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Three dimensional tracking of gold nanoparticles using digital holographic microscopy

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In this paper we present a digital holographic microscope to track gold colloids in three dimensions. We report observations of 100 nm gold particles in motion in water. The expected signal and the chosen method of reconstruction are described. We also discuss about how to implement the numerical calculation to reach real-time 3D tracking. © 2012 Optical Society of America

1. Introduction

The tracking of nano-scale biological markers in motion is a challenging project, that could lead to a better understanding of dynamics in biological systems. Since digital holography gives access to the whole light field in a volume from a single hologram [1, 2], this technique is suitable to reconstruct the field scattered by gold particles in three dimensions, and then determine their positions. This localization can be done without any mechanical scanning of the setup. The 3D tracking in digital holography was demonstrated for micron-size particles in several publications with in-line holography [3–6]. The observation of nano-scale gold particles was also demonstrated in off-axis holography by Atlan et al. [7], and on the membrane of a living cell by Joud et al. [8]. Nano particles could be observed with the combination of off-axis geometry and phase-shifting technique [9], that achieves almost the theoretical noise level [10]. In this paper, we present first our digital holographic microscope, then we explain the reconstruction method. Some results of 3D tracking of 100 nm nano-beads are presented.

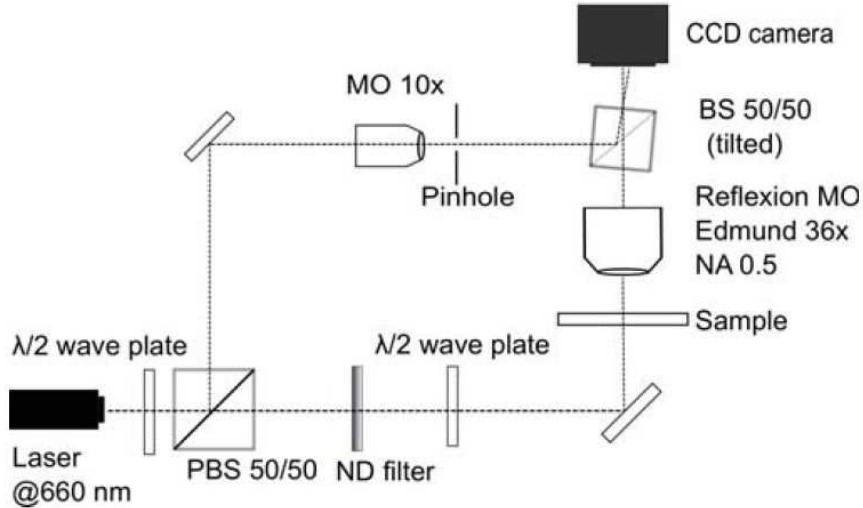


Fig. 1. Experimental setup.

2. Experimental setup

We chose to track 100nm gold beads in Brownian motion in water. These particles are good light scatterers because their optical index in visible light is very low. Moreover they are non cytotoxic and chemically inert [11]. The sample is prepared using a 400 μm deep chamber between two cover glasses filled with a nano-beads solution. The experimental setup is shown on the figure 1. The optical setup uses a 100 mW DPSS laser emitting at 660 nm. The laser beam is split with a polarizing beam splitter. We adjust the ratio of energy between both beams with a half-wave plate placed before the splitter. The first beam, called illumination beam, is focused on the sample. The second beam, called reference beam, is spatially filtered and expanded in a way to cover all the CCD chip. A dark-field microscope objective from Edmund Optic (NA = 0.5 and 36 \times magnification) collects the scattered light and blocks the illumination beam. This dark field configuration is necessary to avoid the saturation of the CCD chip : the Rayleigh-Mie scattering model [12] gives a cross section of 0.015 μm^2 for a 100 nm diameter gold particle at 660 nm. During 1 ms, the number of incident photons is typically 1014 photons at 660 nm, and the area of the illumination beams waist is $\simeq 4 \times 10^{-8} \text{ m}^2$. The number of scattered photons by the nano-bead collected through a numerical aperture of 0.5 is equal to 8×10^6 photon during 1 ms. The ratio of number of photons between the illumination beam and the scattered light is about 10^8 , so it's not possible to record the scattered signal on our 16 bits CCD chip without blocking the illumination beam. The dark field objective allows to use the full dynamic of the CCD chip to record the low scattered signal. A non-polarizing beam splitter behind the microscope objective combines the reference and the scattered signal. This splitter is tilted a few degrees to be in off-axis geometry [13]. The interference pattern is recorded on the 16 bits CCD chip of 1024×1024 pixels.

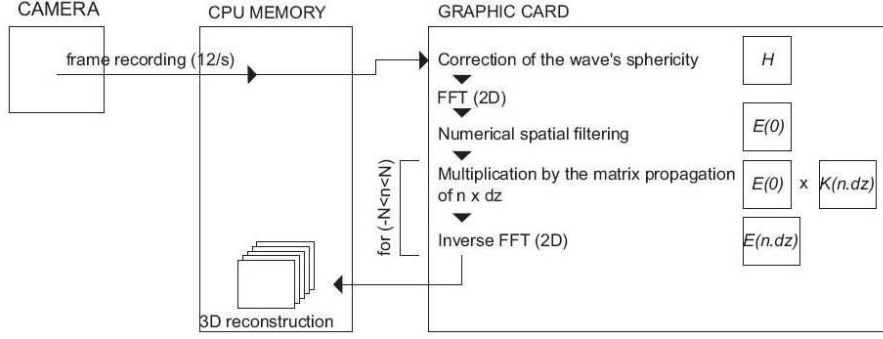


Fig. 2. Steps of the numerical reconstruction.

The observation of particles in motion imposes to limit the exposition time in order to limit the blurring of the signal. The magnification calibration of our setup gives a lateral pixel size of 160 nm. In our case, the diffusion constant of the Brownian motion is equal to $D \simeq 4\mu\text{m}^2.\text{s}^{-1}$ according to the Stokes-Einstein law. So the exposition time must be lower than 3 ms to avoid that the signal is shifted by one pixel. The exposition time of our camera can be set under this limit, but the acquisition period during 2 frames is limited to 80 ms. The travel of 100 nm particles in water during this period is too long to use the phase-shifting technique in order to improve the signal-to-noise ratio [9, 14].

3. 3D reconstruction of the scattered light

The camera record for each frame an intensity I_{ccd} described in the following equation :

$$I_{ccd} = I_{ref} + I_s + E_{ref}E_s^* + E_sE_{ref}^* \quad (1)$$

where I_{ref} and I_s are respectively the intensity of the reference and the scattering light. E_{ref} and E_s are the respective fields. The tilted beam splitter which combines the two fields adds a spatial frequency on the cross terms of interference (the third and fourth terms of the equation (1)). The effect is that these two terms can be separated in the Fourier space of the holograms. Figure 2 summarizes the steps of our reconstruction. First we multiply the hologram by a complex phase matrix $\exp[j\pi(x^2 + y^2)/(\lambda d)]$ where λ is the wavelength and d the distance between the CCD and the output pupil of the microscope objective. This operation is similar to a back-propagation of the hologram to the output plane of the objective. This propagation compensates the sphericity of the wave added by the objective. Then we calculate the Fast-Fourier Transform (FFT) of the corrected hologram. In the Fourier plane, the two first term of equation 1 are in the center, while the cross terms are respectively centered on the frequency added by the off-axis geometry and its complex conjugate. We numerically filter the term $E_sE_{ref}^*$ of equation 1 with a circular mask of radius equal to the apparent radius of the output pupil. The filtered map of the spatial frequencies

$(f[k_x, k_y])$ obtained is multiplied by the following matrix of propagation :

$$K[k_x, k_y, n] = \exp\left(\frac{(n \times \delta z) \cdot j\lambda(k_x^2 + k_y^2)}{2\pi}\right) \quad (2)$$

where δz is the arbitrary step of axial propagation (typically 100 nm) and n an integer. Then we calculate the inverse FFT. The result $\epsilon(n) = \text{FFT}^{-1}[fK]$ is the reconstruction of the field at the distance $n \times \delta z$. We repeat this multiplication by varying the integer n to reconstruct the volume. We get a stack of lateral sections $\epsilon(n\delta z)$ spaced by δz . The positions of the scatterers are determined by the local maximum of the intensity of the whole reconstructed field.

All this numerical reconstruction is implemented on a graphic card unit. We developp our algoritm with the Nvidia CUDA architecture to parallelize all the calculation on the 448 cores of a Nvidia Geforce GTX 470 card. All the steps of the reconstructions, except for the FFTs, need multiplication pixels to pixels and not matrix multiplication. This kind of operation are perfectly adapted for parallelization on graphic cores [15–18]. The FFT steps are made with the CUFFT library. We divided the time of reconstruction by a factor 30 compare to the same reconstruction made only on the CPU (double quad-core Intel Xeon E5520 at 2.27 GHz). We developedp a software for live visualisation of reconstruction using OpenGL library to display the datas calculated on the graphic card.

4. Current results

We are able now to observe 100nm gold nano particles in Brownian motion during few tens of positions. After that we generally lose the targets. The figure 3 shows the observation we are able to do in the present state of the setup. We see on the figure the lateral section where the intensity of the scattered light by the nano-bead is maximum. The PSF of the reconstructed field is plotted for X, Y and Z directions. The lateral PSF width is equal to $1 \mu\text{m}$, and the axial width is equal to $14 \mu\text{m}$. The signal-to-noise ratio of the reconstruction is better than 100. These results are obtained with an exposition time of only 1ms and an acquisition period of 80 ms between two frames.

5. Conclusion

We report in this paper the present performance of our digital holographic microscope. It consists of a Mach-Zender setup in off-axis geometry. A dark field microscope objective collects the light scattered by nano-sized gold particles, which interferes with the reference plane wave on the CCD camera. The scattered light field is numerically propagated from the interference pattern. We used our own algorithm based on the CUDA architecture to reduce the calculation time. The improvement clearly shows that this technology is a very promising tool for digital holography. We are able now to localize 100 nm gold nano particles in Brownian motion from holograms exposed during 1 ms. We expect to obtain similar performance for gold particles in a crowd medium or in a living cell in order to study the diffusion law in these specific media.

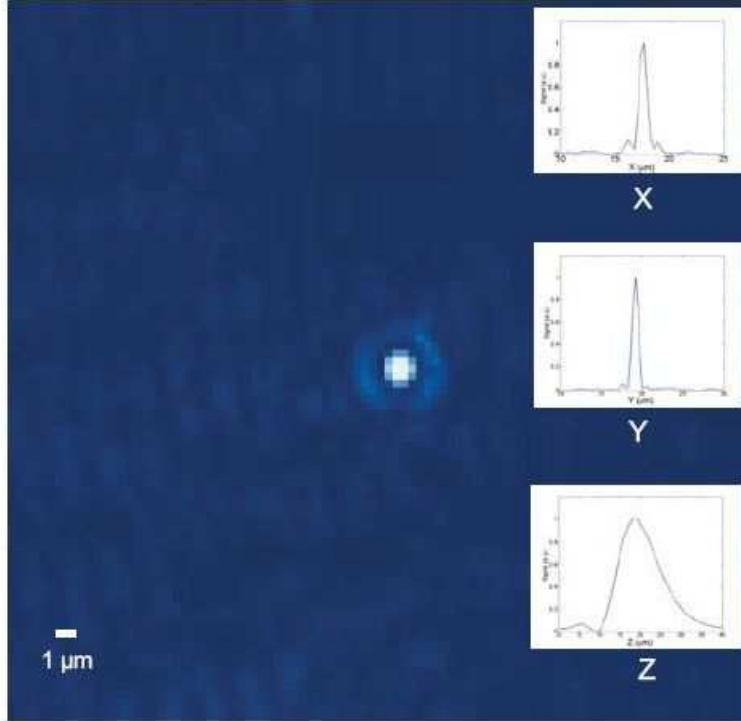


Fig. 3. Intensity of the scattered field by a 100 nm gold particle plotted in the section where the intensity is maximum. The three curves at the left shows the PSF respectively in X , Y and Z directions.

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