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Enhanced multiple ultrasonic shear reflection method for the determination of high frequency viscoelastic properties

V. Cereser Camara^a, D. Laux^{a,*}, O. Arnould^b

^a Institut d'Electronique du Sud, IES, UMR CNRS 5214, Université Montpellier II, CC 082, Place Eugène Bataillon, 34095 Montpellier, Cedex 5, France

^b Laboratoire de Mécanique et de Génie Civil, LMGC, UMR CNRS 5508, Université Montpellier II, CC 048, Place Eugène Bataillon, 34095 Montpellier, Cedex 5, France

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ABSTRACT

In this work, we propose a study dedicated to the influence of the delay line nature in transverse ultrasonic sensors, dedicated to dynamic high frequency elastic moduli of viscoelastic materials estimation. In literature, these shear ultrasonic rheometers are using delay lines in glass or quartz and normal or oblique incidence of ultrasonic rays. The oblique incidence is used in order to improve the sensitivity of the measurements. We theoretically demonstrate in this work that the use of delay lines in polymers is recommended to improve the sensitivity. Due to modifications, performed on a 10 MHz commercial ultrasonic sensor, we experimentally show on glycerin (which is a Newtonian material) that it is possible to multiply by a factor 10 the sensitivity; compared to delay lines in quartz using a normal incidence of rays. Hence, we overpass the accuracy of the oblique incidence approach with a simpler experimental setup.

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1. Introduction

Measurement of material properties using ultrasound has intensively been studied for decades [1]. This technique has been demonstrated to be very efficient for nondestructive examination. The advantage of this method is the direct coupling between ultrasonic quantities and mechanical properties. So, ultrasonic measurements can be considered as continuation of rheology for high frequencies.

In the low frequency range (Hz–kHz), the viscoelastic properties are usually determined by DMA (Dynamic Mechanical Analysis) or rheology. In the ultrasonic frequency range (kHz–GHz), several experimental techniques (ultrasonic pulse transmission technique, thickness shear mode, Bulk acoustic wave, ultrasonic shear wave reflected method, etc.) based on longitudinal or shear waves already exist [2–10]. However, all these techniques present some limitations. Indeed, to study the properties of soft viscoelastic materials, it is difficult to use the ultrasonic pulse transmission technique because of the extremely high attenuation of shear waves propagation in these materials. Resonant methods transform a measured quantity into a frequency shift of an electrical signal. These devices can be used to characterize the mechanical behaviour of materials bonded on their surface.

With such methods, it is necessary to use an algorithm which enables the conversion of the raw data of the impedance into equivalent circuit parameters. Therefore, the dynamic moduli cannot directly be determined with these methods. That is the main drawback of these methods compared to the technique proposed by O'Neil and Mason [11,12]. This latter has been proposed in 1949 in order to compare two types of ultrasonic reflectivity measurements using normal or oblique incident shear waves. The technique uses the complex reflection coefficient (modulus and phase) at an interface between a buffer rod and the material to determine the viscoelastic properties (dynamic moduli, G' and G'') of the material under study. The advantage of the oblique incidence method compared to the normal incidence one is its sensitivity: about 5 times better. Concerning the diffraction effects, the normal incidence wave method requires a shorter buffer rod (around 7 mm) than for the oblique incidence method (around 80 mm) [13]. So, a normal incidence technique seems preferable.

The aim of this work is to demonstrate that using the previously presented ultrasonic shear wave technique in normal incidence and at the cost of some modifications performed on a commercial sensor in order to adapt a delay line in polymer, one can reach a sensitivity at least equal to the one obtained with the same technique in oblique incidence.

The paper is organized as follows: the theoretical backgrounds of ultrasonic shear wave reflection method are presented in Section 2. In particular, we will focus our attention on the influence

* Corresponding author.

E-mail addresses: didier.laux@ies.univ-montp2.fr, laux@lain.univ-montp2.fr (D. Laux).

of delay line on the experimental quantities to be measured and which directly affect the sensitivity of the system. Section 3 describes the design of the transducer. Section 4 presents the experimental setup. At last, the results are presented and commented in Section 5. In particular the effect of delay line attenuation is discussed.

2. Theory

2.1. Ultrasonic shear wave reflection theory [1,11,12]

According to the theory of wave reflection, for the normal incidence of shear waves at a boundary between two elastic materials, the reflection coefficient can be defined as:

$$r = \frac{A_{\text{reflected}}}{A_{\text{incident}}} = \frac{Z_2 - Z_1}{Z_2 + Z_1} \quad (1)$$

where r is the wave reflection coefficient in pressure or stress, defined as the amplitude ratio between the reflected and incident waves, which can be obtained directly from experimental measurements. Z_1 and Z_2 are the shear acoustical impedances of the materials. This acoustical impedance is defined as the product (density) \times (shear velocity). In the case of pure elastic materials, acoustical impedance and r are real parameters. If the viscoelastic behaviour is considered, the acoustical impedance is also a complex quantity (Eq. (2)). Considering now that the material 1 is elastic and that the material 2 is viscoelastic, reflection coefficient can be generalized in a complex format:

$$Z^* = R + jX \quad (2)$$

$$r^* = r_0 e^{j\Phi} = r_0 (\cos \Phi + j \sin \Phi) \quad (3)$$

where ϕ is the phase shift between the incident and the reflected wave, and r_0 is the magnitude or modulus of the reflection coefficient. This means that, when an ultrasonic wave propagating in material 1 is reflected on the interface (1/2), its amplitude decreases and the wave undergoes a phase shift.

The real (R) and imaginary part (X) of the shear impedance of the viscoelastic material, given in Eqs. (4) and (5); can be obtained using Eqs. (2) and (3)

$$R = Z_1 \frac{1 - r_0^2}{1 - 2r_0 \cos \Phi + r_0^2} \quad (4)$$

$$X = Z_1 \frac{2r_0 \sin \Phi}{1 - 2r_0 \cos \Phi + r_0^2} \quad (5)$$

For ultrasonic shear waves, the complex acoustic impedance Z^* is related to the storage (G') and the loss (G'') moduli through the following relationship:

$$Z^* = \sqrt{\rho G^*} = (\rho(G' + jG''))^{1/2}, \quad (6)$$

where ρ is the density of the material studied. Both the storage and loss shear modulus can be expressed as a function of the real and imaginary part of the shear impedance as shown in Eqs (7) and (8).

$$G' = \frac{R^2 - X^2}{\rho} \quad (7)$$

$$G'' = \frac{2RX}{\rho} \quad (8)$$

We can rewrite the storage and loss shear modulus by replacing the Eqs. (4) and (5) in the Eqs. (7) and (8), where ρ is the density of the studied material, ρ_{DL} the density of the delay line and V_{DL} the shear ultrasonic velocity in the delay line.

$$G' = (\rho_{DL} V_{DL})^2 \frac{(r_0^2 - 1)^2 - 4r_0^2 \sin^2 \Phi}{\rho(2r_0 \cos \Phi + 1 + r_0^2)^2} \quad (9)$$

$$G'' = -4(\rho_{DL} V_{DL})^2 \frac{(r_0^2 - 1)4r_0 \sin \Phi}{\rho(2r_0 \cos \Phi + 1 + r_0^2)^2} \quad (10)$$

Experimentally, an ultrasonic transducer made of a piezoelectric crystal and a delay line in silica or glass for instance, is used. It represents the material 1 in the previous paragraph. The material 2 is constituted by the polymer which is studied. For some polymers the phase shift undergone by the ultrasonic wave is measurable on the first echo reflected on the viscoelastic interface. Hence, the method can be used. We can cite studies of polydimethylsiloxane polymers and curing epoxy systems [14,15].

But, in many cases, the phase shift is so small that no measurement is possible on the first echo. But, as the ultrasonic attenuation is small in the delay line, multiple reflections are possible leading to the existence of many echoes. Using this fact, Gasparoux et al. [16] have proposed a multiple ultrasonic reflection device (MUR). They worked with the multiple reflections instead of a simple one, at the interface between the delay line and the material. Then, the complex reflection coefficient, r^* was calculated with the following relationships, where: A_n is the amplitude of the echo number n , in the case of the interface (delay line/air), B_n , the amplitude for the interface (delay line/material), Δt_n the time shift between these two echoes and f the operating frequency (see Fig. 1).

$$r_0 = \left(\frac{B_n}{A_n} \right)^{\frac{1}{n}} \quad (11)$$

$$\Phi = -2\pi f \left(\frac{\Delta t_n}{n} \right) \quad (12)$$

If n echoes are used, the time-lag or phase shift to be measured, is multiplied by a factor n .

All the theory pointed above has considered the impedance of the delay line as a real number. Considering now that the materials 1 and 2 are viscoelastic, and taking into account the attenuation, we can develop a complex impedance theory.

Let Z^* and k^* complex impedance and wave vector respectively in the delay line which is now considered as a damping material. The Eq. (2) can be rewritten as following:

$$Z^* = \rho_{DL} \frac{\omega}{k^*} \quad (13)$$

$$k^* = \frac{\omega}{v_s} - j\alpha \quad (14)$$

In these expressions, α is the ultrasonic wave attenuation and ω the radian frequency ($\omega = 2\pi f$). Then, Z^* can be written as follows:

$$Z^* = R + jX = \rho_{DL}(c + j \cdot b), \quad (15)$$

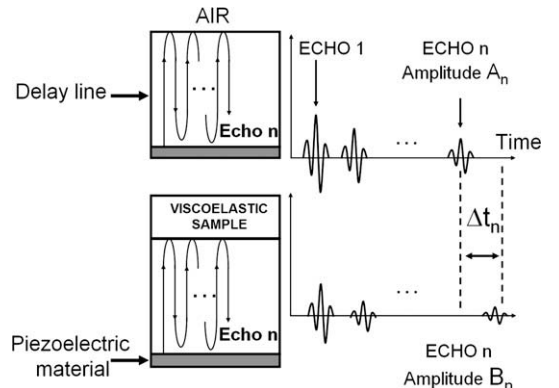


Fig. 1. Schematic representation of the multiple ultrasonic reflection method.

where:

$$b = \frac{v_s^2 \omega^2}{\omega^2 + v_s^2 \alpha^2} \quad (16)$$

and

$$c = \frac{v_s^2 \alpha \omega}{\omega^2 + v_s^2 \alpha^2} \quad (17)$$

At last, using the Eqs. (7) and (8), G' and G'' can be expressed as:

$$G' = \frac{\rho_{DL}((-c(r_0^2 - 1) + 2br_0 \sin \Phi)^2 - (-b(r_0^2 - 1) - 2cr_0 \sin \Phi)^2)}{\rho(r_0^2 + 2r_0 \cos \Phi + 1)^2} \quad (18)$$

$$G'' = \frac{2\rho_{DL}((-c(r_0^2 - 1) + 2br_0 \sin \Phi)(-b(r_0^2 - 1) - 2cr_0 \sin \Phi))}{\rho(r_0^2 + 2r_0 \cos \Phi + 1)^2} \quad (19)$$

In order to increase again the sensitivity of the system, we chose to use the multiple ultrasonic shear wave principle and realise some changes on the sensor, such as: decrease the thickness of the delay line or changing the material of the delay line. Therefore, in the next section, we present the influence of the delay line material on the reflection coefficient.

2.2. Influence of the delay line acoustical impedance

In order to demonstrate the influence of the delay line acoustical impedance on r_o and Φ , we have simulated at 10 MHz the reflection coefficient modulus (Fig. 2) and the time-lag (Fig. 3) for an interface (delay line/glycerin) using Eqs. (11) and (12). This material was chosen because it is known to have a Newtonian behaviour ($G' = 0$ and $G'' = \eta\omega$, where η is the material viscosity) even at high frequencies [17–23]. For the simulation, we have used $T = 20^\circ\text{C}$ and $\eta = 1.3 \text{ Pa s}$, according to literature data.

When the impedance mismatch between the delay line and the material decreases, the total energy transferred to the material increases. Consequently, the reflected energy and the phase become more sensitive. Based on the Figs. 2 and 3, if one wants to increase the time-lag to be measured, a delay line with a small acoustical impedance has to be chosen.

In literature, quartz is generally used as a delay line because the acoustic wave absorption in this material can be neglected. Nevertheless this material has a very high acoustic impedance. In order to minimize the impedance mismatch, we looked for different materials with a low acoustic impedance. Finally, polymers seemed a good option. In order to confirm this possibility, we will present the polymers analyzed in this study.

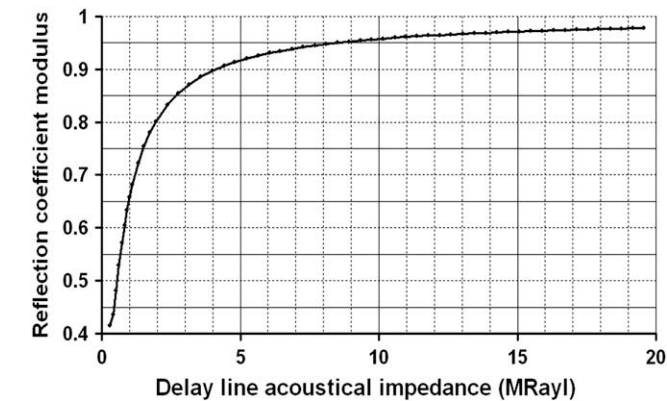


Fig. 2. Reflection coefficient simulation at 10 MHz as a function of the delay line acoustical impedance on glycerin at room temperature (20°C).

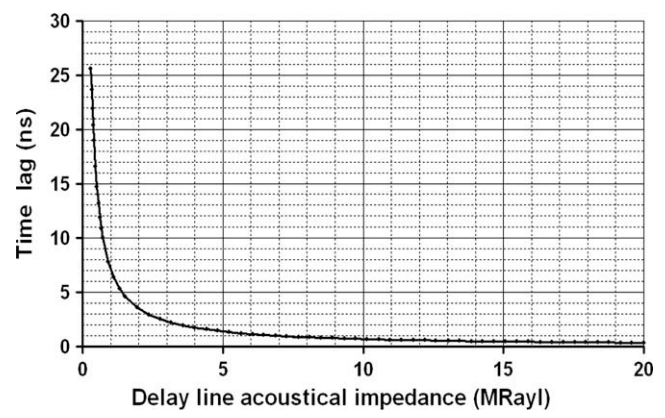


Fig. 3. Time-lag simulation at 10 MHz as a function of the delay line acoustical impedance on glycerin at room temperature (20°C).

2.3. Polymers selected as possible delay line

In order to minimize the impedance mismatch, we have selected eight polymers. To determine their shear velocity, we have proceeded with a classical time of flight method in transmission mode. Knowing the samples thicknesses, the velocity can be calculated from the following equation:

$$v_s = d/\Delta T \quad (20)$$

where v_s is the shear velocity, d is the samples thickness and ΔT the time needed to go from the emitter to the receiver after propagation in the sample. To increase the precision of our measurements, the velocities were measured at least for three different thicknesses and were repeated on each polymer. It may seem surprising that we have not used the phase velocity in this study but these materials have reached (and largely over passed) the glass transition for the considered temperature and frequencies. So, their velocity does not change substantially with frequency. In order to check this point, tests have been performed with four frequencies (0.5–1–5 and 10 MHz). No significant variation has been observed on the velocity.

The values obtained for the density, shear velocity and acoustic impedance as a function of the polymer material are reported in Table 1. Once these parameters determined, we have calculated at 10 MHz the reflection coefficient (Figs. 4a and 4b) and the time-lag (Figs. 5a and 5b) on the glycerin for these materials. Based on the Figs. 4a and 4b and 5a and 5b, we can note that if we use a delay line in polymer instead of quartz, the modulus of reflection coefficient decreases and the time – lag increases substantially. Furthermore, PU is the best polymer: the time shift obtained is largely superior to the time shift given by quartz.

Table 1
Shear velocity and density of the delay lines at room temperature (20°C).

Material	Density (kg m^{-3})	Shear velocity (m s^{-1})	Z_1 (MRayl)
Nylon	1150 ± 23	1045 ± 41	1.20 ± 0.07
Polyurethane (PU)	1160 ± 23	823 ± 27	0.95 ± 0.05
Polypropylene (PP)	870 ± 17	1178 ± 44	1.02 ± 0.06
Teflon (PTFE)	2180 ± 44	547 ± 7	1.19 ± 0.04
Acrylic (AC)	1190 ± 24	1358 ± 50	1.62 ± 0.09
Polycetate (PA)	1420 ± 28	949 ± 51	1.35 ± 0.10
Polycarbonate (PC)	1215 ± 24	930 ± 30	1.13 ± 0.06
Polyester	1100 ± 22	1163 ± 25	1.28 ± 0.05

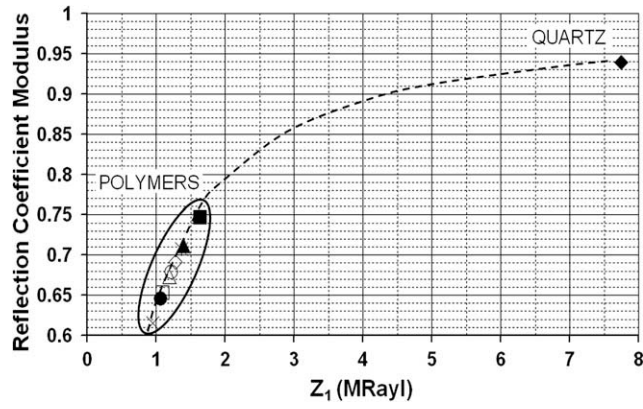


Fig. 4a. Reflection coefficient simulation at 10 MHz as a function of the delay line materials on glycerin at room temperature (20 °C).

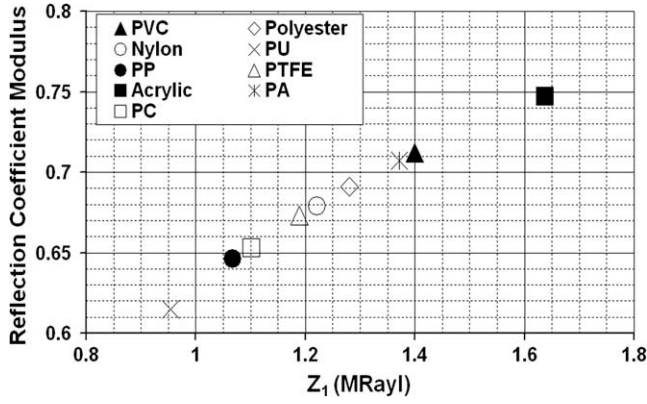


Fig. 4b. Zoom of reflection coefficient simulation at 10 MHz as a function of polymers delay line on glycerin at room temperature (20 °C).

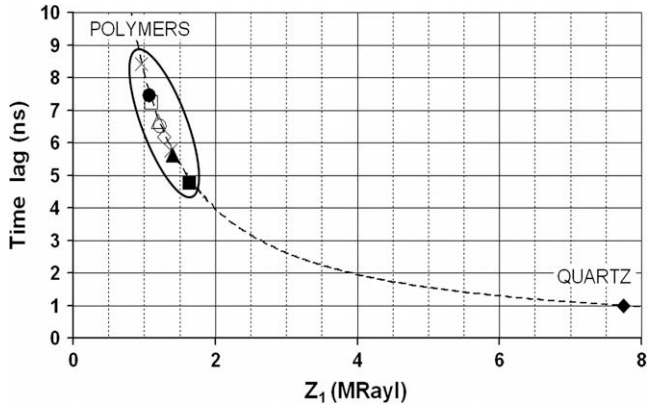


Fig. 5a. Time-lag simulation at 10 MHz as a function of the delay line materials on glycerin at room temperature (20 °C).

3. Design of the transducer

As it is quite difficult to realise a high quality shear ultrasonic transducer, we have decided to use a commercial 10 MHz shear transducer manufactured by Panametrics/Olympus (model V221-BA) and to adapt the polymer delay lines on this transducer. The main advantage is that we are sure to work with high quality shear ultrasonic waves. Indeed, one can check that for these ultrasonic transducers no longitudinal modes remain. Practically, we have

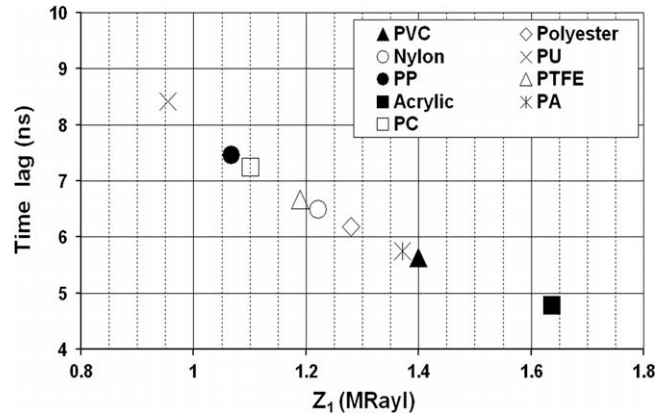


Fig. 5b. Zoom of time-lag simulation at 10 MHz as a function of polymers delay line on glycerin at room temperature (20 °C).

designed plates and settled these plates on the commercial transducer. Considering the ultrasonic velocity in the plate, the thickness has been adapted for each plate in order to have a maximum of nonoverlapping echoes. For example, if we wanted to settle the acrylic plate on the commercial sensor, the thickness of the plate so is evaluated as follows: as in this study we are working with a 10 MHz commercial ultrasonic sensor and knowing that the echoes generated in the plate have got around two periods, we have $2T = 2/f = 0.2 \mu s$ where T is the period and f is the frequency. So the minimal time separating two echoes has to be equal to $0.2 \mu s$. Knowing the shear velocity (Table 1) and using equation (13), the appropriated thickness can be calculated. For an acrylic plate, the thickness is approximately equal to $150 \mu m$. Generally, the thicknesses obtained for each polymer are around a few hundred of micrometers. As high frequency ultrasonic waves do not propagate in air, we used honey as a coupling fluid between the plate and the commercial sensor. This new system (commercial sensor + plate) has the advantage to be disposable and designed according to the working frequency. For instance, if one works with a 5 MHz transducer the thicknesses will be multiplied by a factor 2.

4. Experimental setup

The shear transducer was excited using a pulser/receiver (Panametrics Olympus 5800 PR) and digitized by an oscilloscope (Tektronix TDS 3032). All the measurements were made in a refrigerated incubator (BINDER KB 53) with an accuracy of $\pm 0.1^\circ C$. The signals were recorded on a computer using a standard IEEE GPIB interface. Before each test, the free surface of the system (sensor + plate) was cleaned with ethanol. Then, it was introduced in the incubator and the reference signal (interface plate/air) was recorded. After, the material to be studied was deposited on the free surface of the system and the echoes in the delay line were again acquired. For example, we can see in the Fig. 6 the echoes recorded at the interface: "delay line/air" and "delay line/Glycerin" with a delay line made in polyurethane. As we expected, using a delay line in polymer (PU), the phase shift obtained is clearly measurable even on the first echo.

For each set of measurements, several echoes were recorded. r_0 and the phase shift ϕ were determined with a program elaborated under Labview®.

Concerning the signal processing ($A_1 \dots A_n$) and ($B_1 \dots B_n$) were simply evaluated using the minima and maxima on the echoes. Then, following the procedure given in [16] we plotted $\ln(B_i/A_i)$ versus i , for i ranging from 1 to n . A linear adjustment of this curve directly lead to $\ln(r_0)$. Hence, r_0 was deduced. For the phase shift

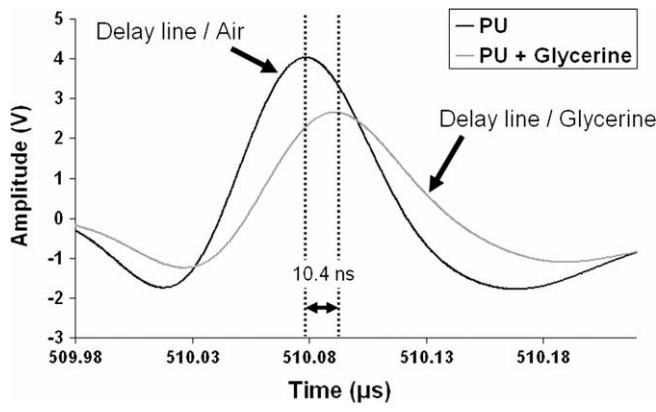


Fig. 6. Experimental echoes recorded at the interface: delay line/air and delay line/glycerin with a delay line made in polyurethane. The measurement was realized at 10 MHz at room temperature (20 °C).

evaluation, we used a cross correlation procedure [24] between the echo i for the interface between delay line and air and the echo for the interface between delay line and viscoelastic material, leading to Δt_i . Then a linear adjustment of Δt_i versus i for i ranging from 1 to n , lead to Φ deduction.

5. Results

In this experimental study, we have used the glycerin purchased from MERCK®. The density (ρ) of the material under study provided by the manufacturer was 1260 kg m^{-3} . For the analysis of this material, no pretreatment was necessary. One observation can be made with respect to its hygroscopic properties. The sample should be tightly closed and protected from light. Glycerin is a material known to have a Newtonian behaviour. In order to confirm this fact, we have measured the viscosity for low frequencies with a AR2000 TA Instruments Rheometer. Results are presented in Fig. 7. For each temperature ranging between 5 and 30 °C the viscosity is not frequency dependent. This clearly demonstrates the Newtonian behaviour of this material. Thanks to a fit performed on the data (viscosity \times temperature) with an Arrhenius law, we found $1.30 \pm 0.01 \text{ Pa s}$ for $T = 20 \text{ °C}$ (the error bars come from a range of repeat measurements).

The values and errors obtained for the reflection coefficient, phase shift and loss modulus as a function of the delay line material are reported in Table 2 [25]. One can notice that according to theory and to viscosity measurements, G'' should be equal to

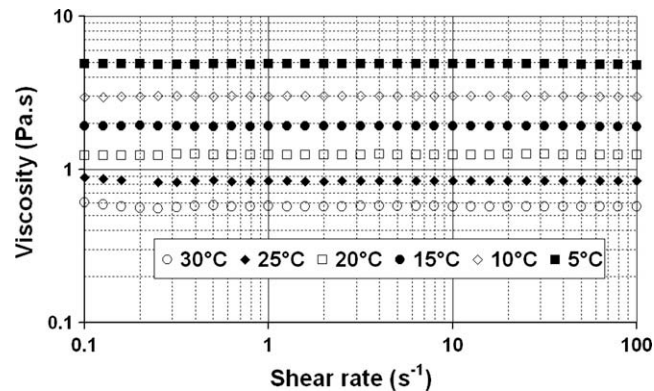


Fig. 7. Steady-state viscosity of glycerin versus shear rate for different temperatures.

Table 2

Experimental results obtained for the reflection coefficient and the time-lag at 10 MHz as a function of the delay line material at room temperature (20 °C).

Delay line material	Z_1 (MRayl)	Reflection coefficient	Time-lag (ns)	G'' (MPa) $\pm 2\%$
Nylon	1.20 ± 0.07	0.756 ± 0.03	7.50 ± 0.14	81.7
Polyurethane (PU)	0.95 ± 0.05	0.732 ± 0.02	10.40 ± 0.20	82.0
Polypropylene (PP)	1.02 ± 0.06	0.732 ± 0.02	8.80 ± 0.17	83.3
Acrylic (AC)	1.62 ± 0.09	0.792 ± 0.03	5.17 ± 0.10	82.0
Polyester	1.28 ± 0.05	0.842 ± 0.02	10.30 ± 0.19	81.5
Glass	8.36 ± 0.04	0.952 ± 0.03	0.94 ± 0.02	81.2

Table 3

Comparison of real part and the modulus of the complex impedance using the experimental results obtained for the attenuation at 10 MHz as a function of the delay line material at room temperature (20 °C).

Material	Attenuation (Np m^{-1})	Real $ Z_1 $ (MRayl)	Im $ Z_1 $ (MRayl)	$ Z_1 $ (MRayl)
Nylon	353 ± 67	1.20 ± 0.07	$7.06\text{E}-3 \pm 2.11\text{E}-4$	1.20 ± 0.07
Polyurethane (PU)	213 ± 36	0.95 ± 0.05	$2.66\text{E}-3 \pm 1.77\text{E}-4$	0.95 ± 0.05
Polypropylene (PP)	455 ± 86	1.02 ± 0.06	$8.74\text{E}-3 \pm 2.62\text{E}-4$	1.02 ± 0.06
Teflon (PTFE)	204 ± 12	1.19 ± 0.04	$2.12\text{E}-3 \pm 1.02\text{E}-4$	1.19 ± 0.04
Acrylic (AC)	205 ± 70	1.62 ± 0.09	$7.16\text{E}-3 \pm 2.15\text{E}-4$	1.62 ± 0.09
Polyacetal (PA)	199 ± 51	1.35 ± 0.10	$4.05\text{E}-3 \pm 1.21\text{E}-4$	1.35 ± 0.10
Polycarbonate (PC)	470 ± 52	1.13 ± 0.06	$7.96\text{E}-3 \pm 2.39\text{E}-4$	1.13 ± 0.06
Polyester	409 ± 61	1.28 ± 0.05	$9.68\text{E}-3 \pm 2.90\text{E}-4$	1.28 ± 0.05

81.7 MPa because $G'' = \omega\eta$. The results given in Table 2 are in good agreement with this value.

Remark 1: one can notice that the material with best sensitivity (PU) does not seem to give the best result compared to glass. However experiments with glass are more difficult because one has to use many echoes (over 10) which have smaller and smaller amplitudes during propagation.

Remark 2: here results are presented at 20 °C. But other measurements at various temperatures gave the same agreement between rheological measurements and ultrasonic approach. For instance, for $T = 10 \text{ °C}$ the viscosity measured with the rheometer is $3 \pm 0.01 \text{ Pa s}$. With ultrasound we found $185 \pm 4 \text{ MPa}$ for $f = 10 \text{ MHz}$ leading to viscosity of 2.94 ± 0.06 according to $G'' = \omega\eta$.

As predicted by theory (Figs. 2 and 3), the best sensitivity is given for the polymer delay line with the lowest acoustic impedance, in our case, the delay line in polyurethane. We can observe that, if we use a delay line in polyurethane instead of quartz, the sensitivity of the system can be multiplied by 10.

In this study, we considered that the materials used as delay line have a low attenuation and therefore this attenuation could be neglected. However, polymers are known as ultrasonic absorbent materials. In order to verify the error associated with the calculation of G'' , we will now use the theory taking into account the complex impedance. In the next section, this point will be discussed.

6. Discussion

To take into account the complex impedance theory and calculate the parameters b and c , we need to know the attenuation of each plate used as a delay line. To determine the attenuation in these materials, we have made various plates of each material in different thicknesses. Thanks to the measurement of the amplitude of a transmitted signal, the attenuation was easily deduced. The values obtained for the attenuation and the comparison between the real and the modulus of the complex impedance are reported in Table 3.

As we can see, the imaginary part of complex impedance can be neglected when compared to the real part. In the case of viscoelastic materials, these low attenuations may seem surprising but at room temperature we are investigating a zone after the glass transition. Hence, $G' \gg G''$ and viscous behaviour is largely inferior to the elastic one. Consequently, the attenuation in the delay line is small. So, considering a real acoustical impedance for the delay lines in polymers was acceptable in the context of this work.

7. Conclusions

Using simple plates in polymers settled on a commercial shear ultrasonic sensor we have demonstrated that the sensitivity of our piezo rheometer could be multiplied by a factor 10. Hence, with a very robust and simple system we obtain a sensitivity at least equal to more complex system using oblique incidence. The validation on glycerin also shows that the accuracy of the system is very good.

For the future, it will be advantageous to build commercial sensors by depositing thin polymer films onto the transducer element. This will allow a perfect coupling and consequently, the generation of a maximum number of echoes. An application of such sensors on classical rheometers could be interesting in order to obtain in the same measurement low and high frequency behaviour of viscoelastic products.

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