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# Evolution of real contact area under shear and the value of static friction of soft materials

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**The frictional properties of a rough contact interface are controlled by its area of real contact, the dynamical variations of which underlie our modern understanding of the ubiquitous rate-and-state friction law. In particular, the real contact area is proportional to the normal load, slowly increases at rest through aging, and drops at slip inception. Here, through direct measurements on various contacts involving elastomers or human fingertips, we show that the real contact area also decreases under shear, with reductions as large as 30%, starting well before macroscopic sliding. All data are captured by a single reduction law enabling excellent predictions of the static friction force. In elastomers, the area-reduction rate of individual contacts obeys a scaling law valid from micrometer-sized junctions in rough contacts to millimeter-sized smooth sphere/plane contacts. For the class of soft materials used here, our results should motivate first-order improvements of current contact mechanics models and prompt reinterpretation of the rate-and-state parameters.**

area of real contact | rough contact | elastomer | static friction | rate-and-state friction

**R**ough solids in dry contact touch only at their highest asperities, so that real contact consists of a population of individual microjunctions (Fig. 1*B*), with a total area  $A^R$ .  $A^R$  is usually much smaller than the apparent contact area,  $A^A$ , that one would expect for smooth surfaces. Since the seminal work of Bowden and Tabor (1), it is recognized that the frictional properties of such multicontact interfaces are actually controlled by  $A^R$  rather than by  $A^A$ . In particular, direct measurements of  $A^R$  on transparent interfaces have been developed (2, 3) and repeatedly found proportional to the friction force, both for multicontacts (4–10) and for single contacts between smooth bodies (1, 11, 12), with the proportionality constant being the contact's frictional shear strength,  $\sigma$ .  $A^R$  is a dynamic quantity with three major causes for variations.

First,  $A^R$  is roughly proportional to the normal load applied to multicontacts (5, 6, 10). This result, which provides an explanation for Amontons–Coulomb's law of friction (friction forces are proportional to the normal force), has been reproduced by many models of weakly adhesive rough contacts under purely normal load (1, 4, 13–16). In the case of independent elastic microjunctions, although each of them grows nonlinearly with normal load, proportionality arises statistically due to randomness in the surface asperities' heights (13). Second, in static conditions,  $A^R$  slowly increases, typically logarithmically, with the time spent in contact (5, 17). This phenomenon, so-called geometric aging (18), is interpreted as plastic (5, 19, 20) or viscoelastic (21) creep at the microjunctions, depending on the materials in contact, and is different from contact strengthening with time at constant contact area (18, 22), so-called structural aging. Third, at the onset of sliding of the interface, the population of already aged microjunctions gradually slips and is replaced

by new, smaller microjunctions. Slip inception is thus accompanied by a drop of  $A^R$  (5, 17), by up to a few tens of percent. This effect is often considered to be the origin of the difference between the peak (static) and steady sliding (kinematic) friction forces (18).

Accounting for these three dependencies together has been a major success in the science of friction because it provides a consistent picture of the physical mechanisms underlying the ubiquitous state-and-rate friction law (5, 18, 20–31), which is obeyed by multicontacts in a variety of materials, from polymer glasses to rocks, through rubber and paper. However, a series of experimental observations reported here and there in the literature over recent decades suggest that the picture may not be fully comprehensive yet. These observations, made on smooth contacts, have repeatedly indicated that the area of apparent contact,  $A^A$ , depends on the value of the tangential load,  $Q$ , applied to the interface. For instance, smooth metallic sphere/plane contacts typically grow as  $Q$  increases (1, 2), due to plastic deformations in the vicinity of the contact (1, 32). Conversely,  $A^A$  decreases when smooth elastomer-based sphere/plane contacts as well as fingertip contacts are increasingly sheared (9, 33–38), presumably due to viscoelastic and/or adhesion effects (33, 36, 38–40). It is therefore tempting to hypothesize that not only smooth but also rough interfaces have a dependence of their contact area on the tangential load,  $Q$ . Such a dependence would directly affect the resistance to sliding of a rough contact, the way we use current contact and friction models to predict the static friction force, and the physical meaning of the parameters of the rate-and-state friction law. To test this hypothesis, we carried out experiments to monitor, in multicontacts involving elastomers or human fingertips, the evolution of  $A^R$  when  $Q$  is increased from 0 to macroscopic sliding.

## Significance

**We investigate the origin of static friction, the threshold force at which a frictional interface starts to slide. For rough contacts involving rubber or human skin, we show that the real contact area, to which static friction is proportional, significantly decreases under increasing shear, well before the onset of sliding. For those soft materials, our results will impact how we use and interpret current contact mechanics and friction models.**

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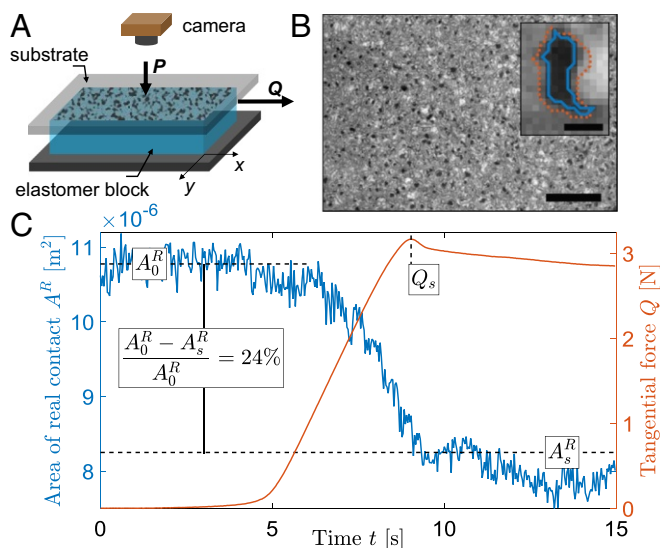
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**Fig. 1.** Monitoring the area of real contact of elastomeric multicontact interfaces. (A) Sketch of the experiment. (B) Typical image of a PDMS/cross-linked PDMS multicontact.  $A^R/A^A \approx 2.05\%$ .  $R_q = 20 \mu\text{m}$ .  $P = 2.08 \text{ N}$ . (Scale bar:  $1.87 \text{ mm}$ .) (B, *Inset*) Zoom-in on a microjunction. Red (resp. blue): contour for  $Q = 0$  (resp. under shear, at the onset of sliding). (Scale bar:  $100 \mu\text{m}$ .) (C) Typical concurrent evolution of the area of real contact (blue) and the tangential force (red), of the multicontact interface shown in B, as a function of time (1 point of 10 shown).  $A_0^R$  ( $A_s^R$ ): initial area (at static friction).  $Q_s$ : static friction force.  $P = 2.08 \text{ N}$ .  $V = 0.1 \text{ mm/s}$ .

### Principle of the Experiments

Fig. 1A shows a sketch of the experimental setup configured for elastomeric contacts, similar to that used in ref. 41 (*Materials and Methods*). A slider made of a flat, smooth bare glass plate is placed in frictional contact onto a rough elastomer block [cross-linked polydimethylsiloxane (PDMS) rms roughness  $R_q$ ] adhering to the table. The slider is driven horizontally, through a steel wire attached in the plane of the contact interface [to avoid torque buildup (42)], by a motorized linear stage moving along  $x$  at constant velocity  $V$  ranging from  $0.05 \text{ mm}\cdot\text{s}^{-1}$  to  $1 \text{ mm}\cdot\text{s}^{-1}$ . The normal load,  $P$ , is applied using dead weights in the range  $0\text{--}7 \text{ N}$  and the tangential force,  $Q$ , is monitored as the slider is driven toward macroscopic sliding. Noninvasive, in situ contact imaging is done in a light-reflected geometry by illuminating the interface from the top with a diffuse white light. Good contrast between real contact and out-of-contact regions is obtained due to heterogeneous reflection properties of the contact interface (Fig. S1): Real contact regions appear dark because light is transmitted through the transparent elastomer and absorbed by a black layer below the elastomer block; out of contact regions appear brighter because light is partly reflected by the glass/air dioptré and partly back scattered by the micrometer rough air/PDMS dioptré. Images of the interface are recorded with a CCD camera in synchronization with the tangential force. The images are efficiently binarized using automatic thresholding (*Materials and Methods*) to identify each microjunction (blue contour in Fig. 1B, *Inset*). The type of substrate (bare glass) is varied (*Materials and Methods*) by coating the slider's glass surface either with grafted PDMS chains or with a layer of cross-linked PDMS. We always start tangential loading 30 s after the contact has first been formed. Because the rate of geometrical aging becomes, in less than 10 s, negligible compared with the shear-induced variations of  $A^R$  described in the next section, it will have a negligible role in those variations. Also, the constant waiting time will ensure that structural aging, if active, will always affect the value of the static friction

force in the same way and thus will not be responsible for its variations.

### The Area of Real Contact Decreases Under Shear

Analysis of multicontact interfaces sheared toward macroscopic sliding revealed the typical behavior shown in Fig. 1C. The area of real contact,  $A^R$ , i.e., the sum of all individual areas of microjunctions, is found to decrease, by up to 30%, under increasing tangential force,  $Q$ . The reduction begins as soon as  $Q$  starts increasing and continues until the macroscopic sliding regime is reached, in which  $A^R$  remains roughly constant around its minimum. Similar observations were made irrespective of the interface type, roughness, normal load, and driving velocity. Note that no abrupt drop of the area of real contact is associated with the onset of sliding, when  $Q$  reaches  $Q_s$ .

Inspection of individual asperities (Fig. 1B, *Inset*) reveals that, under shear, most of them undergo a reduction of their area of real contact, showing that the macroscopic effect actually originates at the microjunction level. Note that since the glass surface is smooth, microjunctions formed under pure normal load remain in contact during shear.

Plotting  $A^R$  as a function of  $Q$  for different normal loads  $P$  applied to a multicontact (Fig. 2A) is an interesting way of identifying the law of area reduction. For all normal loads and all interface types, the decrease of  $A^R$  is found to be well fitted by an empirical quadratic law of the form

$$A^R(Q) = A_0^R - \alpha_R Q^2, \quad [1]$$

with  $A_0^R = A^R(Q = 0)$  the fitted initial area of real contact.  $A_0^R$  increases linearly with  $P$  (Fig. S2), which is classical for rough contacts. All dependences of the area reduction rate on system parameters are lumped into the fitting parameter  $\alpha_R$ .

### Onset of Sliding

The reduction in area of real contact stops soon after the tangential force has reached its maximum, the static friction force  $Q_s$ , which classically marks the onset of macroscopic sliding of the interface. The corresponding value of  $A^R$  is denoted  $A_s^R$ . Data corresponding to the macroscopic sliding regime cluster around a value of  $Q$  slightly smaller than  $Q_s$ . Interestingly, all points marking the onset of sliding in the  $A^R(Q)$  plot in Fig. 2A align well on a straight line going through the origin. This shows that, for our multicontacts,

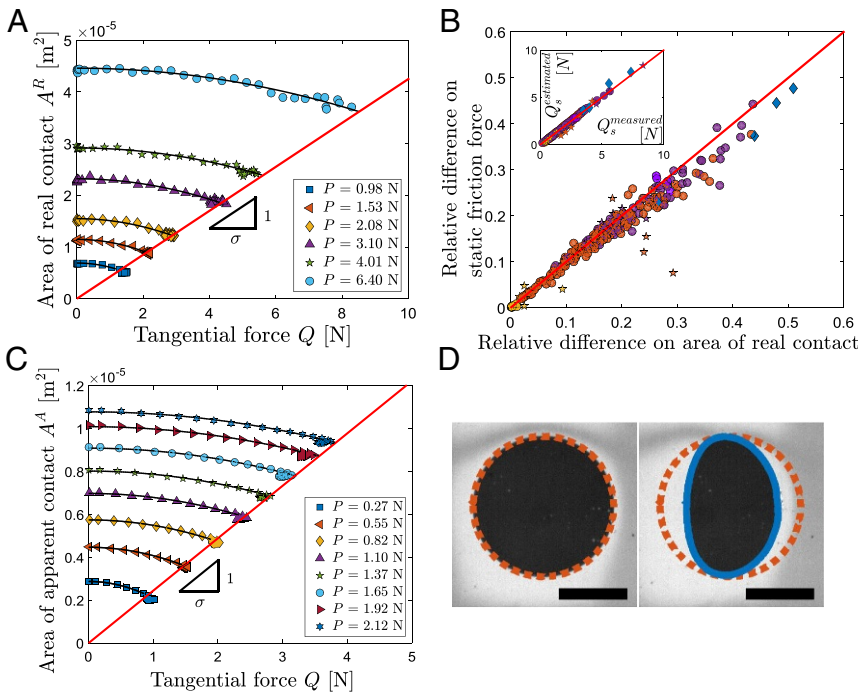
$$Q_s = \sigma A_s^R, \quad [2]$$

with  $\sigma$  being the static contact's shear strength, which characterizes the frictional interaction between the two materials in contact (see *Materials and Methods* for values of  $\sigma$  for all interface types).

Introducing Eq. 2 in Eq. 1 leads to an expression of the relative area decrease along a given experiment:  $(A_0^R - A_s^R)/A_s^R = \alpha_R \sigma^2 A_s^R$ . This expression shows not only that the total area decrease is controlled by  $\alpha_R$ , but also that the shear strength  $\sigma$  has a leading effect on it: The smaller  $\sigma$  is, the smaller the total area drop. This explains why, for PDMS/grafted PDMS interfaces which have the smallest  $\sigma$  (*Materials and Methods*), the area reduction remains small, making it difficult to evaluate  $\alpha_R$  accurately.

### Value of the Static Friction Force

Fig. 2A shows that the static friction force  $Q_s$  of our multicontacts is selected from the intersection of two behavior laws. First,  $Q_s$  obeys the threshold law given in Eq. 2. Second,  $Q_s$  is related to the area of real contact through the reduction law  $A_s^R = A_0^R - \alpha_R Q_s^2$ . Solving for  $Q_s$  in this system of two equations yields



**Fig. 2.** Area reduction and static friction. (A)  $A^R$  vs.  $Q$ , for a PDMS/glass multicontact submitted to various normal loads  $P$  (1 point of 130 shown).  $R_q = 26 \mu\text{m}$ .  $V = 0.1 \text{ mm/s}$ . Solid curves: quadratic fits of the form of Eq. 1. Solid straight line: linear fit through data points corresponding to the onset of macroscopic sliding. See *Materials and Methods* for the value of  $\sigma$ . (B, Inset) Static friction force estimated using Eq. 3,  $Q_s^{\text{estimated}}$ , vs. its measured value,  $Q_s^{\text{measured}}$ , for all experiments, including different velocities. (B, main plot)  $(\sigma A_0^R - Q_s^{\text{estimated}})/\sigma A_0^R$ , as a function of  $(A_0^R - A_s^R)/A_0^R$ . In both plots, the solid straight line has slope 1 and goes through the origin. Purple, PDMS/glass interfaces; yellow, PDMS/grafted PDMS; orange, PDMS/cross-linked PDMS; stars, multicontacts; circles, smooth sphere/plane contacts; blue diamonds, fingertip/glass contacts.  $V = 0.1 \text{ mm/s}$  except light purple circles ( $V = 0.05 \text{ mm/s}, 0.1 \text{ mm/s}, 0.5 \text{ mm/s}, 1 \text{ mm/s}$  for PDMS/glass at  $P = 1.1 \text{ N}$ ). (C)  $A^A$  vs.  $Q$ , for a smooth PDMS/glass sphere/plane contact, presented as in A. One point of 70 is shown.  $R = 9.42 \text{ mm}$ .  $V = 0.1 \text{ mm/s}$ . See *Materials and Methods* for the value of  $\sigma$ . (D) Images of the sphere/plane contact in C for  $P = 0.55 \text{ N}$ . (D, Left)  $Q = 0$ . (D, Right)  $Q = Q_s$ . (Scale bars: 1 mm.)

$$Q_s = \frac{1}{2\alpha_R\sigma} \left( \sqrt{1 + 4\sigma^2\alpha_R A_0^R} - 1 \right). \quad [3]$$

Fig. 2B, Inset represents, for all experiments (various types of interfaces, normal loads, velocities, roughness), the value of  $Q_s$  estimated by Eq. 3 as a function of its measured value. All points align on the equality line, showing good accuracy and robustness of our estimate. How much is Eq. 3 improving the estimate of  $Q_s$  with respect to the uninformed estimate,  $\sigma A_0^R$ , made when one ignores the dependence of  $A^R$  with  $Q$ ? To answer this, we plot in Fig. 2B (main plot) the relative difference between the two estimates as a function of the corresponding relative difference between  $A_s^R$  and  $A_0^R$ . Both differences are found roughly equal, showing that the observed area reductions, up to 30%, can lead to 30% overestimations (resp. underestimations) of  $Q_s$  (resp.  $\sigma$ ) when the only available information about  $A^R$  is its initial value  $A_0^R$ .

This is practically important because most available models for the area of real contact in randomly rough contacts predict only  $A_0^R$ , as they consider interfaces under purely normal load (e.g., refs. 4, 13–16). A first-order improvement of these models would be to include the effect of incipient tangential loading and associated area reduction. They could then provide better estimates of the adhesive, purely interfacial, contribution to static friction quantified by  $\sigma$ . The viscoelastic, bulk contribution to friction would also be better estimated because the models would account for the reduced size of the microjunctions in the loading direction, which controls the excitation frequencies of the viscoelastic bodies.

### A Common Behavior Across Scales

Now that our working hypothesis (in elastomers, the area of rough contacts, like that of smooth contacts, decreases with increasing shear) has been validated, we go farther and compare the reduction laws of  $A^R$  and  $A^A$ . To do this, we carried out additional experiments to measure  $A^A$  on smooth contacts between PDMS spheres of millimetric radius of curvature (*Materials and Methods*) and the same substrates previously used for rough contacts. Under increasing shear, those contacts start circular and

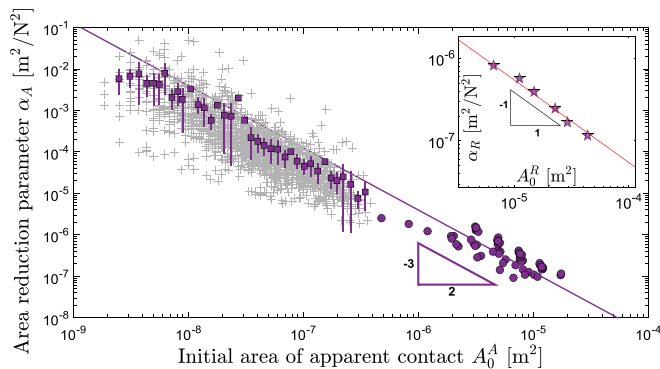
progressively become ellipse-like, as classically found (33–36) (Fig. 2D). As far as the contact area is concerned, for all interface types, sphere/plane contacts behave exactly as multicontacts (compare Fig. 2C and 2A). In particular, the area reduction law is also captured by a quadratic form  $A^A(Q) = A_0^A - \alpha_A Q^2$ , identical to Eq. 1, with  $\alpha_A$  the reduction rate associated with the apparent area of individual contacts, as opposed to  $\alpha_R$  related to the real area of multicontacts. The evolution of  $A_0^A$  with  $P$  is captured by the Johnson–Kendall–Roberts (JKR) model for adhesive sphere/plane contacts (43) (Fig. S3). The threshold law is again  $Q_s = \sigma A_s^A$ . The ingredients behind Eq. 3 being the same as for multicontacts, the estimate of  $Q_s$  for sphere/plane contacts is just as good (circles in Fig. 2B).

Such sphere/plane contacts are often considered good proxies for individual microjunctions in rough contacts. One advantage is that the tangential load can be measured directly for sphere/plane contacts, whereas it is inaccessible for an individual microjunction. This allows us to show, in Fig. 3 (circles), that for PDMS/glass sphere/plane contacts,  $\alpha_A$  decreases with  $A_0^A$  as a power law with an exponent close to  $-3/2$ . We find it true for monocontacts of all types (Fig. S4).

To compare this behavior with that of individual microjunctions, we track, along each experiment, the area evolution of the individual microjunctions. Assuming they also obey a quadratic reduction law like Eq. 1, their individual  $\alpha_{Ai}$  are estimated as (*Materials and Methods*)  $\alpha_{Ai} = (A_{0i}^A - A_{si}^A)/(\sigma^2 A_{si}^A{}^2)$ , with  $\sigma$  the shear strength of the macroscopic contact. The  $\alpha_{Ai}$  are plotted as a function of  $A_{0i}^A$  in Fig. 3 (squares). Strikingly, the dependence of  $\alpha_A$  on the initial area,  $A_0^A$ , appears identical (power law of exponent around  $-3/2$ ) within experimental accuracy for microjunctions and sphere/plane contacts, over four orders of magnitude of  $A_0^A$ . We find it true for interfaces of all types (Fig. S4).

### Behavior of Fingertip Contacts

To illustrate the generality of our results, analogous experiments were carried out on biological contacts between human fingertips and bare glass (Fig. 4 and *Materials and Methods*). Real contact occurs only along the protruding fingerprint ridges (Fig. 4C) (37, 38, 44, 45). The evolution of the area of real contact is shown in



**Fig. 3.** Area reduction across scales:  $\alpha_A$  vs.  $A_0^A$  (PDMS/glass interface). Circles: sphere/plane contacts for all  $R$ .  $V = 0.1$  mm/s. +: raw data for microjunctions within multicontacts ( $R_q = 26$   $\mu$ m). Squares: average of the positive raw data divided into 40 classes. Bars show SD within each class. Line: guide for eyes with slope  $-3/2$ . Inset:  $\alpha_R$  vs.  $A_0^R$  for the same multicontacts. Inset line: guide for eyes with slope  $-1$ .

Fig. 4A as a function of the tangential force applied,  $Q$ . Interestingly,  $A^R$  evolves under shear in a way very similar to that of elastomeric contacts (compare Fig. 4A with Fig. 2A and C). First, we find that a quadratic reduction law like Eq. 1 captures reasonably the data (although a linear fit would also be acceptable). Second, we find a linear threshold law like Eq. 2. As a consequence, Eq. 3 successfully predicts the value of the static friction force of fingertip contacts (blue diamonds in Fig. 2B).

As illustrated in Fig. 4B, we found that fingertip contacts under shear combine features of both sphere/plane contacts and planar multicontacts. As previously shown in the literature (37, 38), like sphere/plane contacts, their area of apparent contact (contours in Fig. 4C) decreases, by typically 40%. What we show here is that, simultaneously, the individual area of each microjunction also decreases, by about 10%. Both effects combine to give a reduction of about 45% of the area of real contact ( $45\% \simeq 40\% + 10\%$  of the remaining 60%).

### Discussion

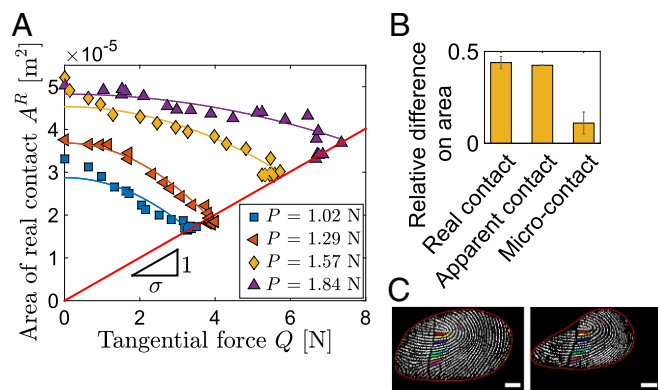
We now discuss the possible physical origins of the reduction in area of real contact and the quantities controlling the value of the reduction parameter  $\alpha_R$ . As mentioned in the Introduction, reduction of the area of apparent contact  $A^A$  under shear has already been observed on smooth sphere/plane elastomeric contacts (33, 35, 36). Because we showed that  $A^A$  and  $A^R$  actually follow analogous reduction behaviors (Fig. 2A and C), they may very well result from similar phenomena but at different scales. Two approaches have been proposed in the literature to interpret the observations on  $A^A$ .

The first approach focuses on the role of viscoelasticity, relating area reduction to the increase of elastic modulus of a viscoelastic body on which a rigid rough body is steadily sliding. This approach has been used both for smooth spherical (40, 46) and rough planar (14, 47) frictionless indentors and predicts a sliding-velocity-dependent amplitude of the area reduction. Note that in our experiments,  $\alpha_A$  has a measurable, but weak velocity dependence. Loading-induced stiffening was also invoked to explain the apparent contact reduction in fingertip contacts (38). However, although in apparent agreement with our observations, the abovementioned viscoelastic models cannot explain them. The reason is that, in our experiments, the geometry is opposite: The rigid body is smooth and flat. Thus, in a steady sliding regime, the viscoelastic body (sphere or rough plane) experiences a deformation which is constant in time and thus is not affected by viscosity. In those conditions, the viscoelastic models would predict a recovery of the contact area to the value it had

before shearing, i.e., under purely normal load. This is in striking contrast to our sphere/plane experiments, in which both the area and the shape of the steady sliding apparent contact remain significantly modified with respect to the initial situation (Fig. 2D). Additional experiments, in which shear loading is interrupted before the onset of sliding, show that, contrary to what viscoelastic models would have predicted, the area does not come back to its initial value. Those qualitative discrepancies suggest that viscoelasticity is not responsible for our observations.

The second approach focuses on the role of adhesion and describes the motion of the contour of sphere/plane contacts as a crack propagating under mixed-mode loading (opening plus shear). Unfortunately, all existing theoretical models (33, 36, 39) treat the case of axisymmetric shrinking of the contact area, an assumption which is strongly violated in our experiments (Fig. 2D). We believe that those models can anyway help us identify the mechanisms involved in the shear-induced area reduction. The two most recent models (36, 39) consider that the area reduction results from a combination of peeling at the contact's periphery (points in contact are lifted up from the glass) and microslipping in an annular peripheral region of the contact. To assess whether those mechanisms are involved in our experiments, we gently scratched an elastomer sphere to introduce small defects within the contact image that could be tracked during shearing experiments. Those experiments showed that for sphere/plane contacts, the area reduction is indeed related to both predicted contributions: (i) peeling at the trailing edge of the contact, partially compensated by the opposite behavior at the leading edge, collectively responsible for typically half of the total reduction, and (ii) compression of the contact in the loading direction due to heterogeneous slip, responsible for the other half of the reduction.

Given the good qualitative agreement of the adhesion-based models with our experiments, it is worth looking more quantitatively into their behavior. We carried out a numerical analysis of the model of ref. 36 and found that the beginning of the predicted area reduction is well fitted by a quadratic decay with the tangential load, in agreement with our observations. Independent variations of all model parameters allowed us to extract the scaling



**Fig. 4.** Area reduction in human fingertip contacts. (A)  $A^R$  vs.  $Q$ , for various normal loads  $P$  (1 point of 190 shown).  $V = 0.1$  mm/s. Curves: quadratic fits of the form of Eq. 1. Line: linear fit through the data corresponding to the onset of macroscopic sliding, passing through origin. See *Materials and Methods* for the value of  $\sigma$ . (B) Relative area difference between initial and final contact. B, left: area of real contact,  $A^R$  (error bar: segmentation threshold modified by  $\pm 3$  gray levels). B, center: area of apparent contact,  $A^A$  (error bar: same as B, left). B, right: individual area of 10 selected microjunctions (colored in C) that remain in contact all along the experiment (error bar:  $\pm$  SD). (C) Binarized image of a typical contact ( $P = 1.57$  N). Red line: contour of the apparent area of contact. (Scale bar: 3 mm.) C, Left:  $Q = 0$ . C, Right: steady sliding.

relationship  $\alpha_A \sim \frac{R^{0.18}}{E^{0.65} w_0^{0.47} P^{0.86}}$ , with  $R$  the sphere's radius,  $E$  its Young's modulus, and  $w_0$  the interface's work of adhesion. Interestingly, the exponent of the  $P$  dependence is close to  $-1$ . Considering that, for elastic sphere/plane contacts,  $P$  scales as  $(A_0^A)^{3/2}$ , this exponent is in good agreement with the exponent  $-3/2$  found for individual contacts in Fig. 3. Although  $R$  was changed threefold and  $w_0$  twofold, those ranges are not sufficiently large to test the corresponding scalings. The quite large negative exponent associated with  $E$  suggests that  $\alpha_A$  becomes smaller when the contacting bodies are stiffer. This could explain why the reduction of the area of apparent contact under shear has mainly been reported for soft materials, like rubber or human skin, but not for instance for polymethylmethacrylate or glass (5, 17). It also suggests that in stiff plastic materials like metals, the area reduction is likely much smaller than the concurrent plasticity-induced growth of the area, explaining why only the latter has been reported. Although the model of ref. 36 appears scaling-wise consistent with our results on smooth spherical contacts, there is currently no available adhesion-based model for area reduction in rough contacts to compare with our data.

Irrespective of the precise mechanisms involved in area reduction, the phenomenon has important fundamental implications. First, we observed that (i) the reduction of area of real contact in rough contacts is the macroscale consequence of the shrinking of the individual microjunctions (Fig. 1B, *Inset*) and (ii) the reduction parameter  $\alpha_A$  of microjunctions obeys a well-defined scaling law of the form  $\alpha_A = \beta(A_0^A)^{-\gamma}$ . Those two observations suggest that macroscale reduction could be understood from that of the microjunctions, through a statistical average, along the lines of previous statistical friction models (13, 48). In *SI Notes, Mean-Field Model Relating  $\alpha_A$  and  $\alpha_R$* , we indeed derive the expression of the macroscale reduction parameter,  $\alpha_R$ , in terms of the parameters of the microscale scaling law,  $\beta$  and  $\gamma$ , in the simple case of a multicontact made of identical, independent microjunctions. The main outcome of this mean-field approach is that the scaling of  $\alpha_R$  with the initial area  $A_0^R$  is different from that of  $\alpha_A$ . Within the assumptions used, we find that  $\alpha_R \sim (A_0^R)^{-1}$ , independent of the microscopic exponent  $\gamma$ . As shown in Fig. 3, *Inset*, this scaling actually captures very well the observed dependence of  $\alpha_R$  with  $A_0^R$  for our macroscopic, rough contacts. Thus, it is now possible, for elastomers, to incorporate the shear-induced variations of the area of real contact in multiscale friction models like refs. 48–54, through the microscopic law  $\alpha_A = \beta(A_0^A)^{-\gamma}$ .

In the Introduction, we also argued that the success of the rate-and-state friction (RSF) law was due to the fact that it incorporates the three main recognized dependencies of the area of real contact. To what extent is the fourth dependency identified here affecting the way we understand the RSF law? The Rice–Ruina formulation of the RSF law (18, 24–26) involves a parameter,  $B$ , which is also the prefactor of the logarithmic increase of the static friction coefficient with the time spent at rest by the interface. If one neglects structural aging, such an increase is caused by the growth, in the same proportion, of the area of real contact due to asperity creep at rest (geometrical aging). Our results indicate that, at least for elastomers and human skin, before the static friction threshold is reached, the already aged area will decrease as the shear loading is increased. Thus, the area relevant to the static friction coefficient will be smaller than that expected if geometric aging was the only mechanism involved. As a consequence, interpreting the parameter  $B$  as a quantifier of geometrical aging alone leads, for those soft materials, to a systematic underestimation of the rate of geometrical aging of an interface (shown in *SI Notes, Reinterpretation of the Parameter  $B$  in the RSF Law*). We suggest that  $B$  instead represents a combination of the classical geometrical aging and of the shear-induced area variations, an idea already proposed for rocks (28). Our results are thus expected to directly impact (for the class of

soft materials studied here) or inspire the many scientific fields in which friction and RSF in particular are useful, including tribology, earthquake/landslide science, and robot/human haptics.

## Materials and Methods

**Mechanical Aspects.** Driving of the slider is obtained using a motorized translation actuator (Newport LTA-HL). The tangential force  $Q$  is measured using a stiff piezoelectric sensor (Kistler 9217A) placed close to the motor. The  $Q$  signals are digitized and recorded at a sampling rate of 3 kHz (1 kHz for sphere/plane contacts and fingertip contacts). The normal and tangential forces,  $P$  and  $Q$ , are measured with 0.1 mN and 1 mN accuracies, respectively. For planar rough contacts, the slider is driven through a horizontal steel wire of stiffness  $9,700 \pm 200$  N/m. For sphere/plane contacts and fingertips, the slider is driven rigidly through the length of a cantilever beam of bending stiffness  $52 \pm 1$  N/m. The elastomer blocks ( $35 \times 20 \times 2$  mm<sup>3</sup> in  $x,y,z$  for  $R_q = 26$   $\mu$ m,  $21 \times 19 \times 2$  mm<sup>3</sup> for  $R_q = 20$   $\mu$ m) are made of PDMS (Sylgard 184, mass ratio 10:1) degassed during 1 h and cross-linked at ambient temperature during about 150 h. Its Poisson ratio is  $\nu = 0.5$  (incompressible material). Its Young's modulus is measured to be  $E = 1.6 \pm 0.1$  MPa [value (error bar): mean (SD) over all experiments using different spheres on PDMS/glass interfaces]. The rough free surface of each elastomer block is obtained by molding the polymer against a roughened steel plate. The height distribution of the steel plate was characterized with a tactile profilometer (Surfscan Somicronic) and found to be Gaussian, with a rms roughness  $R_q$  of either 20  $\mu$ m or 26  $\mu$ m. The smooth spherical PDMS caps used for sphere/plane contacts were obtained by molding against optically smooth concave optical lenses of radius  $R = 7.06$  mm, 9.42 mm, or 24.81 mm.

### Substrate Preparation.

**Bare glass plates.** Bare glass plates are obtained from Mirit Glas. Before experiments, the surface is washed with soapy water, then with ethanol, and eventually with distilled water. This process is repeated three times.

**Glass coated with grafted PDMS chains.** Microscope glass slides are cleaned by immersion in piranha solution [70/30 (vol/vol) of concentrated H<sub>2</sub>SO<sub>4</sub> and H<sub>2</sub>O<sub>2</sub>] for 30 min at 50 °C. The solution is decanted, and the slides are rinsed with deionized water. They are then dried under a stream of N<sub>2</sub> gas, exposed to UV/ozone (cleaning plasma) oxidation for 6 min immediately before the deposition of organosilicon, and finally rinsed with ultrapure water. The entire cleaning process provides activated microscope glass slides, with clean and oxidized surfaces containing mainly Si-OH groups. A 100-mg/mL PDMS solution (in HPLC toluene) is passed through a microfilter to remove impurities. A drop of this solution is deposited onto an activated glass slide, which it is then spin-coated at 2,000 rpm for 30 s. The film is cured at 130 °C for 4 h. The surface is then rinsed in toluene for 2 h and dried with N<sub>2</sub>. The resulting surface is covered with PDMS chains grafted at one end on the glass, with grafting density low enough for the rest of the chain to adsorb on the surface.

**Glass coated with cross-linked PDMS.** A PDMS elastomer base/curing agent mixture (mass ratio 10:1) of Sylgard 184 is poured into a mold composed of two glass plates separated by a polytetrafluoroethylene spacer either 1 mm (sample in Fig. 1) or 150  $\mu$ m (sample in Figs. S2 and S4) thick. After cross-linking at room temperature for 150 h, one glass plate is peeled away, leaving the other with a smooth elastic coating to be used for friction experiments.

**Interfacial Properties.** The work of adhesion of each interface type involving PDMS was obtained by fitting  $A_0^A(P)$  for sphere/plane contacts, using the JKR model (43). The data were obtained on a dedicated apparatus. We found  $w_0(\text{PDMS/glass}) = 27 \pm 1$  mJ/m<sup>2</sup> (agrees with ref. 36),  $w_0(\text{PDMS/grafted}) = 30 \pm 1$  mJ/m<sup>2</sup> (smaller than in ref. 12), and  $w_0(\text{PDMS/cross-linked}) = 65 \pm 3$  mJ/m<sup>2</sup> (larger than in ref. 55). The shear strengths of the various interface types were obtained as in Fig. 2A. For multicontacts,  $\sigma(\text{PDMS/glass}) = 0.23 \pm 0.02$  MPa (agrees with ref. 7),  $\sigma(\text{PDMS/grafted}) = 0.14 \pm 0.02$  MPa, and  $\sigma(\text{PDMS/cross-linked}) = 0.34 \pm 0.05$  MPa (coating thickness 1 mm). For sphere/plane contacts,  $\sigma(\text{PDMS/glass}) = 0.36 \pm 0.01$  MPa (agrees with ref. 56),  $\sigma(\text{PDMS/grafted}) = 0.07 \pm 0.01$  MPa (agrees with ref. 12), and  $\sigma(\text{PDMS/cross-linked}) = 0.23 \pm 0.01$  MPa (larger than in ref. 9).

**Image Analysis.** Images are recorded using a CCD camera (Flare 2M360 MCL, 8 bits, 2,048  $\times$  1,088 square pixels) at 300 frames per second (100 frames per second for sphere/plane and fingertip contacts). The pixel size in multicontact images was typically 25  $\mu$ m. Possible implications of this finite pixel size on area measurements are discussed in *SI Notes, Possible Implications of the Finite Optical Resolution of the Images*. To select the threshold used to binarize images, we used a method fully justified in *SI Notes, Contact Area*

*Measurement*, and summarized here. We fitted the intensity histogram of each image by a sum of two subhistograms: (i) one for the class of out-of-contact pixels (large intensities), the shape of which (distorted Gaussian) was inspired by the histogram of images fully out of contact, and (ii) one for the class of in-contact pixels (Gaussian). The threshold was taken at the intersection between the two subhistograms, which minimizes the probability to select a wrong class during thresholding. Along one experiment, the calculated threshold remains stable within  $\pm 2$  gray levels. It is thus taken as constant for each experiment at its mean value. It is found to increase by about 10 gray levels as the normal load increases from 1 N to 6 N. Tracking was performed as in ref. 57. To estimate  $\alpha_{Ai}$  of microjunctions (Fig. 3), individual values of  $A_{0i}^A$  and  $A_{fi}^A$  are the (nonquantified) initial and final values of the sigmoid fitted onto  $A_i^A(t)$ .

**Fingertip Experiments.** They were done similarly to those in ref. 45. The protocols were approved by the Board of Directors of the Laboratoire de Tribologie et Dynamique des Systèmes. The subject (one of the authors) gave his informed consent. The right forefinger (male, 24 y old, right-handed Caucasian) is pointing upward and constrained in a fixed position at about

$30^\circ$  from the surface (bare glass). The glass is pressed under constant normal load, in the range 1–2 N, and moved at constant speed  $V = 0.1$  mm/s in the distal direction. Before each experiment, the fingertip is cleaned with ethanol using a nonwoven paper to limit dust contamination. The glass is cleaned the same as for PDMS/glass experiments. Each experiment starts after a waiting time of 1 min (time necessary for the contact size to stabilize). The shear strength of our fingertip/glass interfaces was measured to be  $\sigma = 0.20 \pm 0.01$  MPa.

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