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NMR signal acquisition in the Doubly Tilted Rotating Frame

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Target audience

The work presented here is intended for NMR physicists. It presents some new concepts which could enable in vivo solid state NMR spectroscopy and imaging. **Purpose**

The main effect of dipolar interaction is to destroy the macroscopic NMR signal and prevent solid state NMR/MRI. In this work we propose to acquire the magnetization of a sample in the Doubly Tilted Rotating Frame (DTRF), which enables the averaging of dipolar interactions without any physical rotation. Our objective is to open the way to a new class of solid state NMR experiments which could be used *in vivo*.



Methods

In 1955 Redfield demonstrate that dipolar interaction а averaging effect can occur while the sample is subject to a RF irradiation [1]. « strona » Numerous work has been achieved along this path with the development techniques of relying on irradiation periods followed by signal acquisition periods [2-4]. One drawback of these techniques is that a strong RF has to be periodically switched on and off on a usecond scale. Instead of placing the system in the DTRF then putting it back periodically to the

Fig 2: Temporal signal acquired on a PVA sample putting it back periodically to the before, during and after an on-resonant RF irradiation aboratory frame for the signal of 5.8µT acquisition, we have chosen to

keep it in the DTRF during the whole process [5] (Fig.1). Acquiring the signal during a strong RF irradiation is challenging. It require a strong decoupling between the emission and reception coils. Furthermore, to avoid saturation of the ADC converter, in this preliminary experiments, the preamplifier of the MRI system was bypassed, thus limiting the dynamic of the signal of interest.

Results

Using a purely geometrical decoupling technique we were able to achieve an Emission-Reception decoupling above 30dB. On our 4.7T Bruker AVANCE1 Biospec hardware, without saturating the ADC dynamic. This decoupling was good enough to allow signal acquisition during an RF irradiation up to 23μ T. A signal of 8k complex points was acquired during 409.6ms on a polyvinyl-alcohol (PVA) gel during and after an on-resonance RF of 5.8μ T (Fig.2). We also acquired under similar conditions a signal from a 50% water/ethanol mix (Fig.3).

Discussion

Figure 2 shows that the signal exhibit a DTRF free induction signal (DTRF-FID) and

we demonstrated that while the T_2 of the PVA sample used was 2±1ms in the laboratory frame, it was extended to 23±6ms in the DTRF. Fig 3 shows that it is possible to accurately achieve an MRS experiment in the DTRF. Still, to compare the spectra acquired in the laboratory frame and DTRF, we had to preprocess the DTRF-FID to remove the residual baseline emission signal clearly seen as an offset in Fig 2. **Conclusion**

It is possible to acquire a NMR signal during an RF irradiation. The chemical shift properties of the sample are kept in the DTRF and the T_2 range of the sample in the laboratory and DTR frames clearly shows that even using a small RF amplitude of just 5.8µT, we can achieve a 10-fold increase of signal life. These two points demonstrates the potential of this technique that could be further extended for short T_2 tissues investigation.

References

[1] Redfield AG, Nuclear magnetic resonance saturation and rotary saturation in solids, Phys. Rev. 98(1955) 1787-1809.

[2] Lee M, Goldburg WI. Nuclear-magnetic-resonance line narrowing by a rotating RF field. Phys. Rev. A, 140 (1965), p. 1261.

[3] Matsui S et al, Improved Resolution in Solid-State NMR Imaging by Self-Phase Encoding, J. Magn. Reson., 112(1995) 130-133.

[4] Grenier D et al, Dipolar contrast for dense tissues imaging, J. Magn. Reson., 147(2000) 353-356.

[5] Grenier D, Saint-Jalmes H. Patent, PCT EP2011/071960, (December 6, 2011).

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Fig 1: Principle of a dipolar-free signal acquisition in the DTRF



Fig 3: Ethanol spectra obtained from: (a) a classical FID ; (b) a postprocessed DTRF-FID