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▶ To cite this version:

Rostyslav Bilyy, Solomiya Paryzhak, Kostiantyn Turcheniuk, Tetiana Dumych, Alexandre Barras, et al.. Aluminum oxide nanowires as safe and effective adjuvants for next-generation vaccines. Materials Today, 2019, 22 (58-66), 10.1016/j.mattod.2018.10.034. hal-01944313

HAL Id: hal-01944313 https://hal.science/hal-01944313v1

Submitted on 17 Dec 2018

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Aluminum oxide nanowires as safe and effective adjuvants for **next**-generation vaccines

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Improving efficiency of an adjuvant, material that enhances the body's immune response to an 16 antigen, has become vital for the development of safer, cheaper, and more effective next-generation 17 vaccines. Commercial vaccines typically use aluminum salt-based adjuvant particles, most commonly 18 aluminum oxyhydroxide (AlOOH) and aluminum hydroxide (Al(OH)₃) based often referred to as 19 "alum". Despite their broad use, their adjuvant properties are rather moderate. This is even worse in the 20 case of aluminum oxide (Al₂O₃)-based adjuvant. While being more robust and less cytotoxic, Al₂O₃ is a 21 Q4 significantly less effective adjuvant than above-mentioned Al compounds and is consequently not 22 commonly used. Here, we report on the remarkably enhanced adjuvant properties of Al₂O₃ when 23 produced in the form of nanowires (NWs). Based on recent advances in understanding neutrophil 24 activation by inert nanoscaffolds, we have created ultra-long Al₂O₃ NWs with a high aspect ratio of 25 \sim 1000. These NWs showed strong humoral immune response with no damaging effect on the 26 microvasculature. Since only the change of shape of Al adjuvants is responsible for the excellent 27 adjuvant properties, our finding holds great promise for rapid implementation as safer and more 28 effective adjuvant alternative for human vaccines. The mechanism behind human blood-derived 29 neutrophil activation with Al₂O₃ NWs was found to be sequestering of Al₂O₃ NWs by neutrophils via 30 formation of neutrophil extracellular traps (NETs). 31

33 Introduction

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Vaccination has made an enormous contribution to global health and is considered one of the greatest medical accomplishments for achieving global safety against dangerous diseases. Since the efficiency of a particular vaccine correlates directly with the percentage of a given population that has been vaccinated, the vaccine market requires cost-effective and efficient solutions to attain broad vaccination coverage [1]. The technologies involved in manufacturing different types of vaccines influence strongly vaccine costs. The high price of antigen expression makes many vaccines less affordable to (and thus less used by) low-income population [2]. Adding effective adjuvants to vaccine formulation enhances vaccines in two possible ways: (a) it allows the use of smaller antigen doses or physically small adjuvant molecules (meaning synthetic pathogenic components instead of attenuated risky pathogens) and (b) it leads to enhanced antibody titers, decreasing the number or revaccinations and maintaining the reliable antibody levels during whole life [3]. Furthermore, improving the efficiency of adju-

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vants to enhance the body's immune response to an antigen would allow the development of next generation of safer, more effective, and more affordable vaccines.

Aluminum (Al) salt-based adjuvants (most commonly in the form of aluminum oxyhydroxide (AlOOH), aluminum hydroxide (Al(OH)₃) are used in human vaccines since 1930s and are commonly referred to as "alum" [4-6]. The presence of oxygencontaining groups on their surface [7-9] provides fast antigen adsorption and yield a vigorous response from the immune system compared to alternatives [10]. While aluminum oxide (Al₂O₃) is more robust, it is significantly less effective than other Al-based adjuvants and is commonly much less used. Furthermore, Al salt-based adjuvants exhibit relatively low cytotoxicity as compared to pathogen stimulants or virusomes and have proven to cause a fewer number of local severities [11,12].

Recent studies showed that the shape and dimensions of the adjuvant particles may affect the immune response against protein and peptide antigens [13,14]. For example, enhanced adjuvant activity of small, elongated particles (nanorods or nanosticks) of AlOOH and Al(OH)3 with diameters of 4-20 nm and aspect ratio of 8–10 was recently reported [14–16], although the origin of the improved performance remained largely unclear.

75 Earlier, some of us demonstrated that different size nanoparticles thrust the activity of neutrophils, which boosts the immune 76 system response toward co-injected antigens [17,18]. This mech-77 78 anism of neutrophils activation is highly dependent on the size of the particles, e.g. bacteria, fungi, nano- and microparticles 79 80 [18,19]. It results in the formation of neutrophil extracellular traps (NETs), which effectively isolate foreign bodies and sup-81 82 press local self-limiting inflammation [20]. The mechanism of 83 NETs' action is realized by the entrapping of foreign particles by unbound DNA and histones, both decorated by toxic pro-84 teinous content of neutrophils' granules [21]. Formation of NETs 85 was recently demonstrated as an important player responsible for 86 adjuvant action of injected alum, reported to recruit neutrophils, 87 88 and their activation leading to stimulation of DNA sensors and provoking local inflammatory response [22]. 89

90 Since the NETs' formation is particles' size-dependent, we hypothesized that the utilization of high-aspect ratio Al-based 91 vaccine adjuvants can greatly contribute to establishing more 92 potent immune responses through neutrophils' activation. 93 94 Unfortunately, relatively expensive synthesis of nanorods (due to the use of harsh chemicals, elevated reaction temperatures, 95 and low reaction yields), which was demonstrated earlier [14], 96 as well as their potential damages to the smallest blood vessels 97 98 may become barriers for their use in low-cost vaccination.

99 In this article, we have chosen to investigate if Al₂O₃ nanowires (NWs) can activate neutrophil cells upon injection to the 100 body and possibly enhance adjuvant properties over other Al-101 based adjuvants. We choose to compare our findings to 102 aluminum-based adjuvants, commonly used in commercially 103 available vaccine formulations. Our interest was partially trig-104 gered by our recent discovery of an innovative approach for 105 ultra-low-cost synthesis of γ-alumina NWs (γ-Al₂O₃ NWs) of vari-106 107 able dimensions and controllable aspect ratio [23,24]. These nanomaterials are produced by exposing bulk Al alloys to alco-108 109 hols at near room temperature and atmospheric pressure, followed by heat treatment in air. No catalysts, toxic metals, 110 external stimuli, or costly synthesis systems are required. We 111 expect the future industrialization will allow formation of these 112 γ -Al₂O₃ NWs at a cost of a few dollars per pound, which is almost 113 negligible for vaccination applications. The tests conducted for 114 the first time on 20- to 60-micron-long, 20-40 nm diameter, 115 \sim 1000 aspect ratio NWs substantially exceeded our expectations 116 and demonstrated γ -Al₂O₃ NWs to be extremely effective vaccine 117 adjuvant, inducing excellent humoral immune response. Quite 118 remarkably, γ -Al₂O₃ NWs did not damage the microvasculature 119 of the tissues and were found to be easily entrapped by NETs 120 and passivated. When compared with state of the art commercial 121 Al-based adjuvant, the proposed low-cost γ -Al₂O₃ NWs were 122 found to be both more efficient and safer. Our findings highlight 123 great promises of NWs for substantial breakthroughs in the 124 development of safer, more effective, and more affordable 125 vaccines. 126

Results and discussion

127 γ-Al₂O₃ NWs have been synthesized by the protocol described by 128 some of us previously [23]. It relies on the de-alloving of bulk Al-129 Li alloy in ethanol at 60 °C for 24 h, which yields Al ethoxide 130 NWs. Subsequent heat-treatment at 800 °C for 1 h results in 131 the formation of γ -Al₂O₃ NWs, as shown in the scanning elec-132 tron microscopy (SEM) micrograph (Fig. 1a). The microstructure 133 of the NWs is uniform. The average NWs' thickness is ~ 20 nm, 134 average length 20–60 μ m, and aspect ratio exceeding \sim 1000. 135 We believe that the dimensions of the NWs are sufficient to acti-136 vate neutrophils (typically 12-17 µm in diameter). In particular, 137 of a typical length of $35 \,\mu m$ [25], the crystals of monosodium 138 urate, which are formed in the condition of the gout, can be 139 effectively ingested by the neutrophils [26,27]. The crystallinity 140 of the γ -Al₂O₃ NWs was revealed by the transmission electron 141 microscopy micrograph (TEM, Fig. 1b). The γ -Al₂O₃ NWs are 142 polycrystalline with an average crystal diameter of 15-20 nm. 143 The rough surface and sharp ends of the γ -Al₂O₃ NWs can pro-144 mote the membrane damage in neutrophils, resulting in the pro-145 motion of the NET formation [18]. The characteristic selected 146 area electron diffraction (SAED) pattern in Fig. 1b area exhibits 147 strong and prominent diffraction rings indexed as 311, 222, 148 400, and 440 reflections of γ -Al₂O₃ (Fig. 1c). Thermogravimetric 149 analysis (TGA) shows clearly the conversion of Al(OEt)3 NWs to 150 Al₂O₃ NWs (Fig. 1c). Organic carbon- and hydrogen-containing 151 groups, which constitute almost \sim 40 wt.% of the mass, burn in 152 air until 400 °C. In the range of 500-1000 °C, the mass of the 153 Al₂O₃ NWs is stabilized. The high-angle XRD pattern (Fig. 1d) 154 of the Al₂O₃ NWs displays diffraction peaks at 20 of 14.66°, 155 37.18°, 39.03°, 45.36°, 60.15°, and 66.70°, indexed as (2.2.0), 156 $(3\ 1\ 1)$, $(2\ 2\ 2)$, $(4\ 0\ 0)$, $(5\ 1\ 1)$, and $(4\ 4\ 0)$ crystal planes of γ -157 Al₂O₃ NWs, respectively. The chemical composition of γ -Al₂O₃ 158 NWs was further validated by FTIR (Fig. 1e) and XPS analysis 159 (Fig. 1f). The FTIR spectrum exhibits a broad band centered at 160 3495 cm^{-1} due to OH (stretching) band and/or adsorbed water. 161 There is a general lack of peaks related to oxygen-containing 162 groups besides the presence of bands related to AlOOH, such as 163 the bands at 3298, 3091, 1070, and 1165, assigned to $v_{as}(Al)$ -164 OH, v_s (Al)–OH, stretching vibrations, and δ_{as} Al–O–H modes for 165 Materials Today • Volume xxx, Number xx • xxxx 2018



Characterization of γ -Al₂O₃ nanowires: (a) SEM micrograph; (b) TEM micrograph and SAED; (c) TGA; (d) XRD pattern; (e) FTIR; (f) XPS survey (inset) and characteristic of the Al_{2p} core level.

166 AlOOH. The bands below 1000 cm^{-1} at 864, 749, and 583 cm⁻¹ 167 are caused by the formation of the γ -Al₂O₃ phase. Furthermore, 168 the XPS survey spectrum, together with the high-resolution 169 core-level spectrum of Al_{2p} (74.6 eV), is shown in Fig. 1f,g (inset). 170 The atomic ratio between Al_{2p}/O_{1s} is 0.65 close to that of the the-171 oretical value of 0.66 for γ -Al₂O₃.

172 A commercial Al-based adjuvant (alum) (Fig. S1a) and commercial aluminum oxide microparticles (Al₂O₃ MPs) (Fig. S1b) 173 were used as control materials throughout this study. Fig. S1c 174 shows X-ray diffraction (XRD) patterns of alum. The XRD pat-175 terns indicate that alum has an aluminum oxide hydroxide (y-176 177 AlO(OH)) (boehmite) structure with the average crystallite size 2.2 nm (Fig. S1). Zeta-potential measurements in water at 25 °C 178 (Fig. S1d) indicate that alum adjuvant formulation has a positive 179 180 surface charge of $+6.6 \pm 0.3$ mV (Table S1). This is only slightly higher than that of the γ -Al₂O₃ NWs with a surface charge of 181 +2.2 \pm 1.5 mV. Surprisingly, using Al₂O₃ MPs, a negative surface 182 183 charge was recorded. The positive surface charge of γ -Al₂O₃ NWs may be advantageous to facilitate the electrostatic binding of 184 negatively charged proteins. Indeed, incubation of γ -Al₂O₃ 185 NWs in water supplemented with 0.2% ovalbumin (OVA) results 186 187 in a material with negative (about -25.6 mV) surface charge due to the adsorption of OVA. The same was true for the alum 188 adjuvant. 189

190 The cell toxicity of γ -Al₂O₃ NWs was tested on HeLa and 191 U87MG cell lines after 24-h incubation (Fig. S2a–b). In addition, and in the belief that γ -Al₂O₃ NWs will be mainly processed by macrophages, cytotoxicity studies of this cell type were included (Fig. S2c).

The cytotoxicity of the different materials was evaluated based on cell viability assessment by MTS assay relative to controls as proposed by Kong et al. [28]: non-toxic >90% cell viability, slightly toxic 65–90%, toxic 35–65%, severe toxic <35%. All the nanostructures appeared nontoxic for HeLa cells after 24 h of exposure even at high concentrations. This was also true for Al₂O₃ MPs alone. Using U87MG human brain cells, in the case of γ -Al₂O₃ NWs at concentrations >100 µg mL⁻¹, the nanostructures proved to be slightly toxic after 24 h of exposure. The same was observed for alum. Interestingly, Al₂O₃ MPs had a different cytotoxic behavior on these cell lines: at concentrations between 200 and 400 µg mL⁻¹, the structures were slightly toxic and reached toxic levels for concentrations >500 µg mL⁻¹.

In order to test adjuvant properties of γ -Al₂O₃ NWs, we have 208 determined both parts of immune responses, namely humoral 209 and cellular immune responses. Immunization experiments were 210 performed on Balc/c laboratory mice using chicken egg OVA as 211 model antigen. The presence of anti-ovalbumin antibodies, both 212 IgG and IgM types, was measured before immunization (day 0), 213 as well as after 14 and 35 days of immunization (Fig. 2a,b, 214 Fig. S3, Fig S4a–b). The humoral immune response after a second 215 vaccination caused by the " γ -Al₂O₃ NWs + OVA" was signifi-216 cantly stronger compared to that effect of "alum + OVA" 217

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(a)

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Blood sampling DTH challenge Blood sampling Blood sampling Immunization Immunization DTH reaction ▼ **** * * *** 7 ۵ 14 21 28 35 Time (days) (b) (c) 250 2.0 DTH reaction alum + OVA % Y-Al2O3 NWs + OVA 200 arti-OVA IgG, E450 Footpad swelling, 1.5 Al₂O₃MPs + OVA 150 OVA 1.0 100 50 0.5 0.0 14 35 6 n 24 48 72 96 Time (days)

FIG. 2

Humoral and cellular immune responses in Balb/c mice provoked by OVA using alum, γγ-Al₂O₃ NWs, Al₂O₃ MPs, or OVA alone acting as adjuvants: (a) experimental design and (b) humoral immune response. Anti-OVA IgG-specific levels in serum (humoral immune response), each dot represent the response of specific animal; sera dilution was 1:2000; (c) cellular immune response; DTH reaction measured as a foot swelling. Data are M ± sem for all studied animals in the group; n = 12, 13, 4, 5, correspondingly.

(Fig. 2b), as indicated by the significantly higher amount of anti-218 OVA IgG antibodies formed 35 days after immunization at the 219 dilution factor of 1/2000. Further analysis of antibody titers 220 221 (dilution factor at which antibody is still effective) revealed (Fig. S3) that titers of antibodies obtained after γ -Al₂O₃ NWs 222 223 + OVA immunization were 1/64000; after the use of alum -1/16000, for Al₂O₃ MPs and OVA alone, they were as low as 224 1/2000 and 1/1000, correspondingly; the cut-off was set to 0.5 225 OD value (Fig. S3). Both adjuvants were not inducing acute-226 227 phase antibodies of IgM type (Fig S4b), which signifies that there is no inflammation left. 228

The cellular immune response was assessed using an estab-229 lished model of delayed type hypersensitivity (DTH) reaction 230 [29], modified by us to be less invasive animal treatment protocol 231 232 [18]. The DTH is a part of the cell-mediated immune response associated with Th1 reactivity in response to insoluble foreign 233 antigens. It is a localized inflammatory reaction prototypical 234 in vivo assay to study cell-mediated host immune response medi-235 ated by CD4+ T lymphocytes (small leukocytes, white blood 236 237 cells). These cells promote T-helper cell type 1 (Th1) production of interferon- γ (a soluble cytokine). This immune response is 238 characterized by an influx of innate immune cells, with macro-239 phages and the dendritic cells predominating. Therefore, after 240 the formation of antibodies (day 28), mice were challenged with 241 242 OVA injected between the fingers of the footpad (right foot), while PBS served as control and injected to the left foot 243 (Fig. 2a). Footpad swelling, being proportional to the strengths 244 of cellular immune response, was measured in dynamics for 245

few days, until swelling disappeared. The DTH reaction (usually 246 evaluated at 6-24 h after antigen exposure) was comparable for 247 both groups of animals, immunized with OVA in the presence 248 of either alum or γ -Al₂O₃ NWs (Fig. 2c), while it was significantly 249 lower for Al₂O₃ MPs or OVA alone. The swelling of the footpad 250 faded after 72 h of the DTH challenge, which correlates with 251 the normal responsiveness to the antigen. Absence of exagger-252 ated cellular response with much stronger humoral response 253 for γ -Al₂O₃ NWs makes them immunologically favorable agents 254 for the use in vaccines. 255

Time (hours)

Some of us have recently shown that nanoscaffolds may be 256 able to induce activation of polymorphonuclear neutrophils to 257 form neutrophil extracellular traps [18], networks of extracellular 258 fibers produced as an immune response to neutralize infection 259 [30]. Localization of neutrophils leads to localized self-limiting 260 inflammation, which results in isolation of inflammatory stimuli 261 with NETs [31] and, as discovered recently, is an important trigger of alum action [22]. This phenomenon is mainly responsible for the strong self-limiting (fast resolved) inflammation caused by some nanoparticles [18] (best illustrated by gout attack, caused by monosodium urate needle-like crystals, to be as spontaneously resolved as it appears).

Since y-Al₂O₃ NWs provoked increased humoral immune response, we were interested to follow up the fate of the γ -Al₂O₃ NWs upon injection in the body. We used a lately described mouse air pouch model [32], where sterile air is injected under the skin at the back of the mouse to form a cavity, which is being infiltrated with immune cells followed by γ -Al₂O₃

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Formation of neutrophil extracellular traps (NETs): sequestering of γ -Al₂O₃ NWs and alum by aggregated NETs after 24 h of incubation in mouse air pouch. Dotted red circles show capillary damage and edema. No significant damage to capillaries is observed after γ -Al₂O₃ NWs' treatment.

274 NWs' injection (1 mg γ -Al₂O₃ NWs per mouse). Within 24 h after 275 NWs' injection, mice were sacrificed, and their skin was observed for aggregated NETs and visual damage by microphotography. 276 For both γ -Al₂O₃ NWs and alum, we have observed abundant for-277 mation of aggregated NETs entrapping injected Al compounds 278 279 (Fig. 3., S5). However, micro-capillary damage and edema were 280 significantly less visible for γ -Al₂O₃ NWs than for commercial alum. It is known that swelling and edema often arise at the 281 place of vaccine injection, which is accompanied by the release 282 of histamines [33]. However, the exact molecular mechanism 283 of how injection of alum results in edema remains unknown 284 [22,34]. Therefore, the remarkable properties of γ -Al₂O₃ NWs of 285 not causing edema are highly beneficial for potential applica-286 tions as adjuvants. Their utilization will result in less swelling, 287 edema, and irritation at the place of injection. 288

To elucidate the mechanism of the γ -Al₂O₃ NWs' adjuvant 289 properties and related neutrophil activation, we tested their abil-290 ity to stimulate NETs' formation in human blood-derived neu-291 trophils. For this reason, we obtained a venous blood from 3 292 healthy volunteers and isolated neutrophil population in sterile 293 conditions. Then neutrophils were placed in multi-well plate 294 295 containing Sytox Green, a fluorescent dye, which senses extracellular DNA (those externalized from neutrophils in the case of 296 NETs' formation). Positive strong (phorbol myristyl acetate, 297 PMA) and weak (48 mM bicarbonate) inducers of NETs' forma-298 299 tion were applied to cell well, simultaneously with γ -Al₂O₃ NWs, alum, or Al₂O₃ MPs. Fig. 4 shows the data of neutrophil 300

activation, isolated from 3 different healthy donors. From the mean fluorescence intensity (MFI) level, it is evident that γ -Al₂O₃ NWs exhibit immediate to strong NET formation upon the contact with the isolated neutrophils. The same was true for alum, the structure of which can also be regarded as 1D material (please see elongated shapes of the fibers in Fig. S1A). In contrast, the Al₂O₃ MPs did not induce such an effect. This is an important finding, which confirms that the improved humoral response of γ -Al₂O₃ NWs is most likely to be linked to their outstanding structural characteristics. Based on our previous findings, we suspect that a combination of high aspect ratio and small diameter of γ -Al₂O₃ NWs effectively activates neutrophils by causing local disturbances in lipid bilayer composition followed by membrane re-cycling. The same level of neutrophils' activation, although seen for alum, does result in the membrane damaging and lower levels of humoral immune response as compared to the γ -Al₂O₃ NWs. It also corroborates our hypothesis that not only the chemical composition, but also the shape and size of the adjuvant may have a profound effect on activation and interaction with NETs.

Based on obtained data, we propose the mechanism of 321 enhanced action of γ -Al₂O₃ NWs as an adjuvant. γ -Al₂O₃ NWs 322 adsorb antigens and upon injection release them; this results in 323 local macrophage and neutrophil activation (Fig. 5a). Macro-324 phages process the antigens and stimulate antibody production 325 through plasma cells (Fig. 5b). Additionally, at the early time 326 upon neutrophil contact with γ -Al₂O₃ NWs, the former release 327 NETs and cytokines, and significantly enhance antibody produc-328 tion (Fig. 5b). Within 24 h, γ -Al₂O₃ NWs are sequestered by 329 NETs, which limits the inflammation caused by the presence of 330 the foreign γ -Al₂O₃ NWs' particles (Fig. 5c). The γ -Al₂O₃ NWs 331 reside locally within the traps without damaging the microvascu-332 lature or causing local inflammation. Sufficient concentration of 333 antibodies is achieved in the body as the result of the " γ -Al₂O₃ 334 NWs' adjuvant + antigen" vaccination.

Conclusions

This study demonstrates for the first time the extremely promis-337 ing performance of long (20-60 microns) small diameter (20-338 40 nm), high aspect ratio (>1000) y-Al₂O₃ nanowires (NWs) as 339 a material that enhances the body's immune response to an anti-340 gen. The results are particularly encouraging because Al₂O₃ is 341 commonly considered to be rather ineffective as an adjuvant. 342 Compared to conventional Al₂O₃ microparticles, y-Al₂O₃ NWs 343 exhibited noticeably reduced cell toxicity and dramatically stron-344 ger neutrophil activation. Furthermore, y-Al₂O₃ NWs showed 345 improved humoral immune responses, resulting in 4-fold 346 (1/64000 vs 1/16000) higher antibody titers and significantly less 347 damages to microvasculature when compared to alum, a com-348 monly chosen vaccine adjuvant. Our study further revealed that 349 γ -Al₂O₃ NWs can effectively activate polymorphonuclear neu-350 trophils to form neutrophil extracellular traps (NETs), thereby 351 explaining their outstanding properties. The following neutral-352 ization of the NWs in the aggregated NETs explains the self-353 limiting nature of the NWs' inflammatory effect, which makes 354 NWs safer candidates for common vaccines. We expect the 355 ultra-low cost of the NWs' synthesis in combination with their 356

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FIG. 4

RESEARCH: Original Research

Activation of peripheral blood-derived neutrophils upon the contact of Al-based adjuvants. Data of three different healthy donors (a-c) are presented. Intensity of NETs' formation is presented as a mean fluorescent intensity of Sytox green dye upon the contact with extracellular DNA: γ-Al₂O₃ NWs and alum but not Al₂O₃ MPs cause rapid activation of human peripheral blood neutrophils (d-f), which is noticeable during the first minutes of incubation. Strong (PMA) and weak (48 mM bicarbonate) inducers of NETs' formation show their response after 120 min.



FIG. 5

Brief schematics of the process of the immunization by the γ -Al₂O₃ NWs-OVA (see text for description).

357 extremely promising performance may open the door to new 358 families of next-generation adjuvants for better, safer, and cheaper human vaccines. We also expect that modifying NWs' 359 surface chemistry and optimizing their dimensions and mor-360 phology may boost their performance further. 361

Materials and methods 362

Materials 363

Aluminum oxide (Al₂O₃), Aluminum hydroxide (Al(OH)₃, alu-364 365 minum (99.999% pure), lithium (99.99% pure), anhydrous ethanol (EtOH), and ovalbumin (OVA) were purchased from Sigma-Aldrich and used as received.

Fabrication of γ -Al2O3 NWs

According to the previous study of transformation from bulk alloys to oxide nanowires [23], a bimetallic Al-Li alloy (50 at.% lithium) was exposed to anhydrous ethanol (\geq 99.5%) to yield soluble Li alkoxide and white precipitate Al alkoxide nanowires (Al(EtO)₃ NWs). After initial delithiation, Li alkoxides were decanted and then Al(EtO)₃ NWs were washed by extra dry alcohol. The produced Al(EtO)₃ NWs were cast on polyethylene, and 375

ethanol was evaporated at room temperature under argon protec-376 tion. The final step of the Al(EtO)₃ NWs' transformation into 377 Al₂O₃ NWs involved calcination at 1000 °C in air at atmospheric 378 pressure. 379

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380 Materials characterization

Scanning electron microscopy (SEM) images were obtained using 381 an electron microscope ULTRA 55 (Zeiss, France) equipped with a 382 thermal field emission emitter and three different detectors (EsB 383 detector with filter grid, high efficiency In-lens SE detector, and 384 Everhart-Thornley Secondary Electron Detector). Transmission 385 electron microscopy (TEM) images were recorded on a JEOL 386 TEM 4000EX (JEOL, Japan) operating at 300 kV. Thermogravi-387 metric analysis (TGA) was conducted on TGA Q50 analyzer (TA 388 instruments, USA) under air atmosphere at a heating rate of 5 °-389 C⋅min⁻¹. The powder X-ray diffraction (X'Pert PRO Alpha-1, 390 USA) was performed using Cu-Ka radiation to identify the crys-391 talline phase of the composite. X-ray photoelectron spectroscopy 392 (XPS) was performed using a PHI 5000 VersaProbe-Scanning 393 ESCA Microprobe (ULVAC-PHI, Japan/ USA) instrument at a base 394 pressure below 5×10^{-9} mbar. Core-level spectra were acquired 395 396 at pass energy of 23.5 eV with a 0.1 eV energy step. All spectra were recorded with 90° between X-ray source and analyzer and 397 with the use of low-energy electrons and low-energy argon ions 398 for charge neutralization. After subtraction of the linear back-399 ground, the core-level spectra were decomposed into their com-400 401 ponents with the mixed Gaussian-Lorentzian (30:70) shape lines using the CasaXPS software. Quantification calculations 402 were conducted using sensitivity factors supplied by PHI. Fourier 403 transform infrared (FTIR) spectra were recorded using a ThermoS-404 cientific FTIR instrument (Nicolet 8700) at a resolution of 405 4 cm^{-1} . Dried sample (1 mg) was mixed with KBr powder 406 (100 mg) in an agate mortar. The mixture was pressed into a pel-407 let under 10-ton load for 2-4 min, and the spectrum was recorded 408 immediately. Sixteen accumulative scans were collected. The sig-409 nal from a pure KBr pellet was subtracted as the background. 410 411 Zeta-potential measurements were performed using a Zeta-sizer Nano-ZS (Malvern Instruments Inc. Worcestershire, UK) in clear 412 disposable zeta cell. Samples were diluted to $10 \,\mu g \,m L^{-1}$ for 413 Al₂O₃ MPs, γ -Al₂O₃ NWs, and 0.2% for alum in Milli-Q water 414 and were run at 25 °C in quintuplicate with automatic parameter 415 selection (>12 runs). 416

417 Cell viability and internalization

The HeLa cell line derived from cervical carcinoma [ATCC® CCL-418 2TM, ECACC, Sigma–Aldrich, Saint-Quentin Fallavier, France] and 419 the U-87 MG cell line derived from human brain (glioblastoma 420 astrocytoma) [ATCC[®] HTB-14[™], Sigma–Aldrich, Saint-Quentin 421 422 Fallavier, France] were cultured and maintained in Dulbecco's Modified Eagle's medium (DMEM, Gibco®) supplemented with 423 10% fetal bovine serum (FBS, Gibco®) and 1% penicillin-strepto-424 mycin (Gibco[®]) in a humidified incubator at 37 °C and 5% CO₂. 425 Cells were seeded at a density of 10⁴ cells/well in a 96-well 426

plate and grown for 24 h before assay. The culture medium was 427 replaced with a fresh medium that contains $\gamma\text{-Al}_2\text{O}_3$ NWs and 428 429 alum hydroxide 2% at different concentrations. After 24 h, the 430 old medium was aspirated, washed with PBS and replaced with a fresh medium. The cell viability was evaluated using Uptiblue (Interchim) method. Briefly, 10 µL of the Uptiblue solution was added to each well containing 100 µL of DMEM with 10% FBS and the plate was incubated for 4 h in the humidified incubator. The fluorescence of each well (excitation 540 nm/emission 590 nm) was measured using a microplate reader (PHERAstar FS, BMG LABTECH GmbH, Germany). Each condition was replicated five times and the mean absorbance value of non-exposed cells was taken as 100% cellular viability.

Cytotoxicity studies on macrophages

The human monocytic THP-1 cells were cultured and maintained in culture in Roswell Park Memorial Institute medium (RPMI 1640, Invitrogen) supplemented with 10% fetal bovine serum (FBS, Gibco®), 1% penicillin-streptomycin (Gibco®) and 50 μM β-mercaptoethanol in a humidified incubator at 37 °C and 5% CO2. THP-1 monocytes were differentiated into macrophages by a 5-day incubation with 20 nM phorbol 12-myristate 13-acetate (PMA, Sigma) and seeded at a density of 1.5×10^4 cells/well in a 96-well plate. The culture medium was replaced with a fresh medium without β -mercaptoethanol that contains the compounds from 0 to 400 μ g mL⁻¹. After 24 h, the cell viability was evaluated using Calcein-AM and PI co-staining. The cells were stained without any washing by addition of 10 µL of Calcein-AM/PI mix solution (45 µM/30 µM) in each well and incubated at 37 °C for 30 min. Subsequently, the stained cells were observed with $4 \times$ objective (GFP and Texas Red filter cubes) using a Cytation[™] 5 Cell Imaging Multi-Mode Reader (BioTek Instruments SAS, France).

Animals

Six-week-old male Balb/c mice were used. The mice were housed 460 in cages covered with air filters in a temperature-controlled room 461 with a 12-h light and 12-h dark schedule and kept on a standard 462 diet with drinking water available ad libitum. Studies involving 463 animals, including housing and care, method of euthanasia, 464 and experimental protocols, were approved by the Ethics committee of Danylo Halytsky Lviv National Medical University, protocol 20180226/2 & 20130624/6; all experiments were designed to comply with principles of the 3Rs (Replacement, Reduction 468 and Refinement). Totally, 34 mice were analyzed: 12 mice immu-469 nized with alum + OVA, 13 mice immunized with γ -Al₂O₃ NWs 470 + OVA, 4 mice immunized in Al₂O₃ MPs + OVA, 5 mice immu-471 nized with OVA alone; immunization was done in 3 indepen-472 dent experiments. 473

Mice immunization model

For correct comparison, Al₂O₃, Al₂O₃ NW, and Al(OH)₃ were used as pure compounds and prepared as dispersions just before 476 immunization after pre-heating to 150 °C for 2 h to eliminate 477 LPS. The dispersions of 'alum + OVA', 'Al₂O₃ MPs + OVA', and 478 'γ-Al₂O₃ NWs + OVA' were prepared by mixing OVA and an adju-479 vant (Al₂O₃, γ -Al₂O₃ NWs or alum) in phosphate-buffered saline 480 (PBS) by means of the sonication at 44 kHz for a duration of 481 10 min at 25 °C until a homogenous clear dispersion is achieved. 482 Suspensions were prepared immediately before the injection. 483 The 50 µL of 'adjuvant (20 mg mL-1) + 50 µL OVA (1 mg mL-1)' 484

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in PBS were injected intraperitoneally (PI) in mice at day 1 and day 15 of the experiment. The DTH test was performed 28 days after the 1st immunization by injection of 50 μ L of OVA in PBS (100 μ g mL⁻¹) into the right hind paw. Injection of 50 μ L of PBS into the left hind paw was used as a control. The thickness of the paw was measured with a caliper (B110T; Kroeplin Laengenmesstechnik) before the injection and 6, 24, 48, 72, and 96 h after it, as described previously [18]. Blood was collected from mouse tail before experiment started (day 0), before second immunization (day 14), and at the end of experiment (day 35). No more that 50 μ l of blood was collected to prevent damage to the animal. Serum was isolated (usually 20 μ l per mice) and immediately frozen.

Air pouch model

Air pouch model [32] was performed by injection of 5 mL of sterile air subcutaneously into the back of Balb/c mice to form an air pouch. In two days, an additional 2 mL of sterile air were blown into the pouch. Two days later, 4 mg of γ -Al₂O₃ NWs, 4 mg of alum in PBS, 4 mg of Al₂O₃ MPs, or PBS only was injected into the air pouches of each mice. Next day, mice were sacrificed, and the air pouch membranes were analyzed.

506 ELISA procedure

For determination of serum anti-OVA IgG and IgM, immunosor-507 bent NUNC MaxiSorp plates were coated with 50 µL of a 5 µg/mL 508 solution of chicken egg albumin in 100 mM carbonate-509 bicarbonate buffer (pH 9.6). Plates were incubated overnight at 510 4 °C and washed three times with phosphate-buffered saline sup-511 plemented with 0.05% Tween (PBS-T). The plates were blocked 512 with 100 µL of 4 % BSA in PBS-T for 2 h at 37 °C. To follow the 513 514 dynamics of Ab production all serum samples were diluted 1:2000 in washing buffer. Detection was done with goat anti-515 mouse IgG(H+L)-HRP (Jackson ImmunoResearch, 115-035-003) 516 for IgG or goat anti-mouse IgM-HRP (Jackson ImmunoResearch, 517 115-035-020) for IgM, diluted in washing buffer (1:10000). For 518 519 determination of IgG antibody titers, samples collected at day 35, after second immunization, were diluted 1:1000, 1:2000, 520 521 1:4000, 1:8000, 1:16000, 1:32000, 1:64000, and 1:128000. 522 50 µL of prepared solution was added to the well and incubated at 37 °C for 1 h, after that the plates were washed again. Detec-523 tion was done using goat anti-mouse IgG(H+L)-HRP (Jackson 524 525 ImmunoResearch, 115-035-003), which were diluted in washing buffer (1:10000), added to the plates (50 µL per well) and 526 incubated at room temperature for 1 h. After the corresponding 527 washings, the assay was developed with TMB (3,3',5,5'-tetrame 528 thybezidine) containing H_2O_2 as a substrate (50 μ L per well). 529 530 The reaction was stopped with 50 µl of 1 N sulfuric acid and absorbance was read at 450 and 620 nm reference wavelength 531 at Perkin-Elmer HST 7000 BioAssay reader. To account for differ-532 ences between plates, values were corrected using a standard 533 serum applied on each plate. 534

535 Analysis of DNA externalization

Human granulocytes were isolated from heparinized venous
blood of normal healthy donors by Lymphoflot (Bio-Rad) density
gradient centrifugation, as described [35]. The granulocyte-rich
layer on top of RBCs was taken and subjected to hypotonic lysis

of RBCs. Isolated granulocytes were cultured in 96-well culture 540 plates at 5×10^6 cells per milliliter with special inducers of NETosis and with the fluorescent nucleic acid dye Sytox green (Life 542 Technologies). The fluorescence was measured in kinetics for 3 h using BioAssay Reader HTS7000 (Perkin Elmer), excitation 544 480/15 nm, emission 535/20 nm. 545

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Acknowledgments

Sila Nanotechnologies, Inc; the Centre National de la Recherche 547 Scientifique (CNRS), the University Lille 1, the Hauts-de-France 548 region, the CPER "Photonics for Society", the Marie 549 Sklodowska-Curie action (H2020-MSCA-RISE-2015, PANG-550 690836), Volkswagen-Stiftung grant #90361, and Ministry of 551 Healthcare of Ukraine are acknowledged for financial support. 552 Servier Medical Art is acknowledged as a source of some illustra-553 tive materials. We thank S. Peshkova for technical assistance. 554

Author contributions

RoBi and SS conceived the idea; RoBi, SP, and TD performed556immunization, animal experiments, neutrophil isolation, and557ex vivo experiments; RaBo, AB, FW, and SZ performed physical558characterization; AB performed cell culture testing; KT and FW559synthesized NWs; RB, SS, GU, and KT wrote the manuscript.560

Data availability

The raw/processed data required to reproduce these findings cannot be shared at this time due to technical or time limitations. Q5 563

Appendix A. Supplementary data

Supplementary data to this article can be found online at 565 https://doi.org/10.1016/j.mattod.2018.10.034. 566

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