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Timing Paradox of Stepping and Falls in Ageing: Not so quick and quick(er) on the trigger.

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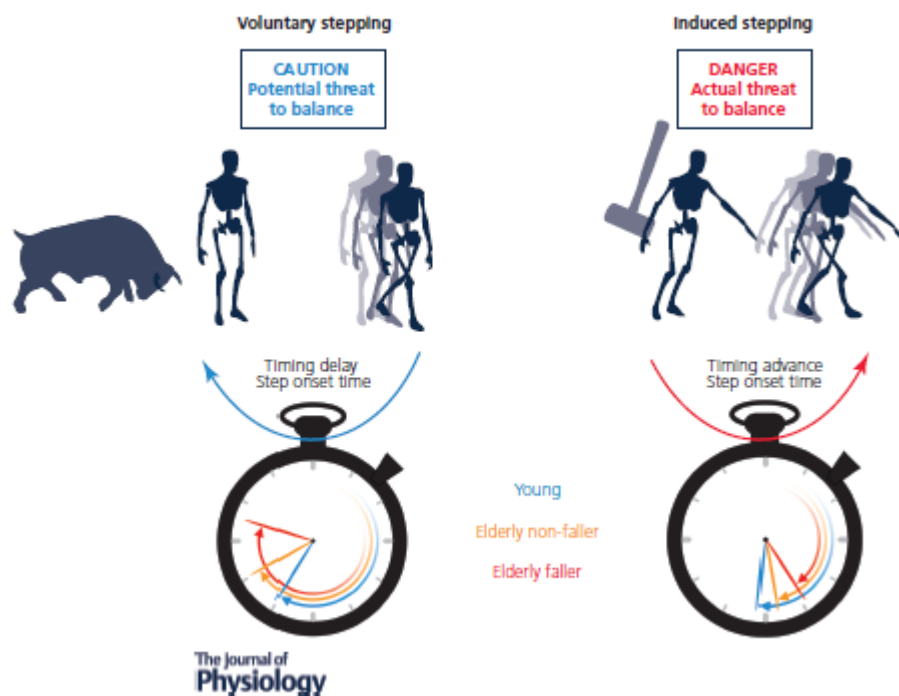
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Abstract

Physiological and degenerative changes affecting human standing balance are major contributors to falls with ageing. During imbalance, stepping is a powerful protective action for preserving balance that may be voluntarily initiated in recognition of a balance threat, or be induced by an externally imposed mechanical or sensory perturbation. Paradoxically, with ageing and falls, initiation slowing of voluntary stepping is observed together with perturbation-induced steps that are triggered as fast as or faster than for younger adults. While age-associated changes in sensorimotor conduction, central neuronal processing and cognitive functions are linked to delayed voluntary stepping, alterations in the coupling of posture and locomotion may also prolong step triggering. It is less clear, however, how these factors may explain the accelerated triggering of induced stepping. We present a conceptual model that addresses this issue. For voluntary stepping, a disruption in the normal coupling between posture and locomotion may underlie step-triggering delays through suppression of the locomotion network based on an estimation of the evolving mechanical state conditions for stability. During induced stepping, accelerated step initiation may represent an event-triggering process whereby stepping is released according to the occurrence of a perturbation rather than to the specific sensorimotor information reflecting the evolving instability. In this case, errors in the parametric control of induced stepping and its effectiveness in stabilizing balance would likely occur. We further suggest that there is a residual adaptive capacity with ageing that could be exploited to improve paradoxical triggering and other changes in protective stepping to impact fall risk.



Introduction

The inherently unstable nature of human standing requires postural motor actions for body orientation and balance stabilization that must be effectively integrated with other goal-directed actions to allow safe and efficient movement function. During actual or anticipated loss of balance, multi-segmental postural movements of the limbs such as stepping are commonly executed, and represent powerful protective actions for preserving balance by reconfiguring the body center of mass (CoM) - base of support (BoS) relationship. This requires that the motion of stepping limb be appropriately controlled to match the ongoing motion of the CoM. Stepping may be voluntarily initiated proactively in recognition of an impending threat to balance, or externally induced by a mechanical or sensory perturbation. Importantly, the ability to step quickly is a critical factor in arresting a fall (van den Bogert *et al.*, 2002).

With older age, physiological and degenerative changes involving multiple systems contributing to standing balance are major risk factors for falls and mobility disability. These changes are manifested as impairments in several motor control functions that compromise protective stepping behavior, effective stabilization of balance, and fall avoidance (Tinetti *et al.*, 1988; Rogers & Mille, 2003; Lord *et al.*, 2007). In this symposium review, we will address ageing deficits in only one of these control functions, the triggering of protective stepping.

Triggering Voluntary Stepping

A pedestrian standing at ease or walking on urban terrain may quickly sidestep to avoid an anticipated collision from oncoming pedestrian traffic that may destabilize balance or cause injury;

one may step to extend their base of support and guard against an expected threat to balance; another may suddenly back step onto a curb when the crosswalk stop signal flashes to preempt being flattened by vehicular traffic. Whereas voluntary step initiation or gait initiation may be viewed as actions that accomplish locomotion transport, a voluntary “protective step” is internally triggered in order to avoid a perturbation of balance by altering the CoM-BoS relationship to increase stability, or to avoid injury that might be imminent or is anticipated. The initiation of such proactive volitional stepping often involves motor planning and includes active changes in the CoM-BoS configuration that precede stepping through a sequence of muscle activations, joint moments, and corresponding changes in the ground reaction forces and center of pressure (CoP). These motor actions propel the CoM in the direction of stepping and towards the single stance limb for weight transfer and medio-lateral (M-L) stability prior to stepping (Carlsoo, 1966; Breniere *et al.*, 1987). Hence, anticipatory postural adjustments (APAs) precede and accompany the initiation of stepping and are adaptively scaled in amplitude and duration in accordance with the distance and speed of the first step (Breniere *et al.*, 1987).

The anticipatory nature of the postural-step coupling appears to involve a role for motor prediction in coordination. In an attempt to explain this coupling, we formulated a conceptual framework based on a forward internal model (Figure 1) involving neural processes that predict (estimate) the future state of the system given the current (actual) state and the sensorimotor control signals (Davidson & Wolpert, 2005). To trigger voluntary proactive stepping, the integrated networks for posture and locomotion are activated in parallel to generate a postural command that reconfigures the CoM-BoS relationship, and a locomotion command for stepping. Using internal and external feedback information, the forward model would determine if the APAs have achieved a sufficiently stable postural-balance state by estimating the position-velocity relationship between the COM and BOS before initiating the step and completing the postural phase. Hence, the neural circuits for triggering stepping would normally be actively delayed until the APAs that generate the weight transfer from bipedal to single leg stance support have achieved single stance limb loading (Massion *et al.*, 2004; Mille *et al.*, 2014).

With older age, the time to initiate voluntary stepping under reaction time (RT) conditions generally increases (Luchies *et al.*, 2002; Rogers *et al.*, 2003a; Melzer & Oddsson, 2004), and this initiation delay is greater for older adults with impaired balance and higher fall risk (Medell & Alexander, 2000; Lord & Fitzpatrick, 2001; St George *et al.*, 2007). The time to perform a rapid step increases more than for younger adults when the direction of stepping is uncertain during choice reaction time (CRT) conditions, or when a dual task activity is performed concurrently suggesting that increased cognitive demands worsen the differences in step triggering linked with older age (Lord & Fitzpatrick, 2001; Luchies *et al.*, 2002; Rogers *et al.*, 2003a; Melzer & Oddsson, 2004; St George *et al.*, 2007). Such RT delays are often attributed to age-related changes in sensorimotor speed and central neural processing. In this regard, associations between slowed RT stepping performance and white matter hyperintensities (WMHs) affecting the integrity and function of neural networks linked with sensorimotor processing and cognitive executive processes have been shown (Sparto *et al.*, 2008; Zheng *et al.*, 2012). With an increased WMH volume, CRT slowing appeared to be mediated through slower cognitive processing and not through reduced sensorimotor functioning (Zheng *et al.*, 2012). An association between greater levels of WMHs and prospective falls also appeared to be independent of diminished cognitive executive function and sensorimotor performance indicating a role for vascular health in preserving balance performance and preventing falls with ageing (Zheng *et al.*, 2011).

The slower voluntary stepping with ageing is frequently accompanied by deficits in initial postural adjustments such as errors in directional selection, number of postural movements, reduced peak force, longer time to peak force, and prolonged duration especially for individuals at higher fall risk under dual-task conditions (Melzer *et al.*, 2007, 2010; Cohen *et al.*, 2011; Sparto *et al.*, 2013). These postural changes that precede step initiation, suggest that a disruption in the normal coupling between posture and locomotion elements of stepping may contribute to step triggering delays through suppression of the locomotion network based on an estimation of the evolving state conditions for stability (see Figure 1) (Mille *et al.*, 2012). In support of this postulation, recent work has shown that the onset of rapid voluntary stepping in older and younger adults can be made faster by externally assisting with M-L APAs (Mille *et al.*, 2007), while impeding the performance of APAs can delay the onset timing (Mille *et al.*, 2014) (Figure 2). Additionally, during CRT stepping, older adults make more errors in postural preparation that further delay step onset timing with greater forward excursion of the body in association with response inhibition deficit (Cohen *et al.*, 2011). Furthermore, incongruous stimulus-response cues caused older adults to make more postural adjustments than they typically would with stimulus-response compatibility, indicating errors in postural preparation selection (Sparto *et al.*, 2013). During these erroneous trials, the onset of postural adjustments was earlier than during compatible cueing trials, indicating a failure to inhibit an inappropriate initial postural adjustment. Consequently, with additional postural adjustments, step onset was delayed compared with steps where postural errors did not occur. Overall, these findings suggested that deficits in inhibitory function involving response preparation may detrimentally affect proactive stepping by interfering with posture-locomotion coupling and delaying stepping.

Triggering Induced-Stepping

Stepping can also be induced by an externally applied mechanical or sensory perturbations. The initiation timing of externally induced reflex-like stepping can be more rapid than voluntary stepping (McIlroy & Maki, 1996; Luchies *et al.*, 1999, 2002; Rogers *et al.*, 2003a). As shown in (Figure 1), an externally applied mechanical perturbation modifies the CoM-BoS relationship. This postural disturbance is detected by multi-sensory systems that transmit information about the evolving state of balance instability that can be used by the central nervous system (CNS) to predict the consequences to stability based on the internal representation of the body. In turn, posture and locomotion networks are activated to trigger induced stepping with the required direction, timing, and amplitude needed to compensate for the perturbation. Unlike voluntary stepping, APAs are normally either absent or diminished in magnitude and effectiveness during induced stepping, and this appears to compromise M-L stability (McIlroy & Maki, 1999; Rogers *et al.*, 2001).

Based on a hierarchical model of strategy selection according to the amplitude of the postural challenge, induced stepping reactions have been traditionally thought to occur after relatively large postural disturbances where postural movements that maintain stationary foot-ground contact such as ankle and hip strategies fail to prevent the CoM from exceeding the mechanical limits of the BoS (Shumway-Cook & Woollacott, 2001). This perspective has been refuted by more recent work showing that reactive stepping often normally occurs well-before the limits of stability are exceeded even for smaller intensity perturbations as determined by the instantaneous

position and velocity of the CoM relative to the physical limits of the BoS (Maki & McIlroy, 1997; Pai & Patton, 1997; Pai *et al.*, 1998; Hof *et al.*, 2005; Patton *et al.*, 2006; Carty *et al.*, 2011). Thus, stepping does not depend solely on the mechanical constraints of the position of the CoM exceeding the BoS as many studies have shown that stepping occurs more frequently than predicted by this model (McIlroy & Maki, 1993; Pai *et al.*, 1998, 2000).

Consistent findings across studies have shown that older individuals step more often and with smaller perturbations than younger adults (McIlroy & Maki, 1993; Pai *et al.*, 1998; Rogers *et al.*, 2001; Mille *et al.*, 2003). This suggests that physiological factors rather than solely mechanical reasons determine step triggering. Recent observations have indicated that, at first step lift-off following lateral postural disturbances, the area used to move the net CoP for decelerating CoM motion was reduced for older fallers compared with non-fallers indicating reduced functional limits of dynamic stability (Fujimoto *et al.*, 2015). This finding implied that although the CoM motion state for fallers is located farther from the BoS boundary than for Non-Fallers indicating a greater stability margin in relation to their BoS, they might have approached their functional limit for CoP movement requiring them to step. Diminished excursion of the CoP, likely through impaired neuromechanical control of hip abduction-adduction torques, precipitated greater instability for at risk individuals when stepping was triggered. Thus, the functional limit might represent a more sensitive estimation of lateral balance stability.

Experimental determination of the threshold for triggering induced stepping in response to forward waist-pull perturbations (Mille *et al.*, 2003) showed that the threshold boundary had a characteristic sigmoidal relationship between position and velocity of the pelvis relative to the BoS, with distinct position thresholds for both low- and high-velocity waist-pulls (Figure 3). The boundary had a forward limit (T_L) that, when exceeded, always made subjects step no matter how slowly they were pulled. As velocity increased, the threshold position that triggered a step shifted nearer to the ankle joint center. Eventually a pull velocity was reached above which velocity had no further effect and a position threshold (T_H) was identified behind which subjects never stepped (Figure 3). Older subjects stepped more often than the young (69% vs. 40% of trials). For the older subjects, T_L and T_H were closer to the ankles, and the transition between T_L and T_H occurred at lower velocities (Figure 3). The physiological factors that could explain this threshold were investigated by studying the association of the boundary characteristics with a range of sensorimotor physiological tests (Mille *et al.*, 2003). Overall, many sensorimotor factors were associated with T_L and T_H . However, these associations were not present when age was removed as a factor. Thus, although the older subjects stepped more often, this cannot be attributed directly to the sensorimotor factors tested. It can be explained, however, by stepping as a triggered response to the perturbation event rather than to later sensory input about body movement reflecting the evolving state of instability.

Timing Paradox of Step Triggering with Ageing and Falls

As reviewed above, older adults are slower initiating voluntary stepping and this increase in RT has been associated with a greater risk of falls. Paradoxically, the initiation timing of induced protective stepping is as fast for older persons as for younger adults or even faster for those at greater risk of falls (Pai *et al.*, 1998; Luchies *et al.*, 1999; Rogers *et al.*, 2001, 2003a; Mille *et al.*, 2013). When considered together, these observations suggest that induced stepping among older

adults is pre-selected as a strategy based on an internal representation estimate of system dynamics wherein it is recognized from experience that pre-stepping compensatory responses (e.g., ankle torque strategy) are inadequate (Woollacott, 2000; Okada *et al.*, 2001), and predetermines that a step will be needed when an input trigger arrives even before the step may actually be necessary.

The foregoing proposition has been further investigated by introducing experimental conditions involving contextual uncertainty about balance stability that alter the initiation timing of stepping. If a pre-selection strategy was used, then combining an imperative voluntary RT instruction set with the potential for perturbation would delay the triggering of reactive stepping in the presence of uncertainty about the impending state of stability that could accompany stepping (Rogers *et al.*, 2003a). With this paradigm, the premature triggering of a forward step would potentially exacerbate instability through synchronization of instructed proactive stepping and forward perturbation-induced stepping. When older subjects initiated instructed rapid stepping in response to a light cue (Proactive certain), step initiation tended to be slower than for younger adults (Figure 4). However, older subjects were as fast as the young to initiate a reactive step in response to a postural perturbation (Reactive certain). When a voluntary step was initiated under the threat of a forward perturbation (Proactive uncertain) step initiation was delayed, particularly in older subjects who remained slower than the young. On the other hand, when subjects performed RT stepping and were perturbed forward before the reaction cue was activated (Reactive uncertain), younger and older individuals demonstrated a contextual dependent capacity to delay substantially (by 200–300 ms) the triggering of reactive protective stepping. This indicated that the initiation timing for triggering a reactive step does not reflect entirely an immediate necessity or a last resort response to balance instability. While stepping occurred 50 ms earlier for the old during the reactive certain condition, their initiation timing during reactive uncertain trials occurred 130 ms earlier than for the young (Figure 4). Thus, the trend for older individuals to trigger stepping earlier was exacerbated by the contextual uncertainty about balance stability. At least for these experimental conditions, perturbation-induced stepping was apparently not triggered directly by specific sensory input reflecting the state of balance stability but appeared to involve a pre-selection process that was initiated before it may have actually been needed. With balance uncertainty, subjects might have prolonged their initiation timing to a threshold level that more directly approached their mechanical limits of stability to recover balance and step initiation timing might have been estimated via on-line sensory information.

The earlier triggering of induced stepping with ageing and falls might reflect a decision to step rather than a necessity. Psychophysical studies have shown that the threshold for detecting an event is lower than the threshold for detecting the specific properties of movement (Hall & McCloskey, 1983; Refshauge *et al.*, 1995). Sensory information about the occurrence of an event does not have information about movement size and direction. When a mechanical perturbation occurs (Figure 5), those with greater fall risk might step in response to event-detection rather than to specific movement detection information. This would explain the earlier timing of induced stepping with older age and fall risk and the ineffectiveness of the first step observed for many of these individuals (Mille *et al.*, 2013).

Conclusions

The features of the age-related differences in the triggering of voluntary and induced stepping and their relationship with the risk of falls are compatible with the conceptual theoretical model that we propose. The characteristic delay in initiating rapid voluntary stepping with ageing, especially when spatial or temporal uncertainties about the nature of the task are not known in advance (e.g. CRT) or when cognitive demands are increases (e.g. dual task performance), is somewhat counterintuitively accompanied by an equivalent or earlier triggering of externally-induced stepping. While the triggering delay in voluntary RT stepping has generally been attributable primarily to changes in neuronal conduction and central processing, the specific neural substrates and processes that underlie this slowing remain to be elucidated. For example, although white matter hyperintensities linked with sensorimotor processing and cognitive executive functions may play a role in delaying voluntary stepping (Zheng *et al.*, 2012), alterations in motor preparation or response generation integrating posture and locomotion that involve cortical and brainstem networks may also undergo changes with age that prolong step triggering (Drew *et al.*, 2004; Jacobs & Horak, 2007; MacKinnon *et al.*, 2007; Rogers *et al.*, 2011). Furthermore, older individuals with motor slowing and altered coordination show a reduced capability to modulate GABA-mediated cortical inhibitory processes that appears to be related to age-related loss of white and gray matter and increased brain activation in cortical and subcortical areas (Levin *et al.*, 2014).

In future work, it would be important to determine whether or not age-related changes in the ability to modulate motor cortical or brainstem excitability and inhibitory processes during response preparation and generation of stepping, or in suppressing stepping actions, are linked with altered protective stepping and falls. These processes have been previously shown to be affected by older age for isolated single joint and limb movements (Fujiyama *et al.*, 2012; Levin *et al.*, 2014), and to a lesser extent during stepping (Jacobs and Horak, 2007; MacKinnon *et al.*, 2007; Rogers *et al.*, 2011). Determining the associations between ageing impairments in structural and/or functional integrity of brain networks with changes in CNS modulatory mechanisms and motor deficits are additional gaps and emerging areas that could be fruitful to investigate. Given the pervasive sarcopenic changes in skeletal muscle accompanying older age with diminished motor performance (Addison *et al.*, 2014; Cruz-Jentoft *et al.*, 2014; Inacio *et al.*, 2014), better understanding of the relative contributions of neural and muscular deficits and their interaction to altered neuromotor control of stepping and other balance stabilizing actions is another promising line of study in this area.

For induced stepping, the fact that steps are triggered more often and earlier within the CoM-BoS position-velocity state space, and may be as fast or faster than for younger adults, is consistent with the postulation that older people at greater risk of falling might step in response to an event-detection strategy rather than to specific movement detection information. Although the causal factors underlying this possibility are currently unknown, it is conceivable that heightened arousal or anxiety related to one's vulnerability to falls may be contributing to a lower threshold for triggering stepping (Pai *et al.*, 1998; Carpenter *et al.*, 2004). A further and intriguing possibility is whether or not external perturbations of posture induce startle reactions that may be interspersed with postural responses and differentially integrated and modulated with age and fall risk. Studies have shown a superimposition of startle reflex activity on the postural response during first trial balance and freefall perturbations, and that postural responses can be accelerated by a startling acoustic stimulus even when the perturbation direction is not known in advance (Oude Nijhuis *et al.*,

2010; Campbell *et al.*, 2013; Sanders *et al.*, 2015). It is possible that the presence of startle reaction coincident with the balance response may interfere with the parametric control of protective stepping and its effectiveness in stabilizing balance. Therefore, a further direction for future studies would be to determine whether or not age-related changes in startle contributions involving brainstem and cortical pathways influence the triggering of induced stepping responses in relation to fall risk.

Finally, from a rehabilitation standpoint, the capacity for both volitionally triggered and perturbation-induced protective stepping to be at least acutely improved with step training interventions among older individuals, suggests that there is a residual adaptive capacity that can be exploited to advance therapeutic approaches to enhance balance function and reduce the risk of falls (Rogers *et al.*, 2003b; Mille *et al.*, 2009; Barrett *et al.*, 2012; Yungher *et al.*, 2012). Therefore, it appears that targeting improvements in age-associated paradoxical triggering of voluntary and induced protective stepping could be a useful goal of rehabilitation interventions. In this regard, however, an important gap in current understanding is in determining the underlying CNS and neuromotor mechanisms that drive activity and exercise-based adaptations in motor performance to improve protective balance and other motor actions. Greater insights into these areas should be valuable for optimizing the design of effective balance rehabilitation and fall prevention interventions by providing directives for tailored programs that target the specific problems for different health conditions and individuals.

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Figure legends

Figure 1. Conceptual model of posture and locomotion coupling during the initiation of stepping.

To initiate voluntary stepping, posture and locomotion networks are activated in parallel to generate motor commands (black arrows) where the posture network acts on the stepping controller. These motor outputs modify the body center of mass–base of support (CoM-BoS) relationship. Efferent copies of the motor commands and sensory information about the actual state of the body can be used by the CNS (internal feedback loops - green arrows) to estimate the future state of instability produced by the evolving movement, and modify in advance the two commands based on an internal representation of the body and external environment (forward model). On-line sensory

information can also modulate posture and locomotion commands via external feedback information (grey arrows). For perturbation-induced stepping, an external mechanical perturbation (red arrows) modifies the CoM-BoS relationship. Multi-sensory systems transmit information about the evolving state of instability that can be used by the CNS to estimate its consequences using the internal representation of the body, and to activate posture and locomotion networks to initiate a suitably directed, timed, and scaled induced step to compensate for the perturbation. Again, these commands can be modified via internal or external feedback processes.

Figure 2. Posture and locomotion coupling during voluntary stepping.

During voluntary stepping, single limb stance support is normally achieved prior to stepping. If anticipatory postural adjustments (APAs) are unexpectedly modified by external assistance (data presented in black - group mean and SD of 8 older subjects - adapted from Mille *et al.*, 2007) or resistance (data presented in green - group mean and SD of 12 young women - adapted from Mille *et al.*, 2014), step onset timing is then either advanced (Assisted) or delayed (Resisted) compared to the control condition (Normal) so that step onset occurs when the estimated conditions for stability are achieved. When APAs are assisted, older individuals initiated volitional stepping as fast as younger adults performance in the un-assisted baseline condition. The bottom panels show the averaged time profiles from a representative younger adult during baseline rapid step initiation (in blue - average of 10 trials) and during mechanically resisted step initiation (in red - average of 15 trials). All records were synchronized with the onset of the net CoP displacement (vertical dotted line) at time zero. The shaded regions represent ± 1 SD. The vertical displacement of the stepping ankle marker indicates a delay in the first step onset time and increased step height. The mean EMG activity of stepping leg muscles shows a delay of the step motor command [illustrated by the rectus femoris (RF) and the tensor fasciae latae (TFL) activity], and a modification of the step motor command with the appearance of a phasic activation bursts in soleus (SOL) and gastrocnemius medialis (GAST) when a postural perturbation is randomly applied, whereas no modification in the onset of the tibialis anterior (TA) activity was observed.

Figure 3. Experimental determination of perturbation-induced stepping threshold.

Younger and older adults received 124 randomly applied displacement-velocity forward waist-pull perturbations to determine the threshold for triggering induced stepping. **A)** The threshold for forward -induced stepping was determined using a linear-motor pulling the subject forward via a flexible cable attached around the upper pelvis. The pulls started at an unexpected time and proceeded at the test velocity until, on reaching the test displacement (D), the cable tension is released and the subject can lean back if a step has not already been initiated. This is illustrated in the pull displacement profile (D) as a function of time. The initial position of the subject was estimated from the initial location of the center of pressure (CoPi) relative to the ankle joint center. D was added to the CoPi to estimate the final position of the pelvis at the end of the pull relative to the ankle (P). This reflected how far in front of the axis of the ankles the pelvis moved at the end of the pull. **B)** The threshold boundary was then described using a modified Boltzmann function which is a negative, inverse exponential of velocity. Four parameters, represented in the graph, described

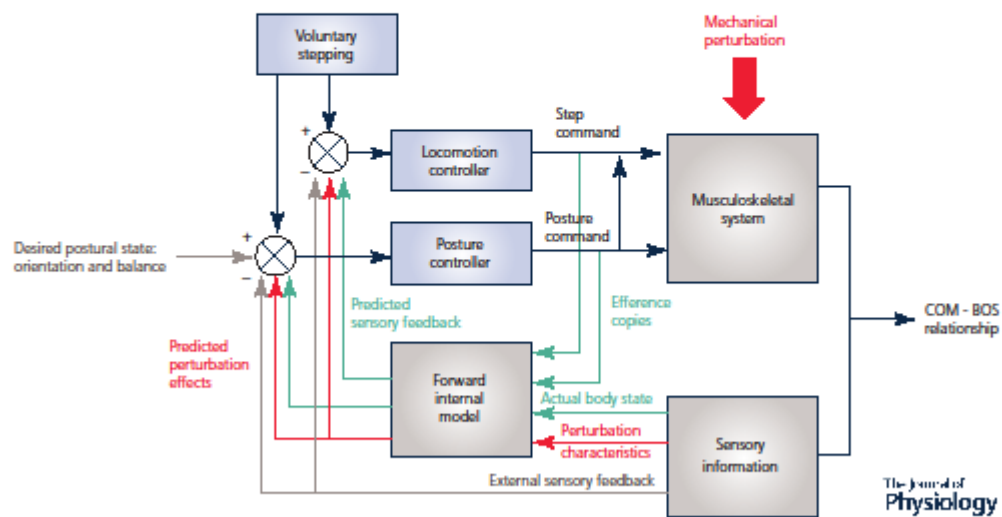
the low-velocity plateau (T_L) and the high-velocity plateau (T_H) levels, the velocity that produces the mid-range response (V_{50}), and the slope (S). The inverse of the slope is directly proportional to the maximal steepness of the function, which occurs at mid-range. **C)** Typical stepping records for a young and an older subject. Each circle corresponds to a pull trial, marked as either a step (yellow) or no step (white). At each velocity, a threshold position (red diamond) was identified halfway between the most anterior position (largest value) that did not produce a step and the most posterior position (smallest value) that produced a step. The Boltzmann function was fitted (Gauss-Newton non-linear least-mean-squares algorithm) to these threshold position points to describe the threshold boundary (solid line) (Adapted from Mille *et al.*, 2003).

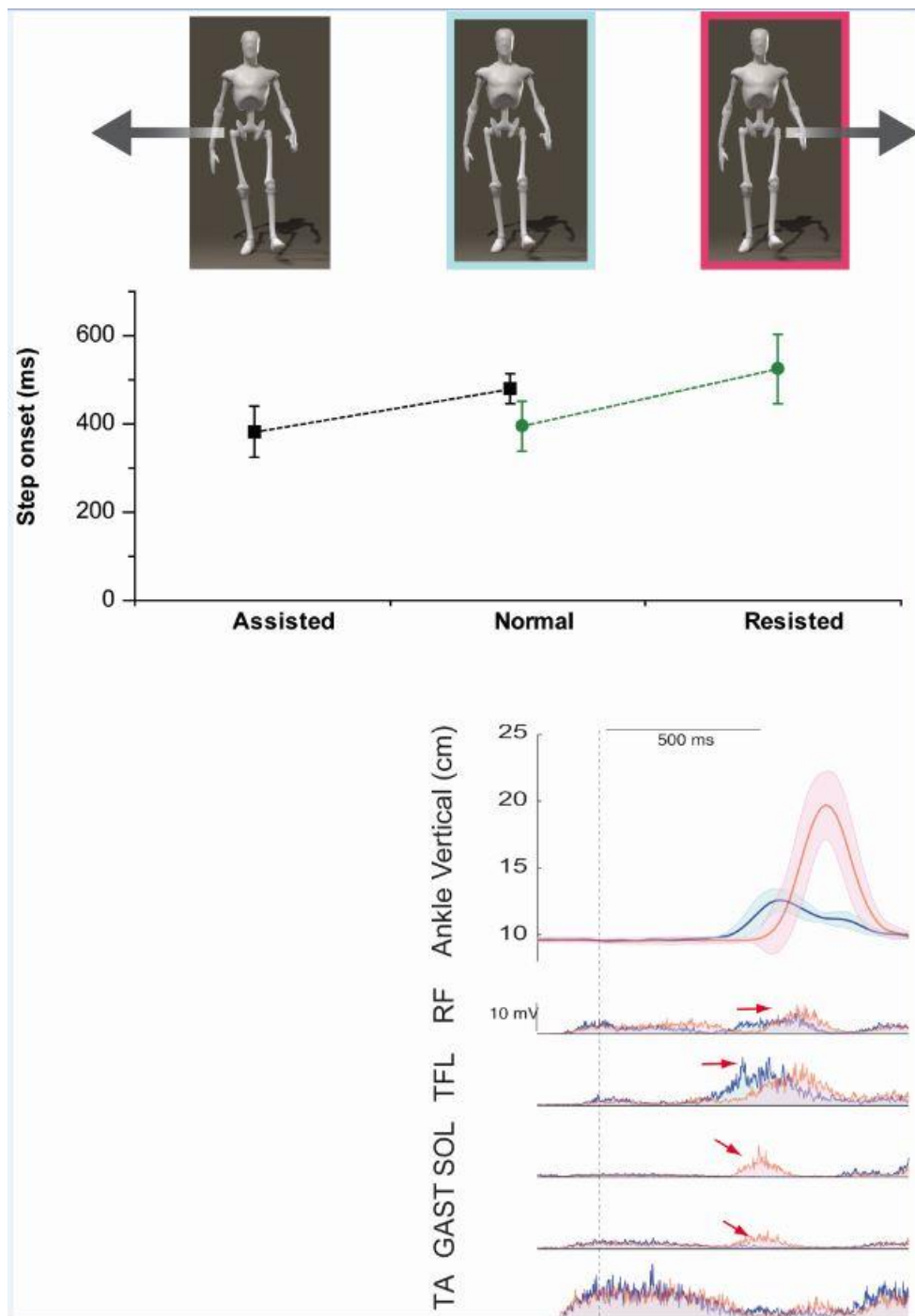
Figure 4. Effects of age and contextual uncertainty on the timing of step initiation.

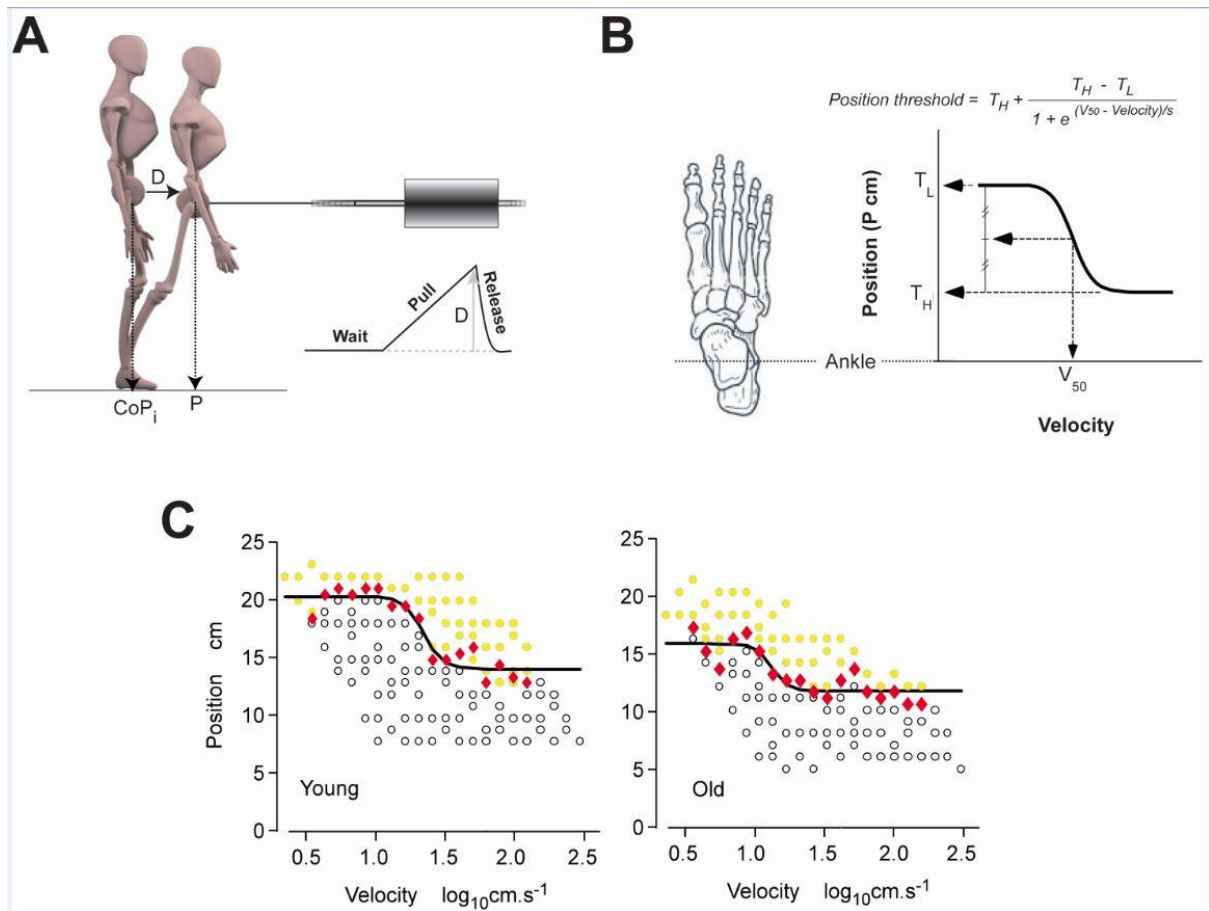
The loading-unloading forces registered by a force platform beneath the stepping limb provided timing information about the instant of first step lift-off under four different experimental conditions: Voluntary Certain ((instructed reaction time (RT) stepping without perturbations)), Induced Certain (perturbation-induced stepping without instruction), Voluntary Uncertain (instructed RT stepping with threat of random perturbations), Induced Uncertain (instructed RT stepping with actual random perturbations). In the Induced Uncertain trials, the perturbation was presented at different times prior to the imperative RT light cue. When older subjects initiate a voluntary step in response to a light cue (Voluntary Certain), step initiation is slower than for younger adults. Paradoxically, older subjects are as fast as the young to initiate a step in response to the postural perturbation (Induced Certain). When a voluntary step was initiated under the threat of a perturbation (Induced Uncertain) step initiation timing was delayed, particularly in the old who remained slower than the young. When subjects performed RT stepping but were perturbed prior to the imperative go-cue (Induced Uncertain), both groups delayed the onset of stepping. This indicated that the initiation timing for triggering induced stepping did not reflect entirely an immediate necessity or a last resort response to balance instability (values represent group means and SDs for 32 older subjects and 14 young - adapted from Rogers *et al.*, 2003).

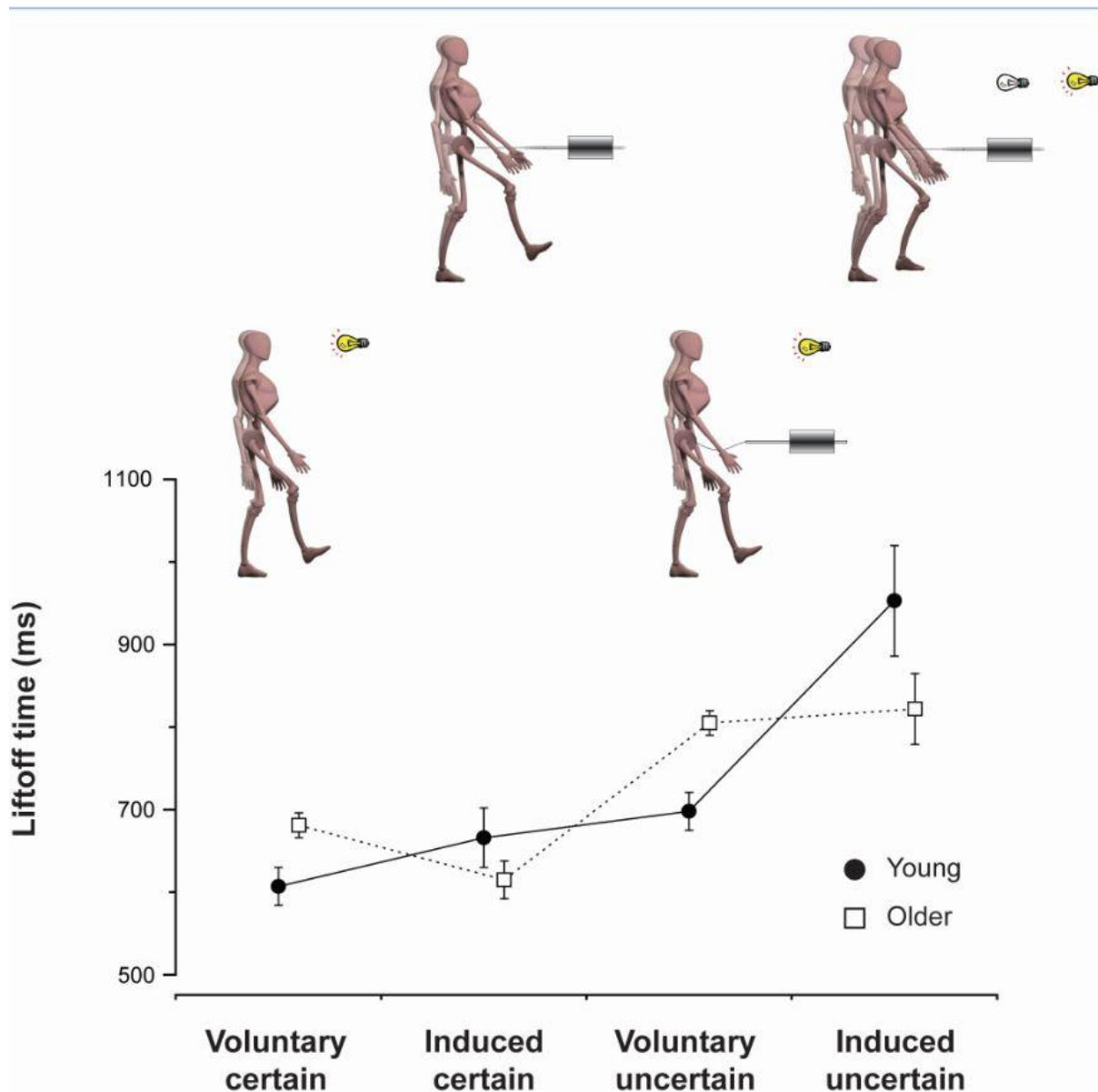
Figure 5. Conceptual model of induced-step triggering with ageing and fall risk.

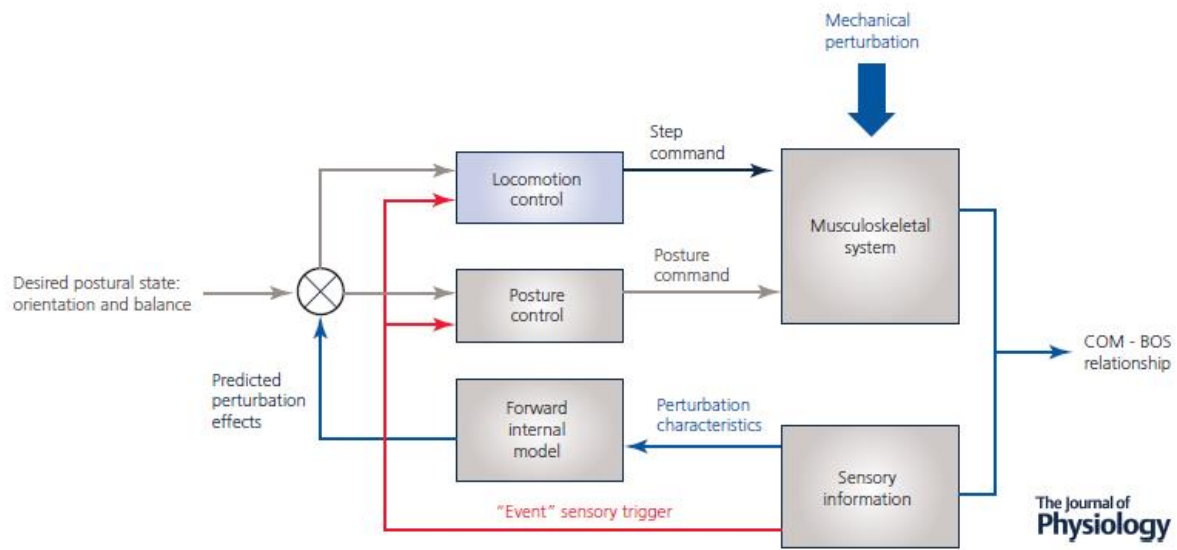
An external postural perturbation modifies the CoM-BoS relationship. Instead of using on-line processing of the perturbation characteristics to estimate the state of evolving instability (based on an internal representation of the body) and trigger initiate an induced-step with the correct direction, timing, and amplitude to compensate for the perturbation (see Figure 1), particularly older adults at greater risk of falling might react to event-information (red arrow) that would trigger a preset stepping response that is not adaptively tuned to the perturbation characteristics.











Biographies:

Mark W. Rogers received his undergraduate degree in Physical Therapy from the University of Connecticut, Storrs and graduate degrees from the University of Massachusetts, Amherst and the University of Iowa, Iowa City followed by postdoctoral studies at McGill University, Montreal, Canada. His research interests are focused on human neuromotor control of balance and locomotion in health and disease including the interaction of neural, musculoskeletal, and behavioral systems that underlie function and its restoration through rehabilitation.

Marie-Laure Mille has a PhD in Motor Control from the Aix-Marseille University. She started focusing on protective stepping and ageing during her postdoctoral fellowship at Northwestern University. She has broad interests in human sensorimotor control processes in health and disease with a focus on the coordination of posture and locomotion. She has a tenured position at the University of Toulon and is furthering her research at the Movement Sciences Institut in Marseille.

