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► **To cite this version:**

Sébastien Levilly, Jérôme Idier, David Le Touzé, Perrine Paul-Gilloteaux, Félicien Bonnefoy, et al.. Spatio-temporal filtering of blood flow in 4D Phase-Contrast MRI. Society for Magnetic Resonance Angiography, 29th Annual International Conference (SMRA 2017), Oct 2017, Stellenbosch, South Africa. 61, pp.3163 - 3178, 2015. hal-01720378

**HAL Id: hal-01720378**

**<https://hal.science/hal-01720378>**

Submitted on 1 Sep 2020

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# Spatio-temporal filtering of blood flow in 4D Phase-Contrast MRI

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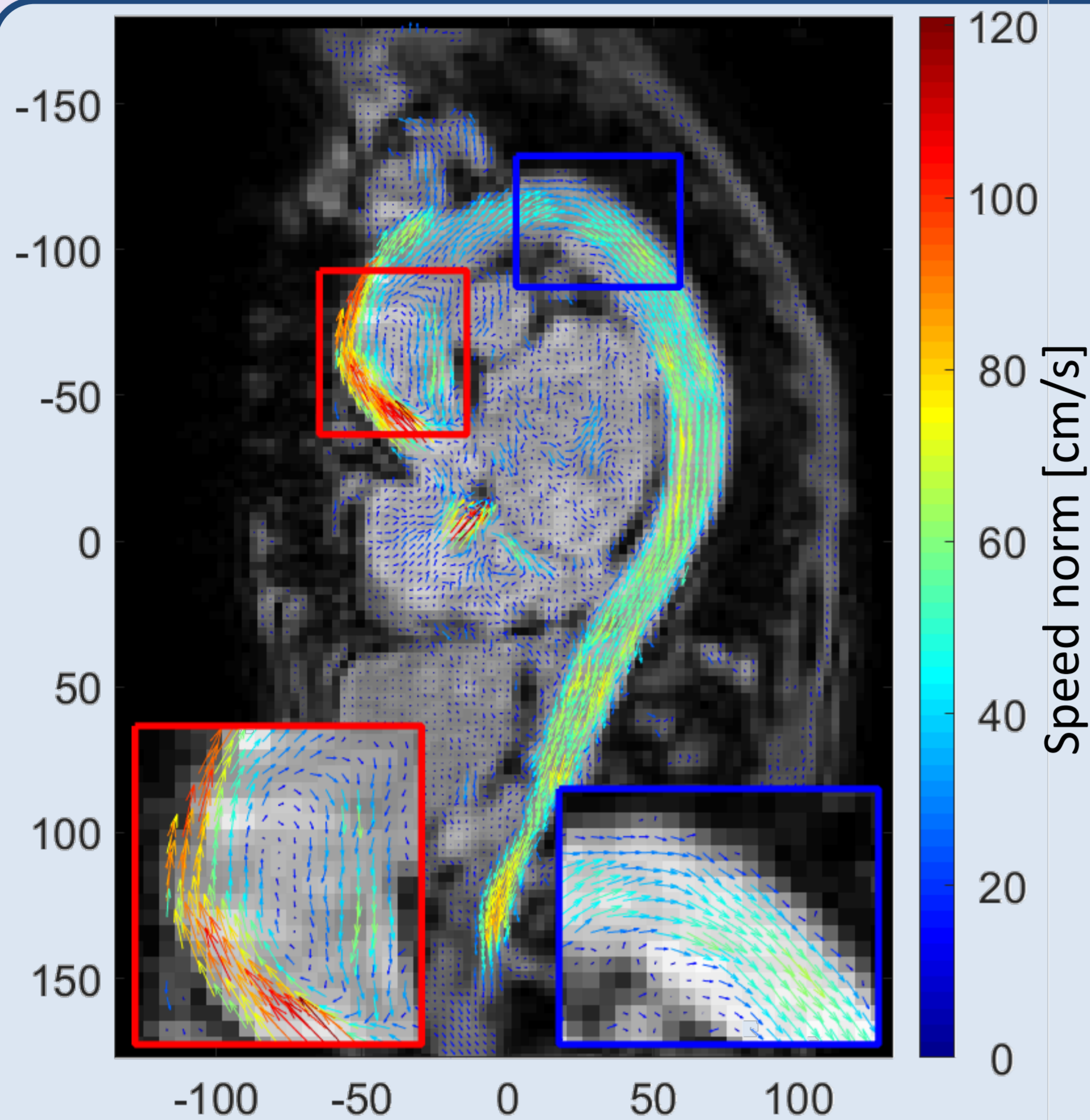


Figure: Cardiovascular image obtained by 4D flow Phase-Contrast MRI (anatomy and speed).

## Context

### 4D flow PC-MRI:

- Acquisition time: 8-20 min
- Resolution: [2,8x2,8x2,2 mm<sup>3</sup> ; 30ms]

### Technological constraint:

Measurements are subjected to :

$$SNR \propto \log \left( K \times \frac{T_{\text{acquisition}}}{N_{\text{voxels}}^3} \right)$$

with  $K$  a system and patient linked constant.

- ➔ **Low reliability of biomarkers values**
- ➔ Wall Shear Stress [Boussel et al., 2009]

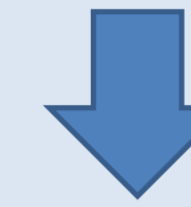
### MRI-Quantif project objective:

Enhance biomarkers estimation reliability in 4D flow PC-MRI.

## Contribution

Denoise the speed vector field in the region of interest on the same data grid.

**Strategy:** Inverse problems theory



A priori knowledge on the vector field

➔ The vector field represents the speed vectors of the blood flow in the vessels.

➔ Simplest fluid mechanics hypothesis:
 

- Incompressibility [Dehghani Tafti et al., 2011; Busch et al., 2013; Song et al. 1993; Bostan et al., 2015]

## Problem statement

### Hypotheses:

- Incompressible fluid
- Time regularity

$$\hat{V} = \underset{s.c. V \in \mathcal{M}_0}{\operatorname{argmin}} \{ \|V_m - V\|^2 + \lambda \|D_t V\|^2 \}$$

with  $V_m$  the data vector,  $\lambda$  the time penalization weight,  $D_t$  a finite-difference matrix in time such that  $D_t V = V_{t+1} - V_t$ .

$\mathcal{M}_0$  is the divergence-free vector field:

$$\mathcal{M}_0 = \{ v \in \mathbb{R}^{3 \times N_{\text{voxels}}} \mid D_s v = \vec{0} \}$$

with  $D_s = (D_x \ D_y \ D_z)$  a discrete version of the divergence operator.

### Solution:

Application of two separable operators:

$$\hat{V} = (I + \lambda D_t^T D_t)^{-1} P V_m$$

with  $I$  the identity matrix and  $P$  the orthogonal projector on  $\mathcal{M}_0$  for all acquisition times [Song et al., 1993]. This projector can be written for a given instant as:  $P_0 = I - D_s^t (D_s D_s^T)^{-1} D_s$ .

## Results

### Synthetic data: Womersley flow [Womersley, 1955]

#### Hypotheses:

- Incompressible, homogeneous, Newtonian and non-stationary
- Circulates in a cylinder (1cm radius)
- Input: Cardiac flow [Puelz et al., 2017]

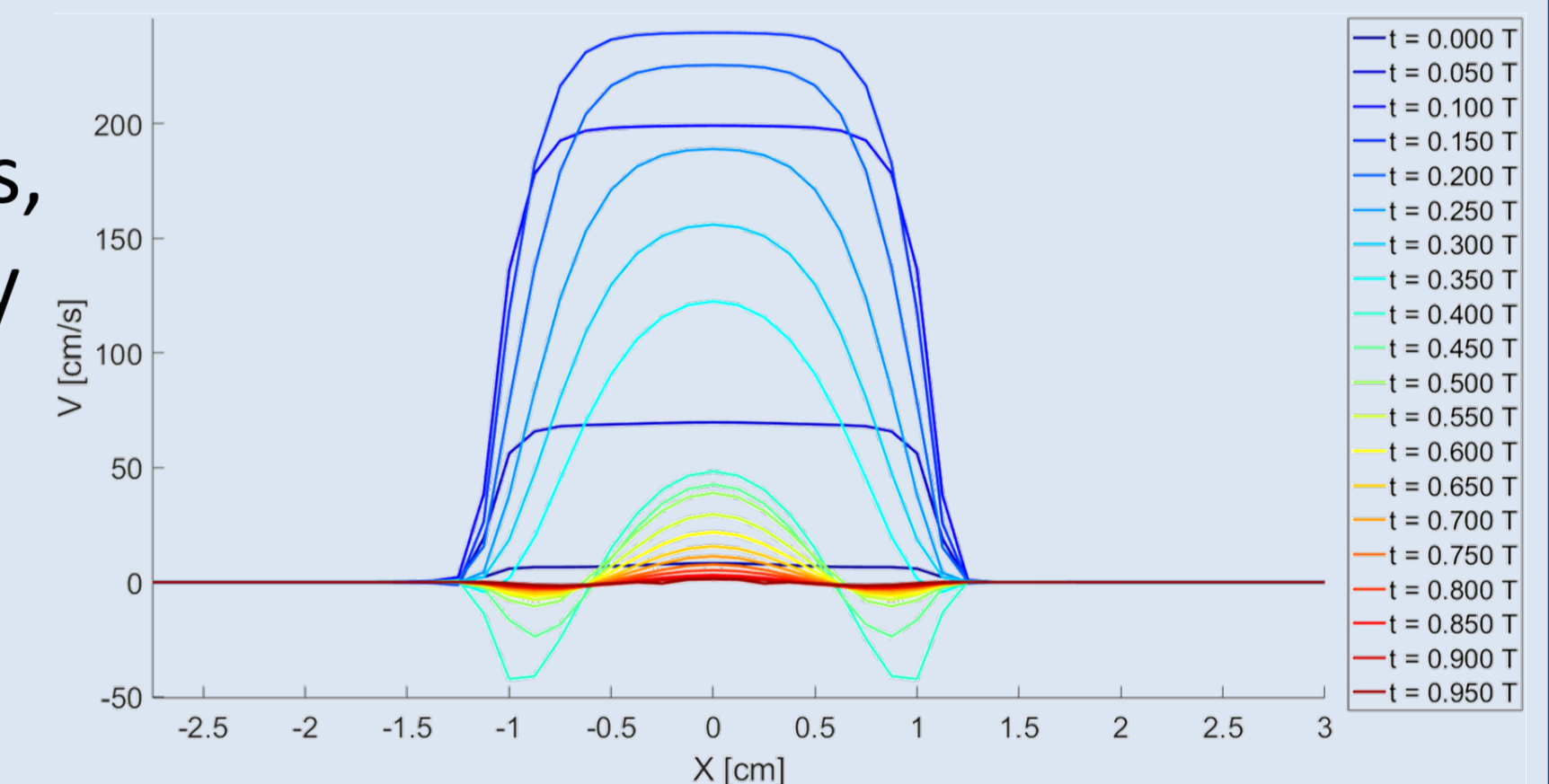


Figure: Analytical flow of Womersley over time

### Studied problem: 2D+time simulation [2.5x2.5mm<sup>2</sup>; 46ms]

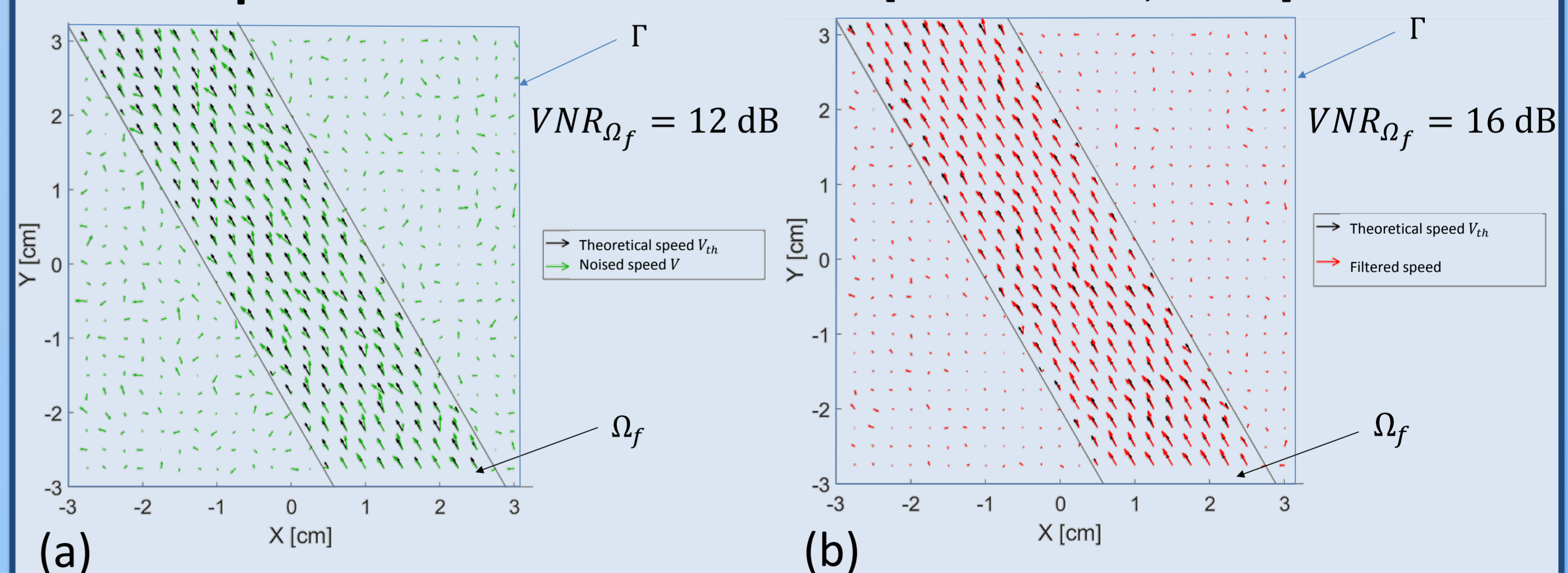


Figure: Noised vector field (a) and filtered vector field (b) at a given instant with the velocity-to-noise ratio defined as:  $VNR = 20 \log \left( \frac{\|V_{th}\|}{\|V - V_{th}\|} \right)$ .

$VNR_{\Omega_f}$ input	$VNR_{\Omega_f}$ after spatial-only filtering	$VNR_{\Omega_f}$ after spatio-temporal filtering
9 dB	12 dB	13,9 dB
12 dB	14,7 dB	16,2 dB
15 dB	17,7 dB	18,3 dB
30 dB	27,4 dB	27,4 dB

Table: Velocity-to-noise ratio after spatial (incompressibility projection) and spatio-temporal filtering for different  $VNR_{\Omega_f}$  inputs ( $\lambda$  is chosen to optimize the  $VNR_{\Omega_f}$ ).

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## Conclusion

- Solving of a problem including incompressibility and time regularity hypotheses;
- Direct and simple solution using two separable operators;
- Significant improvement of the  $VNR_{\Omega_f}$  within the vessels.