



**HAL**  
open science

## Integrated microfluidic device for the separation, decomposition and detection of low molecular weight S-nitrosothiols

Gerson Duarte-Junior, Abdulghani Ismail, Sophie Griveau, Fanny d'Orlyé,  
José Alberto Fracassi da Silva, Wendell Coltro, Fethi Bedioui, Anne Varenne

► **To cite this version:**

Gerson Duarte-Junior, Abdulghani Ismail, Sophie Griveau, Fanny d'Orlyé, José Alberto Fracassi da Silva, et al.. Integrated microfluidic device for the separation, decomposition and detection of low molecular weight S-nitrosothiols. *Analyst*, 2019, 144 (1), pp.180-185. 10.1039/c8an00757h . hal-02159778

**HAL Id: hal-02159778**

**<https://hal.science/hal-02159778>**

Submitted on 19 Jun 2019

**HAL** is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

1           **Integrated microfluidic device for the separation,**  
2           **decomposition and detection of low molecular weight**  
3           **S-nitrosothiols**

4  
5   Gerson F. Duarte-Junior<sup>a,b</sup>, Abdulghani Ismail<sup>a</sup>, Sophie Griveau<sup>a</sup>, Fanny  
6   d'Orlyé <sup>a</sup>, José Alberto Fracassi da Silva<sup>e</sup>, Wendell K. T. Coltro<sup>b</sup>, Fethi  
7   Bedioui <sup>a</sup>, Anne Varenne<sup>a\*</sup>

8  
9   <sup>a</sup> Chimie ParisTech, PSL Research University, INSERM 1022, CNRS 8258 ,  
10   Paris Descartes, Unité de Technologies Chimiques et Biologiques pour la  
11   Santé, 75005 Paris, France

12   <sup>b</sup> Instituto de Química, Universidade Federal de Goiás, Campus  
13   Samambaia, Goiânia, GO, 74690-900, Brazil

14   <sup>c</sup> Instituto de Química, Universidade Estadual de Campinas, UNICAMP,  
15   Campinas, SP, 13083-970, Brazil

16  
17   \*Corresponding Author. (anne.varenne@chimieparistech.psl.eu)

## 18 **Abstract**

19 S-nitrosothiols (RSNOs) are considered as biological circulating stocks of  
20 nitric oxide (NO) that have many roles *in-vivo*. The variation of RSNOs  
21 proportion occurs in several diseases, which makes them potent  
22 biomarkers. The identification and quantitation of each RSNO is therefore  
23 important for biomedical studies. For now, miniaturized devices have been  
24 used to detect RSNOs, based on their total quantitation without a preceding  
25 separation step. This study reports on an original and integrated  
26 microdevice allowing for the successive separation of low molecular weight  
27 RSNOs, their decomposition under metal catalysis, and the quantitation by  
28 amperometric detection of the produced nitrite, leading to their quantitation  
29 in a single run. For this purpose, a commercial SU-8/Pyrex microfluidic  
30 system was coupled to a portable and wireless potentiostat. Different  
31 operating and running parameters were optimized to achieve the best  
32 analytical performance allowing for LODs of 20  $\mu\text{M}$ . The simultaneous  
33 separation of S-nitrosoglutathione and S-nitrosocysteine was successfully  
34 obtained within 75 s.

35



## 37 **Introduction**

38 S-Nitrosothiols (RSNOs) are nitric oxide (NO) carrier molecules that play  
39 important roles in several physiological functions (vasodilatation and  
40 relaxation<sup>1, 2</sup>, antiplatelet aggregation<sup>3, 4</sup>, antimicrobial<sup>5</sup>, regulation and  
41 signaling protein function<sup>6</sup>...) and pathological events (neurodegenerative  
42 diseases such as Parkinson and Alzheimer<sup>7</sup>, apoptosis<sup>8</sup>, chronic obstructive  
43 pulmonary disease<sup>9</sup>, preeclampsia<sup>10</sup>, diabetes<sup>11</sup>...). RSNOs can be divided  
44 into low molecular weight (LMW) and high molecular weight (HMW)  
45 RSNOs. Although there is no defined border in terms of molecular mass, it  
46 is common to use the term “low molecular weight” for peptides and  
47 aminoacid S-nitrosothiols (such as S-nitrosoglutathione (GSNO) and S-  
48 nitrosocysteine (CySNO)) and “high molecular weight” for s-nitrosylated  
49 proteins (such as S-nitrosoalbumin (AlbSNO) and S-nitrosohemoglobin  
50 (HbSNO)). RSNOs store, transport and release NO. They can also inter-  
51 exchange NO through transnitrosation reaction<sup>13</sup>. The variation of RSNOs  
52 concentration has been shown to occur in many diseases<sup>12</sup>. For all these  
53 reasons, the development of powerful methodologies for the simultaneous  
54 quantitation of all RSNOs in a biological sample is crucial.

55 Numerous methods have been developed for RSNOs analysis, based on  
56 direct or indirect detection. **Examples of direct detection** consist in the

57 separation of RSNOs from other species by capillary electrophoresis (CE)  
58 or liquid chromatography followed by mass spectrometric or  
59 spectrophotometric detection<sup>14</sup>. For example, the simultaneous separation  
60 of S-nitrosoglutathione (GSNO) and S-nitrosocysteine (CySNO) was  
61 performed by our group using conventional CE equipped with capacitively  
62 coupled contactless conductivity detection but in a conventional system<sup>15</sup>.  
63 In another work, the simultaneous separation of GSNO, GSH, glutathione  
64 sulfonic and sulfinic acid by CE coupled to mass spectrometry was  
65 obtained<sup>14</sup>. Most standard methods developed for RSNOs quantitation  
66 reported in the literature remain indirect. They are based on the detection of  
67 their decomposition products<sup>16</sup>, through homolytic or heterolytic cleavage of  
68 S-NO bond generating NO or NO<sup>+</sup> leading finally to NO<sub>2</sub><sup>-</sup>. These  
69 decomposition products are then detected by spectrophotometry,  
70 fluorimetry, electrochemistry or chemiluminescence<sup>16, 17</sup>. Various reagents  
71 have been used to decompose RSNOs, such as metal cations<sup>18</sup> (Hg<sup>2+</sup>,  
72 Cu<sup>+</sup>), light<sup>19</sup> and heat<sup>20</sup>, leading to different decomposition products: NO is  
73 generated<sup>18</sup> if Cu<sup>+</sup>, light or heat are employed, whereas nitrite is directly  
74 generated<sup>18, 21</sup> when Hg<sup>2+</sup> or Ag<sup>+</sup> are used.

75 Nowadays, miniaturization in chemical analysis has become a powerful tool  
76 contributing to reduce the samples/reagents amount, analysis time and

77 waste generation. Such an approach can be beneficial for the quantitation  
78 of RSNOs. Indeed, our group has recently reported on the colorimetric  
79 analysis of RSNOs in a microfluidic paper-based analytical device<sup>22</sup>. This  
80 system allowed to perform analysis of total RSNOs in plasma samples  
81 without any separation step. Other approaches were proposed by Hunter et  
82 al. for NO<sup>23</sup> and total RSNO detection<sup>24</sup> (after light decomposition) using a  
83 single PDMS microfluidic channel with amperometric detection. In all cases  
84 no separation of RSNOs occurred before detection in these miniaturized  
85 devices. Also, Gunasekara et al<sup>25</sup> used microchip capillary electrophoresis  
86 (MCE) with amperometric detection to separate a NO donor  
87 (DEA-NONOate or Proli-NONOate) from NO and nitrite in less than one  
88 minute. Tu et al.<sup>26</sup> used MCE with fluorescence detection to separate and  
89 detect NO, reduced glutathione (GSH) and cysteine (Cys). Herein we report  
90 the design and optimization of a single-run MCE analytical strategy allowing  
91 for the first time the simultaneous quantitation of two low molecular weight  
92 RSNOs (S-nitrosoglutathione and S-nitrosocysteine), thanks to the  
93 integration of successive electrokinetic separation, RSNO decomposition by  
94 Hg<sup>2+</sup> to nitrite and nitrite quantitation by amperometry.

## 95 **Experimental**

### 96 **Chemicals**

97 All reagents were of analytical grade and used as received. L-arginine  
98 (ARG), 2-(N-morpholino) ethanesulfonic acid (MES), acetic acid (HAc), L-  
99 histidine (His), sodium tetraborate, Sodium Nitrite, N-acetyl-p-aminophenol  
100 (Paracetamol), Mercury(II) Chloride, EDTA, hydrochloric acid, sodium  
101 phosphate monobasic, sodium phosphate dibasic, L-cysteine (Cys) and  
102 reduced glutathione (GSH), were purchased from Sigma Aldrich (St. Louis,  
103 MO, USA). All aqueous solutions were made using ultra-pure water with a  
104 resistivity of 18.2 MΩ.cm from a Pure Lab Flex system (ELGA Labwater,  
105 France).

### 106 **Synthesis of S-nitrosothiols**

107 GSNO was synthesized as described elsewhere<sup>27</sup>. Briefly, an equimolar  
108 amount of nitrite was added to the equimolar amount of GSH and HCl. The  
109 resulting pure solid was rinsed once with 80% acetone, twice with 100%  
110 acetone and three times with diethyl ether and then stocked in the dark at  
111 20 °C.

112 S-Nitrosocysteine (CySNO) was daily synthesized using the method  
113 described by Peterson and coworkers<sup>28</sup>. Briefly, solutions of 5 mM CysNO



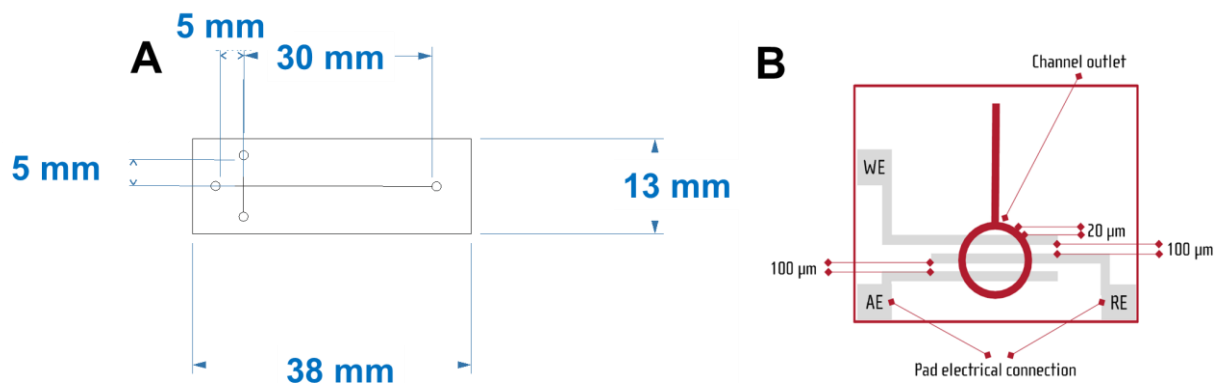
114 were prepared by reacting cysteine with an equimolar concentration of  
115 nitrite in acidic medium (0.1 M HCl) in a dark flask to avoid light  
116 decomposition. After 5 min, more than 90% of cysteine was converted into  
117 CysNO. The solution was neutralized by 0.1 M PBS buffer (pH 7.4)  
118 containing 0.5 mM EDTA to prevent decomposition by trace metal cation  
119 contaminants.

120 Final concentrations of RSNOs were determined spectrophotometrically in  
121 aqueous solution at 335 nm ( $\epsilon = 586$  and  $503 \text{ M}^{-1} \text{ cm}^{-1}$  for GSNO and  
122 CysNO, respectively)<sup>29</sup>.

## 123 **Instrumentation**

124 Electrophoretic experiments were performed using a SU-8/Pyrex  
125 microchips with integrated micro band platinum electrodes at the outlet end  
126 of the separation channel from Micrux Technologies (Oviedo, Spain) (MCE-  
127 SU8-Pt001T) (**Figure 1**). Only working (WE) and reference (RE) electrodes  
128 were used, with widths of 50  $\mu\text{m}$  and 250  $\mu\text{m}$ , respectively. The separation  
129 and injection channel length were 35 mm and 10 mm, respectively. The  
130 microchannels width and depth were 50  $\mu\text{m}$  and 20  $\mu\text{m}$ , respectively. A  
131 microfluidic platform (Oviedo, Spain) (MCE-HOLDER-DC02) was used to  
132 interface the microchip with the amperometric detector and the high voltage

133 source. The high voltage source was a programmable HVS448-3000V 8-  
134 channels high-voltage supply (LabSmith Inc., CA, USA) controlled by  
135 Sequence software v.1.165. Amperometric detection was performed by a  
136 modified model 9051, 2-channel, wireless, portable and electrically isolated  
137 potentiostat (Pinnacle Technology, Lawrence, KS. USA) operating in a  
138 two-electrode format at a 5 Hz sampling rate (gain=5 000 000 V/A,  
139 resolution= 30 fA). This potentiostat is isolated which eliminates  
140 interferences from the high voltage power supply system used for the  
141 separation. This potentiostat was controlled by Sirenia Acquisition Software  
142 v.1.7.6. The WE and RE were connected to the corresponding electrodes  
143 using the commercial chip holder.



144  
145 **Figure 1** - Schematic presentation of A) dimensions and B) design of Micrux MCE-SU8-Pt001T chip.  
146 Adapted from<sup>30</sup>

147  
148 C<sup>4</sup>D detection was performed using a commercial detector model ER815  
149 acquired from eDAQ Pty (Denistone East, Australia). A microfluidic

150 platform EDAQ ET121 containing external electrodes was used to interface  
151 a commercial PMMA microchip (model 02-0750-0082-01, ChipShop, Jena,  
152 Netherlands) with the detection system. This microchip layout comprised  
153 separation and injection channels (50  $\mu\text{m}$  wide/deep) with 87 and 10 mm  
154 long, respectively.

### 155 **Electrophoresis and Decomposition procedure**

156 Prior to analysis, microchannels were conditioned with 0.1 M NaOH,  
157 deionized water and running buffer. Samples of RSNOs and paracetamol  
158 (1 mM each) were electrokinetically injected by gated mode<sup>31</sup> by applying  
159 potentials of 800 V and 1000 V to sample and buffer reservoirs,  
160 respectively, while both waste reservoirs were grounded for the loading  
161 step. The injection was performed by floating the potential at the buffer  
162 reservoir for 3 s, giving the start of the separation step. The same  
163 procedure but under reversed polarity was performed for nitrite (1 mM)  
164 quantitation. For the decomposition step,  $\text{HgCl}_2$  (10 mM) was added in the  
165 detection reservoir. Before RSNOs reach the buffer waste reservoir the  
166 polarity was inverted allowing detection of nitrite generated from  
167 decomposition. For amperometric detection of nitrite and paracetamol,  
168 potentials from 0.7 to 1.2 V vs. Pt were applied. Analysis using  $\text{C}^4\text{D}$   
169 detection was realized under the same electrophoretic conditions and

170 detection was performed applying a sinusoidal signal of 600 kHz and  
171 90 V<sub>peak-to-peak</sub>.

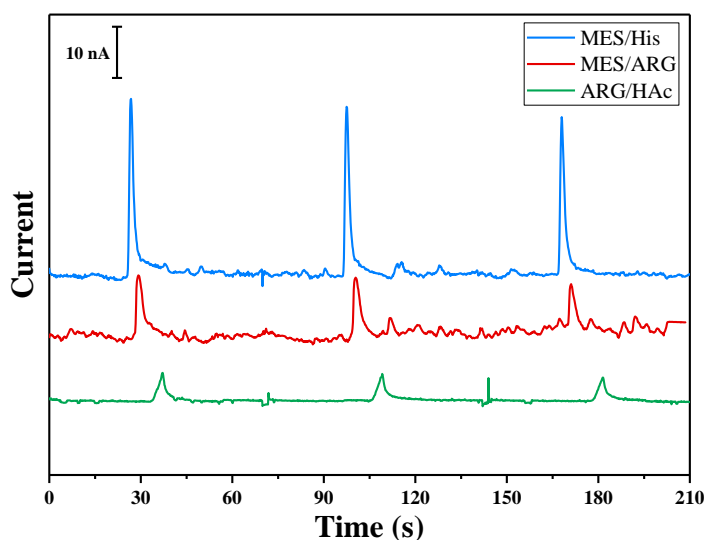
## 172 **Results and discussion**

173 Herein a method for successive separation, decomposition, and detection  
174 of RSNOs is proposed by integrating all the three steps in a microfluidic  
175 device. In order to achieve this goal, the decomposition should be (i) much  
176 faster than the separation process (otherwise the peaks originating from  
177 different RSNOs will overlap) (ii) quantifiable and (iii) the decomposition  
178 product should be stable through the analysis time and operating  
179 conditions. It is well known that the decomposition product of RSNOs  
180 depends on the decomposition agent. As indicated above, the use of  $\text{Cu}^+$  or  
181 light leads to homolytic cleavage and to the formation of  $\text{NO}$ , while the use  
182 of  $\text{Hg}^{2+}$  leads to heterolytic cleavage and to the production of  $\text{NO}^+$  that  
183 transforms immediately to  $\text{NO}_2^-$ . Decomposition of RSNOs by light is slow  
184 (tenth of minutes are needed to decompose the sample<sup>15</sup>) and only partial  
185 decomposition of RSNOs have be obtained by Hunter et al<sup>24</sup> in a  
186 microfluidic device using 530 nm LED.  $\text{Cu}^+$  decomposition is faster than  
187 light decomposition but still insufficient ( $>2 \text{ min}^{32}$ ) in comparison with the  
188 separation time scale. Moreover  $\text{Cu}^+$  is poorly soluble and stable in aqueous  
189 solution and it is usually produced by reduction of  $\text{Cu}^{2+}$  with reducing agent  
190 such as GSH. Decomposition using  $\text{Cu}^{2+}$  is affected by the variation of GSH  
191 concentration in the sample, which is difficult to control<sup>32</sup>. Decomposition

192 using mercuric (II) is instantaneous leading to  $\text{NO}_2^-$  which is stable and  
193 electroactive<sup>33</sup>. Consequently,  $\text{Hg}^{2+}$  was chosen as the decomposition  
194 agent.

195 BGE plays an important role in the migration and electrochemical detection  
196 steps in micro chip electrophoresis (MCE)<sup>34, 35</sup>. As the objective was the  
197 detection of nitrite generated from RSNO decomposition, the BGE  
198 optimization was focused on nitrite signal/noise (S/N) ratio during detection.  
199 Several BGEs usually used for biological samples during MCE were tested  
200 : 20 mM MES / His (pH 6.0), 20 mM MES / Arg (pH 7.5), 20 mM Arg /  
201 Acetic Acid (pH 5.8). Nitrite (1 mM) was injected in the gated mode (see  
202 experimental section), separated and detected by amperometry using these  
203 various BGEs. For each BGE, the detection potential applied between WE  
204 and RE was varied from +0.5 V to +1.5 V keeping constant same  
205 electrophoretic injection and separation conditions. The optimal potential for  
206 nitrite detection in all BGE was 0.7 V. **Figure 2** shows electropherograms  
207 for the separation of nitrite in various BGE. 20 mM MES/His (pH. 6.0)  
208 provided the highest amperometric detection signal. However, it was not  
209 selected for this design as  $\text{Hg}^{2+}$ , that will be used as the decomposition  
210 reagent for RSNO, reacts with histidine to form a precipitate. Although  
211 MES/Arg leads to the highest signal intensity, it however results in the

212 lowest signal to noise ratio. Therefore, the selected BGE, leading to the  
213 highest S/N ratio without interference with other molecules in the solution,  
214 was 20 mM Arg adjusted to pH 5.8 with HAc.



215  
216 **Figure 2** – Electrophoretic separation of 1 mM nitrite in SU-8/Pyrex microchip. BGE: MES (20 mM)/His  
217 (20 mM) pH 6.0 in blue, MES (20 mM)/ Arg (20 mM) pH 7.5 in red, Arg (20 mM) pH 5.8 adjusted with  
218 Acetic Acid in green. Gated injection  $V_1=-800V$ ,  $V_2= -1000V$ , injection time 3s, successive injections: 70s,  
219 detection 0.7 V vs Pt.

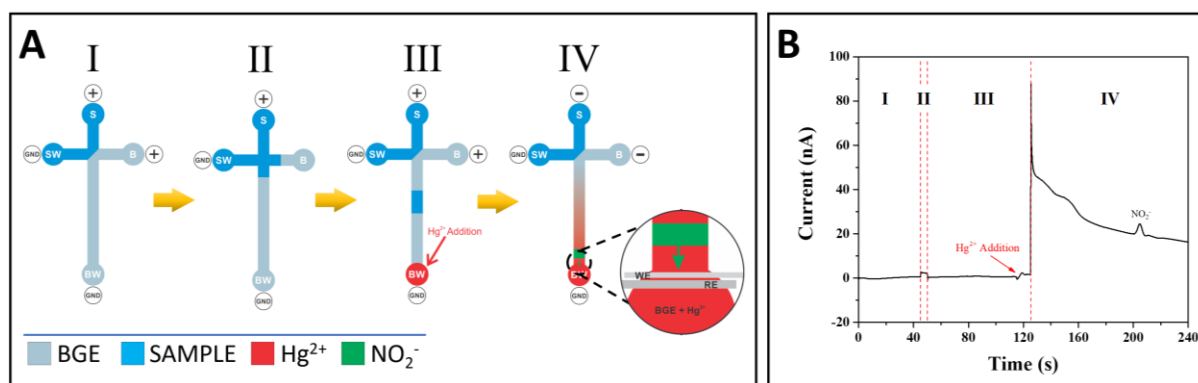
220  
221 For an optimized on-chip integration of the three steps involved in RSNOs  
222 characterization (separation, decomposition and detection) in the microchip,  
223 the apparent mobilities of each of the compounds (different RSNOs, nitrite,  
224 mercury) were determined. The overall procedure was first optimized for  
225 GSNO, as it is the most abundant low molecular weight RSNO. **Control**  
226 **experiments by direct addition of nitrite into the BW reservoir, with or**  
227 **without application of electrophoretic voltage resulted in an amperometric**

228 signal, proving the efficiency of the electrochemical detection step. A  
229 neutral electroactive marker (paracetamol) allowed determining the  
230 electroosmotic mobility as  $1.85 \pm 0.07 \times 10^{-4} \text{ cm}^2 \cdot \text{V}^{-1} \cdot \text{s}^{-1}$  and GSNO  
231 electrophoretic mobility was determined as  $-0.64 \pm 0.06 \times 10^{-4} \text{ cm}^2 \cdot \text{V}^{-1} \cdot \text{s}^{-1}$ ,  
232 employing a C<sup>4</sup>D detector, as GSNO is not electroactive (results not  
233 shown).

234 Under these experimental conditions, GSNO migrates towards the detector  
235 under a positive polarity. The device was primarily developed as follows:  
236 GSNO was electrokinetically injected from the sample reservoir (S) in the  
237 gated mode in positive polarity (see experimental section). Hg<sup>2+</sup> was  
238 introduced in the waste reservoir (connected to the cathode) where it  
239 should decompose GSNO into nitrite upon reaching the buffer waste  
240 reservoir (BW). However, no amperometric signal was observed (results not  
241 shown). One hypothesis is based on the fact that Hg<sup>2+</sup> undergoes diffusion  
242 from the BW within the separation channel, inducing the GSNO  
243 decomposition within the separation channel. As nitrite electrophoretic  
244 mobility under these experimental conditions ( $-4.25 \times 10^{-4} \text{ cm}^2 \cdot \text{V}^{-1} \cdot \text{s}^{-1}$ ) is  
245 higher in absolute value than the electroosmotic mobility, nitrite moves back  
246 to the sample reservoir (S) instead of the BW reservoir where it should be  
247 detected.



248 A new design was then developed, including an additional step allowing for  
 249 voltage inversion just before GSNO decomposition (**Figure 3A**). In this new  
 250 design, the loading, injection and separation steps were performed under  
 251 positive polarity (step I, II and III, respectively),  $\text{Hg}^{2+}$  is added before GSNO  
 252 reaches the channel end in step III, and polarity is inverted (step IV). This  
 253 inversion of polarity leads to the migration of  $\text{Hg}^{2+}$  and GSNO **to** the sample  
 254 reservoir (S). As  $\text{Hg}^{2+}$  migrates faster than GSNO, the migration zone of  
 255  $\text{Hg}^{2+}$  enters that of GSNO, allowing for GSNO decomposition. The  
 256 produced nitrite migrates towards the BW reservoir and is detected (**see**  
 257 **detail in step IV, Figure 3A**). A typical electropherogram obtained  
 258 characterizing all the analytical steps is presented in **Figure. 3B**. Control  
 259 experiments (without  $\text{Hg}^{2+}$  or without GSNO) did not show any signal (data  
 260 not shown).

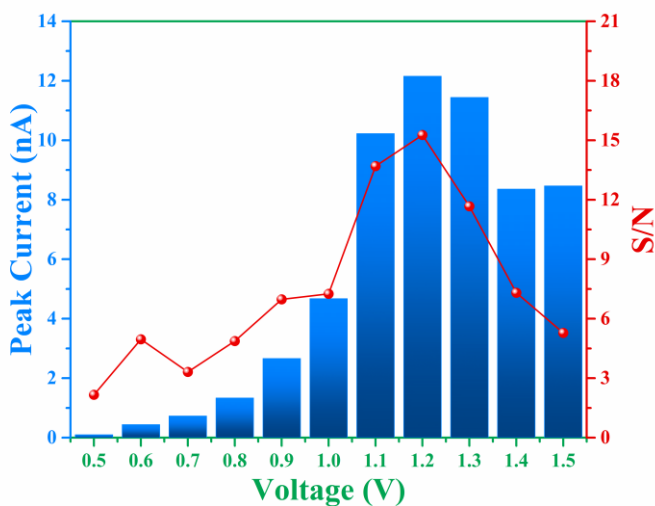


261  
 262 **Figure 3** - (A) Scheme of the main steps for RSNOs quantitation. Loading step (I): Voltages of 800 and  
 263 1000 V are applied during 45 s to the sample (S) and buffer (B) reservoirs, respectively, grounding both  
 264 waste reservoirs (SW and BW). Injection step (II): samples are injected into separation channel by  
 265 floating the voltage applied to B reservoir during 3 s. Migration step (III): The potentials were then re-  
 266 established to step I condition allowing the migration of RSNO sample towards separation channel. 15 s  
 267 before the end of this step,  $\text{Hg}^{2+}$  was added to BW reservoir. Inversion and detection step (IV): In this

268 step the potential polarity is inverted which leads to the migration of  $\text{Hg}^{2+}$  into the separation channel  
269 faster than RSNO leading to RSNO decomposition. This is followed by nascent nitrite (in green) opposite  
270 migration towards the electrodes and detection by applying a potential of 1.2 V vs *Pt*. (B) Typical  
271 electropherogram obtained for GSNO (1 mmol/L) analysis characterising all the steps of the process.

272

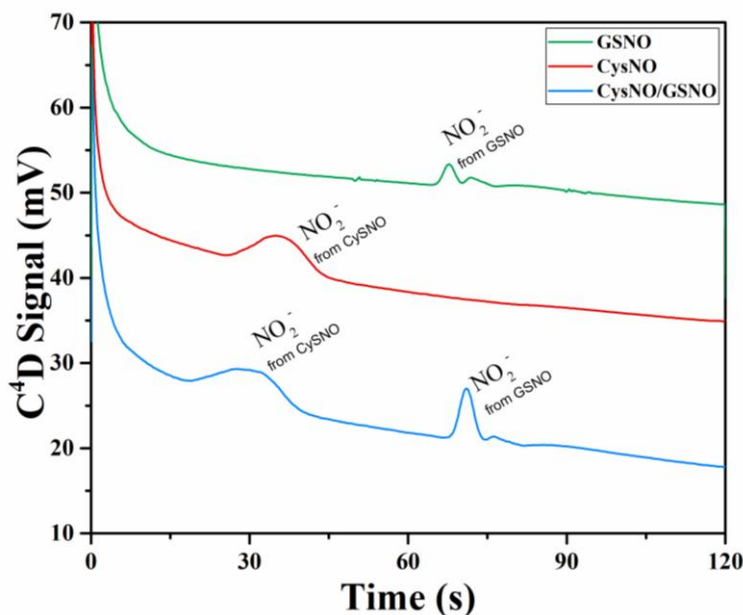
273 Therefore, the overall integrated protocol includes (1) a separation of the  
274 RSNOs under positive polarity, (2) an inversion of the separation polarity,  
275 (3) a decomposition of RSNO thanks to the on-line crossing and mixing of  
276 RSNO and  $\text{Hg}^{2+}$  zones, respectively, due to different migration velocities,  
277 (4) the migration of the produced nitrite to the detector. So as to further  
278 optimize the experimental conditions to improve the limit of detection for  
279 nitrite, three parameters were studied; the BGE ionic strength (from 10 to  
280 50 mM), the detection voltage (from 0.5 to 1.5 V vs *Pt*) and the time of  
281 polarity inversion. Considering the two first parameters, best signal  
282 intensities and S/N ratios for nitrite detection were obtained for a detection  
283 potential of 1.2 V (**Figure 4**).



284  
 285 **Figure 4** - Histogram of peak current (in nA) and signal-to-noise ratio (S/N) of nitrite (1 mM) injection in  
 286 SU-8/Pyrex microchip obtained by variation of the detection potential from 0.5 to 1.5 V vs Pt. BGÉ: 20 mM  
 287 arginine solution adjusted at pH 5.6 with acetic acid.

288  
 289 The time of polarity inversion is a crucial parameter as it should allow for  
 290 the best separation of the RSNOs, their total decomposition and their  
 291 optimal detection. For each studied compound, the electroosmotic and  
 292 apparent mobilities must therefore be determined. For RSNOs of positive  
 293 apparent mobility, the time of inversion should be chosen between the  
 294 migration time of the neutral marker and the one of the RNSOs. This  
 295 parameter was optimized for GSNO and CysNO. CysNO, another important  
 296 nitrosothiol, as it is smaller than GSNO and with similar charge at this pH,  
 297 presents a higher apparent mobility than GSNO. The best signal intensities  
 298 were obtained for an inversion time of 90 s and 75 s, for GSNO and CysNO  
 299 respectively (**Figure 5**). These results indicate the versatility of the

300 procedure for all types of RSNO. In these experimental conditions, the  
301 analytical performances of this methodology were determined for GSNO.  
302 The linearity was verified in the 100-700  $\mu\text{M}$  concentration range ( $y=0.0485$   
303  $x - 5.0485$ ,  $R^2=0.9936$ ) with a LOD of 20  $\mu\text{M}$

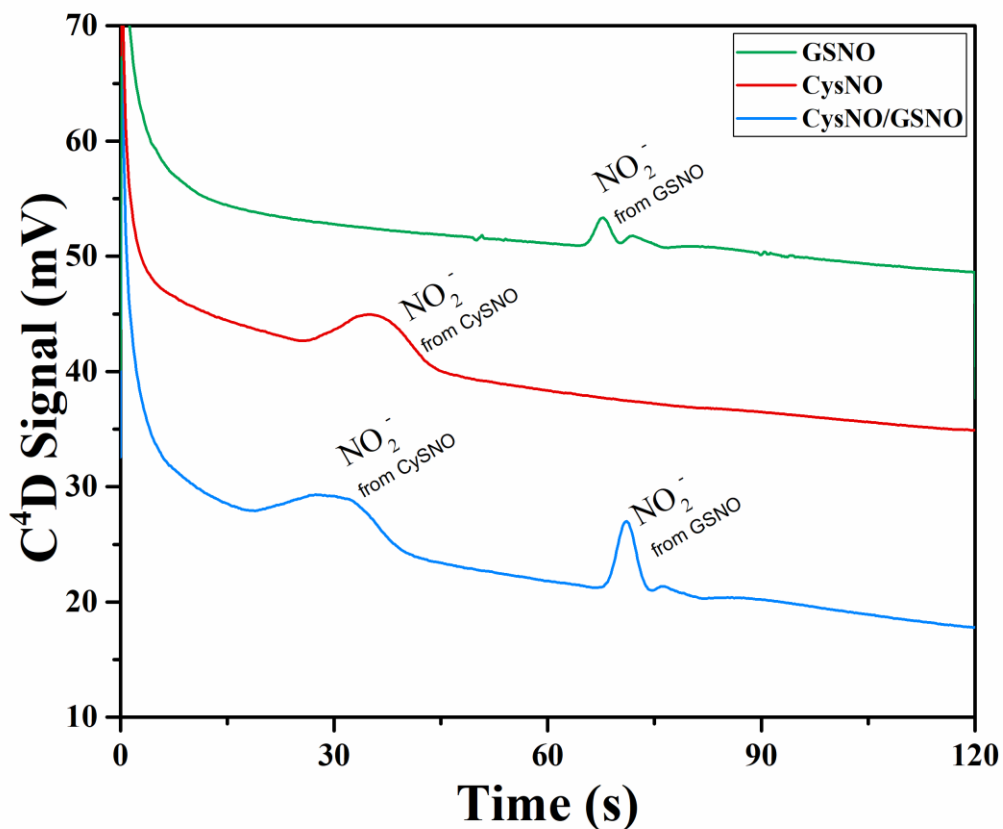


304  
305 **Figure 5** - Electropherograms for detection of 1 mM GSNO (Black) and 1 mM CysNO (Red and Blue) to  
306 determine the time of polarity inversion. In black and red 90 s was used for inversion while in blue 75 s.  
307 BGE: 20 mM arginine solution adjusted at pH 5.6 with acetic acid.

308  
309 The final objective of such a micro-total analysis system is to allow for the  
310 simultaneous quantitation of various RSNOs. Therefore three main  
311 challenges have to be addressed : (i) the efficient separation of the different  
312 RSNOs, (ii) the choice of a unique time of polarity inversion in the process,  
313 and (iii) the efficient detection of the successive nitrite zones produced from  
314 each RSNOs decomposition.

315 The simultaneous separation of GSNO and CysNO was performed so as to  
316 prove the versatility of the system. For this purpose, GSNO and CysNO were  
317 first separated and detected individually. The crucial parameter being the  
318 inversion time, different values were applied from 75 to 90 s. In a second  
319 step, an equimolar mixture of CysNO and GSNO (1 mM each) was  
320 separated and detected. **Figure 6** presents the resulting electropherograms  
321 for an optimized inversion time of 75 s that corresponds to the migration  
322 time of CysNO. As expected the signal arising from GSNO appears after  
323 the one of CysNO, as CysNO has a higher apparent mobility. These results  
324 indicate a powerful simultaneous separation and indirect detection of  
325 GSNO and CysNO. The similar intensities for GSNO and CysNO, injected  
326 at the same concentration indicate that decomposition efficiency is similar  
327 in both cases. This method is therefore applicable for the quantitation of  
328 pharmaceutical RSNOs, future drug candidates. Some work is in progress  
329 for decreasing the LODs to reach biological concentrations (less than 16  
330  $\mu\text{M}^{22}$ ).

331



332

333 **Figure 6** - Electropherograms corresponding to the electrophoretic profile of CysNO (1 mM), GSNO (1  
 334 mM) and mixture GSNO (1 mM) / CysNO (1 mM) in blue, red and black, respectively. Experiments were  
 335 performed in Su-8/pyrex microchip with gated injection. Procedure : (1) 3s injection, (12) application of  
 336 V1=800V, V2=1000V , during 3 minutes (not visible on the graph as it occurs before running the  
 337 electropherogram), (3) addition of  $Hg^{2+}$  at t=0s of the electropherogram, and inversion of polarity V1=-  
 338 800V, V2= -1000V for t=100s. Detection 1V vs Pt. BGE: ARG 20 mM adjusted to pH 5.8 with HAC

## 339 **Conclusions**

340 An original method to simultaneously quantify two low molecular RSNOs in  
341 a mixture using MCE was developed. A commercial microchip of SU-  
342 8/Pyrex microchip and a wireless isolated potentiostat were used. After the  
343 electrokinetic separation step, an inversion of electrokinetic polarity was  
344 necessary to mix the RSNOs with the decomposition agent within the  
345 separation channel and detect the produced nitrite by amperometric  
346 detection at the buffer waste reservoir. Optimization of BGE composition  
347 and detection potential were performed in order to obtain the best signal  
348 intensity and S/N ratio. The LODs were 20  $\mu\text{M}$  for GSNO and CysNO. This  
349 methodology can be applied for the quantitation of pharmaceutical RSNOs,  
350 future drug candidates. Using a more environmental friendly decomposition  
351 reagent such as immobilized gold nanoparticles is envisaged. The method  
352 developed herein has shown to be versatile, opening the way to the  
353 quantitation of complex mixtures of RSNOs.

354

## 355 **Conflicts of interest**

356 The author declares no conflicts of interest.

## 357 **Acknowledgements**

358 Financial support from “Coordenação de Aperfeiçoamento de Pessoal de  
359 Nível Superior (CAPES)” and “French Committee for the Evaluation of  
360 Academic and Scientific Cooperation with Brazil (COFECUB)” (grant n°  
361 802-14) is acknowledged.

## 362 References

- 363 1. B. T. Mellion, L. J. Ignarro, C. B. Myers, E. H. Ohlstein, B. A. Ballot, A. L. Hyman  
364 and P. J. Kadowitz, *Mol. Pharmacol.*, 1983, **23**, 653-664.
- 365 2. J. S. Stamler, D. I. Simon, J. A. Osborne, M. E. Mullins, O. Jaraki, T. Michel, D. J.  
366 Singel and J. Loscalzo, *Proc. Natl. Acad. Sci. U.S.A.*, 1992, **89**, 444-448.
- 367 3. E. J. Langford, A. S. Brown, R. J. Wainwright, A. J. Debelder, M. R. Thomas, R.  
368 E. A. Smith, M. W. Radomski, J. F. Martin and S. Moncada, *Lancet*, 1994, **344**,  
369 1458-1460.
- 370 4. M. W. Radomski, D. D. Rees, A. Dutra and S. Moncada, *Br. J. Pharmacol.*, 1992,  
371 **107**, 745-749.
- 372 5. G. F. P. de Souza, J. K. U. Yokoyama-Yasunaka, A. B. Seabra, D. C. Miguel, M.  
373 G. de Oliveira and S. R. B. Uliana, *Nitric Oxide-Biol. Chem.*, 2006, **15**, 209-216.
- 374 6. C. G. Kevil and R. P. Patel, *Curr. Opin. Investig. Drugs*, 2010, **11**, 1127-1134.
- 375 7. M. Ito, *Annu. Rev. Neurosci.*, 1989, **12**, 85-102.
- 376 8. A. R. Butler and P. Rhodes, *Anal. Biochem.*, 1997, **249**, 1-9.
- 377 9. K. M. Beeh, J. Beier, N. Koppenhoefer and R. Buhl, *Chest*, 2004, **126**, 1116-  
378 1122.
- 379 10. V. A. Tyurin, S. X. Liu, Y. Y. Tyurina, N. B. Sussman, C. A. Hubel, J. M. Roberts,  
380 R. Taylor and V. E. Kagan, *Circ. Res.*, 2001, **88**, 1210-1215.
- 381 11. A. B. Milsom, C. J. H. Jones, J. Goodfellow, M. P. Frenneaux, J. R. Peters and P.  
382 E. James, *Diabetologia*, 2002, **45**, 1515-1522.
- 383 12. M. W. Foster, T. J. McMahon and J. S. Stamler, *Trends Mol. Med.*, 2003, **9**, 160.
- 384 13. B. C. Smith and M. A. Marletta, *Curr. Opin. Chem. Biol.*, 2012, **16**, 498-506.
- 385 14. A. Ismail, F. d'Orlyé, S. Griveau, J. A. F. Da Silva, F. Bedioui and A. Varenne,  
386 *Anal. bioanal. chem.*, 2015, **407**, 6221-6226.
- 387 15. A. Ismail, F. d'Orlye, S. Griveau, F. Bedioui, A. Varenne and J. A. F. da Silva,  
388 *Electrophoresis*, 2015, **36**, 1982-1988.
- 389 16. S. Griveau and F. Bedioui, *Analyst*, 2013, **138**, 5173-5181.
- 390 17. D. Giustarini, A. Milzani, I. Dalle-Donne and R. Rossi, *J. Chromatogr. B*, 2007,  
391 **851**, 124-139.
- 392 18. D. L. H. Williams, *Acc. Chem. Res.*, 1999, **32**, 869-876.
- 393 19. M. M. Veleparampil, U. K. Aravind and C. T. Aravindakumar, *adv. phys. chem.*,  
394 2009, **2009**.
- 395 20. M. G. de Oliveira, S. M. Shishido, A. B. Seabra and N. H. Morgon, *J. Phys.*  
396 *Chem. A*, 2002, **106**, 8963-8970.



- 397 21. H. R. Swift and D. L. H. Williams, *J. Chem. Soc., Perkin Trans. 2*, 1997, 1933-  
398 1935.
- 399 22. A. Ismail, M. O. Araujo, C. L. S. Chagas, S. Griveau, F. D'Orlye, A. Varenne, F.  
400 Bedioui and W. K. T. Coltro, *Analyst*, 2016, **141**, 6314-6320.
- 401 23. R. A. Hunter, B. J. Privett, W. H. Henley, E. R. Breed, Z. Liang, R. Mittal, B. P.  
402 Yoseph, J. E. McDunn, E. M. Burd, C. M. Coopersmith, J. M. Ramsey and M. H.  
403 Schoenfisch, *Anal. Chem.*, 2013, **85**, 6066-6072.
- 404 24. R. A. Hunter and M. H. Schoenfisch, *Anal. Chem.*, 2015, **87**, 3171-3176.
- 405 25. D. B. Gunasekara, M. K. Hulvey, S. M. Lunte and J. A. F. da Silva, *Anal. Bioanal.*  
406 *Chem.*, 2012, **403**, 2377-2384.
- 407 26. F. Q. Tu, L. Y. Zhang, X. F. Guo, Z. X. Zhang, H. Wang and H. S. Zhang, *J.*  
408 *Chromatogr. A*, 2014, **1359**, 309-316.
- 409 27. J.-W. Yoo, G. Acharya and C. H. Lee, *Biomaterials*, 2009, **30**, 3978-3985.
- 410 28. L. A. Peterson, T. Wagener, H. Sies and W. Stahl, *Chem. Res. Toxicol.*, 2007, **20**,  
411 721-723.
- 412 29. R. A. Hunter and M. H. Schoenfisch, *Anal. Chem.*, 2015, **87**, 3171-3176.
- 413 30. <https://www.micruxfluidic.com/en/> Accessed on 04/12/2018
- 414 31. S. C. Jacobson, S. V. Ermakov and J. M. Ramsey, *Anal. Chem.*, 1999, **71**, 3273-  
415 3276.
- 416 32. A. Ismail, S. Griveau, F. d'Orlyé, A. Varenne and F. Bedioui, *Electroanalysis*,  
417 2015, **27**, 2857-2863.
- 418 33. B. Thirumalraj, S. Palanisamy, S.-M. Chen and D.-H. Zhao, *J. Colloid Interface*  
419 *Sci.*, 2016, **478**, 413-420.
- 420 34. P. Kubáň and P. C. Hauser, *Electrophoresis*, 2009, **30**, 3305-3314.
- 421 35. J. L. Beckers and P. Boček, *Electrophoresis*, 2003, **24**, 518-535.

422