



HAL
open science

Enhanced nonlinear imaging through scattering media using transmission matrix based wavefront shaping

Hilton de Aguiar, Sylvain Gigan, Sophie Brasselet

► **To cite this version:**

Hilton de Aguiar, Sylvain Gigan, Sophie Brasselet. Enhanced nonlinear imaging through scattering media using transmission matrix based wavefront shaping. *Physical Review A*, 2016, 94, pp.043830. 10.1103/PhysRevA.94.043830 . hal-01400272

HAL Id: hal-01400272

<https://hal.science/hal-01400272v1>

Submitted on 7 Sep 2023

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

Enhanced nonlinear imaging through scattering media using transmission matrix based wavefront shaping

Hilton B. de Aguiar,^{1,*} Sylvain Gigan,² and Sophie Brasselet^{1,†}

¹*Aix-Marseille Université, CNRS, Centrale Marseille,
Institut Fresnel UMR 7249, 13013 Marseille, France*

²*Laboratoire Kastler Brossel, UMR 8552 of CNRS and Université Pierre et Marie Curie, 24 rue Lhomond, 75005 Paris, France*

Despite the tremendous progresses in wavefront control through or inside complex scattering media, several limitations prevent reaching practical feasibility for nonlinear imaging in biological tissues. While the optimization of nonlinear signals might suffer from low signal to noise conditions and from possible artifacts at large penetration depths, it has nevertheless been largely used in the multiple scattering regime since it provides a guide star mechanism as well as an intrinsic compensation for spatiotemporal distortions. Here, we demonstrate the benefit of Transmission Matrix (TM) based approaches under broadband illumination conditions, to perform nonlinear imaging. Using ultrashort pulse illumination with spectral bandwidth comparable but still lower than the spectral width of the scattering medium, we show strong nonlinear enhancements of several orders of magnitude, through thicknesses of a few transport mean free paths, which corresponds to millimeters in biological tissues. Linear TM refocusing is moreover compatible with fast scanning nonlinear imaging and potentially with acoustic based methods, which paves the way for nonlinear microscopy deep inside scattering media.

I. INTRODUCTION

Nonlinear microscopy (NLM) is established as a powerful approach for label-free imaging in biological tissues. Despite the impact of NLM on many fields, standard nonlinear imaging modalities can however only image at shallow depths, typically a few hundreds of micrometers for biological specimens. The penetration depth is hindered by optical aberrations and scattering, which degrade the spatial quality of focusing and decrease the spatiotemporal coherence of short pulse excitation fields necessary to build up nonlinear processes. In order to enhance the penetration depth, adaptive optics has been introduced to compensate for aberrations from biological samples¹. Although signal enhancements up to two orders of magnitude can be reached, adaptive optics is limited to depths of a few scattering mean free path (typically a millimeter in biological tissues), since it relies on ballistic photons²⁻⁴. It also most often relies on the optimization of an existing nonlinear signal, which inherently limits this technique in case of strong scattering.

Wavefront shaping (WS) can overcome penetration depths limits in highly scattering media, addressing specifically the scattered photons⁵. Despite the random appearance of the outgoing speckle pattern arising from multiple scattering events, it has nevertheless a deterministic relation with the original incoming wavefront, revealed in the Transmission Matrix (TM) of the scattering medium that connects incoming to outgoing fields. By coherently controlling a speckle pattern, one can increase the energy density at targeted positions, resembling a focus that we call "refocus" in what follows to avoid confusion with a focus obtained from ballistic photons. WS has shown to be able to refocus through^{6,7}, or inside⁸ scattering media, thanks to the manipulation of the wavefront phase or amplitude^{9,10}.

The combination of WS and NLM is however so far limited to only a few demonstrations, based on nonlinear feedback optimization¹¹⁻¹³. These methods offer in particular a way to obtain an intrinsic spatiotemporal control of a refocused spot, by the use of degrees of freedom offered by the intrinsic space-time coupling in scattering media¹¹⁻¹⁴. The use of broadband spectral excitation conditions, necessary for nonlinear optical generation, is however limited by the fact that the spectral width of the excitation pulse might be larger than the spectral width of the scattering medium (which is inversely proportional to its Thouless time)^{15,16}, leading to a decrease of optimization efficiency due to the need to compensate both spatial dispersion temporal broadening¹¹. Demonstrations using either a nonlinear guide star¹¹ or an integrated nonlinear signal¹³ have thus led so far to only mild nonlinear enhancements of two orders of magnitude, which is below the optimal expected values.

In this work we address the use of TM-based manipulation to generate nonlinear signals through a scattering medium, under broadband conditions where the spectral width of the excitation is similar or slightly larger than the spectral width of the medium, *i.e.* the spectral correlation width of the speckle. In particular, we take advantage of the fact that spectral decorrelation bandwidths in biological media at 1-2 mm-deep (corresponding to a transport mean free path l_t) are comparable with the bandwidth of common laser sources used for NLM (about 100 fs pulse length)¹⁷. We demonstrate that in such regime a TM acquired using either the *linear* or *nonlinear* feedback is compatible with *nonlinear* signal enhancement. We show that linear-feedback-based TM offers fast nonlinear imaging capabilities and high signal-to-noise conditions. This scheme is moreover applicable to nonlinear imaging *inside* a scattering medium, being compatible with acoustics based approaches⁸. We illustrate the potential of this approach in Second Harmonic Generation (SHG) imaging of thick collagen fibers placed behind scattering media of thicknesses close to l_t , in conditions that would fail using nonlinear feedback optimization.

II. RESULTS

Fig. 1a illustrates the general experimental layout that we use for both nonlinear and linear feedbacks, both based on TM measurements. In both cases, the excitation is spectrally broadband with a pulse length of about 130 fs (800 nm central wavelength). The incident linear beam wavefront is manipulated by a spatial light modulator (SLM) imaged at the backfocal plane of the focusing lens. A nonlinear SHG-active sample is placed at about 500 μm distance after the scattering medium, and imaged on either a pixelized sensitive camera or on a large area integrating detector. For acquisition of the TM (Fig. 1b), we tune the incident wavefront phase, following an approach thoroughly described in Ref.¹⁸ and detailed in the Methods section. The incident wavefront is decomposed on the Hadamard basis — instead of the canonical basis — to benefit from higher fluences at the sample plane. The pixel signal on which the measurement is performed is recorded either at the incident linear wavelength (linear feedback) or at the SHG wavelength emitted from a SHG-active region of the sample (nonlinear feedback). Potassium titanyl phosphate nanocrystals (nanoKTP) of 150 nm diameter are used to monitor the SHG enhancement obtained after both linear and nonlinear feedbacks. These nanocrystals are in particular of superior photostability¹⁹ as compared to fluorescent samples that are likely to photobleach^{13,20}. Quantitative analysis is moreover based on single isolated nanocrystals in order to avoid any bias due to multiple interference sources, such as clustered particles.

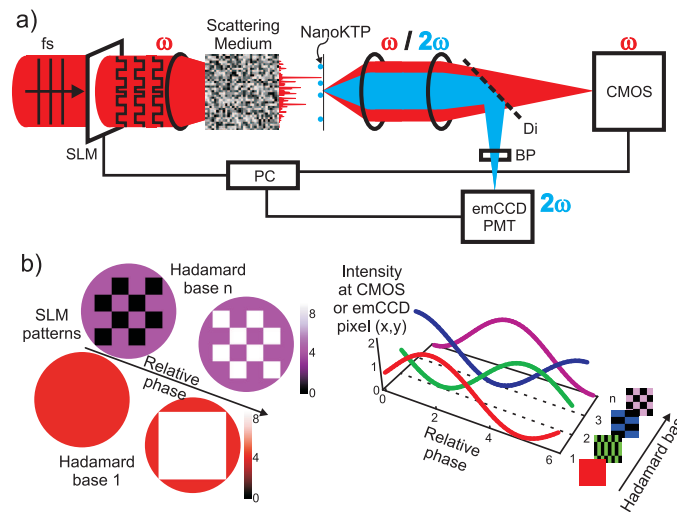


FIG. 1. Wavefront shaping experiments for nonlinear microscopy. a) Simplified experimental layout. The optical wavefront is shaped by an SLM and focused inside the scattering medium. The speckle generated outside the scattering medium excites the nonlinear sources (nanoKTP) placed at a plane further imaged on different detectors (emCCD, CMOS, PMT). b) Methodology used for refocusing using the Hadamard basis. The wavefront phase is swept in respect to a reference field (the unmodified periphery outside a Hadamard base), under broadband illumination condition. At the detectors (a pixel on the emCCD or on the CMOS) a sinusoidal modulation of the intensity is observed, from which each individual phase is stored (per base). After scanning the basis set, the optimal wavefront is used for either enhancing the nonlinear signal (emCCD) or linearly refocusing (CMOS) with the nonlinear signal detected in parallel (PMT).

A. Nonlinear feedback refocusing

Fig. 2a shows SHG images obtained when a single isolated nanoKTP crystal is placed behind a diffuser, using non-optimized and optimized wavefronts. The optimized image is formed after WS has been performed at the nanoKTP position (see Methods section) using the information obtained from a TM measured using a nonlinear feedback. While linear feedback TM is standard⁷, nonlinear feedback still allows measurement of the phase of the TM elements¹¹. This approach evidences the capacity of the nonlinear feedback-based TM to refocus light on this specific isolated nanocrystal and to generate a high nonlinear response.

Remarkably, up to four orders of magnitude nonlinear enhancements are achieved by using a few hundreds of independently controlled SLM segments (N_{SLM}). Fig. 2b shows that the nonlinear enhancement obtained from a single nanoKTP signal depends quadratically on N_{SLM} (the departure at high N_{SLM} is attributed to experimental artifacts such as possible correlations between SLM segments¹⁸). This expected dependence ascertains that the refocused spot preserves optimal nonlinear coherent build-up.

The nonlinear enhancements measured here are far above what has been previously reported in multiply scattering media using even higher N_{SLM} values¹¹. This difference is assigned to the regime used here. Even though the excitation pulse is broadband, its spectral bandwidth lies below the spectral bandwidth of the scattering medium, or similarly the pulse length of 130 fs surpasses the Thouless time of the medium. Note that this lengthening time scales as L^2/D , with D the diffusion constant of the medium (proportional to l_t), and L the medium thickness^{15,16}. These properties can be monitored by the transmitted speckle contrast^{15,16,21}: for the scattering medium used a speckle contrast of 0.98 has been measured, which is indeed the signature of a large medium spectral bandwidth^{15,21}.

Even though nonlinear feedback is able to provide remarkably high enhancements, it still imposes practical constraints. Using 64 controllable SLM segments requires in particular TM acquisition times of the order of minutes, which can be at extreme costs for nonlinear imaging. Furthermore, this methodology also relies on low signals, especially at large depths, and can be only measured in regions where nonlinear signal is emitted. To answer these issues, we address in the next section the use of the overwhelming linearly scattered photons for nonlinear signal enhancements.

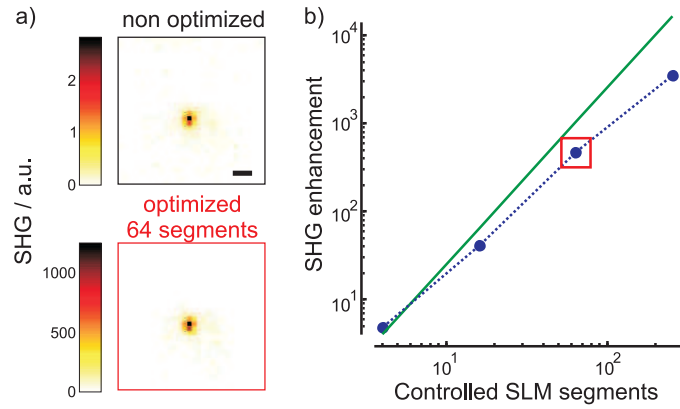


FIG. 2. Nonlinear signal enhancement based on a nonlinear feedback on a single 150 nm diameter nanoKTP crystal through a scattering medium (diffuser). a) SHG wide field images, taken with the emCCD, before (upper panel) and after WS (lower panel). The non optimized image is an average over random wavefronts, whereas the optimized image is a single frame. Scale bar: 1.6 μm . b) Nonlinear SHG enhancement of a single particle versus the number of independently controlled SLM segments (blue markers). The red box refers to the point depicted in a). The green line follows a quadratic dependence of the nonlinear enhancement with respect to linear enhancements estimated after Ref.⁷.

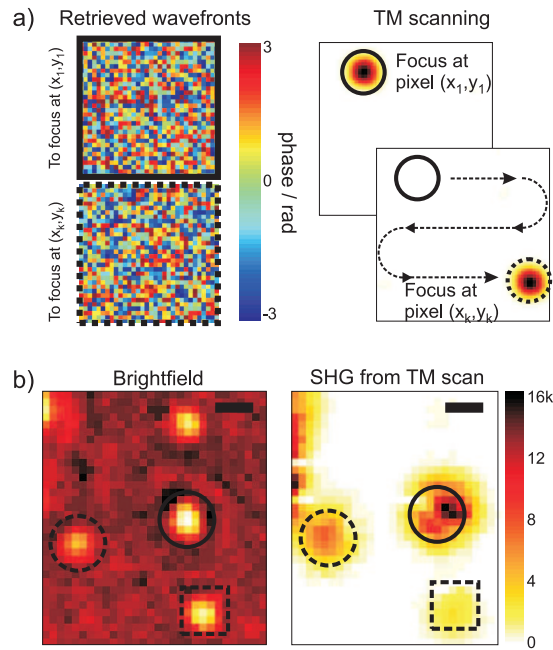


FIG. 3. Nonlinear signal enhancement based on a linear feedback through a scattering medium (diffuser). a) After acquisition of the linear transmission matrix, wavefronts are tailored to refocus the beam at desired positions through the scattering medium. The optimal wavefronts obtained for two different positions are depicted. b) Comparison between a brightfield image (left, revealing the location of the nanoKTP crystals) and the obtained corresponding SHG image (right). The SHG image is obtained by a scanning of the focus positions obtained from the linear feedback optimization procedure. Number of controlled SLM segments: 2^{12} . Scale bar: 0.9 μm .

B. Linear feedback refocusing

The principle of SHG image reconstruction by linear feedback is sketched in Fig. 3. After acquiring the TM of the system, refocus is formed at a desired location, with simultaneous acquisition of nonlinear signals, resembling raster-scanning methodologies. Note that as above, the TM of the medium is measured under spectrally broadband conditions: the measured interferometric modulation is the spectrally integrated modulation measured on the detector. For a medium with negligible temporal broadening, this approach is equivalent to Ref.⁷, whereas for a medium that broadens the pulse, the acquired TM can be seen as the incoherent sum of different spectral contributions. Figure 3a

shows representative incident wavefronts corresponding to the two positions of the refocus, showing no correlation as expected in multiple scattering conditions. The acquisition of the TM procedure for 256 controllable SLM segments takes about 40 s per region of interest (ROI), which is considerably faster than in the nonlinear feedback procedure described above. Note that linear feedback is limited by the SLM speed, rather than signal-to-noise issues as in nonlinear feedback. Alternatively, one could use the memory effect to reconstruct the final SHG image, with a field of view that depends on the scattering medium properties and set-up configuration^{13,22–24}.

To validate the imaging mode methodology, we compare in Fig. 3b the SHG image of isolated nanoKTP crystals acquired by refocus scanning, with a brightfield image taken without the scattering medium. The positions of the three detected nanocrystals are in excellent agreement with the brightfield image. The difference in SHG signal levels is due to the relative orientation of the crystal with respect to the polarization state of the excitation field, indicating that the polarization of the refocused beam is also conserved^{25–29}. Note that the spatial resolution of the final SHG image is ultimately determined by the spatial coherence length of the speckle (the size of the speckle grain). An additional $1/\sqrt{2}$ factor to the resolution comes from the nonlinear nature of the process, as known in NLM conditions. In comparison, the use of a nonlinear feedback might lead to spurious effects if the distribution of nonlinear emitters is complex in the three dimensions of the sample as discussed in Ref.¹³.

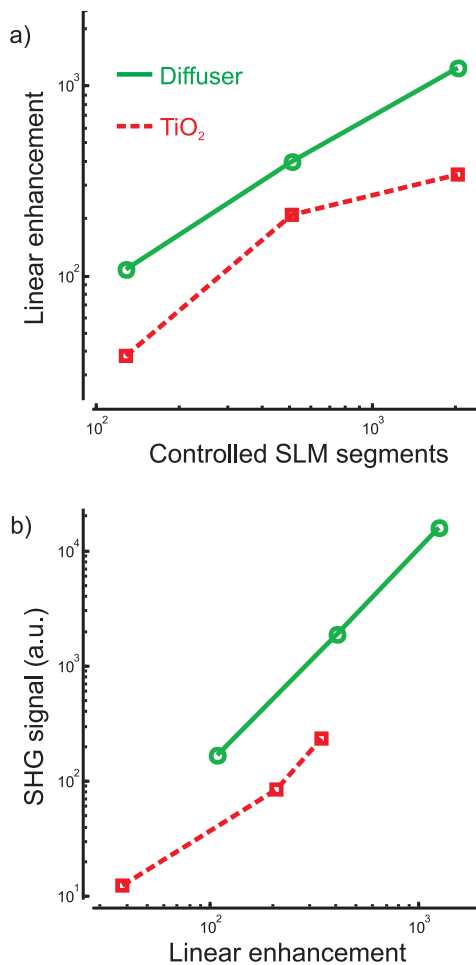


FIG. 4. Linear refocusing and nonlinear efficiencies obtained after linear feedback in two different scattering media, diffuser and 20 μm thick TiO₂ film. a) Linear enhancement obtained as a function of the numbers of SLM segments N_{SLM} . b) SHG signal dependence on the linear enhancement.

Fig. 4 summarizes the imaging enhancement performances evaluated on single nanoKTP crystals, for various N_{SLM} values after two scattering media: a surface diffuser and a multiply scattering medium with a thickness of a few l_t 's. SHG signals are averaged over several nanoKTPs, circumventing the bias due to orientational effects. While the diffuser visibly shows a large spectral bandwidth as compared to the illumination bandwidth, as mentioned above, the 20 μm thickness TiO₂ film exhibits a speckle contrast of 0.59, which departs from this situation. As a consequence, the linear enhancement values (Fig. 4a) are seen to be higher for the diffuser than the TiO₂ film, which is expected

from the less favorable number of accessible spectral modes for the later¹⁵. Under broadband refocusing conditions, the loss in linear enhancement between the two considered media is expected to be about a factor 2 considering the measured speckle contrasts¹⁵, which is close to what is measured here at relatively low number of segments N_{SLM} (high N_{SLM} values are more sensitive to possible artifacts).

Fig. 4b shows nonlinear efficiencies generated after refocusing on nanoKTPs in both scattering media. In order to correct for systematic linear enhancements drifts at high N_{SLM} values, we plot the SHG signal versus the linear focus enhancement. Both media exhibit an almost quadratic dependence of the SHG signal with the linear enhancement, evidencing the capabilities of the linear optimization scheme to preserve the nonlinear coupling quality whatever the number of SLM segments used and spatiotemporal coupling conditions. The signals obtained through TiO_2 are however an order of magnitude lower than for the diffuser. This is visibly a consequence of its lower spectral bandwidth, which is likely to lead to pulse lengthening and thus to lower nonlinear coupling efficiency. SHG signals are nevertheless of high signal to noise ratio and evidence the remarkable capacity of broadband linear refocusing through scattering media to produce efficient nonlinear conversion.

Importantly in the case of the diffuser, the SHG enhancements are the same as obtained in the nonlinear feedback process described above (SHG enhancements could not be quantified for TiO_2 due to the low signal to noise obtained before optimization). This emphasizes that in conditions where medium and laser spectral bandwidth are of similar magnitude, both TM acquisition methodologies lead to efficient spatiotemporal coupling effects, most probably preserving short pulse width after refocusing.

C. Nonlinear bio-imaging behind a scattering medium

We finally apply the linear feedback TM measurement to nonlinear imaging in a biological SHG-active thick sample, made of collagen fibers extracted from rat tail tendons (thickness $120 \mu\text{m}$), a widely studied specimen in SHG microscopy^{30,31}. Fig. 5 shows an SHG image of such sample placed behind a diffuser, acquired after the TM has been measured. To obtain the final SHG image, we first acquired a linear optical image that is used for normalization, allowing correction for possibly remaining spatially non-uniform refocus.

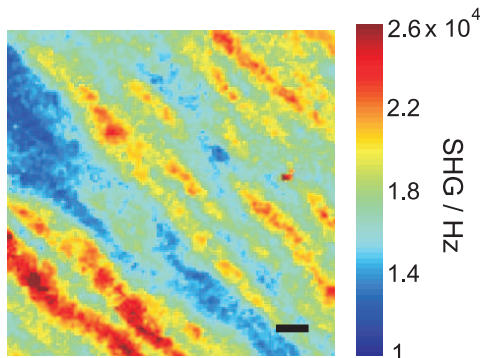


FIG. 5. SHG imaging of rat tail tendon collagen. Scattering medium: diffuser. Number of controlled SLM segments: 2^{10} . Scale bar: $2.3 \mu\text{m}$.

Thick fibers are clearly visible along the diagonal of the image, with a high SHG signal that is clearly above the background signal level. Without WS, a raster-scanning of the focus did not generate a discernible image of the collagen fibers but only a noisy, un-resolved image arising from the speckle excitation. The obtained image is also a remarkable improvement as compared to the use of nonlinear feedback optimization, which gave considerably lower SHG enhancements. This nonlinear sample indeed differ strongly from nanoKTPs since its response is much less sparse: in this regime, the presence of background nonlinear signals from the sample volume and surface is likely to make the nonlinear optimization process biased and much less efficient^{32,33}.

III. DISCUSSION AND CONCLUSIONS

This study shows that the medium spectral correlation width is a key factor for the manipulation of broadband TM in scattering media, as already evidenced in monochromatic regime in multiple scattering media at a few l_t 's^{16,34}. Nevertheless in this regime, and under broadband conditions, both linear and nonlinear feedbacks for acquisition of

the TM lead to considerable nonlinear enhancements. Beyond such depth in anisotropic scattering media such as in biological tissues (*e.g.* $g \sim 0.7-0.99$)³⁵, the fluence is expected to decrease, thus becoming the limiting factor for nonlinear excitation. However, one could forecast the possibility to generate nonlinear signals using higher energy-per-pulse lasers at reduced repetition rate³³.

Our results show that refocusing through a scattering medium using the linear TM can allow faster and more efficient nonlinear imaging. Other advantages of the use of linear feedback can be enlightened. First, nonlinear feedback requires fluorescent^{12,13} or SHG¹¹ active guide stars. Under low signal to noise conditions, the feedback mechanism might thus fail or lead to large optimization times. Conversely, the presence of sparse bright regions in the sample can bias the optimization conditions if a large dynamic range of signals is present in the sample¹³. Second, nonlinear feedback is inherent to the nonlinear mechanism used for the optimization procedure. Spatial and temporal properties of the refocus depend on the size of the nonlinear effective volume, on the nonlinear order (two-, three-photon etc.) of the process used, and on its coherence (SHG versus two photon fluorescence for instance; coherent nonlinear effects indeed involve phase matching conditions that might depend on the object size). Optimization for a given nonlinear process is therefore not necessarily appropriate for other nonlinear processes and samples.

In contrast, we anticipate that a linear feedback in hybrid approaches will enable super penetration of NLM. Considerable advances have been made recently towards the direction of linear refocusing *within* scattering media. In particular, acousto-optic³⁶⁻³⁸ or photoacoustic^{8,39-41} guide stars have been developed to take advantage of the ballistic penetration of acoustic waves in biological tissues. The use of photoacoustic time traces to monitor the TM inside the medium could for instance be advantageously coupled to nonlinear detection, in both backward and forward directions. Furthermore, recent applications of wavefront shaping for optical coherence tomography have demonstrated enhanced penetration depth⁴², with the latter being conveniently coupled with NLM⁴³⁻⁴⁵ thus showing that addressing linear feedback can be considerably more advantageous.

At last, the expected large spectral width of biological media at mm-depth opens interesting prospective for multi-color nonlinear microscopy, such as multi-label fluorescence or coherent Raman (CR) imaging. In CR microscopy if the vibrational resonance lies within the spectral width of the medium, only a single wavelength would be necessary to characterize the TM of the system. Such situation may be found at $0.1 - 0.2 l_t$ depths at which CR microscopy has not yet been able to image^{46,47}. Our observations also suggests that for higher order (>2) processes, *e.g.* three-photon fluorescence, third-harmonic generation or coherent anti-Stokes Raman scattering, enhancements above three orders of magnitude could be generated by using cheaper low resolution SLMs. Because in the present method we are addressing the linearly scattered photons, our conclusions are valid for any nonlinear contrast imaging modality. These results finally pave the way for studies of label-free in-depth imaging in biological media.

IV. METHODS

A. Optical set-up

Short pulses (130 fs, 800 nm, 76 MHz repetition rate, Mira, Coherent) are steered onto a 256x256 pixels reflective SLM (Boulder Nonlinear Systems). The SLM is imaged on the back focal plane of the focusing lens (0.32 NA, achromatic lens, Thorlabs). The scattering medium is placed between the focusing lens and its focus. The nanoKTP crystals (150 nm diameter) are deposited on a coverslip (170 μm), and imaged by an objective (40x, 0.75 NA, Nikon) on a 12-bit CMOS camera (Flea3, Point Grey), and on either an electron multiplying charge coupled device (emCCD, QuantEM, Roper Scientific) for the nonlinear feedback scheme, or on a large area photon counting photomultiplier tube (PMT) for the linear feedback scheme (MP 953, PerkinElmer). The SHG signal is spectrally separated with suitable dichroic mirror (560 nm longpass, AHF Analysentechnik), shortpass (700 nm, FESH0700, Thorlabs) and bandpass (400 ± 10 nm, Chroma Technology) filters.

For both linear and nonlinear feedback based TM acquisition, the wavefront phase of a Hadamard base for the incident field is shifted in respect to a reference field (the region in the periphery of the pattern shown in the SLM) in the range $[0 - 2\pi]$ and the nonlinear/linear intensity is recorded by the emCCD/CMOS cameras, depending on the feedback scheme. After measuring all the Hadamard basis, a Fourier transform is applied on the scan of a single basis thus retrieving the phase of the n th-basis with respect to the reference field. Once all the Hadamard basis are measured, a unitary transformation is applied to obtain the transmission matrix in the canonical basis^{7,18}.

Two different schemes are used for inspection of the signal enhancements depending on the nature of the feedback used for acquiring the TM. In the nonlinear feedback scheme, the wavefront necessary to enhance at a specified position is displayed on the SLM and the nonlinear image taken with the emCCD. In the linear feedback scheme, the retrieved TM contains the information necessary to spatially refocus in the ROI acquired. We then raster-scan the focus using the different elements of the TM at each CMOS pixel within the ROI containing the nanoKTP. In parallel, we collect the SHG signal integrated within the imaged plane by the PMT. A background subtraction was

performed on the SHG images.

B. Samples

Two types of scattering media were used: a commercial diffuser (10° Light Shaping Diffuser, Newport) and a thin TiO₂ film (multiply scattering medium). The TiO₂ film was fabricated by drop cast from a colloidal solution of amorphous 500 nm-diameter TiO₂ plain particles dispersed in water (Corpuscular Inc.). The obtained thickness ($\approx 20 \mu\text{m}$) is expected to be about a few l_t 's^{16,48}. The collagen fibers were extracted from rat tail tendons as in⁴⁹ and placed between two coverlips separated by a 120 μm -thick spacer and filled with agarose solution.

ACKNOWLEDGMENTS

We thank Esben Andressen and Herve Rigneault for initial tests in their setup and fruitful discussions, Ori Katz for technical assistance, Thierry Gacoin and Ludovic Meyer for providing the nanoKTP particles, and Yannick Foucault for characterizing the TiO₂ films. H.B.A. thanks the FEMTO network of Mission pour l'Interdisciplinarité (CNRS, France) for its financial support. This work has been supported by Agence Nationale de la Recherche through contracts ANR-10-INBS-04-01 (France-BioImaging infrastructure network), ANR-11-INSB-0006 (France Life Imaging infrastructure network), ANR-15-CE19-0018-01 (MyDeepCARS), by the A*MIDEX project (ANR-11-IDEX-0001-02), and by the European Research Council (grant no. 278025).

-
- * h.aguiar@fresnel.fr
† sophie.brasselet@fresnel.fr
- ¹ D. Débarre, E. J. Botcherby, T. Watanabe, S. Srinivas, M. J. Booth, and T. Wilson, "Image-based adaptive optics for two-photon microscopy," *Opt. Lett.* **34**, 2495–2497 (2009).
 - ² J. Tang, R. N. Germain, and M. Cui, "Superpenetration optical microscopy by iterative multiphoton adaptive compensation technique," *Proc. Natl. Acad. Sci. U. S. A.* **109**, 8434–8439 (2012).
 - ³ C. Wang, R. Liu, D. E. Milkie, W. Sun, Z. Tan, A. Kerlin, T.-W. Chen, D. S. Kim, and N. Ji, "Multiplexed aberration measurement for deep tissue imaging in vivo," *Nat. Methods* **11**, 1037–1040 (2014).
 - ⁴ D. Sinefeld, H. P. Paudel, D. G. Ouzounov, T. G. Bifano, and C. Xu, "Adaptive optics in multiphoton microscopy: comparison of two, three and four photon fluorescence," *Opt. Express* **23**, 31472–31483 (2015).
 - ⁵ A. P. Mosk, A. Lagendijk, G. Lerosey, and M. Fink, "Controlling waves in space and time for imaging and focusing in complex media," *Nature Photon.* **6**, 283–292 (2012).
 - ⁶ I. M. Vellekoop and A. P. Mosk, "Focusing coherent light through opaque strongly scattering media," *Opt. Lett.* **32**, 2309–2311 (2007).
 - ⁷ S. M. Popoff, G. Lerosey, R. Carminati, M. Fink, A. C. Boccarda, and S. Gigan, "Measuring the transmission matrix in optics: An approach to the study and control of light propagation in disordered media," *Phys. Rev. Lett.* **104**, 100601 (2010).
 - ⁸ T. Chaigne, O. Katz, A. Boccarda, M. Fink, E. Bossy, and S. Gigan, "Controlling light in scattering media non-invasively using the photoacoustic transmission matrix," *Nature Photon.* **8**, 58–64 (2013).
 - ⁹ D. Akbulut, T. Huisman, E. van Putten, W. Vos, and A. P. Mosk, "Focusing light through random photonic media by binary amplitude modulation," *Opt. Express* **19**, 4017 – 4029 (2011).
 - ¹⁰ D. B. Conkey, A. M. Caravaca-Aguirre, and R. Piestun, "High-speed scattering medium characterization with application to focusing light through turbid media," *Opt. Express* **20**, 1733–1740 (2012).
 - ¹¹ J. Aulbach, B. Gjonaj, P. Johnson, and A. Lagendijk, "Spatiotemporal focusing in opaque scattering media by wave front shaping with nonlinear feedback," *Opt. Express* **20**, 29237–29251 (2012).
 - ¹² O. Katz, E. Small, Y. Bromberg, and Y. Silberberg, "Focusing and compression of ultrashort pulses through scattering media," *Nature Photon.* **5**, 372–377 (2011).
 - ¹³ O. Katz, E. Small, Y. Guan, and Y. Silberberg, "Noninvasive nonlinear focusing and imaging through strongly scattering turbid layers," *Optica* **1**, 170–174 (2014).
 - ¹⁴ I. M. Vellekoop, "Feedback-based wavefront shaping," *Opt. Express* **23**, 12189–12206 (2015).
 - ¹⁵ H. P. Paudel, C. Stockbridge, J. Mertz, and T. Bifano, "Focusing polychromatic light through strongly scattering media," *Opt. Express* **21**, 17299–17308 (2013).
 - ¹⁶ D. Andreoli, G. Volpe, S. Popoff, O. Katz, S. Gresillon, and S. Gigan, "Deterministic control of broadband light through a multiply scattering medium via the multispectral transmission matrix," *Sci. Rep.* **5**, 10347 (2015).
 - ¹⁷ O. Katz, P. Heidmann, M. Fink, and S. Gigan, "Non-invasive single-shot imaging through scattering layers and around corners via speckle correlations," *Nature Photon.* **8**, 784–790 (2014).

- ¹⁸ S. M. Popoff, G. Lerosey, M. Fink, A. C. Boccara, and S. Gigan, “Controlling light through optical disordered media: transmission matrix approach,” *New J. Phys.* **13**, 123021 (2011).
- ¹⁹ L. Le Xuan, C. Zhou, A. Slablab, D. Chauvat, C. Tard, S. Perruchas, T. Gacoin, P. Villeval, and J.-F. Roch, “Photostable second-harmonic generation from a single ktiopo4 nanocrystal for nonlinear microscopy,” *Small* **4**, 1332–1336 (2008).
- ²⁰ I. M. Vellekoop, E. G. van Putten, A. Lagendijk, and A. P. Mosk, “Demixing light paths inside disordered metamaterials,” *Opt. Express* **16**, 67–80 (2008).
- ²¹ N. Curry, P. Bondareff, M. Leclercq, N. F. van Hulst, R. Sapienza, S. Gigan, and S. Grésillon, “Direct determination of diffusion properties of random media from speckle contrast,” *Opt. Lett.* **36**, 3332–3334 (2011).
- ²² I. M. Vellekoop and C. M. Aegerter, “Scattered light fluorescence microscopy: imaging through turbid layers,” *Opt. Lett.* **35**, 1245–1247 (2010).
- ²³ G. Ghielmetti and C. M. Aegerter, “Direct imaging of fluorescent structures behind turbid layers,” *Opt. Express* **22**, 1981–1989 (2014).
- ²⁴ S. Schott, J. Bertolotti, J.-F. L. ger, L. Bourdieu, and S. Gigan, “Characterization of the angular memory effect of scattered light in biological tissues,” *Opt. Express* **23**, 13505–13516 (2015).
- ²⁵ D. Bicot, C. Brosseau, A. S. Martinez, and J. M. Schmitt, “Depolarization of multiply scattered waves by spherical diffusers: Influence of the size parameter,” *Phys. Rev. E* **49**, 1767–1770 (1994).
- ²⁶ M. Xu and R. R. Alfano, “Random walk of polarized light in turbid media,” *Phys. Rev. Lett.* **95**, 213901 (2005).
- ²⁷ N. Ghosh, H. Patel, and P. Gupta, “Depolarization of light in tissue phantoms - effect of a distribution in the size of scatterers,” *Opt. Express* **11**, 2198–2205 (2003).
- ²⁸ H. B. de Aguiar, P. Gasecka, and S. Brasselet, “Quantitative analysis of light scattering in polarization-resolved nonlinear microscopy,” *Opt. Express* **23**, 8960–8973 (2015).
- ²⁹ H. B. de Aguiar, S. Gigan, and S. Brasselet, “Polarization-resolved microscopy through scattering media via wavefront shaping,” arXiv:1511.02347 (2015).
- ³⁰ S. Roth and I. Freund, “Second harmonic generation in collagen,” *J. Chem. Phys.* **70**, 1637–1643 (1979).
- ³¹ S. Bancelin, C. Aimé, I. Gusachenko, L. Kowalczuk, G. Latour, T. Coradin, and M.-C. Schanne-Klein, “Determination of collagen fibril size via absolute measurements of second-harmonic generation signals,” *Nat. Commun.* **5** (2014).
- ³² P. Theer and W. Denk, “On the fundamental imaging-depth limit in two-photon microscopy,” *J. Opt. Soc. Am. A* **23**, 3139–3149 (2006).
- ³³ N. G. Horton, K. Wang, D. Kobat, C. G. Clark, F. W. Wise, C. B. Schaffer, and C. Xu, “In vivo three-photon microscopy of subcortical structures within an intact mouse brain,” *Nature Photon.* **7**, 205–209 (2013).
- ³⁴ O. L. Muskens and A. Lagendijk, “Broadband enhanced backscattering spectroscopy of strongly scattering media,” *Opt. Express* **16**, 1222–1231 (2008).
- ³⁵ W. Cheong, S. Prah, and A. Welch, “A review of the optical-properties of biological tissues,” *IEEE J Quantum Elect* **26**, 2166–2185 (1990).
- ³⁶ X. Xu, H. Liu, and L. V. Wang, “Time-reversed ultrasonically encoded optical focusing into scattering media,” *Nature Photon.* **5**, 154–157 (2011).
- ³⁷ Y. M. Wang, B. Judkewitz, C. A. DiMarzio, and C. Yang, “Deep-tissue focal fluorescence imaging with digitally time-reversed ultrasound-encoded light,” *Nat. Commun.* **3**, 928 (2012).
- ³⁸ B. Judkewitz, Y. M. Wang, R. Horstmeyer, A. Mathy, and C. Yang, “Speckle-scale focusing in the diffusive regime with time reversal of variance-encoded light (trove),” *Nature Photon.* **7**, 300–305 (2013).
- ³⁹ F. Kong, R. H. Silverman, L. Liu, P. V. Chitnis, K. K. Lee, and Y.-C. Chen, “Photoacoustic-guided convergence of light through optically diffusive media,” *Optics letters* **36**, 2053–2055 (2011).
- ⁴⁰ D. B. Conkey, A. M. Caravaca-Aguirre, J. D. Dove, H. Ju, T. W. Murray, and R. Piestun, “Super-resolution photoacoustic imaging through a scattering wall,” *Nat. Commun.* **6**, 7902 (2015).
- ⁴¹ P. Lai, L. Wang, J. W. Tay, and L. V. Wang, “Photoacoustically guided wavefront shaping for enhanced optical focusing in scattering media,” *Nature Photon.* (2015).
- ⁴² J. Jang, J. Lim, H. Yu, H. Choi, J. Ha, J.-H. Park, W.-Y. Oh, W. Jang, S. Lee, and Y. Park, “Complex wavefront shaping for optimal depth-selective focusing in optical coherence tomography,” *Opt. Express* **21**, 2890–2902 (2013).
- ⁴³ E. Beaurepaire, L. Moreaux, F. Amblard, and J. Mertz, “Combined scanning optical coherence and two-photon-excited fluorescence microscopy,” *Opt. Lett.* **24**, 969–971 (1999).
- ⁴⁴ J. S. Bredfeldt, C. Vinegoni, D. L. Marks, and S. A. Boppart, “Molecularly sensitive optical coherence tomography,” *Opt. Lett.* **30**, 495–497 (2005).
- ⁴⁵ T. Kamali, B. Považay, S. Kumar, Y. Silberberg, B. Hermann, R. Werkmeister, W. Drexler, and A. Unterhuber, “Hybrid single-source online fourier transform coherent anti-stokes raman scattering/optical coherence tomography,” *Optics letters* **39**, 5709–5712 (2014).
- ⁴⁶ A. J. Wright, S. P. Poland, J. M. Girkin, C. W. Freudiger, C. L. Evans, and X. S. Xie, “Adaptive optics for enhanced signal in cars microscopy,” *Opt. Express* **15**, 18209–18219 (2007).
- ⁴⁷ V. Ntziachristos, “Going deeper than microscopy: the optical imaging frontier in biology,” *Nat. Methods* **7**, 603–614 (2010).
- ⁴⁸ J. Aulbach, B. Gjonaj, P. M. Johnson, A. P. Mosk, and A. Lagendijk, “Control of light transmission through opaque scattering media in space and time,” *Phys. Rev. Lett.* **106**, 103901 (2011).
- ⁴⁹ D. Ait-Belkacem, A. Gasecka, F. Munhoz, S. Brustlein, and S. Brasselet, “Influence of birefringence on polarization resolved nonlinear microscopy and collagen shg structural imaging,” *Opt. Express* **18**, 14859–14870 (2010).