# Online control for Quality Assurance

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## Motivations

• Range uncertainties, margin reduction...

We better trust what we see!

 $\rightarrow$ Improve and secure ballistic precision

- At the pencil beam spot basis (or few selected spots)
- Real time
- Range verification at mm precision (smaller than actual margins)
- According to beam delivery mode (beam species, accelerator...)
- Geometrical constraints (gantries, patient positionning...)
- No reduction of patient workflow
- Affordable cost!

• A system will not be optionnal if the efficiency is proven

## Outline

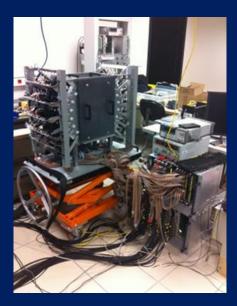
- Positron Emission Tomography
- Prompt gamma:
  - Prompt Gamma imaging
  - Non imaging modalities:
    - Prompt Gamma Spectroscopy
    - Prompt Gamma Peak Integral
    - Prompt Gamma Timing

## PET ion range monitoring

#### $\circ~$ In-room or Off-line:

- Whole fraction verification only
- In-beam PET: acquisition between beam bunches
  - Suitable at low duty cycle (eg synchro-cyclotrons)
  - + short lived isotopes, eg <sup>10</sup>C
  - + No washout
  - Restricted or complicated geometries

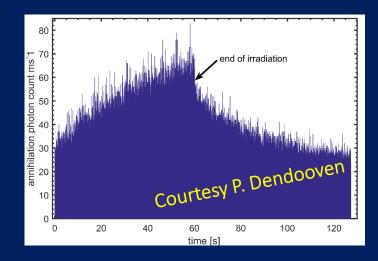
#### Long radioisotope lifetime 🔶 no real-time

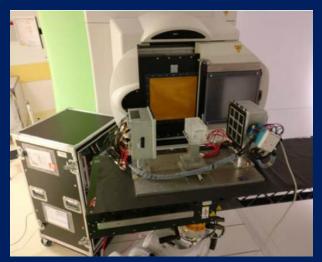


DPGA - (Clermont)



Dual ring OpenPET (NIRS) [Yoshida IEEE TRPMS 2014]

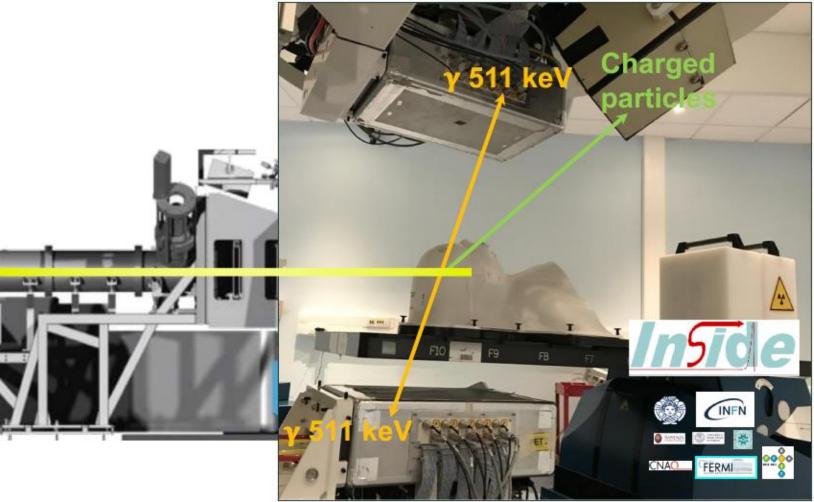




DoPET(INFN) **Topi et al, IEEE TRPMS 2019**<sup>4</sup>

#### INSIDE BI-MODAL IN-VIVO RANGE VERIFICATION SYSTEM

### Courtesy MG Bisogni

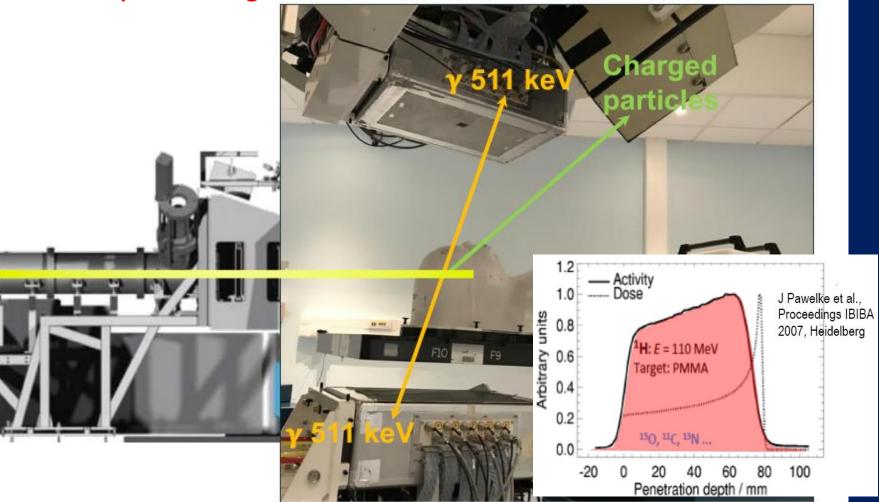


#### INnovative Solutions for In-beam DosimEtry in Hadrontherapy

**ENLIGHT Meeting 2019** 

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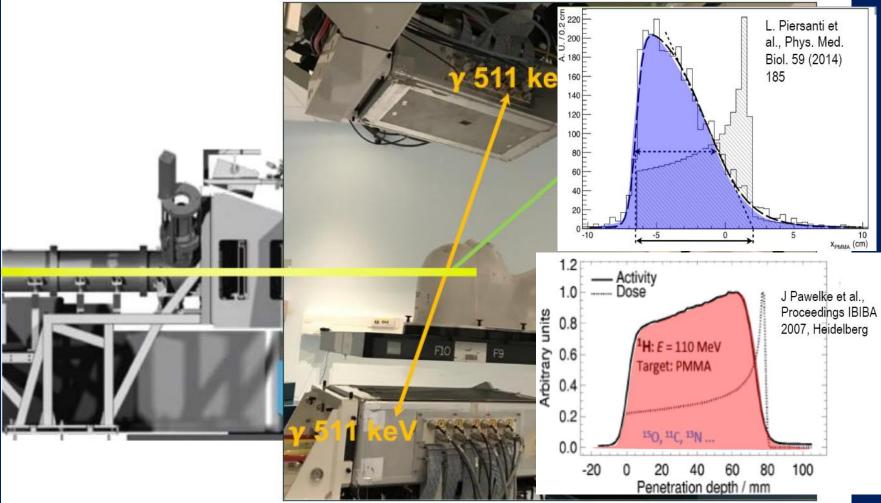
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#### INSIDE OBSERVATIONAL CLINICAL TRIAL

### ClinicalTrials.gov id: NCT03662373

# Courtesy MG Bisogni

Cohort	40 patients treated with particle therapy (20 with protons and 20 with carbon ions)			
Inclusion Criteria	<ul> <li>patients treated at CNAO with protons or carbon ions with horizontal beam line;</li> <li>patients affected by meningioma or squamous cellular rhinopharynx carcinoma treated with proton therapy;</li> <li>patients affected by Adenoid Cystic Carcinoma (ACC) or skull base (clivus) chordoma treated with carbon ion therapy;</li> </ul>			
	<ul> <li>full mechanical compatibility of the INSIDE monitoring system with all medical devices needed during the irradiation;</li> <li>all emergency procedures are possible notwithstanding INSIDE system in the acquisition position;</li> <li>signed written informed consent by patient.</li> </ul>			
Esclusion Criteria	<ul> <li>missing informed consent;</li> <li>not affected by one of the selected pathologies;</li> <li>failure of pre-treatment mechanical compatibility assessment;</li> <li>failure of pre-treatment emergency procedures check;</li> <li>medical or individual reasons.</li> </ul>			



Starts July 2019: first 20 patients, 4-6 weeks monitoring

## Real-time PET for range verification

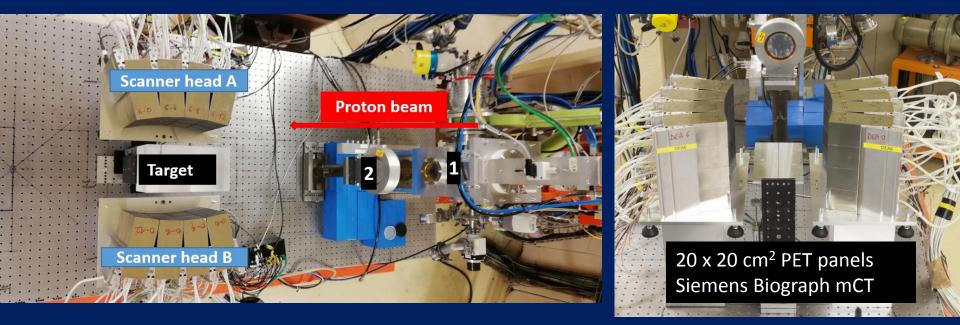
Courtesy P. Dendooven,

S. Brandenburg, I. Ozoemelam, KVI-CART

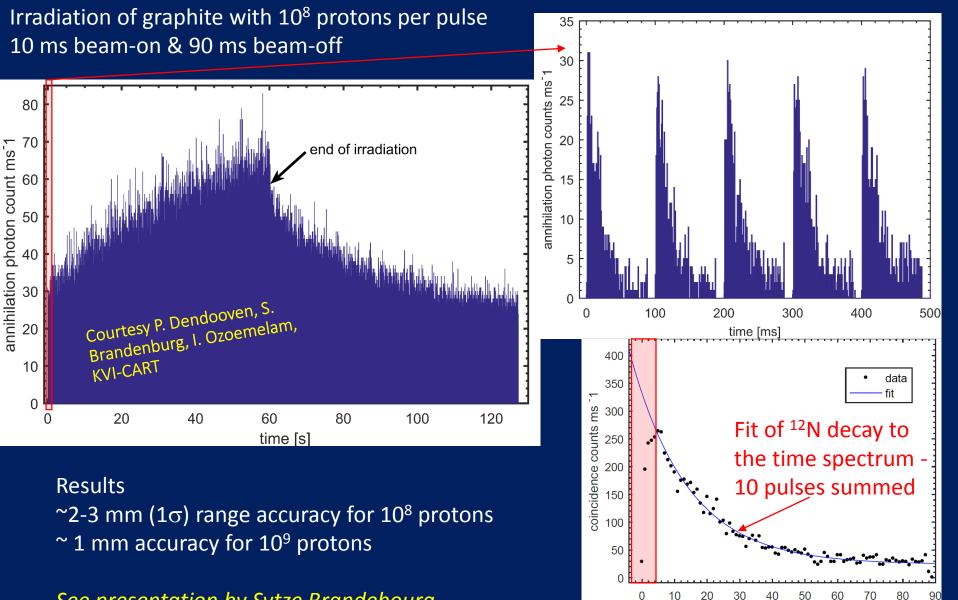
Very short-lived radioisotope: good candidate: N-12 ( $T_{1/2} = 11 \text{ ms}$ ) **Benefits for PET imaging:** 

- maximum number of counts
- minimal biological washout

## **Experimental setup**



## **Real-time PET for range verification**



See presentation by Sytze Brandebourg

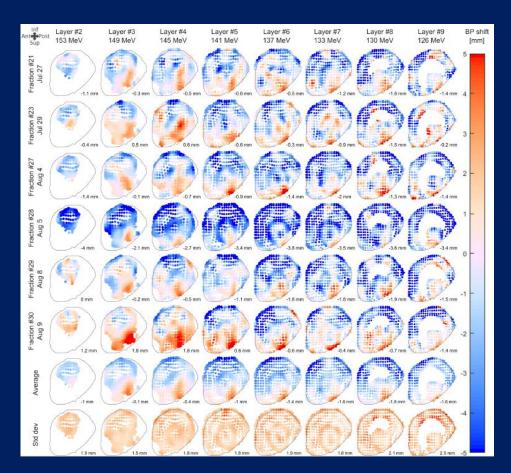
70

pulse time [ms]

# Prompt Gamma: Clinical test of IBA knife-edge camera



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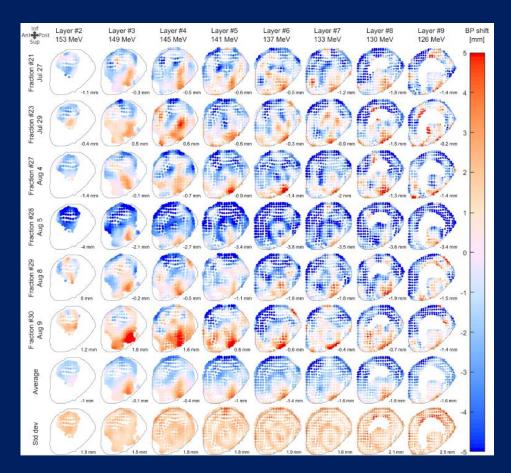


#### Xie et al., Int J Radiat Oncol Biol Phys 2017

Verification during 6 consecutive fractions of head treatment with PBS at Philadelphia → Range uncertainties < margins

Ongoing patient study with PBS at Oncoray-Dresden (Berthold et al, PTCOG 2019)

# Prompt Gamma: Clinical test of IBA knife-edge camera





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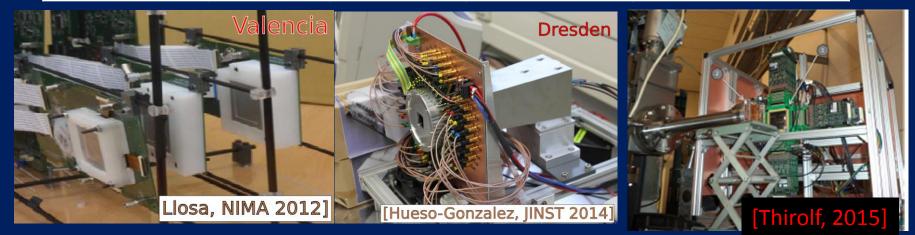
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**Alternative:** Multi-slit collimated camera: comparable performance, larger field of view, inclusion of Time-of-Flight (CLaRyS, Delft, Korea...)

## Compton cameras for hadrontherapy

Group	Scatterer	Absorber	Abs. size (mm)	Status
Valencia	LaBr3	LaBr3	30	In-beam tests
US	CdZnTe	CdZnTe	40	In-beam tests
Dresden	CdZnTe	LSO/BGO	30	tested
Munich	Si	LaBr3	50	Components tested
France CLaRyS	Si	BGO	300	In development



- Assets: higher efficiency at equivalent size Spatial resolution Issues: High rate of random coincidences at clinical beam intensities •
- •

[Ortega PMB 2015], [Rohling PMB 2017], [Fontana IEEE TRPMS 2019] (Lyon)

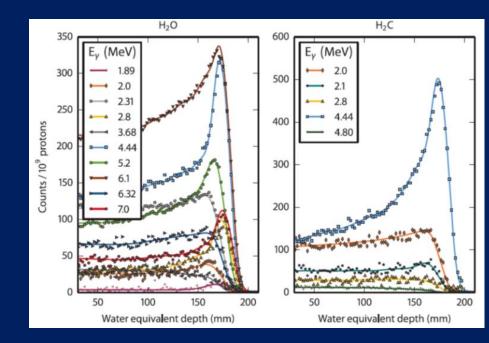
Reconstruction time

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## Prompt Gamma Spectroscopy

## • Idea (Verburg et al, PMB 2014):

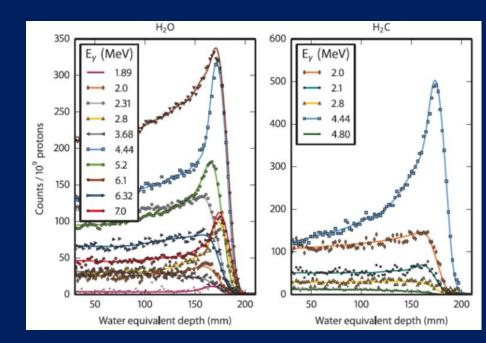
- Individual PG lines depend on
  - proton energy
  - target composition
- High resolution spectroscopy using TOF at given position
  - Collimation
  - synchronization HF cyclotron
- → Range and tissue composition

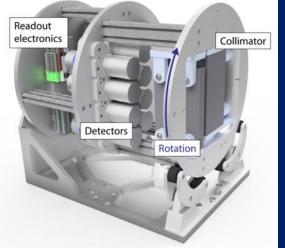


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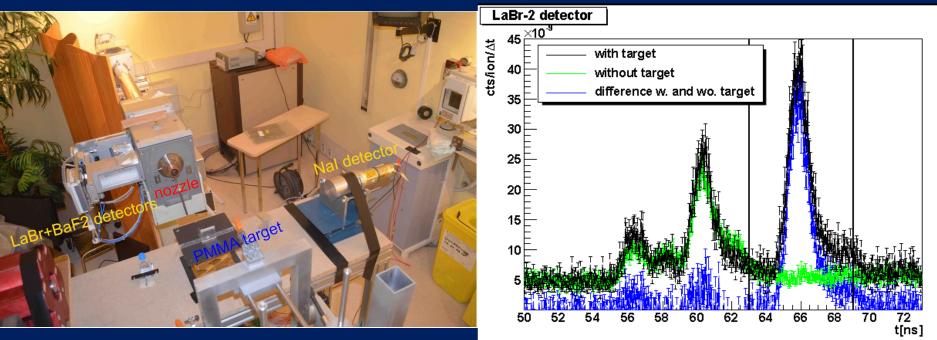




- Prototype (Hueso Gonzáles et al, PMB 2018):
  - Tested at MGH with clinical beams and realistic treatment plans with PBS
  - Ready for clinical tests at MGH (Verburg, PTCOG 2019)
- Extension to He, Li... ions by Seco et al. at HIT synchrotron (beam hodoscope)

## Prompt Gamma Peak Integral

- Basic idea: measure PG issued from the patient (with TOF) with a few detectors around the patient
  - Related to the energy deposited and to the material
  - No severe requirements on TOF precision and energy resolution



Measurements at Essen, HIT, GANIL, CAL, Arronax Protons and carbon

[J. Krimmer, APL 2017]

# Prompt-Gamma Timing

Principle

Golnik et al., PMB 59 (2014) 5399

Detection system

Pausch et al., IEEE TNS 63 (2016) 664

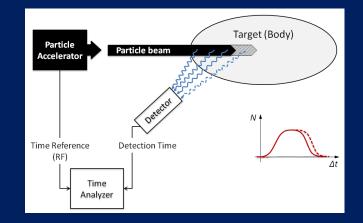
Remaining problems

Werner et al., PMB 64 (2019) 105023

- Instabilities of the time reference caused by accelerator effects
- Integration of proton bunch monitoring in the medical beamline
- Integrating PGT spectrum prediction in IBA's RV software used for PGI

#### Translation to clinical application is on the way.

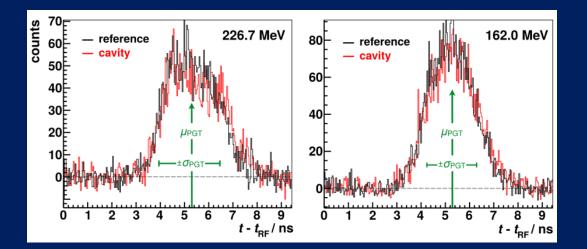






20 mm air cavity in PMMA ~ 1 ns bunch resolution (Werner et al, PMB 2019)

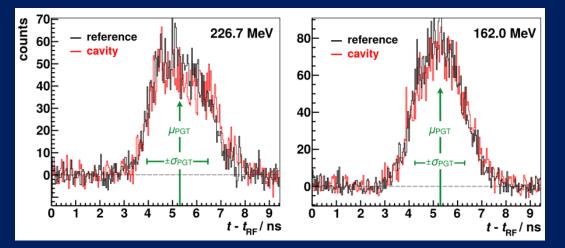
 Best precision achievable = Pulse width (~1 ns)

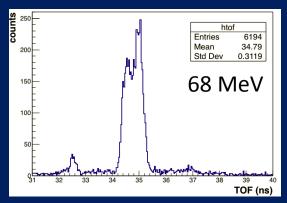


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25 mm air cavity in PMMA Single proton identification with diamond detector in beam (Marcatili et al, submitted APL)

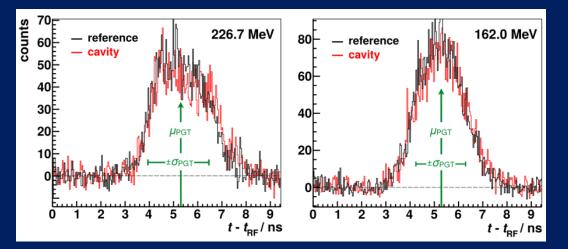


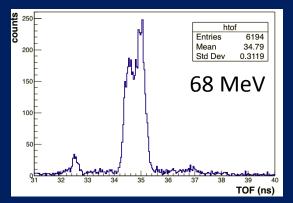


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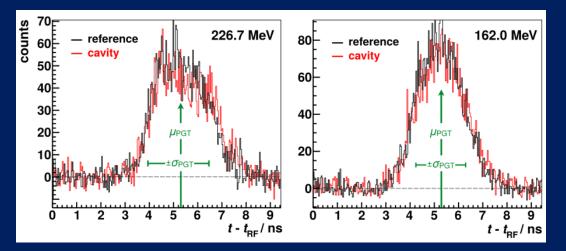


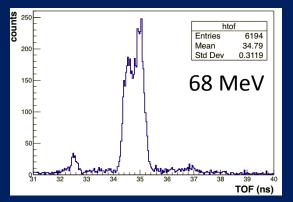
 100 ps timing resolution achieved with diamond beam hodoscope and fast scintillator (see Sébastien Curtoni poster)

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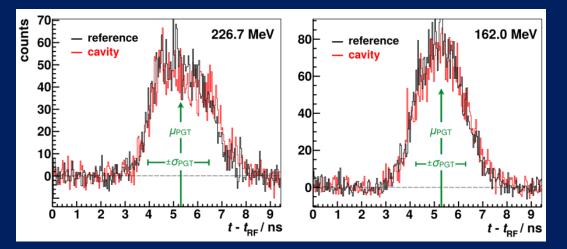


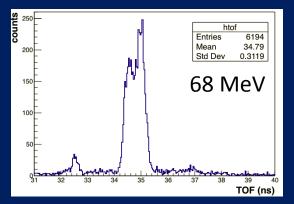
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- 100 ps timing resolution achieved with diamond beam hodoscope and fast scintillator (see Sébastien Curtoni poster)
- Beam reduction to 1 proton/bunch (a few seconds irradiation time increase for few bunches)
- Reconstruction simplified in Compton Imaging (Livingstone et al PTCOG 2019)

## Conclusion

### 15-20 years of developments for range verification

- $\rightarrow$  Clinical tests with PET and PG
- → PET and PG predictions are included in treatment plans Kroniger et al., Med Phys 2015: analytical
  - Tian et al., PMB 2018: MC planning: a few spots "boosted"
- $\rightarrow$  Next generation devices appear (PGS, PGT, PGPI, ...)
- Other promising modalities (Ionoacoustic, Bremsstrahlung, MRI...) + planning imaging (DECT, pCT)
- Strong dependence of the beam temporal structure on the range verification modality

(see paper by G. Pausch et al, NIMA 2019, in press)

- PG will be challenging at higher intensities (Synchro-cyclotron, Flash)
- High performance with reduced intensity

→ Enable one or few spots in 10-30 s at the beginning of a fraction for verification?

## Thanks and Acknowledgements

- G. Bisogni, G. Pausch, P. Dendooven for providing inputs
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