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## **THIN BONE SAMPLE ASSESSMENT USING ULTRASONIC TRANSMITTED SIGNALS BASED ON WAVELET PROCESSING METHOD**

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**ABSTRACT:** The wavelet-based processing (WBP) method based on Meyer-Jaffard algorithm was implemented to simultaneously determine the thickness and velocity of thin cortical bone samples. Two groups of bovine samples were measured by one pair of immersion transducers with nominal frequency 2.25MHz. The WBP method was used to estimate the times of flight (TOF) of two pulses contained by one transmitted signal. The mean relative error of thickness measurement is 6.13%. The mean velocities and their standard deviation for two different groups are  $3399 \pm 131$  m/s and  $3502 \pm 182$  m/s, which lead to the average relative errors from the pulse-mode method of 8.38% and 11.15% respectively. The results demonstrate that the WBP method is able to measure thin bone samples whose thickness is comparable or even less than ultrasound wavelength and provides the potential to assess more reliable initial models for the further imaging process.

### **INTRODUCTION**

Imaging techniques based on the inversion theories can be implemented to reconstruct internal structures of long bones such as tibia and fibula. Two types of reconstruction experiments along different directions have been attempted on bone imaging. Ultrasonic computed tomography (UCT) focusing on the radial measurement around the middle shaft of bones are applied *in vitro* to image the cross-section of femurs of children and estimate the cortical thickness using a 2D-ring antenna and mechanical and electronic steering systems (Lasaygues and Lefebvre, 2001; Lasaygues, 2006). While Zheng (2011) employs similar techniques and methods, yet acquires zero-offset data along the axial direction on the bone surfaces, reconstructs the image of sagittal plane of long bones, and particularly estimates the thickness of top cortical layer. According to Lippmann and Schwinger (1950), the initial models determined before the inversion procedures can greatly influence the inversion results during imaging process. Therefore the pre-determined velocity and thickness of cortex more close to real quantities of the parameters will provide better

initial models (i.e. the background parameters), and moreover lead to better reconstruction results of bone imaging (Lasaygues and Le Marrec, 2008).

Simultaneous determination on thickness and velocity has been developed and applied on other materials, e.g. porous composites (Hsu and Hughes, 1992) and solid plates (Kim *et al*, 2003), using high frequency ultrasound such as 5 or 10 MHz. The wavelet-based processing (WBP) method based on Meyer-Jaffard algorithm were then derived to measure the thickness and velocity of cortical bone samples at the same time with applying only one ultrasonic transmitted signal using low frequency of 1MHz (Loosvelt and Lasaygues, 2011). The goal of this study is to investigate the feasibility and robustness of the WBP method under transmission mode on assessing thin bone samples, whose thickness are approximate or smaller than the ultrasound wavelength.

## METHODS AND EXPERIMENTS

### Wavelet-based processing (WBP) method

As indicated by Loosvelt and Lasaygues (2011), the times of flight (TOF) corresponding to different pulses in the same transmitted signal can be detected by taking correlations between the cross-correlation function of the signal and a pre-determined analyzing pattern. With the two estimated TOFs and the reference velocity and direct reference transmission time in medium (water in this case), the thickness (e) and velocity ( $V_e$ ) of the object can be calculated using equations as below

$$e = V_{\text{ref}} \left[ t_0 - \frac{3t_1 - t_2}{2} \right] \quad (1)$$

and

$$V_e = V_{\text{ref}} \left[ \frac{2t_0 - 3t_1 + t_2}{t_2 - t_1} \right] \quad (2)$$

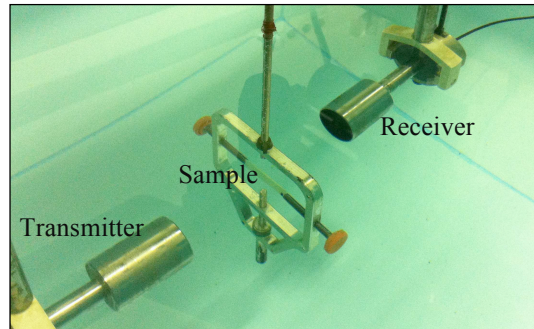
where,  $V_{\text{ref}}$  is the reference velocity of ultrasound in water,  $t_0$  is the traveling time from transmitter to receiver in water only (reference transmission time),  $t_1$  is the transmission time with sample in between, and  $t_2$  is the multiple transmission time with one reflection in sample (indicated as (Loosvelt and Lasaygues, 2011)).

### Samples and experiments

Two groups of bovine cortical bone samples were measured by one pair of immersion transducers (Imasonic®) with nominal frequency 2.25MHz. The thickness of 14 samples measured by caliper is ranged from 0.93 to 2.32 mm, approximately corresponding to 0.6 to 1.5 wavelengths referring to cortical bone tissue. The samples in Group 1 marked as numbers (1-6) were cut parallel to the radial direction, while the samples in Group 2 marked as letters (A-H) were cut parallel to the transverse direction. Due to the different orientation of bone matrix, the bone samples from two groups reveal slightly different acoustic properties.

Figure 1 shows the experimental setup for the measurement in transmission mode. The sample was located at the focal spots of transducers (~150mm from the transducer). With application of function generator (TTI® TGA1241), the WBP method was applied to estimate the TOFs for two pulses ( $t_1$  and  $t_2$ ) contained in the same transmitted signal. The TOFs were then used to calculate thickness and velocity of the samples using Eq.(1) and (2). The high-frequency transducers with nominal frequency 7MHz and 10MHz were also employed in pulse-mode method for the

comparison between different ultrasonic methodologies. As demonstrated in (Loosvelt and Lasaygues, 2011), the pulse-mode method uses two reflection and one transmission shots to eventually achieve the thickness and velocity, separately.



**Figure 1.** Experimental setup for the transmission measurement of thin bone samples.

## RESULTS AND DISCUSSIONS

Table 1&2 illustrate the results of thickness and velocity measurement for all 14 samples, and the relative errors (denoted as “error” in the tables) were calculated by dividing the difference between ultrasonic measurements (from the pulse-mode or WBP transmission methods) and physical measurements (thickness from caliper or velocity from pulse-mode method using 7MHz transducers ) by physical results.

For the thickness measurement showed in Table 1, the errors are literally increased from less than 1% up to 14% with the decrease of sample thickness; especially when the thickness is comparable or less than 1mm ( $\sim 0.6$  wavelength), the errors incredibly grow up to more than 10% due to the inaccuracy of TOF detection resulting from the interference between approaching pulses in the transmitted signal. The mean relative error of all samples is 6.13% referring to the physical measurement, which is a bit greater than the results from the 7MHz pulse-mode method (4.96%) yet much smaller than the results from 10MHz (13.67%). The reason for this phenomenon can be contributed to the influence on measurement accuracy and precision by the frequency of transducers. The higher frequency will result in higher precision, yet the results will be greatly affected by noises at the same time, for example the larger errors in 10MHz measurement. In consideration of the lower frequency applied, the WBP method shows equivalent performance as the pulse-mode method using higher frequency such as 7MHz, moreover reduces the impact of low SNR resulting from high frequencies such as 10MHz.

As shown in Table 2, the mean velocities for two different groups are 3399 m/s and 3502 m/s, which lead to the discrepancies from the pulse-mode method using 7MHz transducers of 8.43% (referring to 3712m/s of Group 1) and 11.52% (referring to 3958 m/s of Group 2), respectively. The two possible reasons for these misfits are the dispersion in different frequency ranges applied to two methods and the dehydration due to low temperature during preservation between two experiments. On the other respect, the standard deviations (STD) are 131 m/s for Group 1 and 182 m/s for Group 2, which are both smaller than the results from the pulse-mode method. Moreover, most of the relative errors are ranged from 4% to 17% for both groups, and their means are 8.38%

and **Table 1**. Thickness and comparison among different ultrasonic methods and caliper measurement. The errors are calculated by dividing the difference between the ultrasonic measurement and caliper results by caliper results.

Sample	Caliper (mm)	7MHz		10MHz		WBP	
		Value (mm)	Error	Value (mm)	Error	Value (mm)	Error
1	2.14	2.13	0.37%	2.21	3.41%	2.18	1.77%
2	1.51	1.52	0.38%	1.81	19.87%	1.57	3.87%
3	2.32	2.23	4.05%	2.62	12.70%	2.33	0.52%
4	1.82	1.88	3.17%	1.97	8.18%	1.89	3.66%
5	1.64	1.55	5.24%	1.70	3.54%	1.71	4.24%
6	1.26	1.32	4.68%	1.35	6.61%	1.29	2.48%
A	1.06	1.11	4.71%	1.17	10.61%	1.21	14.08%
B	1.51	1.60	6.08%	1.74	14.90%	1.61	6.33%
C	0.98	1.10	12.45%	1.50	53.44%	1.11	13.01%
D	0.93	0.86	7.33%	1.01	9.16%	1.04	12.14%
E	1.33	1.39	4.74%	1.44	8.21%	1.36	2.43%
F	1.24	1.34	8.25%	1.37	10.84%	1.34	8.25%
G	0.97	1.02	4.74%	1.19	22.16%	1.06	9.58%
H	1.29	1.33	3.19%	1.39	7.70%	1.33	3.46%
Mean			4.96%		13.67%		6.13%

**Table 2.** Velocities and comparison among different ultrasonic measurements. The errors are calculated by dividing the difference between the WBP method and pulse-mode method with 7MHz by the latter results.

Group 1					Group 2				
Sample	7MHz (m/s)	10MHz (m/s)	WBP		Sample	7MHz (m/s)	10MHz (m/s)	WBP	
			Value (m/s)	Error				Value (m/s)	Error
1	3684	3732	3541	3.87%	A	3927	3598	3319	15.47%
2	3542	4052	3168	10.55%	B	3603	3391	3568	0.97%
3	3852	3479	3432	10.90%	C	3528	2939	3306	6.29%
4	3645	3679	3498	4.04%	D	4339	3338	3357	22.64%
5	3866	3838	3352	13.29%	E	3865	3598	3533	8.59%
6	3684	3739	3404	7.61%	F	4267	3547	3521	17.49%
					G	4062	3310	3865	4.84%
					H	4073	3537	3548	12.89%
Mean	3712	3753	3399	8.38%	Mean	3958	3407	3502	11.15%
STD	125	189	131		STD	289	221	182	

11.15%, respectively. Especially, there is no apparent distinction on the measurement under the condition of various sample thickness. Even with the samples thinner than 1mm such as C and G, the errors can be as small as around 5%. It indicates that the wavelet-based processing method is a more consistent and robust approach for the velocity estimation.

## CONCLUSIONS

The results demonstrate that the WBP method is able to measure thin bone samples whose thickness is comparable or even less than ultrasound wavelength. The results match well with the mechanical measurement and other ultrasonic methods using high-frequency transducers. However when the thickness is below 1mm, larger errors are yielded due to the uncertainty of TOF determination. Although there is variance between the WBP and pulse-mode method on velocity estimation, the results are still comparable regarding the different experimental conditions and nominal frequencies. Moreover the results of WBP method are relatively more consistent, which provides the potential to assess a more reliable pre-determined velocity for the further inversion process.

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## REFERENCES

- Hsu D.K. & Hughes M.S. (1992). "Simultaneous ultrasonic velocity and sample thickness measurement and application in composites", *J. Acoust. Soc. Am.*, 92(2), 669-675.
- Kim Y.H, Song S.J. & Lee J.K. (2003). "Simultaneous measurements of the ultrasonic wave velocity and thickness of a solid plate made from one side of the plate", *Meas. Sci. Technol.*, 14, N13-N16.
- Lasaygues P. (2006). "Assessing the cortical thickness of long bone shafts in children, using two-dimensional ultrasonic diffraction tomography", *Ultrasound in Med. & Biol.*, 32(8), 1215-1227.
- Lasaygues P. & Lefebvre J.P. (2001). "Cancellous and cortical bone imaging by reflected tomography", *Ultrasonic imaging*, 23, 55-70.
- Lasaygues P. & Le Marrec L. (2008). "Ultrasonic reflection tomography vs. canonical body approximation: experimental assessment of an infinite elastic cylindrical tube", *Ultrasonic Imaging*, 30(1), 29-43.
- Lippmann B.A. & Schwinger J. (1950). "Variational Principles for Scattering Processes. I.", *Physical Review*, 79(3), 469-480.
- Loosvelt M. & Lasaygues P. (2011). "A wavelet-based processing method for simultaneously determining ultrasonic velocity and material thickness", *Ultrasonics*, 51, 325-339.
- Zheng R. (2011). *Ultrasonic imaging and cortical thickness determination of long bones (PhD)*. University of Alberta, Edmonton, Canada,