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Tunable Functionality and Toxicity Studies of Titanium Dioxide Nanotube Layers

E. Feschet-Chassot^a, V. Raspal^a, Y. Sibaud^a, O. K. Awitor^{a,*},
F. Bonnemoy^b, J.L.Bonnet^{b,c}, J. Bohatier^{b,c}

^a*Clermont Université, Université d'Auvergne, C-BIOSENS, BP 10448, F-63000
Clermont Ferrand*

^b*Clermont Université, Université Blaise Pascal, UMR CNRS 6023, LMGE, BP 10448,
F-63000 Clermont Ferrand*

^c*Clermont Université, Université d'Auvergne, Laboratoire de Biologie cellulaire, BP
10448, F-63000 Clermont Ferrand*

Abstract

In this **study**, we have developed a **simple** process to **fabricate** scalable titanium dioxide nanotube layers which show a tunable functionality. The titanium dioxide nanotube layers were prepared by electrochemical anodization of Ti foil in 0.4 wt% hydrofluoric acid solution. The nanotube layers structure and morphology were characterized using x-ray diffraction and scanning electron microscopy. **The surface topography and wettability were studied according to the anodization time. The sample synthesized displayed a higher contact angle while the current density reached a local minimum.** Beyond this point, the contact angles decreased with anodization time. Photo-degradation of acid orange 7 in aqueous solution was used as a probe to assess the photocatalytic activity of titanium dioxide nanotube layers under UV irradiation. We obtained better photocatalytic activity for the sample **fabricated** at higher current density. Finally we used the Ciliated Protozoan *T. pyriformis*, an alternative cell model used for in vitro toxicity studies, to predict the toxicity of titanium dioxide nanotube layers in a biological system. We did not observe any characteristic effect in the presence of the titanium dioxide nanotube layers on two physiological parameters related to this organism, non-specific esterases

*Corresponding author

Email address: koawitor@iut.u-clermont1.fr ()

activity and population growth rate.

Keywords:

Anodization, Titanium Dioxide Nanotubes, Contact Angle, Photodegradation, Toxicity.

1. Introduction

2 Research into developing nanotubes with **interesting** properties by con-
3 trolling the nanostructure topography has attracted great interest because of
4 their variety of applications. In 2001, Gong and co-workers [1] reported the
5 fabrication of vertically oriented highly ordered TiO₂ nanotube arrays up to
6 approximately 500 nm length by anodization of titanium foil in an aqueous
7 HF electrolyte. Since then, substantial efforts have been devoted to the self
8 organisation and growth of TiO₂ [2, 3, 4]. Titanium dioxide nanotube layers
9 are used as photo-catalysts in water and environmental purification, as well
10 as **biological** and biomedical applications [5, 2, 6]. In particular, Titanium
11 dioxide nanotubes are used as a **biomaterial** for implants, drug delivery plat-
12 forms, tissue engineering and bacteria killing [7, 8, 9, 10, 11, 12, 13]. Another
13 interesting propriety of TiO₂ is its tunable wettability effect [14, 15]. The
14 ability to modify surface topography and to control wetting behavior is useful
15 for biomedical applications. Surface roughness, contact angle, surface energy
16 are the main factors in understanding the biology media and material inter-
17 action. In this work, we present recent results on TiO₂ nanotubes fabricated
18 by anodization of Ti foil in 0.4 wt% hydrofluoric acid solution to produce a
19 self-organized porous film structure versus the anodization time. Such TiO₂
20 nanotube surfaces are of interest in order to change the wettability proper-
21 ties of titanium oxide films. The nanotube layers were characterized using
22 x-ray diffraction and scanning electron microscopy. We have investigated the
23 surface wettability of as-anodized samples obtained at different anodization
24 times. The as-grown sample synthesized while the current density **reached**
25 a local minimum displayed higher contact angle. The surface of the oxide
26 was covered at this point with a high density of fine pits. **We report on**
27 **the photo-degradation of acid orange 7 (AO7) in aqueous solutions**
28 **which was used as a probe to assess the photocatalytic activity of**
29 **titanium dioxide nanotube layers under UV irradiation.** We obtained
30 better photocatalytic activity for the sample **fabricated** at higher current
31 density. Finally we **used** the Ciliated Protozoan *T. pyriformis* to predict the

32 toxicity of titanium dioxide nanotube layers towards biological systems.

33 **2. Experimental Details**

34 *2.1. Sample preparation*

35 To fabricate anodic TiO₂ nanotube layers, we used Ti foil (Goodfellow
36 99.6% purity) with a thickness of 0.1 mm. The Ti foils were degreased by
37 successive sonication in trichloroethylene, acetone and methanol, followed by
38 rinsing with deionized water, dried in the oven at 100°C and finally cooled
39 in the desiccator. Anodization was carried out at room temperature (20°C)
40 in 0.4 wt% HF aqueous solution with the anodizing voltage maintained at
41 20 V.

42 *2.2. Surface characterization*

43 The surface topography characterization was performed using a Zeiss
44 Supra 55 VP scanning electron microscope (SEM) **with secondary emis-**
45 **sion and in lens detector. The accelerating voltage and the work-**
46 **ing distance are respectively 3kV and 5mm. The crystalline struc-**
47 **ture and phase of the TiO₂ nanotube layers were determined by X-**
48 **ray diffraction (XRD) using a Scintag XRD X'TRA diffractometer**
49 **with CuK_α ($\lambda = 1.54 \text{ \AA}$) radiation. The CuK_β radiation is filtered**
50 **through a nickel filter. The diffraction pattern was achieved be-**
51 **tween 20 and 80° with a step angle of 0.05° and a scanning speed**
52 **of 0.01° per second.**

53 *2.3. Contact angles*

54 Surface wettability **was** investigated using a drop shape analysis system
55 (EasyDrop, Kruss, Hambourg, Germany). The contact angle of 3 μL ses-
56 sile droplet of deionized water was measured on the surface under ambient
57 conditions.

58 *2.4. Photo-degradation*

59 Photocatalytic experiments were conducted in 3 mL of AO7 solution
60 (from Acros Organics) with a concentration of $5.0 \cdot 10^{-5}$ mol/L, placed in a
61 cylindrical Pyrex glass reactor. The surface area of the anodized samples was
62 approximately 3.5 cm². The glass reactor was irradiated with polychromatic
63 fluorescent UV lamps (Philips TDL 8 Watt (total optical power 1.3 Watt),
64 300 mm long, wavelength range 315-400 nm) in a configuration providing

65 about 0.9 mW/cm² at the sample surface. The photocatalytic decomposi-
66 tion of AO7 was monitored by the decrease in the solution's absorbance at a
67 wavelength of 485 nm using a UV-Vis spectrometer (Perkin Elmer Lambda
68 35).

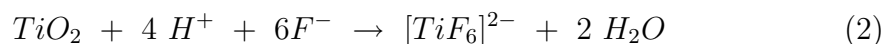
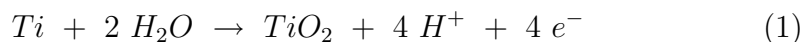
69 2.5. Toxicity assessment

70 The potential toxicity of TiO₂ nanotube surfaces was evaluated with
71 *Tetrahymena pyriformis* using two tests previously validated : inhibition of
72 an enzymatic activity and effect on population growth rate. For non-specific
73 esterases activities quantification, a *T. pyriformis* culture in an exponential
74 growth phase (in PPYS medium) was centrifuged at 300 rpm, and the su-
75 pernatant was discarded. The *T. pyriformis* pellet was suspended in Volvic
76 mineral water. After counting cells under a microscope, dilution was done to
77 obtain about 4000 cells/mL. 1 mL of this dilution was incubated for 1h with
78 the different Ti layers at 28 °C under UV or without UV irradiation. After
79 incubation, Ti layers samples were removed and 1 mL of **Fluorescein diac-**
80 **etate (FDA)** at 4.8 μM was added (2000 cells/mL in final). Each toxicity
81 test included two controls : FDA in Volvic water to measure self degradation
82 of this substrate and FDA with *Tetrahymena pyriformis* (untreated cells).
83 After 30 min, the fluorescence was measured by a spectrofluorimeter (Kon-
84 tron SFM 25, Kontron, Milan, Italy) with a 485 nm excitation filter and
85 a 510 nm emission filter. Experiments were repeated three times for each
86 sample. To test the inhibition of development of populations in an exponen-
87 tial growth phase, we prepared 8 erlenmeyer flasks (40 mL): 2 for control
88 cultures and 6 for the samples to be tested (Ti foil, unannealed TiO₂ and
89 TiO₂ annealed at 500 °C). The samples were deposited at the bottom of the
90 erlenmeyer flasks and 3 mL were **removed** at 0h, 3h, 6h and 9h to measure
91 the optical density (OD) at 535 nm.

92 3. Results and discussion

93 3.1. TiO₂ Nanotube growth process and Layer Characteristics

94 The anodization growth was governed by a competition between anodic
95 oxide formation and chemical dissolution [16] of the oxide as soluble fluoride
96 complexes according respectively to reactions (1) and (2) :



97 Figure 1 shows a characteristic density current time curve for Ti anodiza-
 98 tion in our operating conditions and figure 2 shows SEM images of the TiO₂
 99 grown at different stages of growth corresponding to the points a, b, c and d.
 100 We can notice that after an initial exponential decay of the current density
 101 to a local minimum around 10 mA.cm⁻² about 70 s. The structure of the
 102 film at this point led to the formation of randomly generated pits on the
 103 oxide which were shown in figure 2a. The pits were approximately 30 nm in
 104 diameter.

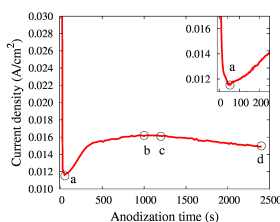


Figure 1: Typical density current time curve for Ti foil anodization. Anodization was carried out at room temperature (20°C) in a 0.4 wt% HF aqueous solution with the anodizing voltage maintained at 20V. Inset in upper right hand corner shows a blow up of the time behavior from 0 to 250 s.

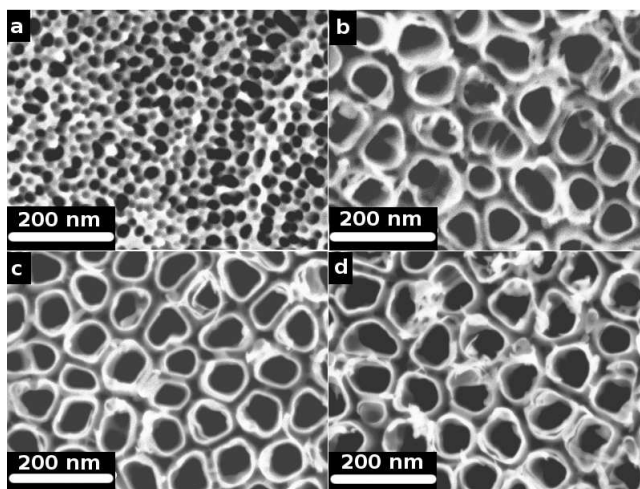


Figure 2: SEM top-view images of samples taken while density current was at local minimum (a), local maximum (b) and at the anodization time of 20 min and 40 min respectively (c, d).

105 After the current density increased to a local maximum of 12,7 mA.cm⁻²

106 in 1000 s, we **observed** ordered nanotube arrays with approximately 85 nm
 107 in diameter as evidenced by figure 2b. After 20 min and 40 min of growth,
 108 we observed in figure 2c and 2d ordered nanotube arrays with approximately
 109 100 nm and 105 nm in diameter respectively. We summarize in figure 3, the
 110 evolution of the diameter of the pores. Between 70 and 1000 s, we **observed**
 111 a linear evolution of the diameter versus time with a high slope. Similarly,
 112 the trend is weak between 1000 and 2400 s. At 2400 s, we reach the maximum
 113 diameter. This shows that the dissolution rate of oxide is predominant over
 114 the oxide growth velocity. So in a steady state, the pore diameters do not
 115 depend on the anodization time despite enlargement of the pore diameters
 116 due to the dissolution of the mouth of the nanotubes as reported elsewhere
 117 [17].

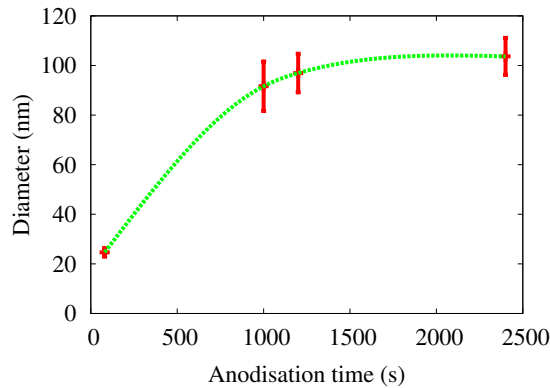


Figure 3: The evolution of the diameter of the pores of **samples** (a), (b), (c) and (d).

118 We summarize in figure 4 the X-ray diffraction patterns of Ti foil and
 119 TiO_2 nanotube layers anodized for 40 min before and after annealing at
 120 500°C in oxygen for 2 h according to the paper published elsewhere [2]. The
 121 unannealed TiO_2 nanotube layer exhibits only the peaks from titanium metal
 122 foil under the nanotube layer, while the annealed sample exhibits the main
 123 lattice phases of anatase and rutile (figure 4).

124 3.2. Contact angles

125 The influence of TiO_2 nanotubes on Ti on bone cell-materials interac-
 126 tion has been reported [18]. In this study, we have evaluated the contact
 127 angle behavior on TiO_2 nanotube layers which have pronounced topologi-
 128 cal features and increased surface areas. Contact angles were measured for

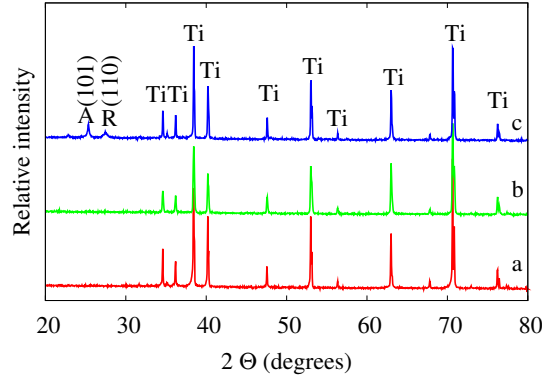


Figure 4: X-ray diffraction patterns of Ti foil (a), as grown during 40 min (b) and annealed TiO_2 nanotube layers at 500°C in oxygen for 2 h (c). Lattice planes indicate anatase (A), rutile (R) and titanium (Ti).

129 each as-anodized sample. Each sample was dried in the oven for 30 min and
 130 cooled 15 min in the desiccator before measurements. We observe in figure 5,
 131 optical images of water droplets on as-grown TiO_2 nanotube layers. Results
 132 indicated a higher contact angle for the sample covered with pits obtained
 133 at local minimum density current (70 s). Beyond this particular point, the
 134 contact angles value decreases with anodization time. So we have performed
 135 a scalable surface functionality without any chemical treatment.

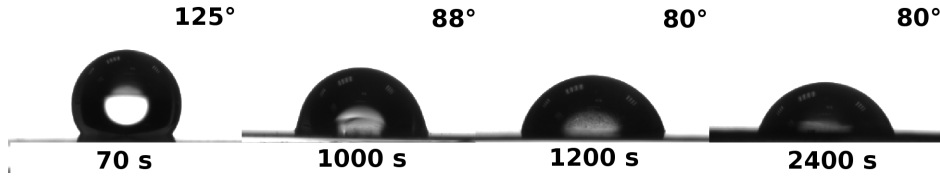


Figure 5: Optical images of water droplets on as-grown TiO_2 nanotube layers. Surface at local minimum density current (70 s); surface at local maximum density current (1000 s); surface after 20 min of growth (1200 s) and surface after 40 min of growth (2400 s).

136 3.3. Photo-catalytic activity measurement

137 The photo-degradation of AO7 in the presence of TiO_2 nanotubes under
 138 different conditions is summarized in figure 6. This shows the AO7 concen-
 139 tration versus time as determined by the solution's absorbance at 485 nm.
 140 The initial concentration of the AO7 was $5.0 \cdot 10^{-5}$ mol/L. $C(0)$ is the initial

141 concentration of AO7 while $C(t)$ is the concentration after time, t , of con-
 142 stant UV irradiation in 315-450 nm wavelength range. The variation of the
 143 concentration of AO7 in the presence of the TiO_2 layer without irradiation
 144 after 5 h is less than 1%. Thus the effect of adsorption of the dye on the TiO_2
 145 surface is negligible. Curve 6(e) shows the variation in the concentration of
 146 AO7 in the presence of unannealed TiO_2 nanotubes under UV irradiation.
 147 This result indicates that AO7 is not substantially degraded in the presence
 148 of amorphous TiO_2 nanotube layers. Curves 6(a), 6(b), 6(c) and 6(d) corre-
 149 sponding to the TiO_2 nanotube layers grown during 70 s, 1000 s, 1200 s, 2400
 150 s respectively and annealed at 500°C illustrate photo-degradation of AO7.
 151 These results show the decay of organic molecules with UV irradiation in
 152 the presence of the annealed nanotubes. We observed the strongest photo-
 153 catalytic activity for the sample grown during 1200 s. We **cannot** draw any
 154 correlation between surface wettability and photocatalytic activity.

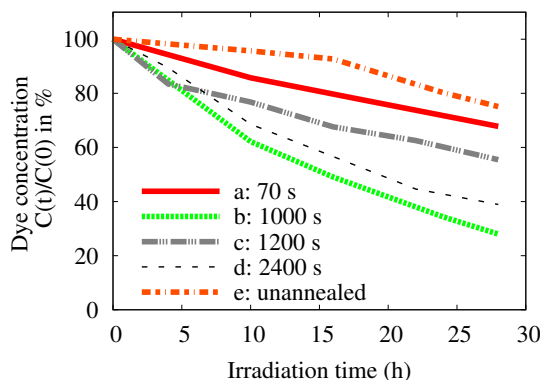


Figure 6: Photo-degradation of acid orange 7 (AO7) dye under UV-lamp irradiation at wavelengths of 315-400 nm in the presence of a TiO_2 nanotube layer, as measured by the absorbance of the irradiated dye at 485 nm. $C(0)$ is the initial concentration of AO7 (5×10^{-5} M) and $C(t)$ is the concentration after time, t , of irradiation. (e) unannealed TiO_2 nanotube layer; (a), (b), (c), (d) TiO_2 nanotube layers grown during 70 s, 1000 s, 1200 s, 2400 s respectively and annealed at 500°C .

155 The effect of irradiation of the sample grown for 1000 s with polychro-
 156 matic light (315-400 nm) on the UV-Vis spectrum is **shown in figure 7**.
 157 Absorbance for increasing irradiation time decreases from the upper curve
 158 toward the lower curve.

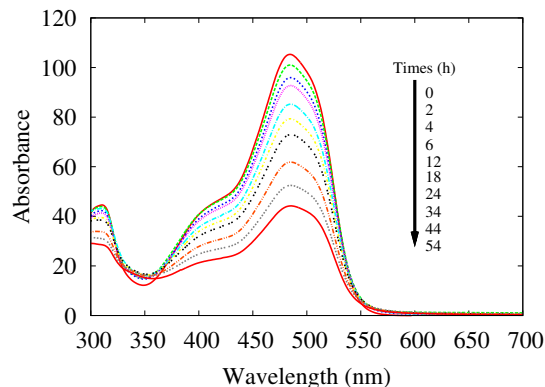


Figure 7: Effect of irradiation with polychromatic light (315-400 nm) of AO7 in the presence of TiO₂ nanotube layers grown during 1000 s and annealed at 500°C on the UV-Vis spectrum in the 300-700 nm range.

159 3.4. Toxicity tests

160 The cellular toxicity of TiO₂ based nanofilaments [19], nanoparticles [20]
 161 was studied. The authors concluded that these nanofilaments and nanopar-
 162 ticles are cytotoxic. However, in other studies, no toxic effects were observed
 163 with TiO₂ nanoparticles [21, 22]. Similarly the effects of radical reactivity
 164 generated by TiO₂ on cells under UV irradiation **is** still controversial [23, 24].
 165 **As far as we know**, no study has been conducted on the toxicity of TiO₂
 166 nanotube layers. In this work two different tests of toxicity have been made
 167 with the Ciliated protozoan *T. pyriformis* as described in detail elsewhere
 168 [25]. This organism is an alternative eukaryotic cell model including the es-
 169 tablished fibroblastic cell lines used **in vitro** toxicity studies. All the tests
 170 were carried out with titanium foil, amorphous and crystalline TiO₂ nan-
 171 otube layers. The cristalline samples showed photocatalytic activities. We
 172 studied their influence under UV radiation on the toxicity tests. The test
 173 of inhibition of non-specific intracellular esterase activity was based on the
 174 hydrolysis of fluorescein diacetate (FDA) by *T. pyriformis* and quantifica-
 175 tion of fluorescein released **for** 30 min. Esterases are ubiquitous enzymes
 176 present in all living organisms and are considered as good biomarkers of cel-
 177 lular activities. The aim of this test was to determine the evolution of the
 178 percentage of the *T. pyriformis* activity over the control in the presence of
 179 Ti foils, amorphous and crystalline TiO₂ nanotube layers without UV irra-
 180 diation **without UV**) and with constant UV irradiation (**With UV**) at a
 181 wavelength of 315-400 nm. We can observe an effect of titanium foil but

182 no significant effect of the amorphous and crystalline TiO₂ nanotube layers.
 183 The UV light radiation did not disturb the results (Figure 8) **despite** the
 184 photocatalytic activities of cristalline samples. Furthermore, *T. pyriformis*
 185 population growth rate test allows us to include different physiological distur-
 186 bances which could have been caused by the three types of layers. Growth
 187 was followed photometrically with a measure of optical density ($\lambda = 535$
 188 nm) every 3 hours. Reduction in growth compared to a control culture is
 189 indicative of toxicity.

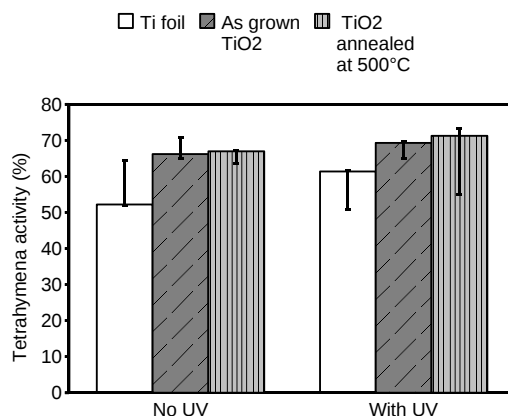


Figure 8: *T. pyriformis* activity over the control in the presence of Ti foil, amorphous and crystalline TiO₂ nanotube layers without UV irradiation (No UV) and with constant UV light (With UV) at wavelength range 315-400 nm.

190 The purpose of this test was to determine a 50% inhibition of growth rate
 191 in treated cultures (increase in 50% of the generation time compared to a
 192 control culture). We did not observe any characteristic effect related to the
 193 inhibition of protozoa growth for Ti foils, amorphous and crystalline TiO₂
 194 nanotube layers (Figure 9). We can conclude through these two tests that
 195 the TiO₂ nanotube layers are not toxic.

196 4. Conclusions

197 We have demonstrated the fabrication of controllable as-grown surfaces
 198 of titanium dioxide nanotube layers. The contact angles measurements show
 199 clearly the correlation between surface topography and surface wettability.
 200 We have shown the ability of the titanium dioxide nanotube layers to degrade

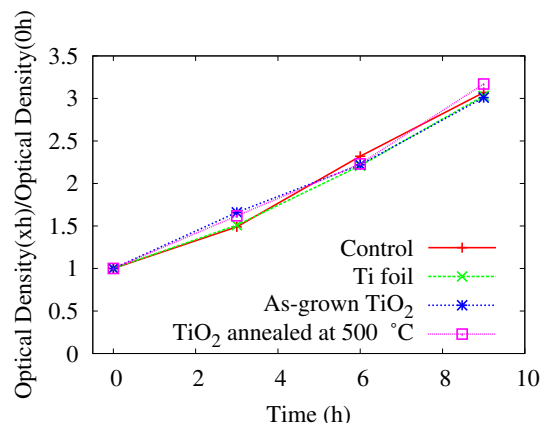


Figure 9: Growing populations of *T. pyriformis* in the presence of titanium foil, amorphous and crystalline titanium dioxide nanotube layers.

201 AO7. Such surfaces **do not** show any characteristic *in vitro* toxicity effect in
 202 a biological system. In conclusion, we have developed **a simple process** to
 203 **fabricate** active surfaces of titanium dioxide with scalable nanotube layers
 204 and tunable functionalities.

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