



Hydroxyapatite-TiO₂-SiO₂-Coated 316L Stainless Steel for Biomedical Application

Djahida Sidane, Hafit Khireddine, Fatima Bir, Sabeha Yala, Alex Montagne, Didier Chicot

► To cite this version:

Djahida Sidane, Hafit Khireddine, Fatima Bir, Sabeha Yala, Alex Montagne, et al.. Hydroxyapatite-TiO₂-SiO₂-Coated 316L Stainless Steel for Biomedical Application. Metallurgical and Materials Transactions A, 2017, 48 (7), pp.3570-3582. <10.1007/s11661-017-4108-8>. <hal-01565674>

HAL Id: hal-01565674

<https://hal.science/hal-01565674v1>

Submitted on 22 Aug 2017

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.



HAL Authorization



Science Arts & Métiers (SAM)

is an open access repository that collects the work of Arts et Métiers ParisTech researchers and makes it freely available over the web where possible.

This is an author-deposited version published in: <http://sam.ensam.eu>
Handle ID: <http://hdl.handle.net/null>

To cite this version :

DJAHIDA SIDANE, HAFIT KHIREDINE, FATIMA BIR, SABEHA YALA, Alex MONTAGNE, Didier CHICOT - Hydroxyapatite-TiO₂-SiO₂-Coated 316L Stainless Steel for Biomedical Application - Metallurgical and Materials Transactions A - Vol. 48, n°7, p.3570–3582 - 2017

Any correspondence concerning this service should be sent to the repository

Administrator : archiveouverte@ensam.eu

Hydroxyapatite-TiO₂-SiO₂-Coated 316L Stainless Steel for Biomedical Application

DJAHIDA SIDANE, HAFIT KHIREDINE, FATIMA BIR, SABEHA YALA, ALEX MONTAGNE, and DIDIER CHICOT

This study investigated the effectiveness of titania (TiO₂) as a reinforcing phase in the hydroxyapatite (HAP) coating and silica (SiO₂) single layer as a bond coat between the TiO₂-reinforced hydroxyapatite (TiO₂/HAP) top layer and 316L stainless steel (316L SS) substrate on the corrosion resistance and mechanical properties of the underlying 316L SS metallic implant. Single layer of SiO₂ film was first deposited on 316L SS substrate and studied separately. Water contact angle measurements, X-ray photoelectron spectroscopy, and Fourier transform infrared spectrophotometer analysis were used to evaluate the hydroxyl group reactivity at the SiO₂ outer surface. The microstructural and morphological results showed that the reinforcement of HAP coating with TiO₂ and SiO₂ reduced the crystallite size and the roughness surface. Indeed, the deposition of 50 vol pct TiO₂-reinforced hydroxyapatite layer enhanced the hardness and the elastic modulus of the HAP coating, and the introduction of SiO₂ inner layer on the surface of the 316L SS allowed the improvement of the bonding strength and the corrosion resistance as confirmed by scratch studies, nanoindentation, and cyclic voltammetry tests.

I. INTRODUCTION

HYDROXYAPATITE (Ca₁₀(PO₄)₆(OH)₂, HAP) is found to be the preferred bioactive ceramic due to its chemical, structural, and biological similarity to the inorganic component of human bones and to its direct bonding capability to surrounding tissues.^[1] However, the mechanical weakness of the HAP limits its practical applications to those requiring little or no load-bearing locations. Therefore, to widen the applicability of the HAP to the sites bearing substantial load, such as dental or hip implant, a coating system including HAP on the metallic implant is being used. Metallic materials such as 316L stainless steel (316L SS), Co-Cr alloy, Ti, and Ti-6Al-4V alloy are widely used biomaterials for hard tissue replacement due to their superior tensile strength, fracture toughness, corrosion resistance, and biocompatibility with the internal human environment.^[2-5] 316L SS is used in orthopaedic medical fields due to its unique property of biocompatibility, cost

effectiveness, and corrosion resistance.^[6,7] It is shown that the introduction of an intermediate thin layer of titania (TiO₂), which possesses combined advantages of biocompatibility and corrosion resistance properties,^[8,9] between the metal substrate and the HAP layer significantly improves the mechanical properties and corrosion resistance of the HAP coatings.^[10-14] On the other side, a large number of articles have reported that the addition of TiO₂ as secondary phase into HAP coatings improved the mechanical and bonding strength of the HAP coatings.^[15-17] Moreover, it is recognized that silica (SiO₂)-based sol-gel systems usually have a high content of surface silanol groups, which have been reported to promote *in vitro* and *in vivo* nucleation of apatite.^[18,19] Galliano *et al.*^[20] reported that the silica films deposited on 316L SS substrate were able to reduce both the corrosion attack on the steel and the iron diffusion to the sample surface. However, not much study has been reported on the effect of silica-coated 316L SS on the structure, mechanical, and electrochemical behavior of the TiO₂-reinforced hydroxyapatite coatings (TiO₂/HAP). Therefore, the objective of the current study is to investigate the hydrophilic properties of SiO₂ film, which can improve the bonding capability of the TiO₂/HAP layer with the substrate and provide a first barrier against corrosion of the 316L SS in simulated human body fluids. Further, nanoindentation test is performed using the continuous stiffness measurement (CSM) mode in order to determine the

variation of the hardness and elastic modulus of the coatings as a function of the indenter displacement.

Finally, the addition of titania phase into HAP and the use of silica as a bonding oxide layer between the TiO₂/HAP top layer and the substrate are studied within the objective to improve the mechanical properties, bonding strength, and corrosion resistance of the hydroxyapatite-TiO₂-SiO₂-coated 316L SS system.

II. MATERIALS AND METHODS

A. Experimental Details

Tetraethyl orthosilicate (TEOS, Fluka 98 pct) was mixed with methyltriethoxysilane (MTES, Fluka 98 pct) in equimolar ratio. Hydrochloric acid (0.1 N) and acetic acid (HOAc) were added as catalysts, and their role is to increase the hydrolysis and condensation. The reaction rate to the concentrations of the chemical species present in the reaction mixture (H₂O + HOAc)/(TEOS + MTES) was 1.7.^[20] After stirring the solution under room temperature conditions for 24 hours, a transparent viscous sol was obtained. Precursor solution for HAP coating was prepared by dissolving phosphorous pentoxide (P₂O₅, Prolabo 100 pct) (0.5 mol/l) and calcium nitrate tetrahydrate (Ca(NO₃)₂·4H₂O, Fluka 98 pct) (1.67 mol/l) in absolute ethanol,^[21] and then the two solutions were mixed and continuously stirred for 24 hours at room temperature. Titanium isopropoxide (TIP, Fluka 100 pct) was used as a titania precursor. The reactivity towards water is modified by acetic acid (molar ratio of TIP/HOAc = 1/10) which is also used as catalyst. 2-methoxy ethanol was added to adjust the viscosity of the solution.^[22] This solution was vigorously stirred under room temperature conditions. For the preparation of the composite sols, HAP and TiO₂ solutions were mixed with different volumes: 0, 20, and 50 vol pct TiO₂, and then the solutions were continuously stirred for 14 hours.

The 316L SS used as the substrates with dimensions of 20 × 10 × 5 mm was mechanically polished using different silicon carbide grit papers from 120 to 1200 grades. A mirror polishing was done using diamond paste of 2 and of 0.7 μm in the final step. The substrates were ultrasonically degreased with acetone and washed with running double-distilled water, and then they were dried at 423 K (150 °C) for 10 minutes.

Table I. The Composition of SBF Solution at 310 K (37 °C)

Order	Reagent	Amount
1	NaCl	7.996 g
2	NaHCO ₃	0.350 g
3	KCl	0.224 g
4	K ₂ HPO ₄ ·3H ₂ O	0.228 g
5	MgCl ₂ ·6H ₂ O	0.305 g
6	CaCl ₂	0.278 g
7	Na ₂ SO ₄	0.071 g
8	(CH ₂ OH) ₃ CNH ₂ (Tris)	6.057 g
9	HCl (1M)	appropriate amount for adjusting pH (pH 7.42)

Finally, the substrates were immersed in the HAP and TiO₂/HAP sols and dipped in the suspensions at a speed of 80 mm/min, and then dried and annealed at 773 K (500 °C) for 60 minutes. The obtained coatings are referenced as follows: 20 vol pct TiO₂ (H80T20), 50 vol pct TiO₂ (H50T50). The SiO₂ layer was coated on the surface of the substrate at a speed of 100 mm/min, and then dried and annealed at 773 K (500 °C) for 60 minutes. The pure HAP and composite HAP/TiO₂ sols were subsequently dip-coated on the outer surface of the SiO₂ film at a speed of 80 mm/min and annealed at 773 K (500 °C) for 60 minutes. The obtained coatings are referenced as follows: 0 vol pct TiO₂ (HAP-SiO₂), 20 vol pct TiO₂ (H80T20-S), and 50 vol pct TiO₂ (H50T50-S). In addition, pure TiO₂ film was prepared by dipping at a speed of 20 mm/min, and then dried and annealed at 723 K (450 °C) for 60 minutes.^[14]

B. Characterizations

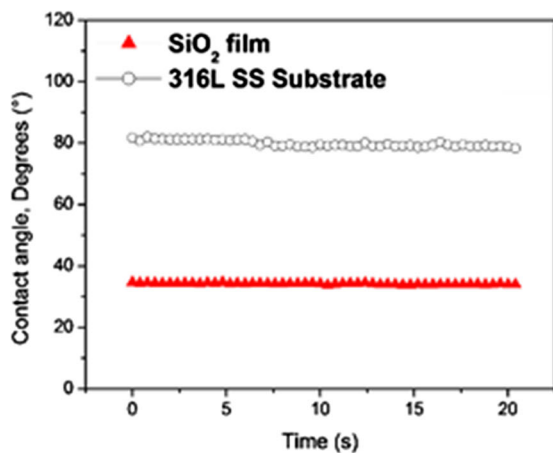
The chemical states of the coatings were characterized by X-ray photoelectron spectroscopy (XPS) with a Thermo L-alpha spectrometer, using monochromatized Al-Kα radiation as the excitation source ($h\nu = 1486.6$ eV), collected at 0 deg from the surface normal, and detected with a hemispherical analyzer. The spot size of the XPS source on the sample was about 200 μm, and the pass energy was set of 20 eV. During data acquisition pressure was kept below 1×10^{-9} Torr. Spectra were fitted using a 10 pct linear combination of Gaussian and Lorentzian profiles. Peak positions obtained after analysis were found essentially constant (± 0.3 eV).

Water contact angles were obtained with a Digidrop Contact Angle Meter (GBX Surface Science Technologies). Measurements were carried out with 3 μl drops of ultra-pure water under ambient atmospheric conditions. Three drops were applied on each sample at different locations, to assure reproducibility and reliability of results.

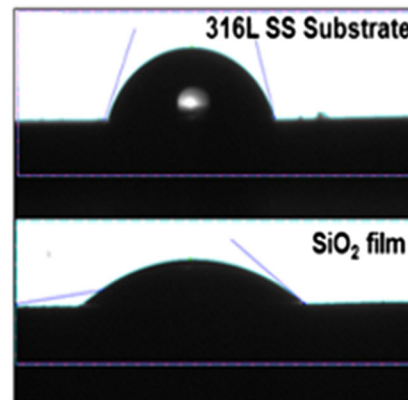
Both the coating thickness and roughness were measured using a profilometry analysis “DEKTA 150 SURFACE PROFILERT” by recording the surface profile of coated and uncoated regions over a single measurement run. The surface of the coating was scanned at an interval of 1000 to 8000 μm. Three different areas were scanned and measured to determine a mean value for the thickness and the roughness parameters.

The surface morphology of the samples was observed with a scanning electron microscope (SEM) (JSM-5400LV, JEOL) operating at 0 to 30 kV, associated with an ultra-thin window Si(Li) detector for the energy-dispersive X-ray measurements (EDX) (GENESIS, Eloise SARL).

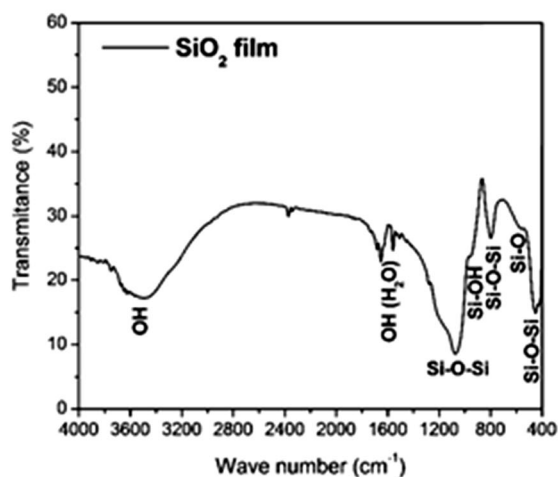
The different phases of the coatings were analyzed by X-ray diffraction Expert Prof Panalytical type MPD/ system vertical θ/θ , using radiation source (Cu-Kα = 1.5406 Å) operating at 40 kV and 30 mA. The XRD diffraction patterns were collected over a 2θ range located between 20 and 80 deg using an incremental step size of 0.02 deg with 6 seconds of acquisition time per



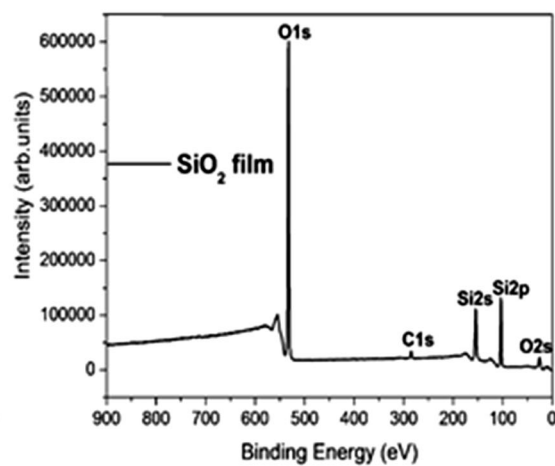
(a)



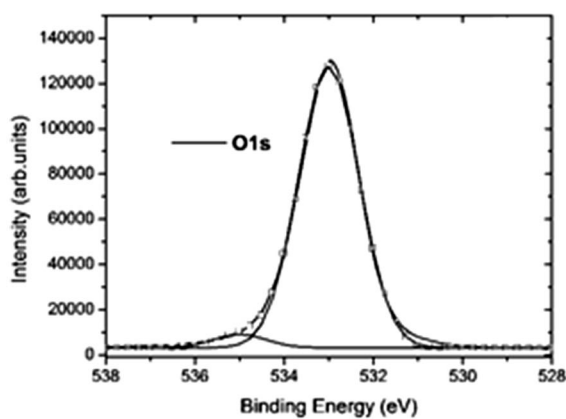
(b)



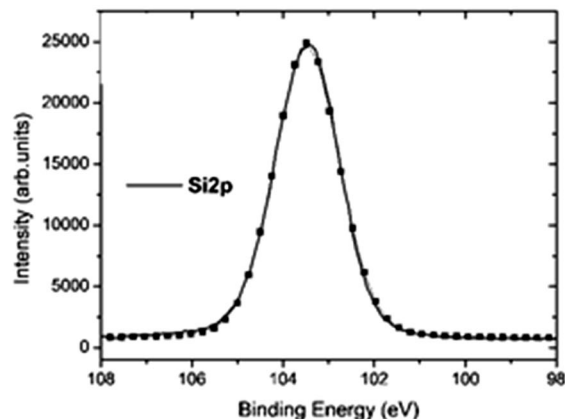
(c)



(d)



(e)



(f)

Fig. 1—(a) Contact angle between water, SiO₂ oxide film, and 316L stainless steel substrate, (b) Images of water droplets on the surfaces of the substrate and SiO₂ film obtained after 20 s (c) FTIR spectrum of the single SiO₂ film, (d) XPS spectrum of the single SiO₂ film, (e, f) The spectra of O1s and Si2p, respectively.

step. The phase identification was performed by comparing the experimental XRD patterns to standards compiled by the International Center for Diffraction Data-Powder Diffraction Files (ICDD-PDF). Data were

treated with Software X'Pert HighScore. The HAP and TiO₂/HAP average crystallite sizes (L) were estimated with broadening XRD peaks using Debye-Scherrer equation:

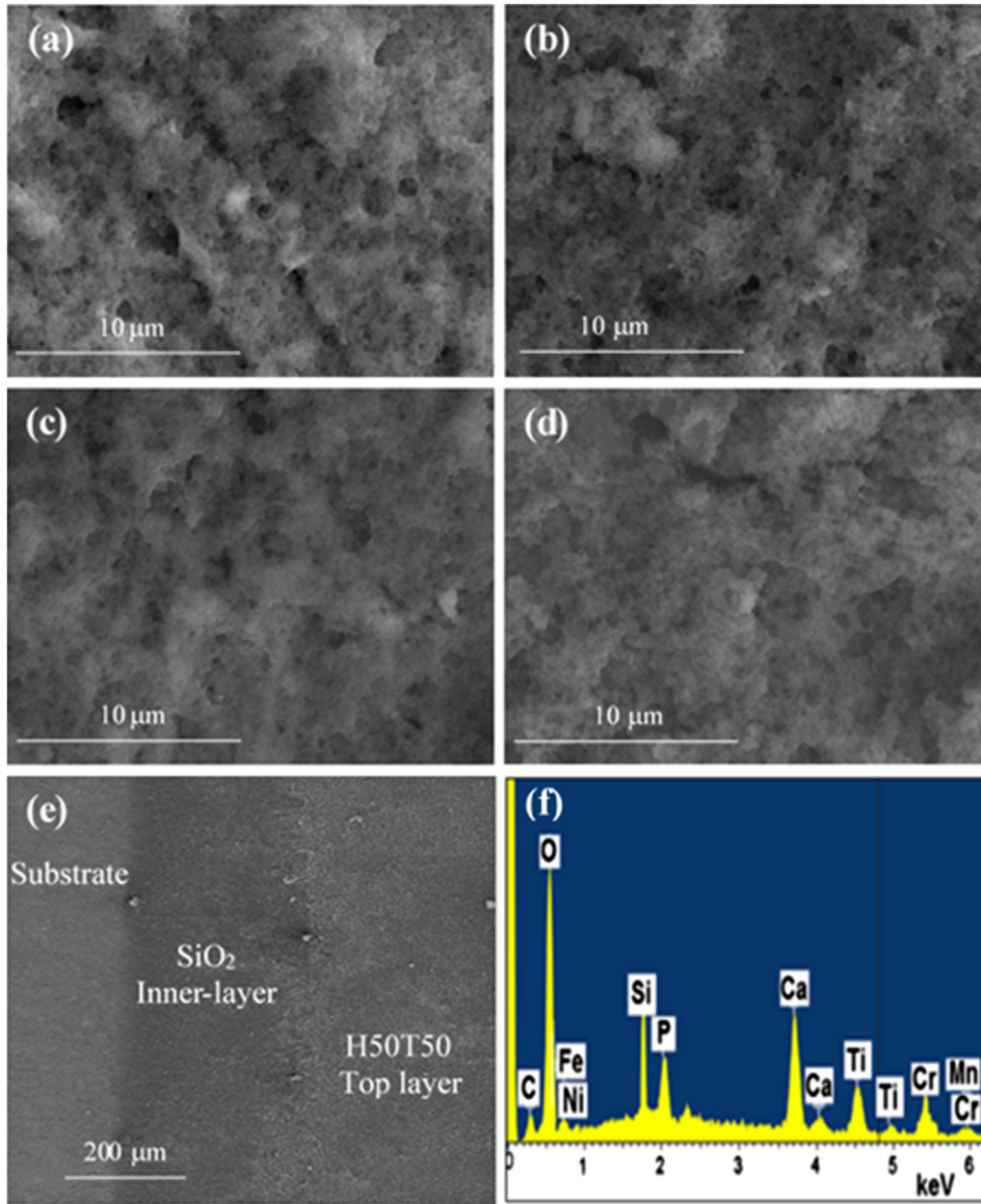


Fig. 2—SEM observations corresponding to (a) H80T20, (b) H50T50, (c) H80T20-S, and (d) H50T50-S coatings, (e) 316L SS substrate-SiO₂-H50T50 interfaces, (f) EDX elemental analysis.

Table II. Structural Parameters of the Uncoated and Coated 316L SS

Sample	Thickness (nm)	Roughness (nm)
316L SS	—	20
HAP	1600	1310
HAP-SiO ₂	1610	921
H80T20	1336	740
H80T20-S	1544	642
H50T50	1110	681
H50T50-S	1310	550

$$L_{hkl} = \frac{K\lambda}{\beta \cos \theta}, \quad [1]$$

where λ is the wavelength of the Cu-K α radiation, β is full width at middle height (the Bragg peak maximum intensity (deg)), θ is Bragg's angle (deg), and K is the Scherrer constant (equal to 0.9 when the width is measured at middle height of the diffraction peak). The mean crystallite size for pure HAP sample was calculated from the (2 1 1) reflection peak.

The structural analysis was carried out using the Fourier transform infrared (FTIR) spectrophotometer

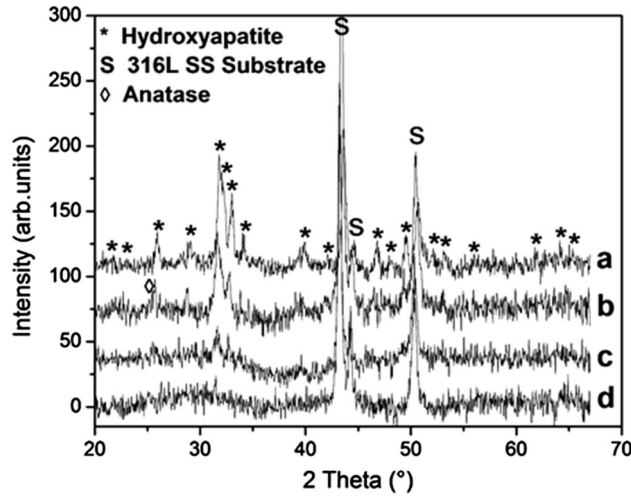


Fig. 3—XRD patterns of the (a) HAP, (b) H80T20, (c) H50T50, and (d) H50T50-S coatings. (*) Hydroxyapatite, (S) Substrate, and (◊) Anatase.

instrument (IRAffinity-1, SHIMADZU). FTIR spectra were recorded in the range of 400 to 4000 cm^{-1} with a resolution of 4 cm^{-1} . The deposited films were scraped off as powders from the substrate and mixed with KBr powder (80 pct in weight), to form an infrared transparent pellet.

Corrosion behavior of the samples was evaluated by potentiodynamic cyclic voltammetry tests by Voltalab (Serial: 913V708/INT), interfaced with a computer, and loaded with VoltaMaster 4 software in simulated human body fluid (SBF) at $310 \pm 274 \text{ K}$ ($37 \pm 1 \text{ }^\circ\text{C}$). The SBF solution was prepared using Kokubo and Takadama's formulation^[23] by dissolving reagent-grade NaCl, NaHCO_3 , KCl, $\text{K}_2\text{HPO}_4 \cdot 3\text{H}_2\text{O}$, $\text{MgCl}_2 \cdot 6\text{H}_2\text{O}$, CaCl_2 , and Na_2SO_4 into distilled water (1 L) and buffered at pH 7.40 with $(\text{CH}_2\text{OH})_3\text{CNH}_2$ and 1M HCl solution (Table I). Before conducting the corrosion studies, the specimens were immersed in SBF solution for 1 hour in order to stabilize the system.^[14] Moreover, a renewed solution was used for each experiment. The exposed area of the samples in the SBF solution was 1 cm^2 . A platinum electrode was used as the auxiliary electrode, and the saturated calomel electrode (SCE) was used as the reference electrode. Corrosion potential (E_{Corr}) and corrosion current density (i_{Corr}) were determined using the Tafel diagram with sweeping potential from -1000 to $+1000 \text{ mV}$ at the rate of 1 mVs^{-1} , and at least three similar results were required to ensure reproducibility.

The adhesion of the coating was estimated using a scratch tester (Millennium in accord with Standard ISO/EN 1071-3) with a spherical Rockwell C diamond indenter of 200 μm in radius. The scratch tests were performed on the coating by applying the load, which increased monotonously at the loading rate of 10000 mN/min while the specimen was shift at the constant speed of 1500 $\mu\text{m/min}$. The applied force immediately started to increase linearly with time. These conditions lead to a total scratch length of 1500 μm . The load at which coating was removed from the substrate is referred as the critical load (L_c). The scratch track was

Table III. Crystalline and Lattice Parameters of HAP and TiO_2/HAP Coatings

	HAP	H80T20	H50T50
a (\AA)	9.410	9.394	9.392
c (\AA)	6.887	6.884	6.870
L_{211} (nm)	135	61.7	30.8

observed using optical microscope. Five tests for each sample were recorded.

Nanoindentation experiments were performed with a Nano Indenter XPTM (MTS Nano Instruments) employing a Berkovich diamond indenter calibrated using a reference sample of known modulus (fused quartz, $E = 72 \text{ GPa}$). The samples were fixed on a metallic support using the heat softening glue crystalbond 509. A regular array of 5×5 indentation tests has been performed at the surface of the different coated materials in order to obtain representative variations of the hardness and the elastic modulus as a function of the indenter displacement. The maximum indentation depth reached by the indenter was fixed at 2000 nm and the strain rate was set constant and equal to 0.05 s^{-1} . The instrument was operated in the continuous stiffness measurement (CSM) mode allowing the computation of the elastic modulus and the hardness continuously during the indentation loading. The harmonic displacement was 2000 nm and the frequency was 45 Hz. The elastic modulus of the coating, E_c , is deduced from the reduced modulus, E_{RC} , given by the instrument, which takes into account the elastic properties, E_i and ν_i , related to the indenter material and the Poisson's ratio of the coating, ν_c :

$$E_c = (1 - \nu_c^2) \left[\frac{1}{E_{\text{RC}}} + \frac{(1 - \nu_i^2)}{E_i} \right]^{-1}. \quad [2]$$

For a diamond indenter, the elastic modulus, E_i , and the Poisson's coefficient, ν_i , are equal to 1140 GPa and 0.07, respectively.^[24] ν_c is taken equal to the mean value of 0.3 because the analysis deals with a multilayered coating.

III. RESULTS AND DISCUSSION

A. Hydrophilic Properties of SiO_2 Surface

The effect of the SiO_2 film on the hydrophilic properties of the 316L SS samples was evaluated by measuring their water contact angles (Figures 1(a) and (b)). Contact angle variations are compared to those measured on the as-prepared 316L SS substrate, *i.e.*, polished and degreased, then dried at 423 K (150 $^\circ\text{C}$), and those measured on the SiO_2 single-layer-coated 316L SS. All the specimens were aged for 60 days in the ambient environment. As shown in Figure 1(a), the contact angle does not vary with time indicating that the shape and/or the size of the water drop applied on the supports did not vary with time during the measurement. The representative images of the water droplets deposited on the substrate and SiO_2 film surfaces are

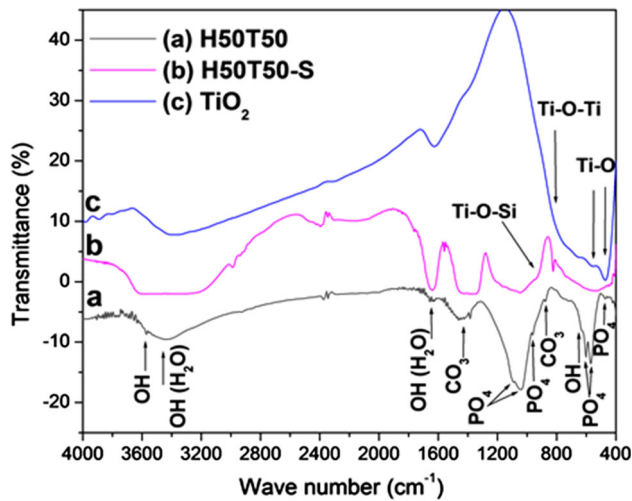


Fig. 4—FTIR spectra of the (a) H50T50, (b) H50T50-S coatings, and (c) TiO_2 film.

presented in Figure 1b. The contact angle measurements indicate that the substrate is partially wetted by water and that wettability of the steel is the lowest, the 316L steel substrate has contact angle of 79.8 ± 0.1 deg, water wets silica rather well than the substrate, and it represents a contact angle of 34.2 ± 0.02 deg. These results are in agreement with the previous works of Houmard *et al.*^[25] and Permpoon *et al.*^[26] showing that silica films prepared by sol-gel method and heat-treated at 773 K (500 °C) continuously exhibited a very slow contact angle increase over a period of 60 days aging, which confirms the natural hydrophilicity of a silica surface due to the hydroxyl content on the film surface.

FTIR analyses performed on the same films after 60 days aging are represented in Figure 1(c). There is a broad band in the range of 3200 to 3800 cm^{-1} corresponding to stretching vibration of different hydroxyl groups associated to absorbed free water and to Si-OH (silanols) groups linked to molecular water through hydrogen bonds as well as isolated free surface silanols. The bands around 1556 and 1656 cm^{-1} correspond to bending vibrations of OH bonds of water molecules. The band around 565 cm^{-1} is attributed to Si-O bonds in an amorphous phase. The bands at 460, 800 cm^{-1} , and in the range of 1000-1220 cm^{-1} are attributed to the bond bending and bond stretching vibrations of the Si-O-Si units in silica. The band at 935 cm^{-1} is assigned to the stretching vibration of a small amount of Si-OH groups.^[27–29]

Figure 1(d) related to the XPS spectrum shows the elemental composition of deposited SiO_2 film. The binding energy peaks are corresponding to Si2s, Si2p, and O1s of SiO_2 film. It is inferred that the C1s peak at 284.7 eV essentially reflects the amount of carbon contamination at the outer surface. Previous studies^[26,30] have shown that alkoxy groups, which might contribute to the C1s peak, are not present in SiO_2 film heated at 500 °C, and alkoxy groups arising from the silica precursors are completely decomposed after annealing at 773 K (500 °C). In addition, XPS analysis

was used to investigate the surface hydrophilic properties of SiO_2 film. The presence of OH groups on the SiO_2 outer surface is studied from the deconvolution of the O1s peak. The O1s peak could be decomposed in two components, *i.e.*, Si-OH and Si-O components, using Lorentzian/Gaussian functions (Figures 1(e) and (f)). The O-H component essentially traduces the presence of surface hydroxyl groups; the O1s region includes two peaks (Figure 1(e)). One component of the O1s peak is attributed to the Si-O (533 eV) and the other one is assigned to the hydroxyl group Si-OH (535 eV). Binding energies of these components were subsequently compared to those of component measured for pure SiO_2 film.^[26] The hydroxyl content (pct) is the ratio of the area of 535 eV component to the total area of the two O1s components. The hydroxyl content for SiO_2 film was calculated as 4 pct. This observation is in accordance with FTIR results, which depicted an amount of surface OH groups for the SiO_2 layer. The deconvolution of the Si2p spectrum into a single Si^{4+} component located at 103.5 eV is presented in Figure 1(f), and the location of this component is very similar to that measured for pure SiO_2 film.^[31]

B. Morphological and Structural Characterization of Sol-Gel-Derived Hydroxyapatite Coatings

Figure 2 shows the surface of the HAP/ TiO_2 deposited on the SiO_2 -coated and uncoated 316L SS substrates. The images show highly intermixed composite phases. From Figure 2(c) and (d), it can be seen that H80T20-S and H50T50-S have the continuous and regular microstructure. Moreover, the deposits cover entire surface of the substrate compared to H80T20 (Figure 2(a)) and H50T50 (Figure 2(b)). Figure 2(e) illustrates the SEM micrograph of the H50T50 top layer/ SiO_2 inner layer/substrate interfaces. Some microcracks are generated in the coating, which can represent the interface separating the H50T50 and SiO_2 layers; otherwise the deposit is mostly uniform throughout the rest areas, and no delamination was observed. The EDX spectrum obtained on the H50T50-S coating indicates the peaks corresponding to the elements that are originating from the substrate, HAP, TiO_2 , and SiO_2 phases; in addition, carbon element was detected.

The thickness and roughness of the sol-gel-derived coatings are collected in Table II. All the coatings presented a thickness less than 2 μm . Pure HAP coating exhibited a higher surface roughness (≈ 1310 nm). The addition of both TiO_2 and SiO_2 decreased the roughness of the coatings up to 550 nm. According to Sidane *et al.*,^[32] the SEM surface examination of the HAP coating exhibited a porous surface composed of spherical agglomerates. After the addition of TiO_2 into HAP phase, it can be seen that H80T20 (Figure 2(a)) and H50T50 (Figure 2(b)) composite coatings have regular surface. The porosity and the agglomerated particles are reduced and almost disappeared after the insertion of SiO_2 inner layer between the composite top layer and the substrate, so the resulted H80T20-S and H50T50-S bilayer coatings have the uniform surface as it is shown in Figures 2(c) and (d).

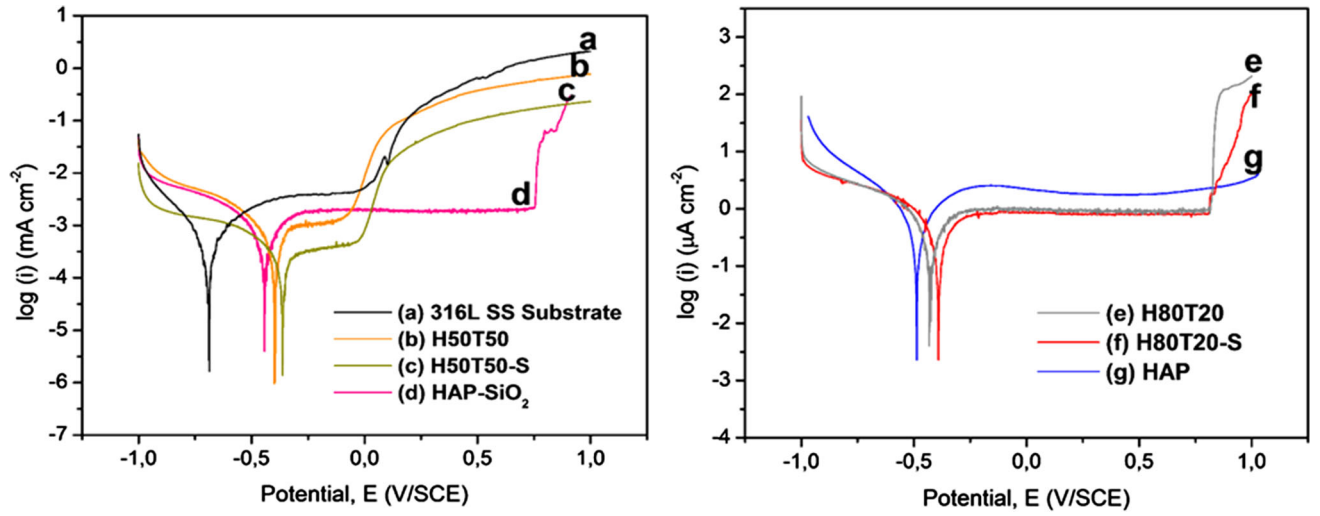


Fig. 5—Potentiodynamic curves of (a) the uncoated 316L stainless steel substrate (b) H50T50, (c) H50T50-S, (d) HAP-SiO₂, (e) H80T20, (f) H80T20-S, and (g) HAP coatings in SBF solution at 310 K (37 °C).

Table IV. Corrosion and Scratch Test Parameters of the Uncoated and Coated 316L SS

Sample	Corrosion Test		Scratch Test	
	E_{Corr} (mV)	i_{Corr} ($\mu A\ cm^{-2}$)	Scratch length (μm)	Critical load, L_c (mN)
316L SS	- 690	1.120	—	—
HAP	- 484	0.849	—	—
HAP-SiO ₂	- 445	0.812	—	—
H80T20	- 423	0.801	820	4820
H80T20-S	- 383	0.724	880	4980
H50T50	- 395	0.758	900	5050
H50T50-S	- 362	0.251	980	5680

The composition and microstructure of the coatings were characterized by XRD analysis (Figure 3). According to the International Center for Diffraction Data (ICDD) patterns, the pattern of the HAP coating (Figure 3(a)) shows peak positions, which correspond to a crystallized HAP structure (PDF no. 09-0432). The HAP characteristic triplet peaks at (211), (112), and (300) planes are observed for 2θ values between 31 and 33 deg, and the peak at the plane (002) is observed for $2\theta = 25.88$ deg. In addition to the existing HAP peaks, diffraction peaks corresponding to steel substrate (PDF no. 00-006-0694) are developed. Addition of 20 vol pct TiO₂ (Figure 3(b)) and 50 vol pct TiO₂ (Figure 3(c)) shows almost similar diffraction pattern such as pure HAP, but the peaks become wider with a change in the position and a decrease in the intensity. The mean peak corresponding to the crystalline structure of anatase ($2\theta = 25.35$ deg) (PDF no. 00-004-0477) is confused with that of HAP ($2\theta = 25.88$ deg). When TiO₂ concentration increases further, a peak shift and the decrease in the XRD peak intensity are observed. This confirms the previous results of Nathanael *et al.*^[15,16] who attributed the initial small decrease in the intensities of the HAP peaks to the small inclusion of TiO₂ in HAP. There are different proposals in the literature for possible Ti substitution mechanisms in HAP structure.

According to Ergun *et al.*^[33] and Riberio *et al.*,^[34] the ionic radius of Ti⁴⁺ (0.68 Å) is much smaller than the ionic radius of Ca²⁺ (0.99 Å), and then the substitution of Ca by low concentrations of Ti can be occurred and results in a decrease in the cell lattice parameters and crystal domain size. Therefore, lattice disorder increased with the increasing of Ti content. Thus, this lattice disorder greatly inhibits the crystallization and makes it difficult to obtain high crystallinity in HAP-modified structure.^[35] Crystallite size and lattice parameters, calculated from diffraction line broadening, are regrouped in Table III. They decrease as the content of TiO₂ increases from 20 to 50 vol pct, respectively. After the deposition of SiO₂ inner layer on the 316L SS substrate, the pattern of H50T50-S (Figure 3(d)) reveals an important shift and reduction in the intensity of HAP peaks. This behavior could be related to a combination between the SiO₂, TiO₂, and HAP phases through chemical bonding. There is no crystalline phase of SiO₂ detected by the X-rays diffraction because the microstructure of the SiO₂ is amorphous.^[32]

Figure 4 shows the FTIR spectra of the H50T50, H50T50-S, and pure TiO₂ coatings. FTIR spectrum of H50T50 (Figure 4(a)) exhibits the well-defined bands associated with the presence of PO₄ groups at 473, 563, 600, 964, 1049, and 1089 cm⁻¹. The broad and

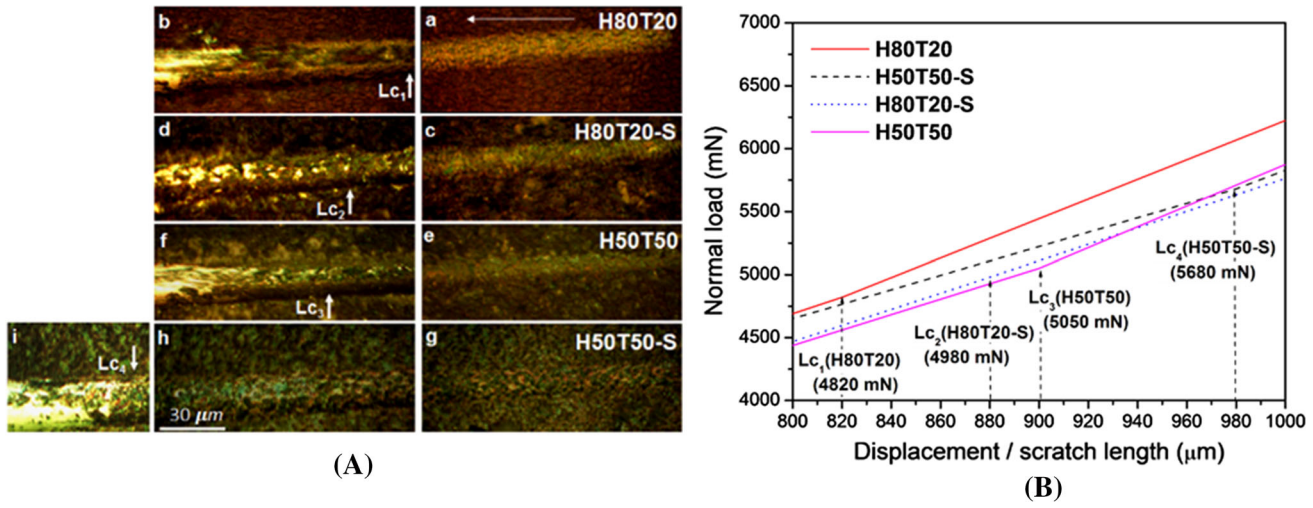


Fig. 6—(A) Optical images representative of the scratch length realized on the surface of (a, b) H80T20, (c, d) H80T20-S, (e, f) H50T50, and (g through i) H50T50-S coatings; load is progressively increasing from right to left; (a), (c), (e), and (g) are related to the initial scratch. (B) Load-displacement graph corresponding to the scratch track presented in the (b, d, f, and h) optical images.

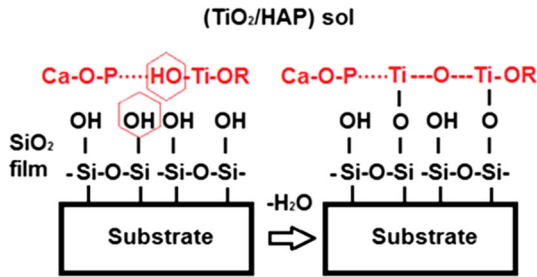


Fig. 7—Schematic diagrams revealing possible bonding mechanism of TiO₂/HAP phases on the surface of SiO₂ film during the immersion in mixed TiO₂/HAP sol, through hydroxyl group association.

Table V. The Elastic Modulus and the Fitting Parameters of the TiO₂/HAP Coatings

	Perriot and Barthel				Avrami			
	E_F (GPa)	E_S (GPa)	x_0	n	E_F (GPa)	E_S (GPa)	k_s	n_s
H80T20	19	176	3.5	2.24	21	177	21	2
H50T50	32	183	5	2.9	33	188	10.4	2.6

1400 to 1540 cm^{-1} . The origin of the carbonate bands is due to the absorption of atmospheric CO₂ into the ethanol solution.^[14,36] In addition, the FTIR spectrum shows the vibrational bands related to the stretching vibration of Ti-O at 467 and 565 cm^{-1} and the asymmetric broad of Ti-O-Ti at about 810 cm^{-1} in the anatase phase of TiO₂ lattice, as shown in Figure 4(c).^[27] An intensity decrease of the OH bands at 3572 and 630 cm^{-1} arising from the stretching and vibrational modes, respectively, of the OH⁻ ions in the hydroxyapatite structure is noticed. These observations are in agreement with the results of XRD patterns. The librational mode of the OH group (632 cm^{-1}) is especially sensitive to substitutions in the apatite structure. The strength of this peak is well known to correlate with the degree of crystallinity of HAP. In the presence of Ti, the area of the OH librational band decreases, suggesting a decrease in HAP crystallinity, and consequently a decrease in crystallite size. The decrease in intensity of the OH peak at 3572 cm^{-1} is also indicative of changes in the HAP structure.^[34] After insertion of SiO₂ inner layer, the FTIR spectrum of H50T50-S (Figure 4(b)) exhibits the bands corresponding with the presence of hydroxyapatite but their resolution decreases. The spectrum exhibits the broadening of absorption bands corresponding to phosphates, hydroxyls, and carbonates with the presence of well-developed bands related to Ti-O and Ti-O-Ti bonds. Indeed, the development of a weaker absorption peak of Ti-O-Si

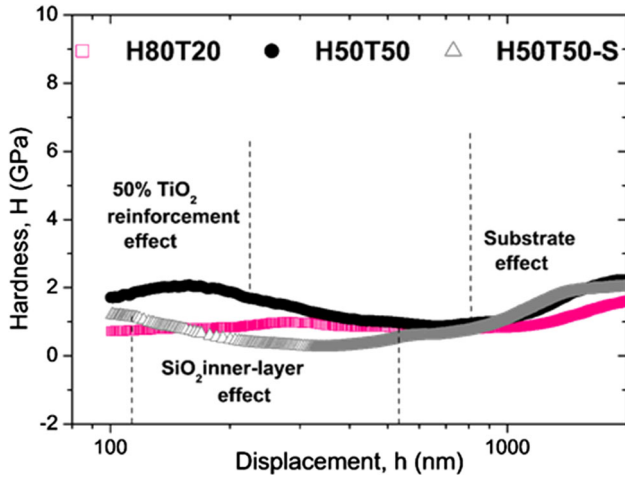
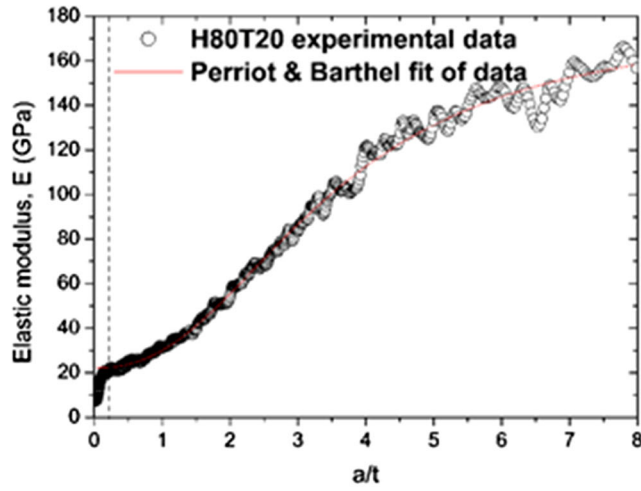
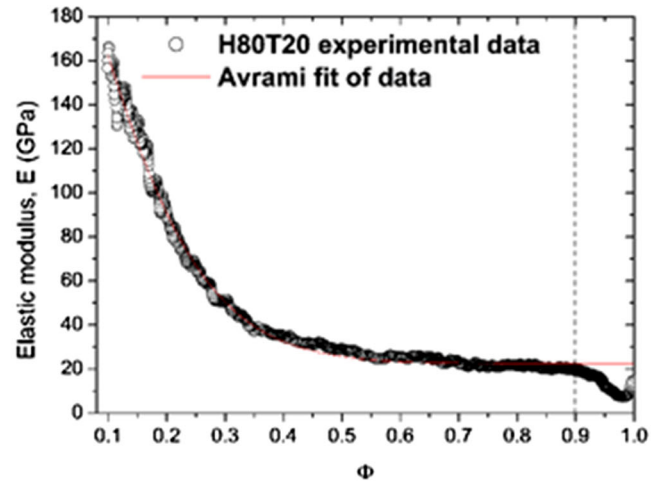


Fig. 8—Hardness vs the indenter displacement performed on H80T20, H50T50, and H50T50-S coatings.

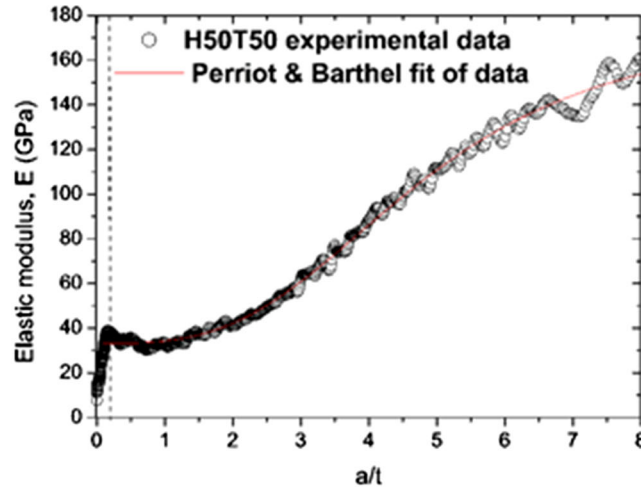
high-intensity band extending from 2500 to 3600 cm^{-1} and the band at 1632 cm^{-1} correspond to the hydrogen-bonded H₂O molecules. The bands of CO₃²⁻ groups are indicated as a singlet at 873 cm^{-1} and in the range of



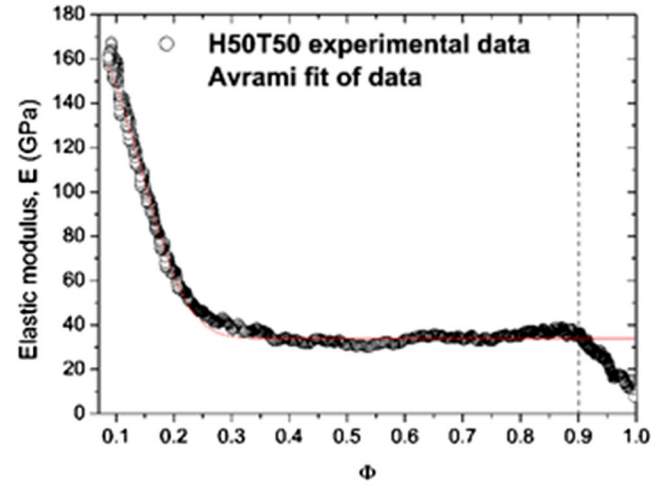
(a)



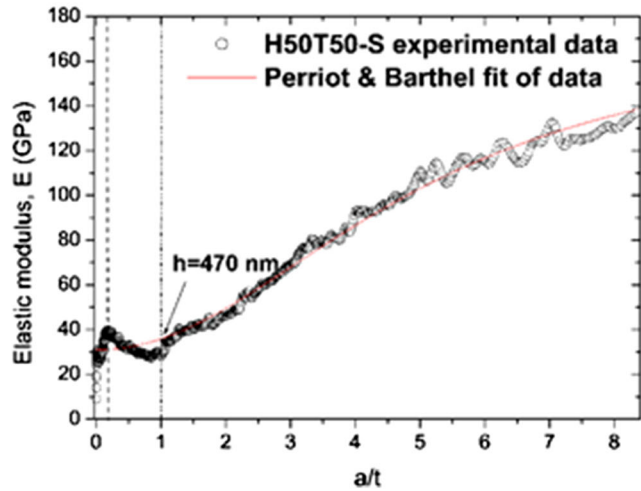
(b)



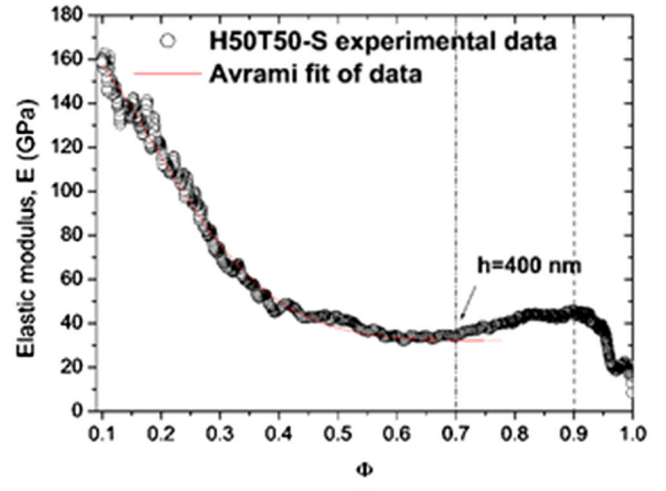
(c)



(d)



(e)



(f)

Fig. 9—Models applied on the indentation data obtained from nanoindentation test performed on (a, b) H80T20, (c, d) H50T50, and (e, f) H50T50-S coatings.

mixed bond at 925 cm^{-1} was observed,^[27] which demonstrates the Ti-O-Si bond formation due to the bonding of Si-OH groups present on the surface of the SiO₂ film underlying layer as shown in the previous section.

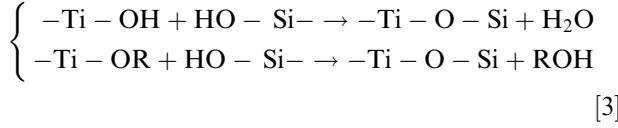
C. Corrosion Resistance

Figure 5 shows the potentiodynamic polarization plots of the coated and uncoated 316L SS substrate specimens immersed in SBF solution at $310 \pm 274\text{ K}$ ($37 \pm 1\text{ }^{\circ}\text{C}$). Results of electrochemical tests revealed the influence of the different deposits on the corrosion resistance of the 316L steel. The corrosion parameters determined from these curves by means of Tafel extrapolation method are summarized in Table IV. The corrosion parameters are corrosion potential (E_{Corr}) and corrosion current density (i_{Corr}). For H50T50-S (Figure 5(c)) and H80T20-S (Figure 5(f)), the potentiodynamic curves were shifted to the right when compared to H50T50 (Figure 5(b)) and H80T20 (Figure 5(e)) curves, respectively. Representative potentiodynamic curve obtained for HAP-SiO₂ (Figure 5(d)) was shifted to the positive potential side compared to pure HAP (Figure 5(g)) and 316L SS sample (Figure 5(a)), respectively. The corrosion resistance of the specimens increases when decreasing i_{Corr} . For the substrate, i_{Corr} was about $1.12\text{ }\mu\text{A cm}^{-2}$, and then decreased to $0.849\text{ }\mu\text{A cm}^{-2}$ for HAP and to $0.812\text{ }\mu\text{A cm}^{-2}$ for HAP-SiO₂ bilayer coating. The i_{Corr} of H80T20-S specimens which is about $0.724\text{ }\mu\text{A cm}^{-2}$ indicates that they are more corrosion resistant than H50T50 ($\approx 0.758\text{ }\mu\text{A cm}^{-2}$) and H80T20 ($\approx 0.801\text{ }\mu\text{A cm}^{-2}$), which are in turn more resistant than HAP-SiO₂. When compared to other specimens, H50T50-S exhibits a lower corrosion current ($\approx 0.251\text{ }\mu\text{A cm}^{-2}$). The noble behavior of the coated 316L SS samples can be attributed to the denser nature of the coating surface, due to the formation of apatite precipitates resulting from the reaction between the calcium and phosphate ions in the SBF solution. Indeed, the presence of the SiO₂ inner layer prevents the electrolyte to infiltrate into the deeper portion of the coating through the pores and cracks existing in the coating causing pitting corrosion. A passive current plateau is noticed on the potentiodynamic polarization curves recorded on HAP-SiO₂ (Figure 5(d)), H80T20 (Figure 5(e)), and H80T20-S (Figure 5(f)). The passivation behavior indicates that protective surface films have been formed on the surface of the specimens exposed to the SBF solution. Potentiodynamic curves recorded on H50T50 (Figure 5(b)) and H50T50-S (Figure 5(c)) are quite similar. The anodic current density increased with increasing potential suggesting the formation of a thin oxide film on the surface of the coatings. The further increase of the anodic current density suggests a degradation of that passive film.^[37,38] Thus, the reinforcement of the HAP coating with TiO₂ and SiO₂ improved the corrosion resistance of the 316L steel substrate. It is noted that the increase of TiO₂ concentration in the hydroxyapatite phase considerably increased the uniformity of the coatings and thereby decreased the surface roughness.^[15] After the insertion

of SiO₂ inner layer on 316L SS substrate, H50T50-S bilayer coating showed a smooth surface, (see Table II; Figure 2) and exhibited a higher corrosion resistance. The significantly reduced corrosion current density in the H50T50-S ($\approx 0.251\text{ }\mu\text{A cm}^{-2}$) clearly demonstrates the improvement obtained in the corrosion resistance. The surface roughness and surface morphology can considerably change corrosion and corrosion rate. A higher corrosion resistance is obtained for surfaces with lower roughnesses.^[39]

D. Bonding Strength

Figure 6A shows the optical microscopy images corresponding to the scratch track realized on the surface of coatings during the scratch force test. Load is progressively increasing from right to left. According to Figure 6A, no visible wear debris were come out from the coatings in the initial stage of small-applied load (Figure 6A(a, c, e, g)). As the load was increased, the cracks appeared on the surface and became more severe until the delamination of the coating from the substrate (Figure 6A(b, d, f, i)). The corresponding load is recorded as the critical load L_c . No important damage is inspected on the scratching surface corresponding to H50T50-S coating (Figure 6A(h)), the failure was occurred only once the load is increased as it is shown in Figure 6A(i). The critical loads (L_{c1} , L_{c2} , L_{c3} , and L_{c4}) at which the coating was removed from the substrate are indicated with white arrow in Figure 6A(b, d, f, i), respectively. They are determined from the curves illustrated in Figure 6B which presents load as a function of the scratch length (displacement) and are regrouped in Table IV. From Table IV, it can be observed that the insertion of the SiO₂ inner layer improved the bonding strength of the H80T20 composite coating to the substrate. H80T20 presents approximately a critical load (L_{c1}) of 4820 mN, while H80T20-S presents approximately a critical load (L_{c2}) of 4980 mN. Addition of 50 vol pct TiO₂ to HAP also improves the bonding strength compared to H80T20. In literature,^[37] it is indicated that an increase in the TiO₂ particles content in HAP matrix leads to the formation of dense coatings with low porosity, thus resulting in coatings with higher hardness and adhesive strength. The H50T50 coating presents approximately a critical load (L_{c3}) of 5050 mN. With the addition of the SiO₂ inner layer on the substrate, the H50T50-S bilayer coating presents a higher bonding strength ($L_{c4} \approx 5680\text{ mN}$). The SiO₂-hydroxylated surface can therefore promote the attachment of the TiO₂/HAP layer on the substrate. As illustrated in Figure 7, such an effect could be due to the formation of Si-O-Ti bridge linking at the interface. The mechanism involved in this interaction is the possibility of the formation of hydrogen bond between the silanol groups, Si-OH, present on the surface of the SiO₂ film and the Ti-OH or Ti-OR groups ($R = \text{OC}_3\text{H}_7$) bonded to the ends of the alkoxide molecules $\text{Ti}(\text{OH})_y(\text{OC}_3\text{H}_7)_{4-y}$, after the hydrolysis of titanium isopropoxide in 2-methoxy ethanol and water,^[40] according to the reaction:



This mechanism is similar to condensation reactions taking place during the sol-gel polymerization process as illustrated in Figure 7. A similar mechanism has been proposed in the research work of Houmard.^[41]

It is reported that the coating thickness should be controlled in such a way as to produce a compromise between the bonding strength and the corrosion properties.^[42,43] Therefore, the H50T50-S thickness (1310 nm) obtained in this study was observed to be the optimized coating for improving both the corrosion resistance and the bonding strength.

E. Mechanical Properties

For hardness measurements of hard coatings on soft substrate, some authors^[44,45] indicate a value close to 10 pct of the coating thickness for the indenter penetration after which the substrate interferes with the measurement. This value can reach 50 pct in the case of soft coating on hard substrate.^[46] Unfortunately, this limit which can vary in a great extent is not a predictable value because it depends both on coating thickness and on the mechanical behavior of the coating, *i.e.*, for a hard coating on a soft substrate or for a soft coating on a hard substrate. To avoid the application of models for which the above-mentioned limit values cannot be defined precisely, a direct determination of the mechanical properties of the material will be preferable. This is rendered possible by means of the continuous stiffness measurement mode, which allows the computation of both the hardness and the elastic modulus as a function of the indenter penetration.^[47] Figure 8 represents the hardness variation as a function of the indenter penetration. As shown in this figure, H50T50 coating presents the highest hardness value close to the external surface. For the indenter penetrations over than 100 nm, the hardness of H50T50 increases notably to reach 2 GPa, while the hardness of H80T20 coating varies slightly. After 200 nm, the hardness of H50T50 coating decreases and tends to that of H80T20. We note that the hardness value of H80T20 and H50T50 coatings can be considered as a constant value for indenter depths between 500 and 800 nm. In this region, the hardness is close to 1.1 and 1 GPa for the H50T50 and H80T20 coatings, respectively. For penetration depths over 800 nm, the hardness continues to increase to achieve a value which should correspond to that of the substrate (≈ 2 GPa). For the H50T50-S coating, the hardness is rather close to that of H50T50 for indenter penetration close to the outer surface (100 nm), and then, it is clear to note that the hardness is influenced by the presence of the SiO₂ inner layer. Above 550 nm, the hardness value tends to that of H80T20 and H50T50 coatings before reaching the substrate hardness over 800 nm in depth. The SiO₂ inner layer does not improve the hardness measurement.

To determine the elastic modulus of H80T20, H50T50, and H50T50-S coatings, a model must be applied for separating the influence of the substrate on the elastic modulus measurement. Indeed, the limit value for the indenter displacement after which the substrate interferes with the measurement is close to 1 pct of the film thickness for a hard film deposited onto a soft substrate^[48,49] and it can reach 20 pct for a soft film deposited onto a hard substrate.^[46,50] Several models have been proposed to extract intrinsic material properties of the film from the composite modulus, which represent the combination of the respective moduli of the film, E_{film} , and of the substrate, $E_{\text{substrate}}$. Most of them are empirical models based on the following relationship:

$$E_{\text{composite}} = E_{\text{substrate}} + (E_{\text{film}} - E_{\text{substrate}})\Phi(x). \quad [4]$$

The relative weight $\Phi(x)$ of each material, as was pointed out by Doerner and Nix,^[50] varies with the penetration depth. Different weight functions are available in literature, and the most commonly used have been proposed by Doerner and Nix,^[51] Mencik *et al.*,^[52] Antunes *et al.*,^[53] and Gao *et al.*^[54] First, we tested the model of Perriot and Barthel^[55] who extended the Gao's function to a larger range of moduli ratios and propose the empirical model in Eq. [5]. This function represents the measured reduced modulus, E_{RC} , as a function of E_{RF} (obtained for the lowest loads and representing the reduced modulus of the film) and E_{RS} (obtained for the highest loads and representing the reduced modulus of the substrate):

$$E_{\text{RC}}\left(\frac{a}{t}\right) = E_{\text{RF}} + \frac{(E_{\text{RS}} - E_{\text{RF}})}{1 + \left(\frac{tx_0}{a}\right)^n}, \quad [5]$$

where x_0 and n are adjustable constants. $a (= h \cdot \tan \Psi)$ is the contact radius of a assimilated conical indenter at the maximum load, Ψ equals to 70.3 deg corresponding to the half-angle of the tip conical indenter, and h is the indenter displacement and t the film thickness. The parameter x_0 is the value of the a/t ratio for which $E_C = (E_{\text{RS}} + E_{\text{RF}})/2$. At the same time, it corresponds to the change in curvature of the (E_C ; a/t) curve plotted in semi-log coordinates.

Additionally, we tested the model suggested by Roudet *et al.*^[56] using the mathematical expression similar to that proposed by Avrami^[57,58]:

$$E_C = E_F + (E_S - E_F)\exp[-k_s \cdot \Phi^{n_s}], \quad [6]$$

where E_C is the composite elastic modulus and E_F , E_S are, respectively, the elastic modulus of the film and of the substrate. K_s , n_s are fitting coefficients, which indicate the magnitude of the curve, and the weight function (Φ) is given by equation Eq. [7]:

$$\begin{aligned} \Phi = & \frac{2}{\pi} \arctan\left(\frac{t}{a}\right) + \frac{1}{2\pi(1 - \nu_c)} \\ & \times \left[(1 - 2\nu_c) \frac{t}{a} \ln\left(1 + \left(\frac{a}{t}\right)^2\right) - \frac{\frac{a}{t}}{1 + \left(\frac{a}{t}\right)^2} \right]. \end{aligned} \quad [7]$$

Finally, Figure 9 presents the two models applied on the complete range of indentation data. The elastic modulus is represented as a function of the weight function (Φ) and of the ratio (a/t). The H80T20 (Figure 9(a) and (b)) and H50T50 (Figure 9(c) and (d)) curves seem to be satisfactorily represented in all the range of the indentation data. In the range of $a/t = 0-0.2$ and $\Phi = 0.9-1$ for the indentation penetration lower than 100 nm, there is some variation in the indentation data related to the insufficient precision of the influence of the indenter tip defect involved in the computation of the contact area. Even the representations are not linear, and the tendencies at the two limits ($a/t = 0.2$) and ($\Phi = 0.9$) converge toward the elastic moduli of the film. The results of both the elastic modulus of the film and of the substrate as well as the fitting parameters are listed in Table V. The values given by the two models are very similar. For the H50T50-S coating (Figure 9(e) and (f)) when Φ is lower than 0.7 and the ratio a/t is higher than 1 (for indenter displacements higher than 400 nm), the elastic modulus variation is adequately represented and tends toward that of H50T50 coating (33 GPa). When Φ is higher than 0.7 and the ratio a/t is lower than 1 (for indenter displacements less than 470 nm), the elastic modulus variation is not adequately represented by the fitting curves. This tendency can be due to the presence of the SiO₂ inner layer.

The hardness and the elastic modulus of the prepared coatings are found to increase as the content of the TiO₂ increases to 50 vol pct. H50T50 possesses the hardness value of 2 GPa at the surface, 1.1 GPa in the core of the coating, and the elastic modulus value of 33 GPa. The hardness variation between the surface and the core of the coating was explained by the initial deposition of some TiO₂ on the underlying substrate, while the remaining TiO₂ formed a composite with HAP and produced the structure.^[16] Further deeper analysis about the mechanical properties of the SiO₂ film will be investigated in the future studies in order to explain the influence of the mechanical behavior of the intermediate SiO₂ layer.

It is noted that the hardness values measured in this study, which are comparable with those reported previously for pure HAP ceramics (1.0-5.5 GPa),^[59] are able to withstand large abrasion forces during implant insertion. The elastic modulus has attracted much research interest because of its critical importance for characterizing various bone pathologies and guiding artificial implant design. The equivalent elastic modulus must be adjusted to not greatly exceed those of bones in order to avoid stress shielding at the bone-implant interface, a major source for bone resorption and eventual failure of the implants. The elastic moduli values measured here are comparable with those of cortical bone (compact bone) ranging from 3 to 30 GPa.^[60,61] H80T20 and H50T50 coatings are promising materials for the hard tissue application. Owing to its higher corrosion resistance and bonding strength, H50T50-S-coated-316L SS has a potential application in orthopedic as a prosthetic implant. Further studies are required to test the bioactivity and biocompatibility

of these promising biomedical materials *in vitro* and *in vivo*. Recently, published work^[62] has shown that the TiO₂/HAP (20 vol pct TiO₂) composite coatings exhibited well biocompatible properties, stem cells attached well onto the surface, proliferated, and presented a polygonal morphology different from the fibroblastic-like morphology found on 316L SS. Moreover, TiO₂/HAP composite improved the corrosion resistance of the 316L SS implant and showed mechanical properties close to that of hard tissue once incubated in physiological conditions for 7 days, highlighting its potential application in hard tissue replacement.

IV. CONCLUSION

The 50 vol pct TiO₂-reinforced HAP layer has been successfully attached on the surface of silica-coated 316L SS by sol-gel method. The surface properties of silica inner layer enhanced the attachment of the TiO₂ and HAP phases through the Si-OH hydroxyl groups and the chemical affinity of TiO₂ toward the HAP, thus suggesting an improvement in the corrosion resistance, bonding strength, elastic modulus, and hardness of the coated 316L SS required for the hard tissue application.

ACKNOWLEDGMENTS

This study was funded by the University of Bejaia from Algeria. The authors are very grateful to MSMP, Arts et Métiers ParisTech of Lille, France, for the help in providing the mechanical analysis.

REFERENCES

1. E.C. Shores, R.E. Holmes: *An Introduction to Bioceramics*, in: L.L. Hench, J. Wilson (Eds.), World Scientific: Singapore, 1993, pp. 181-98.
2. Marc Long, H.J. Rack: *Biomaterials*, 1998, vol. 19, pp. 1621-39.
3. M. Navarro, A. Michiardi, and O. Castaño: *J.A. Planell J. R. Soc. Interface*, 2008, vol. 5, pp. 1137-58.
4. H. Hermawan, D. Ramdan, J.R.P. Djuansjah: *Metals for Biomedical Applications, Biomedical Engineering - From Theory to Applications*, Prof. Reza Fazel (Ed.), InTech, Available from: <http://www.intechopen.com/books/biomedical-engineering-from-theory-toapplications/>, 2011.
5. V.P. Mantripragada, B. Lecka-Czernik, N.A. Ebraheim, and A.C. Jayasuriya: *J Biomed Mater Res A*, 2013, vol. 101, pp. 3349-64.
6. M. Navarro, A. Michiardi, O. Castano, and J. Planell: *J. R. Soc. Interface*, 2008, vol. 5, pp. 1137-58.
7. J.A. Disegi and L. Eschbach: *Injury*, 2000, vol. 31, pp. 2-6.
8. J. Blum, K.L. Eckert, A. Schroeder, M. Petitmermet, S.W. Ha, E. Wintermantel: *Proceedings of the 9th International Symposium on Ceramics in Medicine*, in: T. Kokubo, T. Nakamura, F. Miyaji (Eds.), Col. 9, Otsu, Japan, 1996, pp. 89.
9. S. Nagarajan and N. Rajendran: *Appl. Surf. Sci.*, 2009, vol. 255, pp. 3927-32.
10. H.W. Kim, Y.H. Koh, L.H. Li, S. Lee, and H.E. Kim: *Biomaterials*, 2004, vol. 25, pp. 2533-38.
11. C.E. Wen, W. Xu, W.Y. Hu, and P.D. Hodgson: *Acta Biomater.*, 2007, vol. 3, pp. 403-10.
12. T.P. Singh: Harpreet Singh Hazaar Singh: *J. Therm. Spray Technol.*, 2012, vol. 21, pp. 917-27.
13. P.C. Rath, L. Besra, B.P. Singh, and S. Bhattacharjee: *Ceram. Inter.*, 2012, vol. 38, pp. 3209-16.

14. D. Sidane, D. Chicot, S. Yala, F. Bir, H. Khireddine, S. Ziani, A. Iost, and X. Decoopman: *Thin Solid Films*, 2015, vol. 593, pp. 71–80.
15. A.J. Nathanael, N. Sabari Arul, N. Ponpandian, D. Mangalaraj, and P.C. Chen: *Thin Solid Films*, 2010, vol. 518, pp. 7333–38.
16. A.J. Nathanael, D. Mangalaraj, and N. Ponpandian: *Compos. Sci. Technol.*, 2010, vol. 70, pp. 1645–51.
17. H. Li, K.A. Khor, and P. Cheang: *Biomaterials*, 2003, vol. 24, pp. 949–57.
18. P. Li, C. Ohtsuki, T. Kokubo, K. Nakanishi, N. Soga, T. Nakamura, and T. Yamamuro: *J. Am. Ceram. Soc.*, 1992, vol. 75, pp. 2094–97.
19. P. Li, C. Ohtsuki, T. Kokubo, K. Nakanishi, N. Soga, and K. de Groot: *J Biomed Mater Res*, 1994, vol. 28, pp. 7–15.
20. P. Galliano, J.J. Damborenea, M.J. Pascual, and A. Duran: *J. Sol-Gel Sci. Technol.*, 1998, vol. 13, pp. 723–27.
21. S. Kim and P.N. Kumta: *Mater. Sci. Eng. B*, 2004, vol. 111, pp. 232–36.
22. A. Balamurugan, S. Kannan, and S. Rajeswari: *Mater. Lett.*, 2005, vol. 59, pp. 3138–43.
23. T. Kokubo and H. Takadama: *Biomaterials*, 2006, vol. 27, pp. 2907–15.
24. J.E. Field and R.H. Telling: *The young modulus and poisson ratio of diamond*, Research Note, Cavendish Laboratory, Cambridge, 1999.
25. M. Houmard, E.H.M. Nunes, D.C.L. Vasconcelos, G. Berthomé, J.-C. Joud, M. Langlet, and W.L. Vasconcelos: *Appl. Surf. Sci.*, 2014, vol. 289, pp. 218–23.
26. S. Permpoon, G. Berthomé, B. Baroux, J.C. Joud, and M. Langlet: *J. Mater. Sci.*, 2006, vol. 41, pp. 7650–62.
27. L. Zhang, Z. Xing, H. Zhang, Z. Li, X. Wu, X. Zhang, Y. Zhang, and W. Zhou: *Appl Catal B*, 2016, vol. 180, pp. 521–29.
28. P.K. Jal, M. Sudarshan, A. Saha, S. Patel and B.K. Mishra: *Colloids Surf. A: Chem. Phys. Eng. Asp.*, 2004, vol. 240, pp. 173–78.
29. V.A. Ermoshin, K.S. Smirnov, and D. Bougeard: *Surf. Sci.*, 1996, vol. 368, pp. 147–51.
30. N. Primeau, C. Vautey, and M. Langlet: *Thin Solid Films*, 1997, vol. 310, pp. 47–56.
31. M. Houmard, D. Riasset, F. Roussel, A. Bourgeois, G. Berthomé, J.C. Joud, and M. Langlet: *Surf. Sci.*, 2008, vol. 602, pp. 3364–74.
32. D. Sidane, H. Khireddine, S. Yala, S. Ziani, F. Bir, D. Chicot: *Metall. Mater. Trans. B*, 2015, vol. 46 B, pp. 2340–47.
33. C. Ergun: *J Eur Ceram Soc*, 2008, vol. 28, pp. 2137–49.
34. C.C. Ribeiro, I. Gibson, and M.A. Barbosa: *Biomaterials*, 2006, vol. 27, pp. 1749–61.
35. H. Anmin, L. Ming, C. Chengkang, and M. Dali: *J. Mol. Catal. A: Chem.*, 2007, vol. 26, pp. 779–85.
36. S. Yala, H. Khireddine, D. Sidane, S. Ziani, and F. Bir: *J. Mater. Sci.*, 2013, vol. 48, pp. 7215–23.
37. S. Yugeswaran, A. Kobayashi, A. Hikmet Ucisik, and B. Subramanian: *Appl. Surf. Sci.*, 2015, vol. 347, pp. 48–56.
38. Y. Huang, Q. Ding, X. Panga, and S. Hana: *Y. Yan Appl. Surf. Sci.*, 2013, vol. 282, pp. 456–62.
39. A.S. Toloei, A. Stoilov, and D.O. Northwood: *WIT Transactions on Engineering Science*, 2013, vol. 77, pp. 193–204.
40. A. Balamurugan, S. Kannan, and S. Rajeswari: *Mater. Lett.*, 2005, vol. 59, pp. 3138–43.
41. M. Houmard: PhD. Thesis, INP Grenoble, France, 2009.
42. B. Aksakal, M. Gavali, and B. Dikici: *J. Mater. Eng. Perform.*, 2010, vol. 19, pp. 894–99.
43. A. Büyüksagisa, N. Çiftçi, Y. Ergün, and Y. Kayali: *Prot. Met. Phys. Chem.*, 2011, vol. 47, pp. 670–79.
44. H. Buckle: *The Science of hardness testing and its research applications in ASM*, J.W. Westbrook and H. Conrad, eds., Metals Park, OH, 1973, pp. 453–91.
45. Y. Sun, T. Bell, and S. Zheng: *Thin Solid Films*, 1995, vol. 258, pp. 198–204.
46. Z.H. Xu and D. Rowcliffe: *Thin Solid Films*, 2004, vols. 447–448, pp. 399–405.
47. W.C. Oliver and G.M. Pharr: *J. Mater. Res*, 1992, vol. 7, pp. 1564–83.
48. T. Chudoba, N. Schwarzer, and F. Richter: *Surf. Coat. Technol.*, 2002, vol. 154, pp. 140–51.
49. F. Cleymand, O. Ferry, R. Kouitat, A. Billard, and J. von Stebut: *Surf. Coat. Technol.*, 2005, vol. 200, pp. 890–93.
50. T. Ohmura, S. Matsuoka, K. Tanaka, and T. Yoshida: *Thin Solid Films*, 2001, vol. 385, pp. 198–204.
51. M.F. Doerner and W.D. Nix: *J. Mater. Res.*, 1986, vol. 1, pp. 601–09.
52. J. Mencik, D. Munz, E. Quandt, E.R. Weppelmann, and M.V. Swain: *J. Mater. Res.*, 1997, vol. 12, pp. 2475–92.
53. J.M. Antunes, J.V. Fernandes, N.A. Sakharova, M.C. Oliveira, and L.F. Menezes: *Int. J. Solids Struct.*, 2007, vol. 44, pp. 8313–34.
54. H. Gao, C.H. Chiu, and J. Lee: *Int. J. Solids. Struct.*, 1992, vol. 29, pp. 2471–92.
55. A. Perriot and E. Barthel: *J. Mater. Res.*, 2004, vol. 19 (02), pp. 600–08.
56. F. Roudet, D. Chicot, X. Decoopmana, A. Iost, J. Bürgi, J. Garcia-Molleja, L. Nosei, and J. Feugeas: *Thin Solid Films*, 2015, vol. 594, pp. 129–37.
57. M. Avrami: *J. Chem. Phys.*, 1940, vol. 8, pp. 212–24.
58. M. Avrami: *J. Chem. Phys.*, 1941, vol. 9, pp. 177–84.
59. J. Song, Y. Liu, Y. Zhang, and L. Jiao: *Mater. Sci. Eng. A*, 2011, vol. 528, pp. 5421–27.
60. X. Wang, S. Xu, S. Zhou, W. Xu, M. Leary, P. Choong, M. Qian, M. Brandt, and Y. Min: *Xie: A review Biomaterials*, 2016, vol. 83, pp. 127–41.
61. A.J. Nathanael, Y.M. Ima, T.H. Oha, R. Yuvakkumarb, and D. Mangalaraj: *Appl. Surf. Sci.*, 2015, vol. 332, pp. 368–78.
62. D. Sidane, H. Rammal, A. Beljebbar, S.C. Gangloff, D. Chicot, F. Velard, H. Khireddine, A. Montagne, and H. Kerdjoudj: *Mater. Sci. Eng. C*, 2017, vol. 72, pp. 650–58.