example, by performing calculations with each model in clinical conditions and trying to correlate 176 them to clinical data; it would be fruitful to bridge over the advances in research and the clinical routine of particle 177 therapy.
- 178 In conclusion, we showed in this paper that NanOx predictions for three cell lines irradiated by monoenergetic ions were 179 more often more accurate than the ones issued from 5 other biophysical models; however, in some cases the difference 180 with respect to the LEM IV and the MKM was small, and some theoretical calculations were missing. More reliable 181 conclusions may be derived if an experimental dataset characterized by lower biological variability was available, and if 182 all the biophysical models were tested more systematically for a wide range of irradiation configurations.

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189 DECLARATION

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190 The authors declare no conflicts of interest.

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Figure 1: Evolution of the slope α with LET for HSG, V79 and CHO-K1 cells irradiated by hydrogen, helium, carbon, oxygen and neon ions. The experimental values gathered from the PIDE database [17] are compared with the predictions provided by the four versions of the LEM (when available), the MKM and NanOx. The data relative to the LEM and the MKM are extracted from [8, 16]. All the models are evaluated considering a single set of parameters for each cell line, which have been chosen as they optimize the agreement with the experimental points.



Figure 2: χ^2 associated to each radiobiological model on the basis of the experimental and predicted points of Figure 1. The symbols represent the values computed separately for HSG, V79 and CHO-K1 cells irradiated by hydrogen, helium, carbon and neon ions. The solid lines, instead, are for visual guidance purposes only.

Cell line	Model parameters					
	LEM (I/II/III)	LEM IV	MKM	NanOx		
	$\alpha_x = 0.313 \text{ Gy}^{-1}$	$\alpha_x = 0.316 \text{ Gy}^{-1}$	$\alpha_0 = 0.313 \text{ Gy}^{-1}$	$z_0 = 15654 \text{ Gy}$		
	$\beta_x = 0.062 \text{ Gy}^{-2}$	$\beta_x = 0.062 \text{ Gy}^{-2}$	$\beta{=}0.062~\mathrm{Gy}^{-2}$	$\sigma{=}549~{ m Gy}$		
HSG	$D_t = 30/6/19 {\rm Gy}$	$D_t = 7.5 \text{ Gy}$	$R_d{=}0.02~\mu{\rm m}$	h = 179439		
	$R_N = 5 \ \mu \mathrm{m}$	$R_N=5 \ \mu { m m}$	R_n =4.6 μm	$\beta_G = 0.096 \text{ Gy}^{-2}$		
				$R_{SV}=7 \ \mu {\rm m}$		
	$\alpha_x = 0.184 \text{ Gy}^{-1}$	$\alpha_x=0.129~{ m Gy}^{-1}$	$\alpha_0 = 0.184 \text{ Gy}^{-1}$	$z_0 = 22789 \text{ Gy}$		
	$\beta_x = 0.020 \text{ Gy}^{-2}$	$\beta_x = 0.049 \text{ Gy}^{-2}$	$\beta {=} 0.020 \text{ Gy}^{-2}$	$\sigma{=}8117~{ m Gy}$		
V79	$D_t = 70/15/60 \text{ Gy}$	$D_t=3~{ m Gy}$	$R_d{=}0.1~\mu{ m m}$	h = 225841		
	R_N =4.2 μm	$R_N=5 \ \mu { m m}$	$R_n = 4.2 \ \mu \text{m}$ $\beta_G = 0.041 \ \text{Gy}^-$			
				R_{SV} =4.9 $\mu { m m}$		
	$\alpha_x = 0.228 \text{ Gy}^{-1}$		$\alpha_0 = 0.228 \text{ Gy}^{-1}$	$z_0 = 14507 \text{ Gy}$		
	$\beta_x = 0.020 \text{ Gy}^{-2}$		$\beta = 0.020 \text{ Gy}^{-2}$	$\sigma{=}2781~{ m Gy}$		
CHO-K1	$D_t = 40/9.5/55 \text{ Gy}$		R_d =0.12 μm	h = 104810		
	R_N =4.7 μm		R_n =4.0 μm	$\beta_G = 0.063 \text{ Gy}^{-2}$		
				$R_{SV}{=}5.9~\mu{\rm m}$		

Table 1: Values of the LEM (I-IV), MKM and NanOx parameters with which the predicted $\alpha(LET)$ curves of Figure 1 have been obtained. The set of parameters of each model was determined to optimize the agreement with the experimental data, as reported in [8, 13, 16].

Irradiation	Model:					
configuration	LEM I	LEM II	LEM III	LEM IV	MKM	NanOx
HSG, He ions	0.988	0.195	0.335	0.097	0.050	0.048
HSG, C ions	1.887	1.060	0.794	0.201	0.209	0.202
HSG, Ne ions	0.054	0.046	0.082	-	0.034	0.046
V79, H ions	-	-	-	0.055	-	0.175
V79, C ions	0.344	0.287	0.176	-	0.167	0.102
V79, Ne ions	0.069	0.054	0.043	-	0.020	0.036
CHO-K1, C ions	0.048	0.038	0.045	-	0.047	0.020
CHO-K1, Ne ions	-	-	-	-	-	0.380
CHO-K1, O ions	-	-	-	-	-	0.076

Table 2: Values of the χ^2 estimator for all the models and irradiation configurations presented in Fig.2