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Determining the count median diameter of nanoaerosols by simultaneously measuring their number and lung deposited surface area concentrations

Brief communication

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Abstract

Due to the increasing use of nanomaterials in research and product development, it is probable that the number of situations of occupational exposure to them is also rising. The same is true for the number of workers. Although current research in nanotoxicology is far from conclusive, it is clear that relying on mass concentration and chemical composition alone is not appropriate in all cases and alternative measurement methods and approaches need to be developed.

In this work, we propose a method based on simultaneous size-integrated measurements of two particle concentrations (number and lung-deposited surface area, CNC/NSAM), and on the estimation of the average size of potentially inhaled particles from the combination of these measurements. The proposed method could be part of a measurement strategy that is practical as it would use field-portable, commercially available aerosol instruments. In the absence of instruments providing real-time size-resolved measurements, this original approach can be carried out as considering that the ratio of these concentrations is a monotonous function of particle size. Indeed, the latter function depends only on the geometric standard deviation of airborne particle number size distribution, assumed to be lognormal.

Compared to SMPS data for polydisperse aerosols having three chemical natures with count median diameters ranging from 64 to 177 nm, experimental results were obtained with acceptable relative discrepancies of $\pm 30\%$. Though the method proposed is less accurate than traditional instruments like SMPS, it can be used for workplace air monitoring or as a screening tool to detect the presence of airborne nanoparticles.

Introduction

Although nanomaterials are used increasingly in various fields such as energy, health, cosmetics, materials etc, uncertainties remain regarding their potential health effects. In parallel, the number of occupational inhalation exposure situations is probably rising, leading to the recent proposal of generic strategies for assessing workplace exposure to airborne nanomaterials (e.g. Brouwer *et al.*, 2009; Methner *et al.*, 2010; Ramachandran *et al.*, 2011; Witschger *et al.*, 2012). In addition to chemical composition, these strategies indicate that a variety of parameters is required to characterize exposure to airborne nanomaterials. Among them, particle concentration and size play an important role (e.g. Wang *et al.*, 2011), since they provide information on the quantity and the region of the respiratory tract where inhaled nanoparticles will be deposited and potentially interact.

Although the choice of the metric (number, surface area, mass concentrations) to use is still being debated, investigations into the performances of real-time instruments measuring airborne particle concentrations have risen. Indeed, there is a constant need to increase knowledge on the behavior of instruments used to measure submicron aerosols in both laboratory studies and in workplace environments.

Particle size measurement is a more complex issue.

The gold standard technique employed to determine both overall (agglomerate/aggregate) and primary particle sizes is electron microscopy (EM). Obtaining and analyzing sufficient images in order to have a statistically significant analysis (Mavrocordatos *et al.*, 2007) is not only time consuming, but the duration of sampling and sampling device efficiency must be defined with great care to provide appropriate samples. Furthermore, EM is not time-resolved, which does not allow nanoaerosol source identification or defining the emission levels of specific tasks in workplaces.

The real-time measurement of airborne nanoparticle size distribution can be performed by electrical mobility analyzers (e.g. Scanning Mobility Particle Sizer – SMPS, Fast Mobility Particle Sizer – FMPS), or, to a lesser extent, by low pressure cascade impactors (e.g. Electrical Low Pressure Impactor – ELPI) that provide less size resolution. Due to their measurement principle, SMPSs commonly require radioactive sources to set the particles in a given electrical state-of-charge. Regulations relating to the detention and transport of radioactive sources in certain countries, associated with the cost of these devices, are among the reasons for their limited use in occupational hygiene. Furthermore, according to Leskinen *et al.* (2012), such devices are not ideally suited for monitoring air in the workplace due to their low time resolution. Also, they are not easy-

to-use for novices. Although recent systems (soft X-ray charger, TSI model 3087; annular Dielectric Barrier Discharge, Grimm model 5520) have been designed to avoid the use of radioactive sources, little is known about the performances of these neutralizers. In particular, the maximum concentration limit and particle losses within these devices must be documented, as must be the electrical state-of-charge of the particles described in Kallinger *et al.* (2012). Intensive studies of real-time instruments devoted to the measurement of airborne particle number size distribution (SMPS, FMPS) have been carried out recently (Asbach *et al.*, 2009b; Watson *et al.*, 2011; Joshi *et al.*, 2012; Meier *et al.*, 2012; Kaminski *et al.*, 2013). Their findings highlight acceptable discrepancies between devices that can be attributed to differences in inversion algorithm, multiple charge correction, software versions, and flow rate calibration.

Several portable devices based on particle diffusion charging and sequential electrical measurement have been developed to provide airborne nanoparticle concentration and average size with higher time resolution (< 10 seconds) simultaneously. Examples of such devices are DiSCmini (Matter Aerosol; Fierz *et al.*, 2011; Mills *et al.*, 2013), Nanotracer (Philips Aerasense, discontinued; Marra *et al.*, 2010), and nanoCheck (Grimm model 1.320).

In the absence of size-selective instruments, another approach to determine particle size is based on the simultaneous measurement of size-integrated particle concentrations (number, mass, current). Indeed, measured concentrations can also be used to determine airborne particle number size distribution. Among the key parameters governing such optimization algorithms, the shape of distribution is assumed to be lognormal with a fixed geometric standard deviation.

Although several authors (e.g. Woo *et al.*, 2001; Maynard, 2003; Park *et al.*, 2007a, 2007b; Park *et al.*, 2009, 2011) have applied such methodologies to determine the surface area concentration of airborne nanoparticles, none of them has focused on the possibility of estimating the count median diameter of the aerosols and its reliability against reference data.

In this context, the present study aims at providing new results for estimating the count median diameter of airborne nanoparticles from the simultaneous measurement of the number (CPC, Grimm model 5.403) and lung-deposited surface area (NSAM, TSI model 3550) concentrations. The results were compared to SMPS data for a set of polydisperse test aerosols having three different chemical natures with count median diameters ranging from 64 nm to 177 nm.

Materials and methods

Theoretical background: deriving the count median diameter from the measurement of number and lung-deposited surface area concentrations

The instruments devoted to the measurement of airborne particle surface area concentration do not refer to the geometric surface area of the particles (Bau *et al.*, 2012). More precisely, the lung-deposited surface area concentration, noted $C_{S,LD}$, corresponds to the product of the geometric surface area concentration ($C_N \cdot \pi \cdot d_{\bar{s}}^2$ with C_N the particle number concentration) and the probability (η_{LD}) of a particle to deposit in a given region of the respiratory apparatus:

$$C_{S,LD} = C_N \cdot \eta_{LD} \cdot \pi \cdot d_{\bar{s}}^2 \quad (1)$$

The latter deposition probabilities can be obtained from models based on experimental data (ICRP, 1994; NCRP, 1997), or from fitted simplified equations (Hinds, 1999).

Determining the diameter of average geometric surface area ($d_{\bar{s}}$) from the last equation is complex because particle deposition probability is size-dependent, and requires the surface area per particle of given size (response function, i.e. $C_{S,LD}/C_N$) to be taken into account (Ntziachristos *et al.*, 2007). Furthermore, this function has to be monotonous with particle size to avoid multiple mathematical solutions. This was demonstrated in a previous work (Bau *et al.*, 2012).

Assuming that the airborne particle number is distributed according to a lognormal law with given geometric standard deviation (GSD), the diameter of average geometric surface area can be used to calculate the corresponding count median diameter (CMD) by implementing the following equation (Hatch and Choate, 1929):

$$d_{\bar{s}} = CMD \cdot \exp(\ln^2 GSD) \quad (2)$$

It results from equations 1 and 2 that measuring in parallel the size-integrated number and lung-deposited surface area concentrations of airborne particles allows determining their count median diameter (CMD).

We performed theoretical calculations based on the response function obtained for lognormal-distributed aerosols with a GSD varying from 1.03 to 2.5 in order to provide a panel of curves allowing a wide range of possible GSDs, as shown in Figures 1 and 2. To obtain these graphs, spherical particles with unit densities were assumed in the deposition

model from ICRP. Furthermore, aerosol size distributions were supposed to be mono-modal.

The curves provide the evolution of the ratio $C_{S,LD}/C_N$ with the GSD of an aerosol with a given CMD indicated on the right side of each curve. In other words, these graphs allow determining the CMD of an aerosol when the ratio of its lung-deposited surface area to number concentration is measured and the GSD is known (or assumed). We believe these graphs are useful for NSAM users because this approach allows both estimating and monitoring the particle count median diameter in real-time.

Figures 1 and 2

More practically, the methodology proposed in this paper relies on to the following procedure:

- 1) Measure in parallel the number (C_N) and lung-deposited surface area ($C_{S,LD}$) concentrations,
- 2) Calculate the ratio $C_{S,LD}/C_N$ from experimental data,
- 3) Assume / Set the GSD of the particle size distribution,
- 4) Read the corresponding CMD from Figure 1 or 2 depending on the region of the respiratory apparatus considered.

Figures 1 and 2 show that the GSD of the distribution starts affecting the theoretical response function beyond 1.4. Furthermore, for a given concentration ratio (response), increasing the GSD of the aerosol leads to a decrease in particle count median diameter. For example, monodisperse 100 nm particles will present the same response as a polydisperse aerosol with a modal diameter of 80 nm and a GSD of 1.8. Although the number size distributions are very different, the corresponding lung-deposited surface areas are similar due to the shift in the lung-deposited surface area distribution. Indeed, the latter varied with particle size according to a power law with exponent between 1.5 and 1.3 in a range from 10 nm to 700 nm for alveolar and tracheobronchial deposition, respectively.

Generation, measurement setup and characterization of the test aerosols

The accuracy of the approach was evaluated by comparing the CMD derived from measured concentrations with a reference diameter. Experiments were carried out with

test aerosols produced by the CAIMAN (Characterisation of Aerosol Instrumentation used to Measure the Aerosols of Nanoparticles) facility, based on a spark discharge generator (PALAS GFG-1000). The elements composing this test bench and its capacity to produce nanoaerosols were described by Jacoby *et al.* (2011).

Three different electrodes were used in this work: carbon (graphite, pure), aluminium (93.11% pure), and silver (99.99% pure). The aerosols produced were then measured simultaneously by a Scanning Mobility Particle Sizer (SMPS) and a Nanoparticle Surface Area Monitor (NSAM).

The SMPS is composed of a Differential Mobility Analyzer (DMA, Grimm Vienna Type, $Q_{\text{aerosol}} = 0.3 \text{ L}\cdot\text{min}^{-1}$, $Q_{\text{sheath}} = 3 \text{ L}\cdot\text{min}^{-1}$) equipped with an Am^{241} radioactive source and a Condensation Nucleus Counter (CNC, Grimm model 5.403, $Q = 0.3 \text{ L}\cdot\text{min}^{-1}$) placed in series to provide particle number size distributions and total number concentration (by integrating the number size distribution in all the measurement channels of the SMPS). The NSAM (TSI model 3550, $Q = 2.5 \text{ L}\cdot\text{min}^{-1}$, see e.g. Fissan *et al.*, 2007; Shin *et al.*, 2007) provides particle lung-deposited surface area concentration in either the alveolar ('alv') or the tracheobronchial ('tb') region of the respiratory apparatus. Detailed information regarding the performances of the NSAM can be found in Asbach *et al.* (2009a) and Bau *et al.* (2009, 2011, 2012).

For the measurement of number concentrations in workplace environments, the use of a CNC is recommended due to its time resolution and higher portability. In our experiments, number and lung-deposited surface area concentrations measured were used to calculate the CMD of the aerosol according to the abovementioned procedure. Since both 'alv'- and 'tb'- deposited surface area concentrations were measured for each test aerosol, two CMDs were determined. This allows concluding whether 'alv'- or 'tb'-based CMDs are similar.

The number size distributions of the nanoaerosols produced were measured by the SMPS that provided the reference count median mobility diameters (CMMD). Each experimental condition was kept for 30 to 40 minutes to ensure aerosol stability and a sufficient number of scans for the determination of the average number size distribution by the SMPS. Indeed, each scan requires between 4 and 5 minutes (depending on the range of diameters covered). In the case of C- and Al-based aerosols, the number size distributions were corrected for variations in agglomerate charging efficiency, in line with Lall & Friedlander (2006). The primary particle diameters used for this calculation are equal to 16 nm for both elements, as indicated in Bau *et al.* (2012).

In addition to Henry's diagrams, chi-square statistical tests were performed on each of the number size distributions; the results highlight lognormal distributions ($P < 0.001$) for all the cases of this study. For the different configurations tested, the CMMD of the polydisperse aerosols ranged from 64 nm to 177 nm (GSD from 1.45 to 1.53), and number concentrations ranged between 10^4 cm^{-3} and $15 \cdot 10^4 \text{ cm}^{-3}$, as indicated in Table 1.

Table 1

Results and discussion

Experimental results

To experimentally validate the approach proposed in this paper, the count median diameters derived from the ratio of lung-deposited surface area to number concentrations were compared with the count median mobility diameters obtained from SMPS measurements. Calculations were performed successively with the input of the true GSD stemming from SMPS (Figure 3a) and with a GSD set at 1.80 (Figure 3b) in agreement with different authors (Harris and Maricq, 2001; Maynard, 2003; Park *et al.*, 2009). Additional elements relating to typical range of aerosol GSDs are provided in John (2001). Table 2 gathers measured and calculated data for a selected case (experimental condition #13 in Table 1).

Figure 3

Table 2

Figure 3 illustrates the existence of a good correlation between count median diameters for the case of known GSDs as well as for the case of a GSD fixed at 1.8. Linear regressions carried out on the different data series present slopes between 0.94 and 1.12, associated with correlation coefficients above 0.90. These findings indicate the possibility of estimating the diameter of a polydisperse aerosol from the simultaneous measurement of its lung-deposited surface area concentration and number concentration to within $\pm 30\%$. This range is in agreement with the technical specifications given for example for the DiSCmini (MatterAerosol) mentioned in the introduction.

Discussion and limits of the method

For each GSD considered, the CMD stemming from 'alv'- and 'tb'-lung-deposited surface area were compared. Statistical analysis of the bias between CMD and reference CMMD is provided in Figure 4 as a Box & Whiskers Plot. This type of graph describes the distribution of data within a population. The box surrounds the median value for the population, with limits at the first and third quartiles, while the error bars correspond to the 95% confidence interval.

Figure 4

Figure 4 confirms that CMDs correlate with the reference CMMDs within $\pm 30\%$ (only 2 data points among 80 were found beyond this interval for NSAM in ‘alv’ configuration with true GSD). It can be observed from Figure 4 that the NSAM configuration (‘alv’- or ‘tb’-lung-deposited surface area concentration) does not influence the value of the corresponding CMD, although less deposition in tb configuration. The input GSD seems to be more influential, though no statistical evidence was demonstrated. As shown in Figure 4, the relative biases are lower (median bias closer to 0%) for the case where GSD is set to 1.8.

Although it was assumed that particles are spherical with unit density, no significant effect of particle composition can be highlighted, as stated earlier concerning the response functions of the NSAM in both configurations (Bau *et al.*, 2012).

Also, it was observed that the total number concentration of the polydisperse test aerosols does not influence the diameter derived from average active or lung-deposited surface area. This point is in agreement with a previous study (Bau *et al.*, 2012), where similar relative number size distributions with total number concentrations varying by a factor of 3 led to a factor close to 3 in the NSAM responses in both configurations ($\pm 10\%$).

Finally, it should be mentioned that the accuracy of the method depends on (1) the order of magnitude of the concentrations measured and (2) the associated uncertainty.

More precisely, the limit of detection (LOD) of the NSAM measured with HEPA-filtered air was found to be $0.1 \mu\text{m}^2.\text{cm}^{-3}$. Considering a number concentration of 10^3 cm^{-3} , the methodology thus becomes applicable as soon as particles are larger than 8 nm and 12 nm for the ‘alv’ and ‘tb’ regions, respectively.

In addition, 10% uncertainty on the concentrations ratio roughly leads to 8% uncertainty on the derived CMD, whatever the configuration of the NSAM (‘alv’ or ‘tb’).

Concerning the upper size limit, theoretical calculations indicate that the response functions ($C_{S,LD}/C_N$) for polydisperse aerosols are no longer monotonous when their CMD reaches roughly 350 nm and 325 nm for the ‘alv’ and ‘tb’ regions, respectively. In the absence of experimental data beyond 180 nm, it can be considered that the method is applicable in a range of sizes from 20 nm to 200 nm.

Conclusion

In the absence of real-time size-resolved instruments, measuring an aerosol in parallel with size-integrated devices can be considered to estimate its average size. Although less accurate than traditional instruments like SMPS, this approach can be useful for workplace air monitoring. Furthermore, it could be used as a screening tool to detect the presence of airborne nanoparticles (without distinction from the background aerosol).

In this work, particle lung-deposited surface area and number concentrations (CNC / NSAM) of airborne nanoparticles were used to determine their count median diameter, based on theoretical calculations for monomodal lognormal aerosols. It can be concluded from the experimental results obtained for 20 polydisperse aerosols, that the approach proposed is valid, whatever the NSAM configuration (alveolar or tracheobronchial lung deposition) and the GSD considered in the calculation. The count median diameters stemming from the calculations show acceptable relative discrepancies of $\pm 30\%$ with a reference diameter obtained by SMPS measurements.

The main limitation of the method lies in the assumption of monomodal lognormal size distribution. Furthermore, data involving aerosols with CMMD beyond 180 nm and with a GSD above 1.6 should be produced and analyzed to extend our observations.

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Table 1. Characteristics of the polydisperse test aerosols produced with CAIMAN.

Condition	Electrode	CMMD (nm)	GSD (-)	$C_N \pm s(C_N)^a$ (10^4 cm^{-3})
1	C	110	1.49	13.66 ± 0.24
2	C	164	1.49	3.90 ± 0.32
3	C	72	1.45	1.58 ± 0.02
4	C	183	1.50	8.37 ± 0.20
5	C	156	1.50	7.99 ± 0.16
6	C	159	1.50	6.38 ± 0.11
7	C	160	1.49	4.72 ± 0.07
8	C	177	1.49	1.96 ± 0.09
9	C	173	1.50	2.21 ± 0.03
10	C	177	1.50	1.76 ± 0.04
11	C	148	1.45	4.90 ± 0.10
12	C	125	1.46	2.21 ± 0.06
13	C	129	1.46	1.19 ± 0.03
14	Ag	73	1.53	4.74 ± 0.05
15	Ag	65	1.53	8.46 ± 0.08
16	Ag	64	1.53	14.93 ± 0.23
17	Ag	66	1.53	4.91 ± 0.05
18	Al	109	1.53	6.13 ± 0.10
19	Al	91	1.53	4.06 ± 0.05
20	Al	92	1.53	2.56 ± 0.02

^a $s(C_N)$ corresponds to the standard deviation of the total number concentration observed for the successive scans.

Table 2. Example of experimental and calculated data for Condition 13.

Parameter	Value
Measured 'alv'-deposited surface area concentration	130.0 $\mu\text{m}^2/\text{cm}^3$
Measured 'tb'-deposited surface area concentration	33.9 $\mu\text{m}^2/\text{cm}^3$
Measured number concentration	11949 cm^{-3}
Measured CMMD	129 nm
Measured GSD	1.46
Calculated ratio $C_{S,LD}/C_N$ in 'alv' configuration	0.0109 μm^2
Calculated ratio $C_{S,LD}/C_N$ in 'tb' configuration	0.0028 μm^2
Calculated CMD in 'alv' configuration with known GSD (1.46)	149 nm
Calculated CMD in 'tb' configuration with known GSD (1.46)	156 nm
Calculated CMD in 'alv' configuration with fixed GSD (1.8)	123 nm
Calculated CMD in 'tb' configuration with fixed GSD (1.8)	134 nm

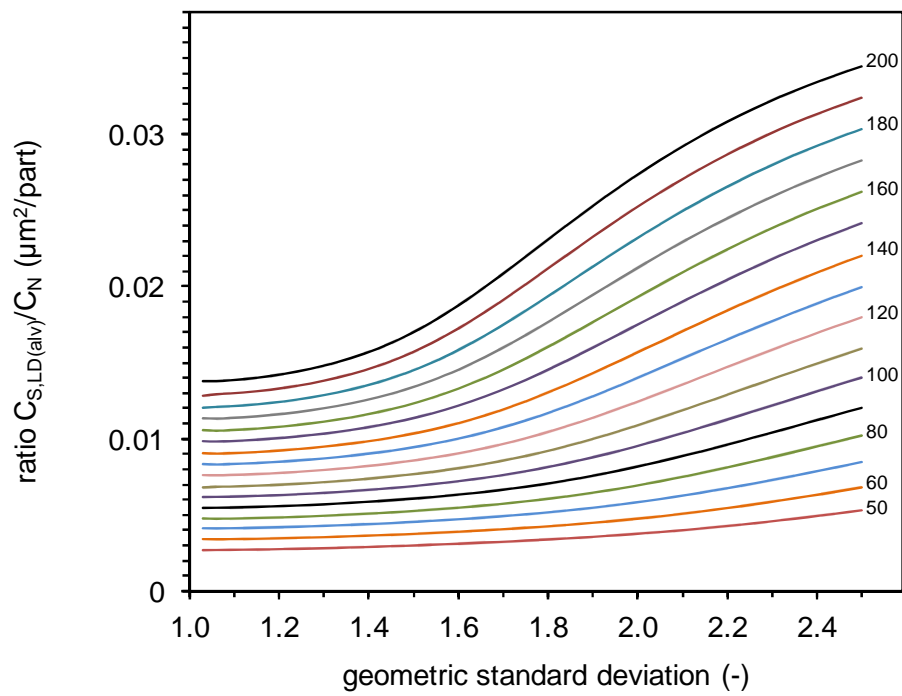


Figure 1. Evolution of the alveolar lung-deposited surface area per particle with the geometric standard deviation of the aerosol size distribution for different count median diameters (indicated on the right in nm).

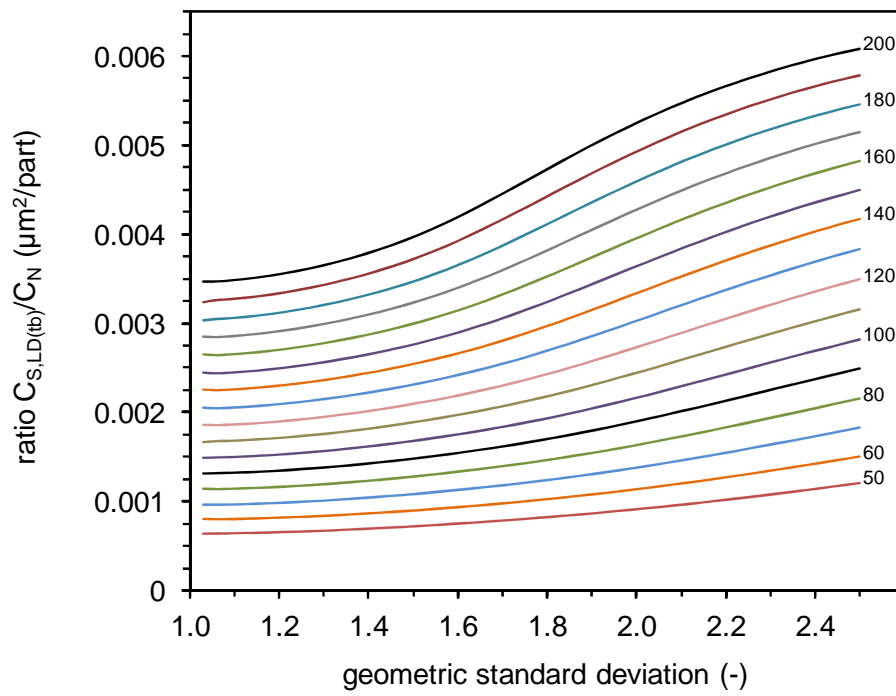


Figure 2. Evolution of the tracheobronchial lung-deposited surface area per particle with the geometric standard deviation of the aerosol size distribution for different count median diameters (indicated on the right in nm).

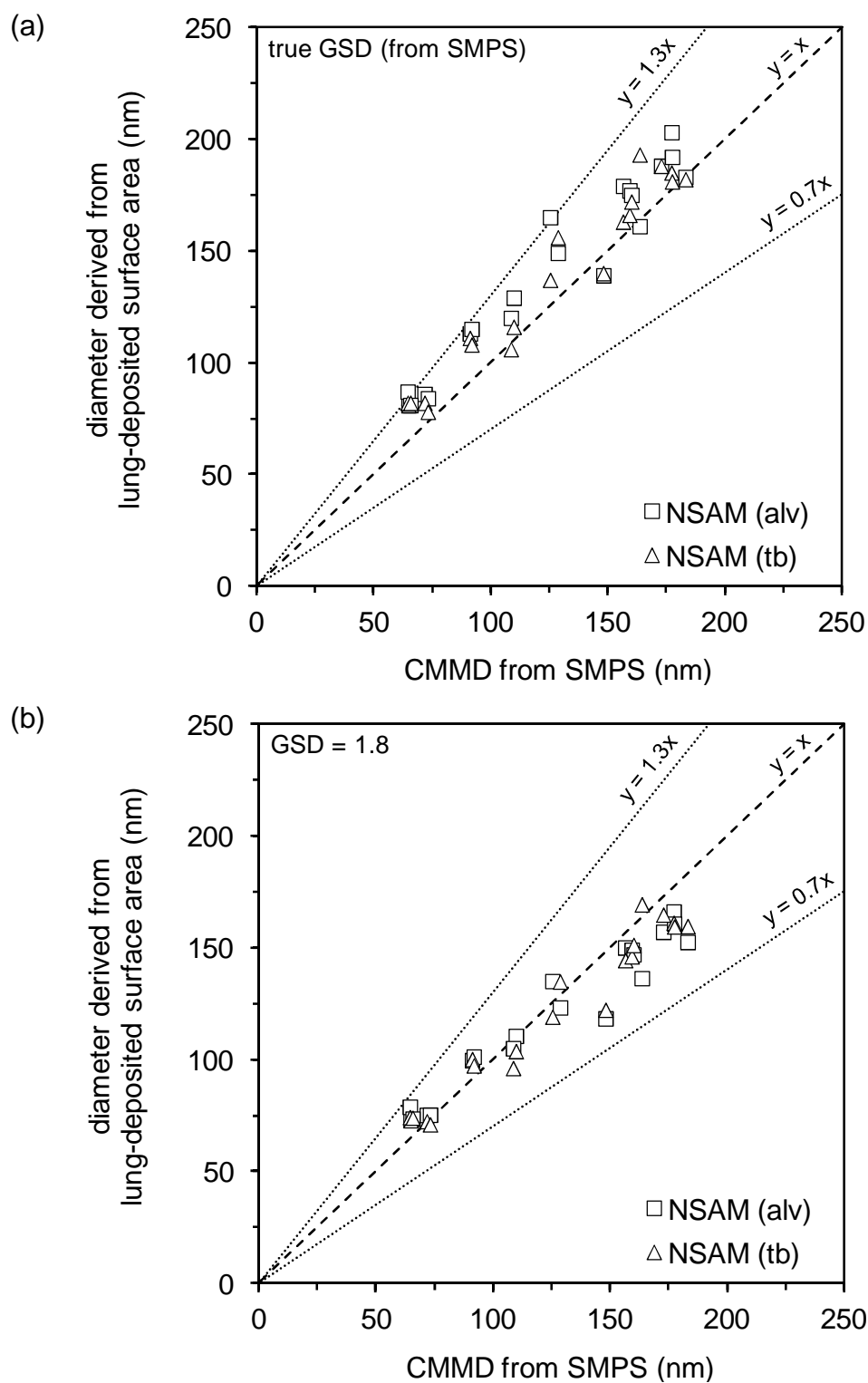


Figure 3. Comparison of the count median diameters derived from lung-deposited surface-area and the count median mobility diameters from SMPS measurements. (a) calculation performed with the input of the true GSD, (b) calculation performed with a GSD set at 1.8. Each data series gathers the results obtained for all chemical substances. The dotted lines correspond to deviations from the bisecting line of $\pm 30\%$.

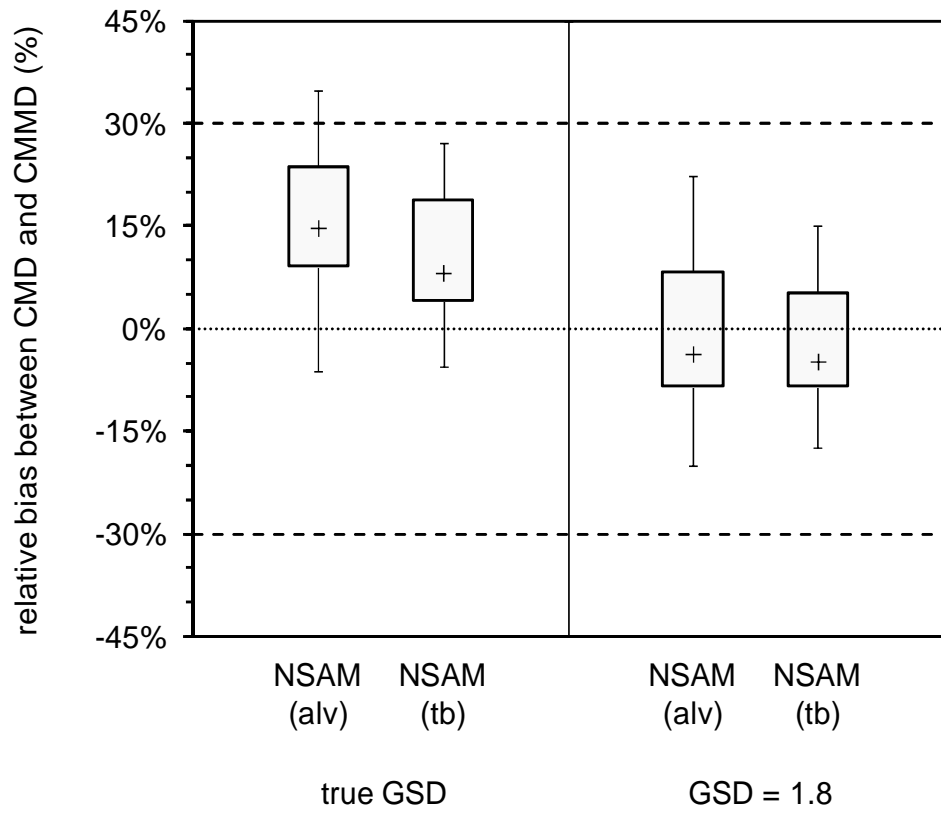


Figure 4. Box & Whiskers plot of the relative differences between calculated and reference median diameters for both configurations of the NSAM ('alv' and 'tb') and the two GSDs considered.