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# Propagation of epileptic spikes revealed by diffusion-based constrained MEG source reconstruction

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**Goal: Study of the propagation of an epileptic spike.**

**Method: 1- cortex parcellation via structural information coming from diffusion MRI (dMRI)**

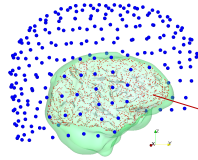
**2- MEG inverse problem on a parcellated source space**

**3- study of the propagation of an epileptic spike via the active parcels**

**Results on real data allowing to study the spatial propagation of an epileptic spike.**

## 1 Preprocessing

- 1- Co-registration of the T1wMRI and dMRI  
[soft FSL]
- 2- Surface meshes extraction  
[soft Freesurfer]
- 3- Computation of the leadfield matrix G  
[soft OpenMEEG]



Each vertex of the WM/GM boundary mesh is:

- Source of a magnetic field
- Seed for tractography

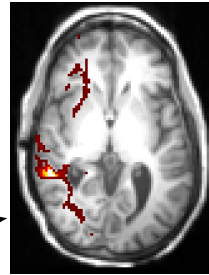
## 2 dMRI-based cortex parcellation

**Connectivity profile of a source CP:**

CP(i) = connectivity value between the source and the ith voxel.

- 4- For each source:  
Computation of its connectivity image.

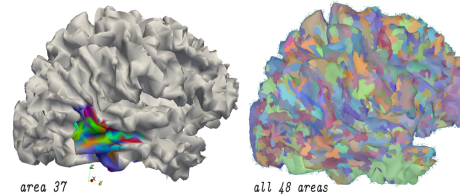
Tool: Probtrackx  
[soft FSL]



## 5- Pre-clustering via Brodmann's atlas

For each Brodmann area, clustering of sources having a close connectivity to all sources:

- 5.1- Computation of the CP-based correlation matrix R [5]
- 5.2- K-means algorithm on R



## 3 MEG inverse problem with parcellated source space

We reduce the initial distributed source space S into s in accordance with the cortex parcellation:

$$S = P \times s \text{ with } P(i, j) = \begin{cases} 1, & \text{if source } i \text{ is in area } j \\ 0, & \text{if not} \end{cases}$$

and compute the reduced leadfield  $G_P$  for the parcellated source space s:  $G_P = G \times P$

Thus, the MEG inverse problem on the parcellated source space using Tikhonov regularization becomes :

$$\min_s \| M - G_P s \|^2 + \lambda \| s \|^2$$

where M contains the MEG measurements.

## 4 Study of the propagation of an epileptic spike

At each time sample, we want to determine the cortical areas at the origin of the activity. We call  $\mathcal{S}_t$  the set of these areas, for a time sample t

For each time sample t, we compute the power  $\mathcal{P}_{p,t}$  of each area p on a sliding time window  $[t - \alpha, t + \alpha]$ :

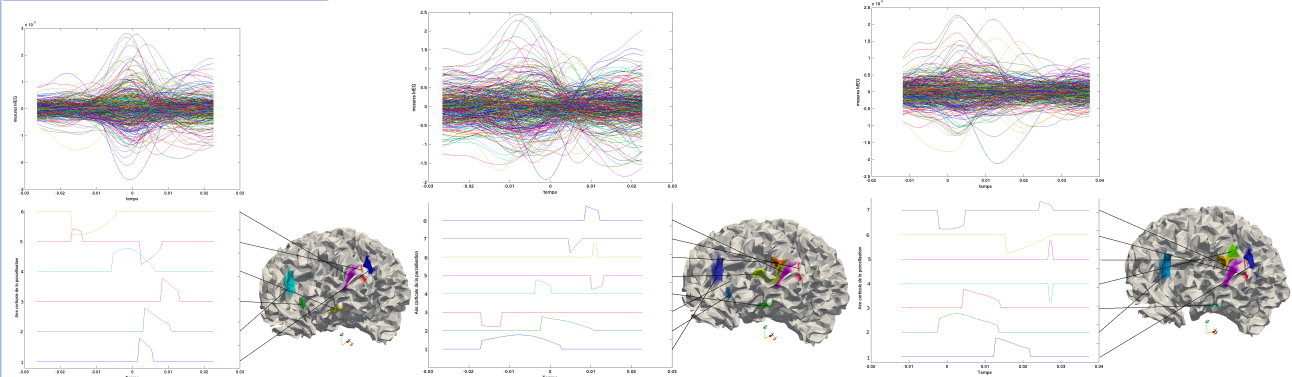
$$\mathcal{P}_{p,t} = \sum_{i=t-\alpha}^{t+\alpha} |s(p,i)|^2$$

$$\mathcal{S}_t = \{p_a : \mathcal{P}_{p_a,t} > F * \max(\mathcal{P}_{p,t}), \forall p\}$$

with F a pourcentage.

## 5 Results & Conclusion

**Results on 3 epileptic spikes of a single subject.**



- Almost the same parcels are activated for all epileptic spikes.
- The direction of propagation changes: from the back of the frontal lobe to the front or opposite direction.
- The time of activation of each parcel characterizes the spike.

- The parcellation allows an easier representation of source space.
- The method reveals differences between spikes (direction of propagation and time of activation of parcels).
- Future works will be to analyse the structural network supporting the propagation.

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