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Needle localization for needle steering under 3D ultrasound feedback

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Introduction

Motivation and objectives

- In needle steering, estimating the needle pose is a critical problem
- In 3D ultrasound volumes, fine needle localization is difficult and requires a combination of estimation and image processing to be successful. Indeed, 3D ultrasound imaging suffers from noise, artifacts and works at a low frequency We propose a needle tip pose estimation method in the context of 3D robotic
 - needle steering under 3D ultrasound feedback, based on multi-rate, multi-



Methods

- sensor fusion [1]
- This estimation feeds a segmentation algorithm for robust needle detection



3D kinematic bicycle model

- The needle tip path is modeled by a bicycle kinematic model [3]
- β_{cut} is the cutting angle of the needle, as deduced from data fitting



Multi-rate unscented Kalman filter

The needle tip pose and curvature are estimated by a multi-rate unscented Kalman filter

All available measurements are taken into account asynchronously



filter updates The the estimation error covariance online to account for poor 3D US quality and expected changes of tissue stiffness

Tools

Robotic device

- PROSPER robot for brachytherapy procedure [2]
- 6 degrees of freedom, needle insertion and rotation module

Ultrasound (US) imaging

3D US imaging in B-mode

- 3D B-mode US volume @ 1Hz
- 3D end-fire probe 4DEC-9/10 with Ultrasonix Sonix RP US system





Echogenic Needle Coating

Needle-related artefacts appear such as comet tail artefacts, reverberation etc.

Results

Pre-operative shear wave imaging (SWE)

- SWE estimates tissues Young's modulus from their response to a shear wave US stimulation
- The needle curvature is proportional to the tissue stiffness



- 51 insertions of 8 cm at 1.5 mm.s⁻¹
- Validation on phantoms and ex vivo tissue sample

Medium	Needle	$E_{mean}(mm)$	$E_{std}(mm)$	$E_{max}(mm)$
Agar	S-BT	0.5	0.3	1.9
Agar	N-BT	0.6	0.3	2.6
Paraffin	$\operatorname{S-PC}$	0.6	0.4	6.0
Pork	N-BT	0.7	0.3	1.7

Needle tip localization error N-BT : Nitinol bevel-tip S-PC : Steel pre-curved





0 50 100 150 200 250 300 Bi-layered Agar phantom and associated SWE Young's Modulus (kPa) The red part is stiffer than the blue one Needle curvature dependency to tissue stiffness	Depth of observation (mm) Needle tip path estimation (green) in the last acquired 3D US Volume Needle tip final position prediction Iast acquired 3D US Volume	
Conclusion	References	
 The tip pose estimation is accurate, robust to needle disappearance and 3D ultrasound imaging artefacts An adapted segmentation method, inherited from [4], uses the resulting ROI for needle tip segmentation in the 3D US volumes The good estimation of the tip behavior and its uncertainties could benefit to adapted control laws and path planning methods 	 G. Lapouge, J. Troccaz and P. Poignet, Multi-rate unscented Kalman filtering for pose and curvature estimation in 3D ultrasound-guided needle steering, Control Engineering Practice, vol. 80, pp. 116-124, 2018 N. Hungr, M. Baumann, JA. Long, and J. Troccaz, A 3-D ultrasound robotic prostate brachytherapy system with prostate motion tracking, IEEE Transactions on Robotics, vol. 28, no. 6, pp. 1382-1397, 2012 R. J. Webster, J. S. Kim, N. J. Cowan, G. S. Chirikjian, and A. M. Okamura, Nonholonomic Modeling of Needle Steering, The International Journal of Robotics Research, vol. 25, no. 5-6, pp. 509-525, 2006 H. Younes, S. Voros, and J. Troccaz, Automatic needle localization in 3D ultrasound images for brachytherapy, International Symposium on Biomedical Imaging (ISBI), IEEE, pp.1203-1207, 2018 	
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