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► **To cite this version:**

Michel Haritopoulos, Julien Roussel, Cécile Capdessus, A.K. Nandi. Cyclostationarity-based Estimation of the Foetus Subspace Dimension From ECG Recordings. XIII Mediterranean Conference on Medical and Biological Engineering and Computing, Sep 2013, Sevilla, Spain. to be published. hal-00839176v1

HAL Id: hal-00839176

<https://hal.science/hal-00839176v1>

Submitted on 12 Jul 2013 (v1), last revised 24 Jul 2013 (v2)

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CYCLOSTATIONARITY-BASED ESTIMATION OF THE FOETUS SUBSPACE DIMENSION FROM ECG RECORDINGS

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Abstract— In this work, a novel method based on the cyclostationary properties of electrocardiogram (ECG) signals is introduced in order to classify independent subspaces into components reflecting the electrical activity of the foetal heart and those corresponding to mother’s heartbeats, while the remaining ones are mainly due to noise. This research is inspired from multidimensional independent component analysis (MICA), a method that aims at grouping together into independent multidimensional components blind source separated signals from a set of observations. Given an input set of observations, independent component analysis (ICA) algorithms estimate the latent source signals which are mixed together. In the case of ECG recordings from the maternal thoracic and abdominal areas, the foetal ECGs (FECGs) are contaminated with maternal ECGs (MECG), electronic noise, and various artifacts (respiration, for example). When ICA-based methods are applied to these measurements, many of the output estimated sources have the same physiological origin: the mother’s or the foetus’ heartbeats. Thereby, we show that a procedure for automatic classification in independent subspaces of the extracted FECG and MECG components is feasible when using a criterion based on the cyclic coherence (CC) of the signal of interest.

Keywords— foetal electrocardiogram, cyclostationarity, cyclic coherence, multidimensional independent component analysis

I. INTRODUCTION

Electrocardiogram (ECG) is one of the most popular diagnostic tools for heart monitoring. Non-invasive electrical activity measurement devices, like electrodes, offer clinicians a versatile tool, without heavy constraints, for preventing complications or diseases due to heart defects. When these measurements come from the thoracic or abdominal regions of a pregnant woman, detecting and separating the foetal electrocardiogram (FECG) from the maternal one (MECG) is not such an easy task, since the FECG has a very low amplitude voltage signal compared to the MECG, and, moreover, the activity measured by the cutaneous electrodes is disturbed by other noise signals, such as random instrumentation noise,

power line signal, breathing or baseline wandering.

In these last decades, various signal processing techniques have emerged and many of them have been customized for FECG extraction purposes ([1], [2], [3]). Among them are blind source separation (BSS) techniques [4] and the underlying mathematical tool which is independent component analysis (ICA). It aims at separating unknown source signals of interest from a mixture of them, observed with the aid of sensors. Numerous methods can be found in the dedicated literature, but only a few make use of the concept of multidimensional independent component analysis (MICA), introduced in the late 90’s. Interested readers can find a recent review on FECG signal processing in [5].

In the rest of the paper, we first present the MICA concept. An introduction to the cyclostationary nature of ECGs and a description of a cyclostationarity measure, called cyclic coherence, follows. Next, a novel FECG classification procedure is proposed and validated on a real world FECG dataset; it is based on the cyclic coherence computation of the ICA estimated components from a set of sensor signals. Finally, conclusions are drawn from this work.

II. ICA AND THE MULTIDIMENSIONAL ICA (MICA) CONCEPT

A. Blind source separation problem formulation and ICA

Jutten *et al* first proposed a simple 2×2 neural network-based self-adaptive algorithm ([6], [7]) as a solution to the separation of independent source signals, and introduced the concept of independent component analysis, which has been theoretically investigated few years later by Comon [8]. The problem in blind source separation (BSS) states as follows: given a set of M observed signals $x_i(t), i \in [1, M]$, find the N unknown sources $s_i(t), i \in [1, N]$, with $N \leq M$, that are hidden in the observations. In matrix form, the problem writes:

$$\mathbf{x}(t) = \mathbf{A}\mathbf{s}(t). \quad (1)$$

where $\mathbf{x}(t) = [x_1(t), x_2(t), \dots, x_M(t)]^\dagger$ and $\mathbf{s}(t) = [s_1(t), s_2(t), \dots, s_N(t)]^\dagger$ denote the mixture vector and

the unknown source vector, respectively, with \dagger the transpose operator and with A an unknown $M \times N$ full rank mixing matrix. The mixture model of eq.1 is the *linear instantaneous noiseless* one, which is widely used in the literature and which only assumes statistically independent source components s_i and at most one Gaussian entry.

B. Multidimensional ICA

A source subspace separation method for FECG extraction has been presented in [9]. In this work, authors use second-order statistics based on the singular value decomposition (SVD) of the observed ECG data matrix to estimate the underlying source subspaces, assuming that the latent bioelectric phenomena generating the foetal and the mother heartbeats are statistically independent. Then, they enhance the accuracy of the proposed algorithm by introducing a higher-order singular value decomposition (HOSVD) technique.

A similar technique is proposed by Cardoso in [10] named multidimensional independent component analysis (MICA). It can be seen as a generalization of the ICA model to multidimensional components. The author illustrates his method with real FECG data. First, he estimates the unknown sources by applying the well known ICA algorithm JADE [11] to a 3-channel real ECG data of an expectant mother. After extraction of the independent components (ICs), he groups two of them into a bi-dimensional component corresponding to the MECG; the choice of these two components is done only after visual inspection and, in this case, that works because mother's and foetus' contributions are clearly distinguishable. After computing the orthogonal projection matrices for each one of the two estimated multidimensional components, a back-projection to the original input space permits to reconstruct the mother and foetal signal contributions to the mixtures.

We demonstrate below how to establish an automated procedure based on the cyclostationary properties of the ECG signals, in order to classify ICA-based extracted ICs into multidimensional components.

III. CYCLOSTATIONARITY MEASURES

A. The cyclostationarity property

The main assumption for this procedure to succeed, is that the foetus' as well as the mother's heartbeats, if they do not exhibit a strict period, they are at least repetitive, i.e. cyclostationary at the frequency α_0 of the heartbeats. A cyclostationary signal is not strictly periodic, but some of its statistical properties are periodic. This same assumption of FECG

cyclostationarity used in previous work [12], together with the *a priori* estimation of the foetus' fundamental cyclic frequency, provided very promising results with regard to the foetal PQRST extraction.

In this context, we use a statistical measure of cyclostationarity as a criterion to decide whether an ICA estimated IC corresponds to the FECG rather than to the MECG subspace. This measure is the cyclic coherence.

B. The cyclic coherence measure

In this work, we use a spectral version of the simple coherence [13] which is a measure of the correlation degree between two signals, $x(t)$ and $y(t)$, at each frequency value f . It is called the cyclic coherence (CC) and it has been introduced in [14]:

$$C_x^\alpha(f) = \frac{E[X(f)X^*(f-\alpha)]}{\left(E[|X(f)|^2]E[|X(f-\alpha)|^2]\right)^{\frac{1}{2}}}, \quad (2)$$

where $X(f)$ and $X(f-\alpha)$ are the Fourier Transforms of $x(t)$ and alpha value frequency-shifted $x(t)$, respectively.

The CC measure is normalised. A CC value near to one for a frequency f , indicates a strong coherence between components of signal $x(t)$ at frequencies f and $(f-\alpha)$.

IV. THE PROPOSED METHOD AND ILLUSTRATION WITH REAL WORLD DATA

To illustrate the proposed method, we worked on the same dataset as in the original MICA work [10], i.e. the well-known *DalSy* database [15], but we considered the whole recordings set. This is an eight-channel cutaneous recordings set from an expectant mother. The first five potentials come from electrodes placed at different locations in the abdominal region of the mother, while the last three recordings come from her thoracic region. All eight signals are recorded simultaneously at a sampling rate of $500Hz$ and each one of them lasts $5sec$ (Figure 1).

A. The classification procedure

We first applied the JADE algorithm to the whole observations vector and then we computed the CCs of the estimated components. A visual inspection of the obtained CCs leads to a preliminary classification of extracted components $\{3,5\}$ into the FECG subspace, components $\{1,4\}$ into the noise subspace and the remaining components $\{2,6,7,8\}$ into the MECG subspace (Figures 2, 3 and 4, respectively). Indeed, in Figure 2 one clearly notices the high values over all

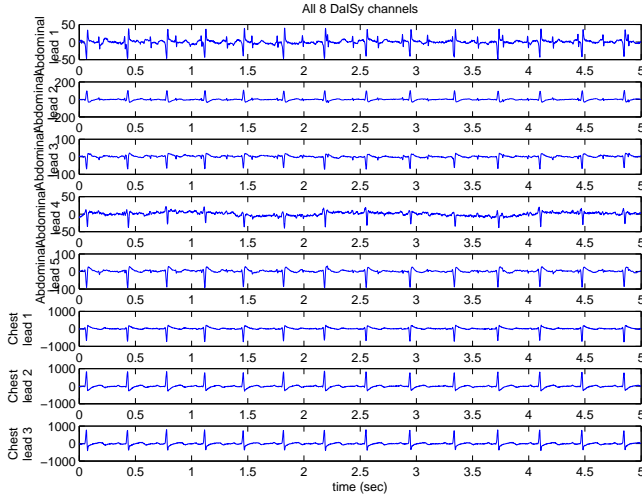


Fig. 1: Eight surface electrodes recordings

the spectral frequencies range, for cyclic frequency around 4.5Hz that corresponds to the fundamental cyclic frequency of the foetus' heart [12], while the second high-valued spectral line corresponds to its second harmonics. On the contrary, no (f, α) couple has a significantly high value in the CCs of JADE extracted components 1 and 4, as one can observe in Figure 3. This is in agreement with the kurtosis values of these two CCs: 4.94 and -0.54 , for components 1 and 4, respectively, while kurtosis values for all other component's CC vary between 22.17 and 43.26. Lower kurtosis values may correspond to noisy background.

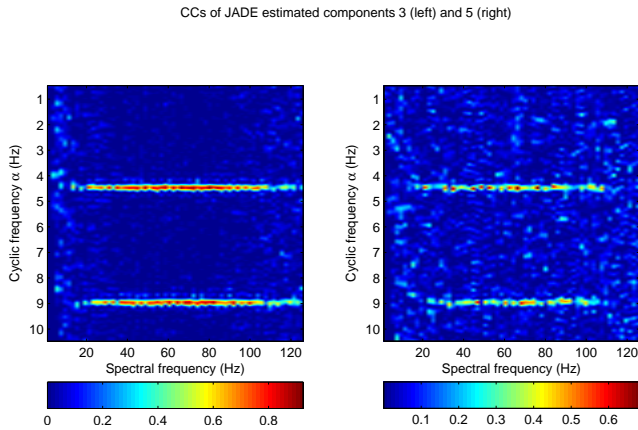


Fig. 2: The 2-dimensional FECG subspace

Things get a little bit different for the MEGC subspace. CCs of JADE estimates 2, 6 and 8 exhibit distinct higher values for cyclic frequency around 2.7Hz into the spectral frequency range $[20, 80]\text{Hz}$ (Figure 4); all three span the sub-

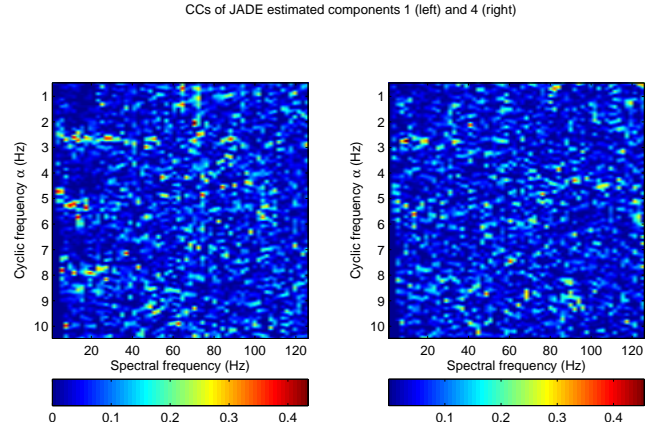


Fig. 3: The 2-dimensional noise subspace

space of the MEGC components. On the other hand, the CC of the JADE estimated component number 7, shows also high values for cyclic frequencies different from the mother's fundamental one and its harmonics. That needs more investigations to interpret, but it is not decisive for the classification procedure of foetal components that this work suggests.

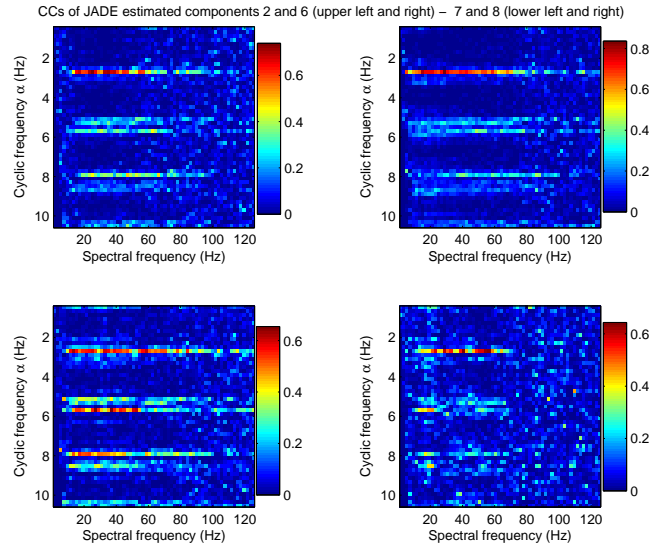


Fig. 4: The 4-dimensional MEGC subspace

Next, we integrate the cyclic frequencies for each CC of the ICA estimated components over the spectral frequencies to obtain the integrated CC (iCC). At this stage to automate the extraction of the noise subspace components, one can compute the standard deviation of each iCC; standard deviation values for this example are $\{0.68; 3.59; 5.29; 0.69; 2.41; 4.20; 4.44; 1.92\}$ for the 1st through to the 8th JADE extracted IC. Looking for standard

deviation values below a low-valued threshold, is an efficient way for isolating ICs whose iCCs do not contain significant information.

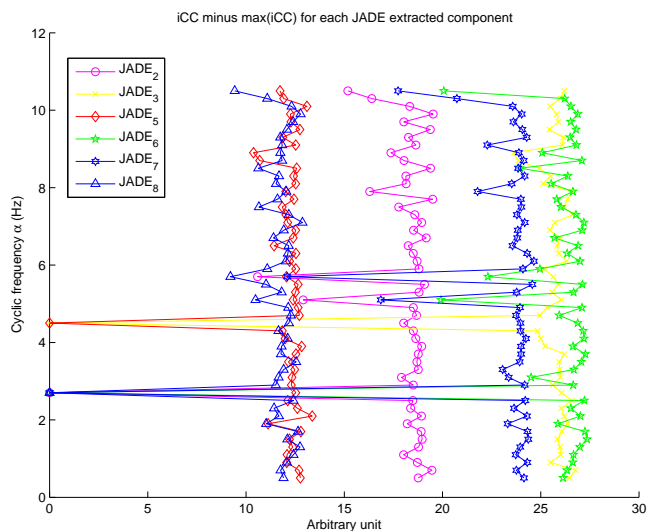


Fig. 5: The two null values of the remaining 6 transformed iCCs do correspond to the FECG's and the MECG's fundamental cyclic frequencies (4.5Hz and 2.7Hz, respectively)

Then, from each one of the previously computed iCCs, one subtracts its maximum value as shown in Figure 5. This is implemented only for extracted components that they do not span the noise subspace, i.e., JADE extracted components $\{2, 3, 5, 6, 7, 8\}$. One remarks that the yellow ($JADE_3$) and red ($JADE_5$) data plots of Figure 5 exhibit both a null value for the same cyclic frequency equal to 4.5Hz (i.e., the foetus' heart cyclic frequency) while the four remaining components have a modified iCC of zero value at 2.7Hz (i.e., the mother's heart cyclic frequency). Finally, one can group blind-separated ICs into 3 independent subspaces: the FECG one spanned by ICs $\{3, 5\}$, a noise one spanned by ICs $\{1, 4\}$ and the MECG subspace spanned by ICs $\{2, 6, 7, 8\}$.

V. CONCLUSION

This work proposes an automated classification procedure of blindly separated independent foetal components from maternal ECG recordings, that consists of four steps:

1. Apply a BSS/ICA algorithm to extract ICs from raw ECG data.
2. Compute the CC and then the iCC for each extracted independent component at the previous step.
3. Classify ICs whose standard deviation value of their iCC is below a threshold into a subspace corresponding to the

noise.

4. Compute the difference between each iCC and its maximum value, and group into the same independent source subspaces the corresponding ICs exhibiting null values for the same cyclic frequencies.

The method is tested on the real world DaSy dataset and gave very promising results. Future research work concerns the validation of this method to simulated foetal ECGs, as well as further investigations about the computed CCs of the MECG source subspace components.

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