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Finger Flexors Fatigue in Trained Rock Climbers and Untrained Sedentary Subjects

F. Quaine
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Abstract

The present series of experiments were conducted to access the surface EMG frequency parameters during repeated fingertip isometric contractions to determine if they can be used as a fatigue index under specific grip used in rock climbing. Electromyograms of the finger flexors and extensors were characterised in ten elite climbers and ten non-climbers. The exercise consisted in reaching 80% of maximal isometric finger force as quickly as possible intermittently with a 5-s contraction followed by 5-s of rest until exhaustion (i.e. when the subject was unable to maintain 80–70% MVC force range for the 5 s). The results clearly indicate that expert climbers performed significantly greater

fingertip force than sedentary subjects (420 ± 46 N vs. 342 ± 56 N). This force was maintained during twelve repetitions (12.88 ± 4.96) in sedentary subjects, whereas the climbers maintained the force during nineteen repetitions (19.33 ± 4.84). The median frequency of both the flexor and extensor EMG power spectra decreased during fatiguing isometric contractions, but at different rates in climbers and non-climbers. In non-climbers, the results replicated previous findings, whereas in climbers the results were novel.

Key words

Muscular fatigue · fingertip force · biomechanics · rock climbing

Introduction

There has been remarkable development in the scope and quality of rock climbing in the last few years. The hands are used as tools for the ascent, and many of the external supporting forces are applied upon the fingers and also distributed through the wrist, elbow and shoulder [3]. Three quarters of elite and recreational sport climbers suffer from injuries of the hand [16]. Only one study exhibited an electromyographic analysis of the arm muscles during climbing [10]. However, this study remains far away from the activity, since the task corresponded to a basic pull-up (the authors focussed more on the muscles crossing the elbow joint rather than fingers muscles). It thus seems important to find out the degree of exertion of the involved finger muscles during a gripping task which accurately mimics the grip used in rock climbing.

Fatigue, defined as the inability to produce the required force [21], is a major factor of fall and injury [3]. The influence of fatigue on EMG parameters during static intermittent sub-maximal voluntary muscle contractions is well documented in the literature [2,9,19]. The EMG frequency parameters decrease toward lower frequencies with fatigue, which mainly results from the decrease in muscle fiber conduction velocity [7]. Few studies have reported muscular endurance data concerning climbers and the mode of investigation varies. Muscular endurance was measured in both sustained and rhythmic isometric handgrip exercises at 40% of maximal voluntary contraction [8]. The results showed no significant different maximal force and endurance time between climbers and non-climbers during sustained contraction, while the intermittent time for climbers was twice as long as for non-climbers.

The purpose of the present study was to analyze fingertip force and electromyographic parameters of elite climbers and non-

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climbers with fatigue in forearm muscles (finger flexors and extensors) in a grip posture close to rock climbing conditions. Knowledge of muscle involvement associated to hold grasping and the constraints it involves on the force production and the rate of fatigue may be useful to prevent musculo-skeletal diseases, to improve simulated handhold shapes and to increase safety.

Material and Methods

Subjects

A total of 20 right hand-preferred male subjects took part in this study. Ten subjects (age: 24 ± 1.8 y; height: 178.1 ± 5 cm; body mass: 74 ± 3 kg) were novices (labeled SED in the text) in rock climbing. Ten subjects (age: 22 ± 1.4 y; height: 177.4 ± 4.5 cm; body mass: 65.6 ± 2 kg) were elite rock climbers (labeled CLB) recruited from the best national French climbers (French 8a or 5.13 a Y.D.S on sight, which corresponds to the world cup level). All subjects gave their written informed consent.

The subjects were seated in a chair and instructed to keep the anterior surface of their forearm on a table. The wrist was fixed thanks to a mitten at 40° of extension in front of the hold. The upper arm was at 45° of abduction, the elbow joint being flexed at 90° . The distance between the hold and the support point of wrist fixation was $1/3$ of the length of the third finger and induced a "crimp" grip posture as proposed by Schweizer [18]. The degree of the flexion was measured using a digital camera located 0.70 m above the device. This camera measured the sagittal index finger posture. Two markers were aligned with the longitudinal axis of the segment. The angle of intersection of the lines of adjacent segments defined the joint angles. They were assumed to be similar for the four fingers. The proximal interphalangeal joints are flexed from 90° to 100° and the distal interphalangeal joints are hyperextended.

The hold consisted of a steel plate ($100 \times 20 \times 3$ mm) covered with a non-skid surface fastened to the force sensor. The fingers gripped the hold on a one centimeter deep surface. The thumb did not act as an additional gripping force. A second stop was fastened behind the elbow. Consequently, the fingertip force generated resulted only from isometric finger flexor muscle contractions.

The subjects warmed up on the device by carrying out a series of twenty contractions for 5 s at 50 N (chosen arbitrarily). After a 3-min rest, the subjects performed three maximal isometric finger flexion contractions for 5 s separated by a 5-min resting period. The highest peak force generated was adopted as maximal voluntary contraction force (MVC). During pre-test experiments, we tested that the warm-up exercise did not induce fatigue in climbers nor in non-climbers.

After ten minutes rest, the subjects carried out as quickly as possible finger flexion contractions at 80% MVC during 5 s followed by 5 s of rest. The contractions were continued until exhaustion, defined as the point when the subjects were unable to maintain -10% of the initial target force (i.e. 80–70% MVC range) for the required 5 s. Each subject was given oral encouragement and was

provided with an ongoing force output which was displayed on a computer screen to confirm his achievement throughout the test.

Surface EMG activity was recorded from extrinsic muscles of the hand during each test session. In power gripping, the extrinsic muscles of the hand, especially the flexor digitorum superficialis and/or profundus, provide most of the force [1]. The flexor muscles were located by asking the subject to flex the four fingers against external resistance while visually observing and palpating the forearm over the contracting muscle. To ensure that the flexor carpi radialis (a wrist flexor) was not contributing significantly to the EMG signal, electrode placement was considered appropriate when the EMG signal was present during fingers' flexion with a voluntary stable wrist, yet absent during wrist flexion with no voluntary finger flexion [4]. Concerning the extensor muscles, the electrodes were placed around the $1/4$ point on a line drawn from the lateral epicondyle to the styloid process of the ulna [1]. The electrodes were located parallel to the assumed longitudinal axis of the muscle fibers. Pre-amplifier electrodes ($\times 600$) were used (input impedance $10\text{ G}\Omega$, common mode rejection ratio = 100 db at 50/60 Hz, bandwidth = 5–1000 Hz) with self adhesive, pregelled silver/silver chloride Medi-Trace (Graphic Controls, Canada) patch. The skin was cleaned (alcohol) and abraded prior to the application of the electrode in a bipolar configuration. Interelectrode distance was 20 mm and interelectrode resistance was inferior to $10\text{ k}\Omega$. A mono-axial load cell (Slumberger, model CD-750) was used to measure the external horizontal force applied to the hold. The signal was amplified (PM, model 1965) and force and EMG were recorded (Mazet Electronique, model Biostim 6082, France) at 1024 Hz.

The number of contractions a subject was able to keep the force level within the 80–70% MVC range was measured and converted into time to fatigue (TF). For each contraction, the raw EMG were low pass filtered (300 Hz cutoff, zero lag fourth order Butterworth filter). Each 5-s squeeze (force and EMG) was divided into 2-s segments adjusted two seconds after the onset of the force increase to eliminate start effects. A Fast Fourier Transform (FFT) with 512 points was used to transform each 2-s EMG segment. Median Frequencies (f_{med}) were computed for each muscle. f_{med} values were expressed relative to their MVC values and used as fatigue indexes. The time-related behavior of f_{med} for each muscle was plotted and the slope of the line of best fit was computed. Each subject provided two slopes (flexor and extensor), one MVC fingertip force and one TF value. All computation procedures were performed using Matlab software (The Math Works, Inc). Descriptive statistics are means \pm SEM. Independent group t-tests of significance were used to identify significant differences in MVC force and TF value between SED and CLB. A two-way ANOVA with repeated measures (2×2 , Subject group \times Muscle) with Tukey post hoc tests was used to analyze the differences in slopes of f_{med} . The interaction Subject group \times Muscle highlights the various changes of EMG frequency parameters in the flexor and extensor between the subjects.

Results

Maximal voluntary force test (Fig. 1)

The comparison of the two groups using a bilateral t-test indicated that the climbers performed significantly greater fingertip forces than the non-climbers ($t = 2.62, p < 0.05$). The maximum forces exerted by the sedentary subjects amounted to 342 ± 56 N, whereas the climbers' MVC equaled 420 ± 46 N.

Time to fatigue results (TF)

The times to fatigue data are presented in Fig. 1. A significant difference between the times to fatigue was observed between SED and CLB ($t = 2.5, p < 0.033$). SED maintained the required fingertip force during 12 contractions, which corresponds to 1 min and 55 s before the grip was released. CLB performed the exercise during 19 contractions which corresponds to 3 min and 5 s.

EMG indices results

Fig. 2 illustrates the drop in f_{med} for each muscle in the sedentary and climber subjects. Negative f_{med} slopes were exhibited for each muscle. The most significant slopes were observed in the sedentary subjects' flexor and extensor (mean slope = 2.09), whereas the ones observed in CLB (mean slope = 0.87) were around 2.5 times inferior.

Statistics

The statistical tests of the slopes differences are illustrated in Fig. 3. The ANOVA results showed a significant effect of Subject group ($F[1,13] = 7.9, p < 0.01$). The f_{med} slope was less marked in the climbers than in the sedentary subjects, whatever the muscle. No significant effect of Muscle was observed. The f_{med} slope in the flexors was similar to the one observed in the extensors, whatever the category of subjects. No significant interaction Subject group \times Muscle was observed. The f_{med} slopes in the flexor and in the extensor were higher in SED and proportionally decreased in CLB.

Discussion

The present study was performed to characterize the forearm muscles exertion during fatigue induced by sub-maximal repetitive rock climbing grip exercise. Fingertip force, time to exhaustion and neuromuscular recruitment adaptation associated to fatigue were analyzed in elite climbers and non-climbers.

The results clearly indicate that expert climbers generate a significantly greater fingertip force than sedentary subjects. This finding confirms previous reports [6], although the present force values were lower. These differences can be explained by the experimental protocol characterized by the requirement of fingertip forces instead of whole hand grip forces [6]. Electromyograms of the finger flexors and extensors in climbers and non-climbers demonstrated that these muscles were similarly involved in the grip. This result does not agree with previous findings which show that co-activation decreases in trained subjects [5,15,17]. Nevertheless, biomechanical considerations show that the external force is applied at the fingertip in rock climbing, which requires specific finger extensor tensions in order to balance finger joint torques [11,18,20].

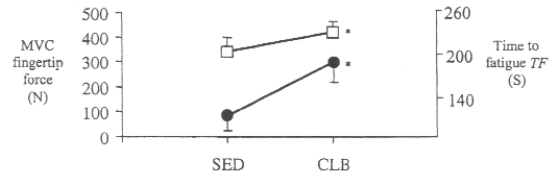


Fig. 1 MVC absolute fingertip force (\square) and time to fatigue (\bullet) in sedentary (SED) and climber (CLB) subjects. Errors bars indicate standard errors. * indicates a significant difference between SED and CLB.

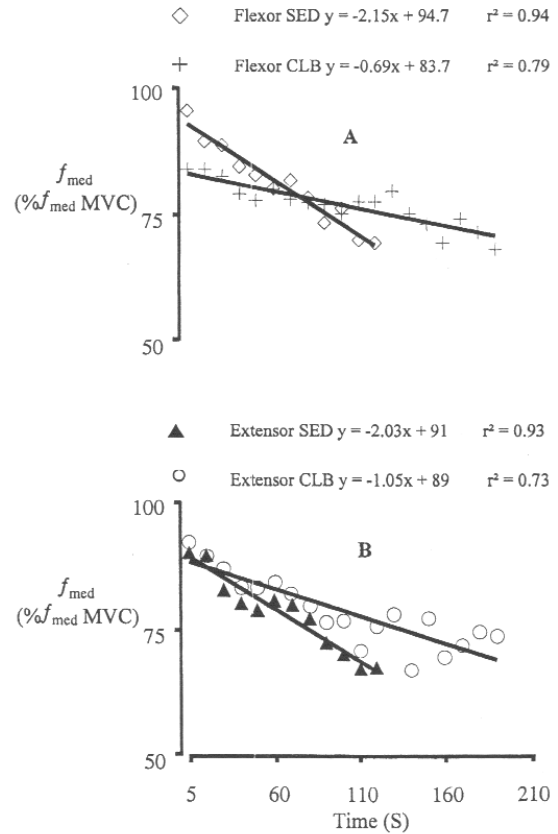


Fig. 2 Relative Median EMG power spectrum frequency (f_{med}) over time during intermittent sub-maximal isometric contraction for flexor

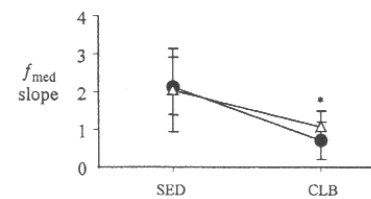


Fig. 3 Mean Relative Median EMG power spectrum frequency f_{med} slopes across subjects ($n = 10$) in sedentary (SED) and climber (CLB) subjects. \bullet represents the flexor and \triangle represents the extensor muscles. Error bars indicate standard errors. * indicates a significant difference between SED and CLB, whatever the muscle.

The climber's time to exhaustion was double that of the non-climbers'. This confirms that climbers have a greater degree of recovery between contractions, since they performed the exercise longer. This result was previously observed during similar exercise performed at lower intensity, i.e. 40% of maximal voluntary contraction [8].

The observed decrease of the median frequency in the non-climbers equaled 23% of pre-fatigue values, whereas it amounted to 8% in elite climbers. In non-climbers, this decrease is in accordance with the model of fatigue of the finger flexors proposed by Petrofsky [13]. This model was based on the percentage of decrease of the median frequency from starting values. It accurately describes fatigue in non-climbers, but does not seem suitable to predict fatigue in trained subjects as elite climbers. The differences observed in the slopes of the median frequency over time explain the durations of exercise noted in elite climbers and non-climbers. The rate of fatigue in non-climbers is more than twice as high as in elite climbers. In all subjects, the resting periods intersperse with periods of fatigue throughout the intermittent exercise. In elite climbers, thanks to their greater vaso-dilatory capacity [8], these periods may be sufficient to reverse the fatiguing effects on the contraction, reducing the accumulation of metabolites [12,14], which induces a smaller reduction of the action potential velocity, and indirectly a smaller reduction of the median frequency. This may thus reduce the lack of force production at the peripheral level and consequently allow them to perform the exercise longer.

Within the limits of the present investigation, the results show that the surface EMG parameters can be used as a fatigue index during repeated fingertip isometric contractions under specific grip used in rock climbing. Elite climbers perform greater fingertip force and present time to exhaustion later than non-climbers, probably by reducing the fatigue at the peripheral level. Nevertheless, before conclusions can be drawn, additional investigations coupling EMG with other parameters (e.g. blood flow, metabolite concentration) must be conducted in other finger grip postures.

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